

# Computational Neuroscience: Neuronal Dynamics

EPFL

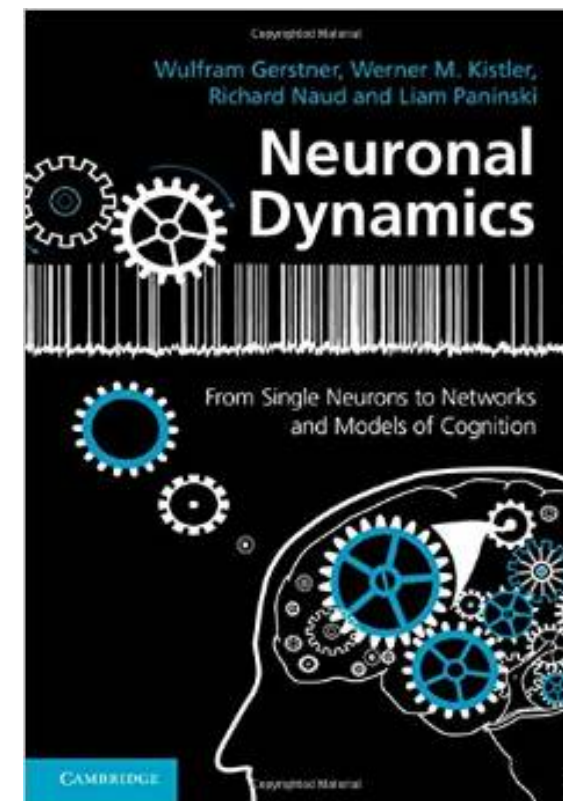
**Week 4**

**Reducing detail:**

**Analysis of 2D models**

*Reading for week 4:*  
**NEURONAL DYNAMICS**  
- Ch. 4.4 – 4.7

Cambridge Univ. Press



✓ 3.1 From Hodgkin-Huxley to 2D

✓ 3.2 Phase Plane Analysis

✓ 3.3 Analysis of a 2D Neuron Model

**4.1 Separation of time scales**

**4.2 Type I and II Neuron Models**

- limit cycles: constant input

**4.3 Pulse input**

- where is the firing threshold?

**4.4. Nonlinear integrate-and-fire**

**Lecture 4 of video series (last 60 minutes)** - further reduction to 1 dimension

<https://lcwww.epfl.ch/gerstner/NeuronalDynamics-MOOCall.html>

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*Week 5,6: Associative Memory, Hebb, Hopfield*

*Week 7,8,9: Networks, cognition, decision*

*Week 10-13: Noise models, noisy neurons,  
coding, and network dynamics*

*Week 14: Neural Manifolds and low-rank networks*

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# How to best use the time in the inverted classroom

☐ prof should spend more time on the Quiz questions

☐ prof should spend less time on the Quiz questions

☐ prof should spend more time on repetition of contents

☐ prof should spend less time on repetition of contents

☐ prof should be more explicit in answering posted questions

☐ prof should be more concise in answering posted questions

☐ it would be great if my classmates asked more questions

☐ it would be great if my classmates asked fewer questions

☐ Overall, the exercises should start after a max of 25 minutes

☐ Overall timing OK as is

Before I start, are there any questions?

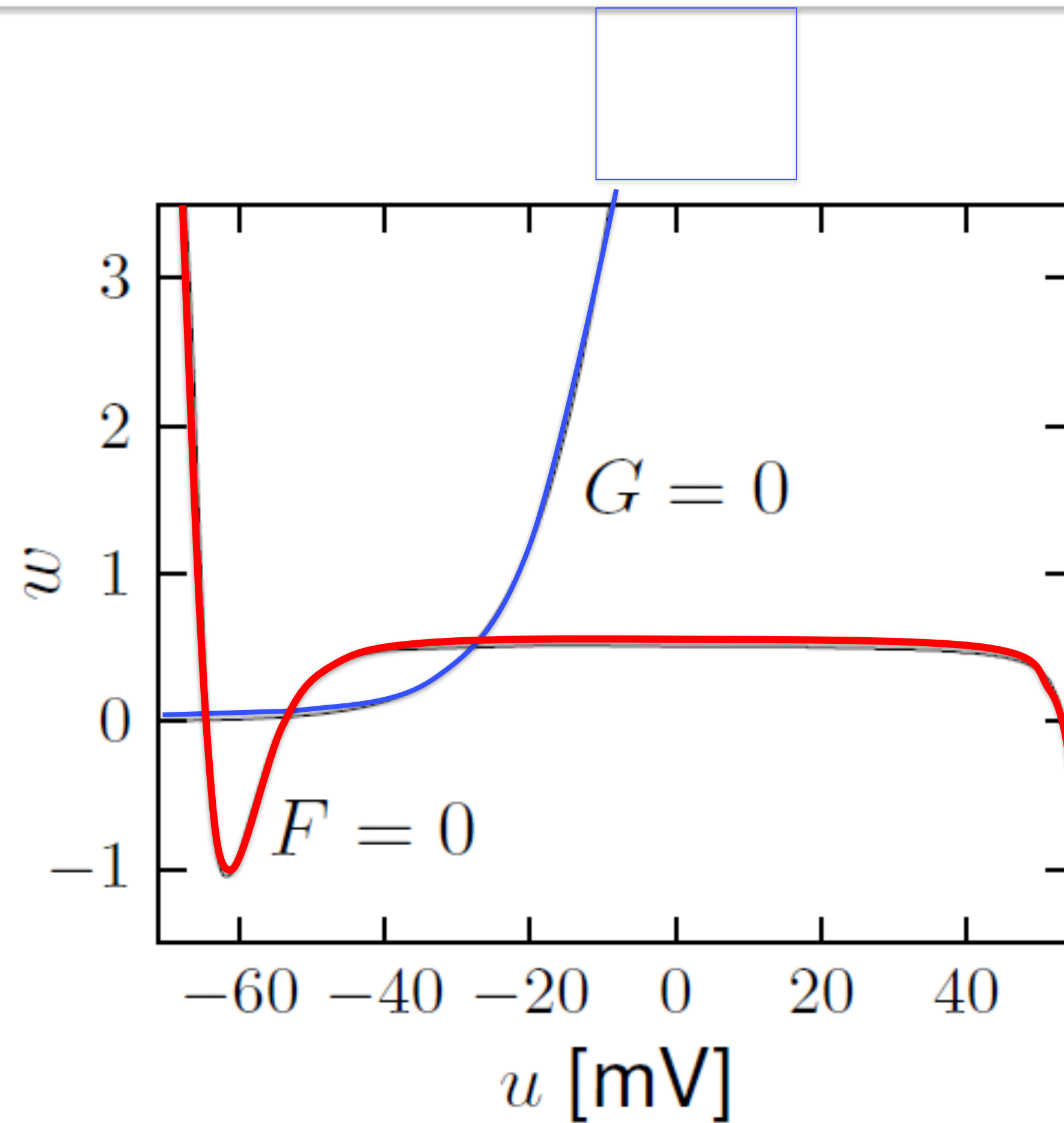
Are there any comments?

## 3.2. Nullclines of reduced HH model

stimulus  
↓

u-nullcline

w-nullcline



*Image: Neuronal Dynamics,  
Gerstner et al.,  
Cambridge Univ. Press (2014)*

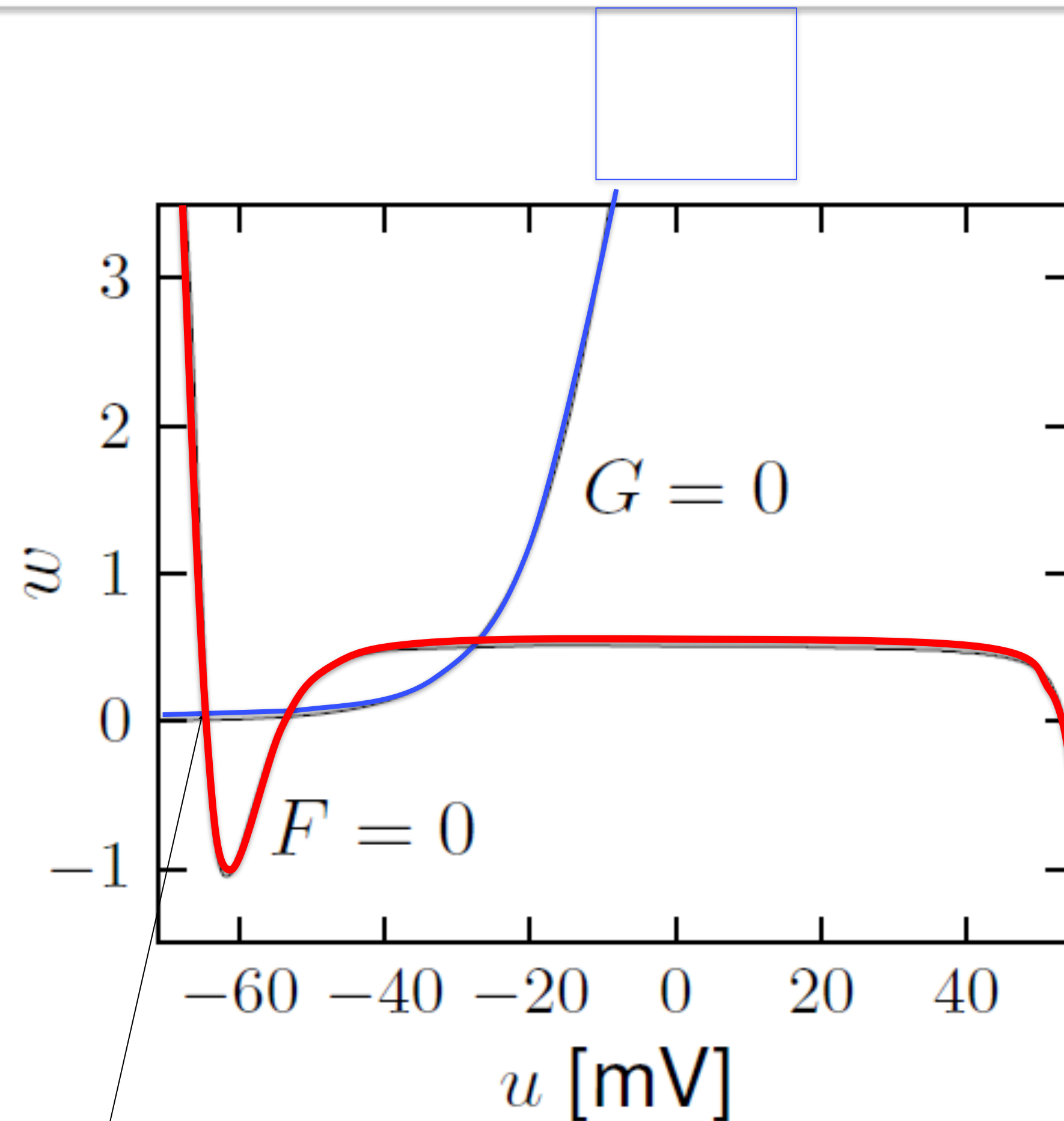


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Stable fixed point

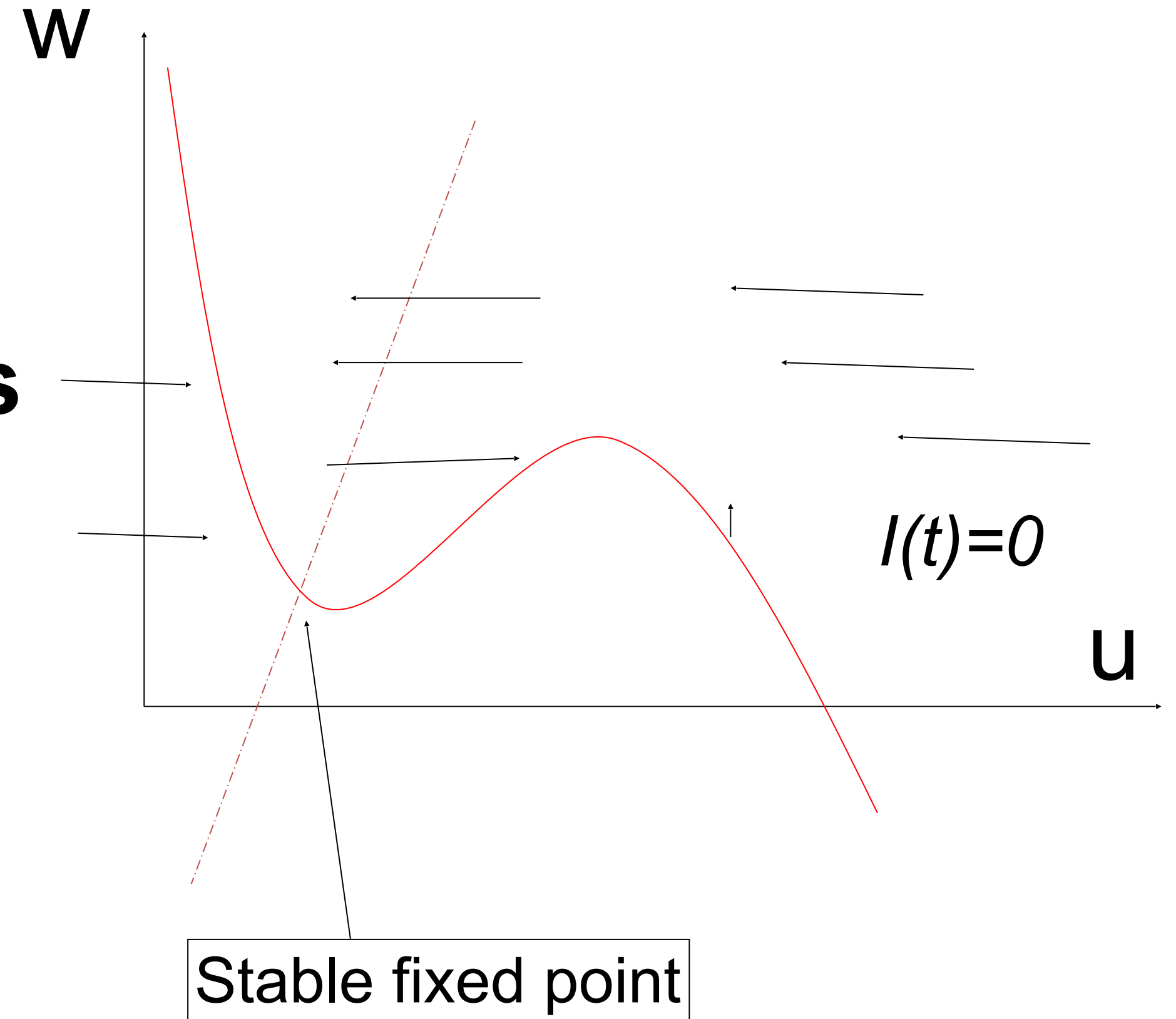
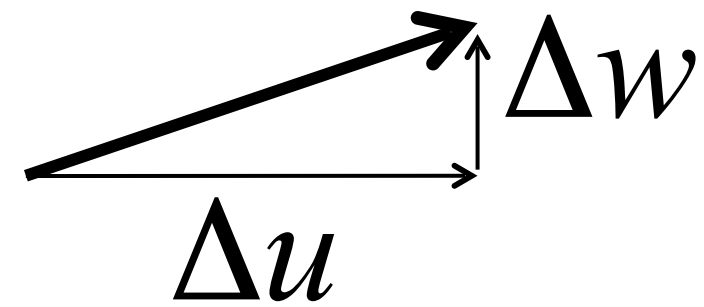
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# 4.1. Second Separation of time scales

stimulus



Separation of time scales

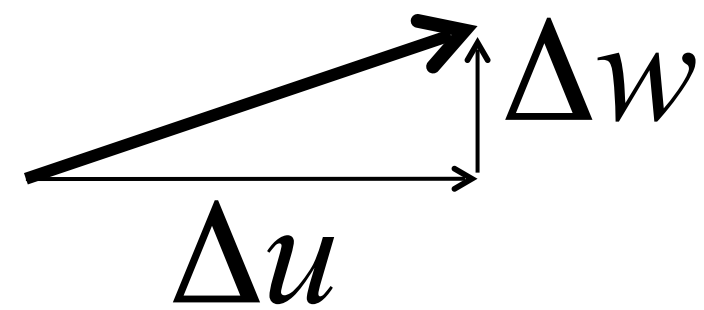


# 4.1. Second Separation of time scales

stimulus

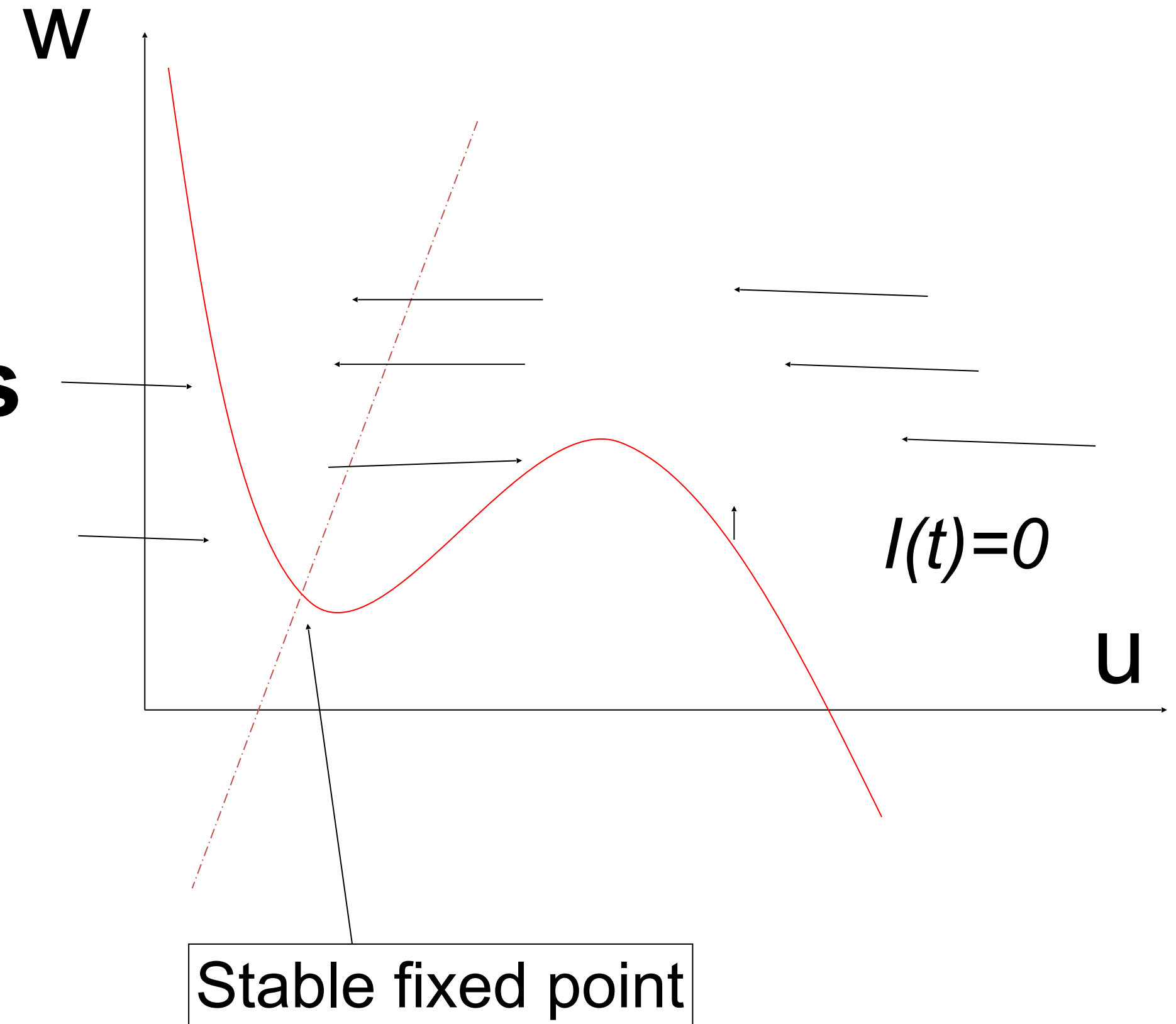


Separation of time scales



$$\longrightarrow \Delta w \ll \Delta u$$

Unless close to nullcline





## 4.1. Summary: Separation of time scales

We have seen a first separation of time scales last week to remove the  $m$ -variable. Today I have introduced a second separation of time scale: the  $w$ -variable is (in reality only a bit) slower than the voltage variable.

For mathematical reasons we considered the limit where  $w$  is MUCH slower than the voltage variable.

In this limit, the flow arrows are all horizontal – except in the region very close to the  $u$ -nullcline.

This condition can be exploited for two interesting stimuli:

- (i) A constant stimulus strong enough to evoke a limit cycle. In this case the trajectory either jumps or follows the  $u$ -nullcline.
- (ii) A pulse stimulus. In this case, the voltage either goes rapidly back to the fixed point or it takes a detour.

We look at both stimulation paradigms again throughout the lecture.

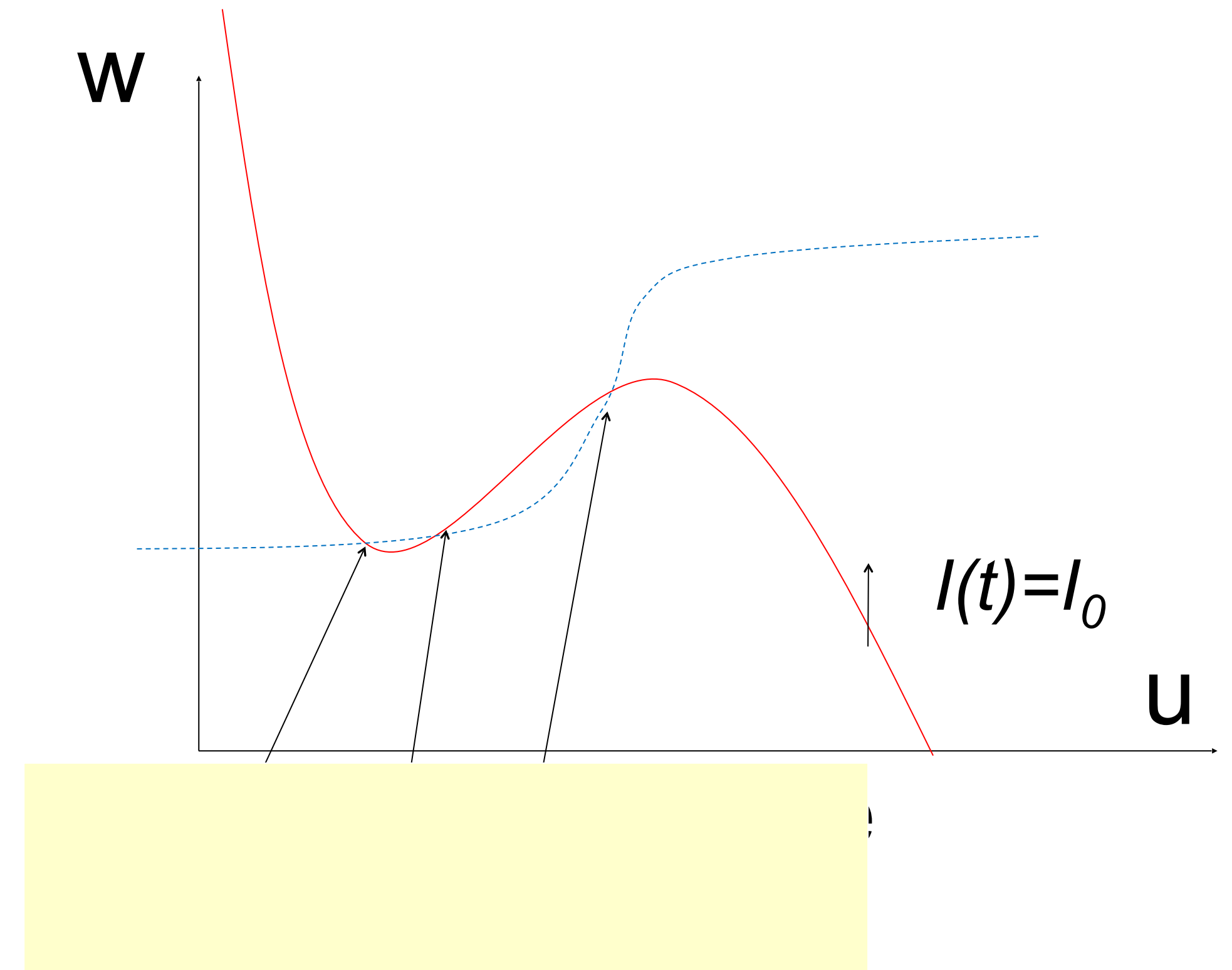
## 4.2. Type I Neuron Models: saddle-node bifurcation

stimulus



$+RI(t)$

constant input



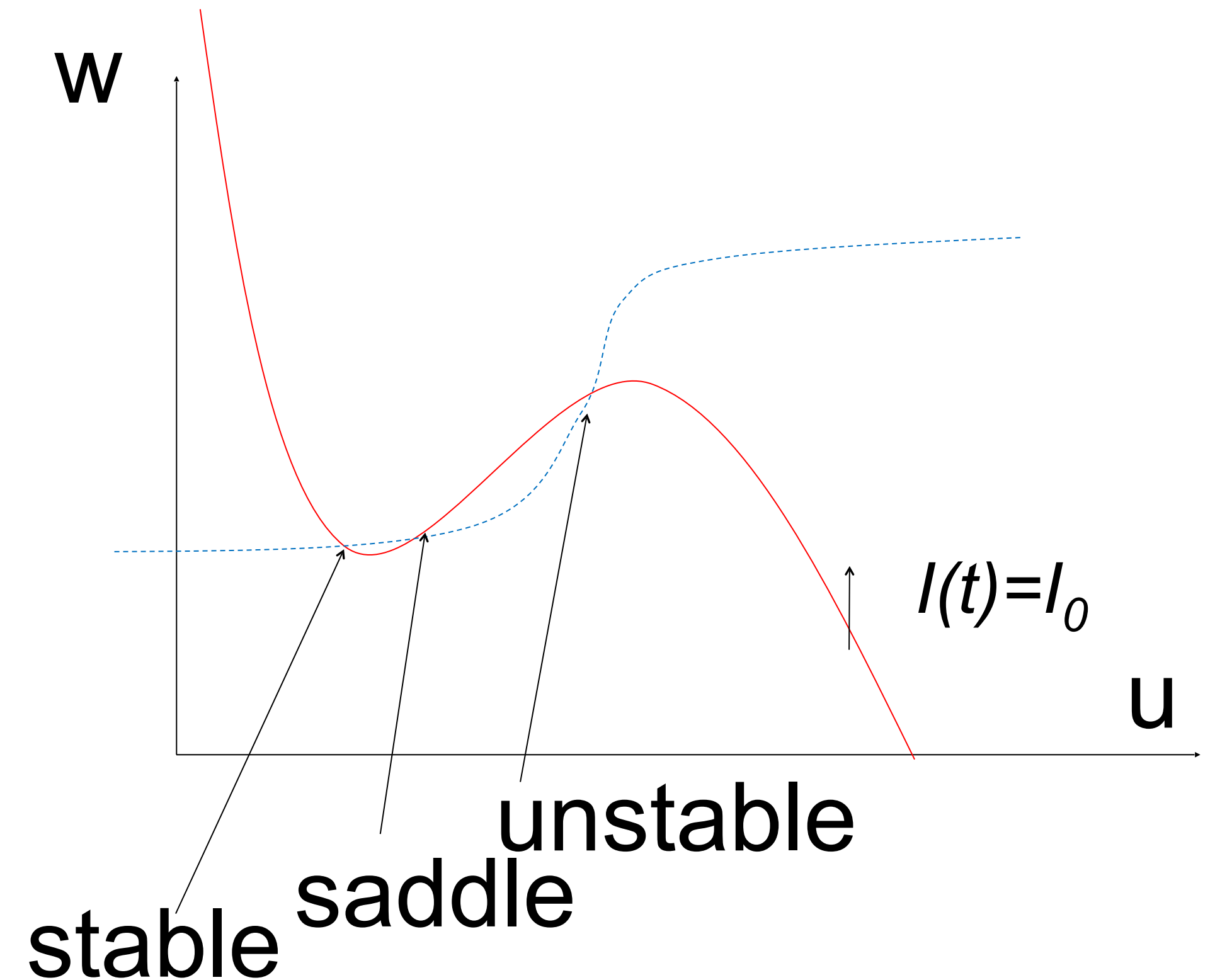
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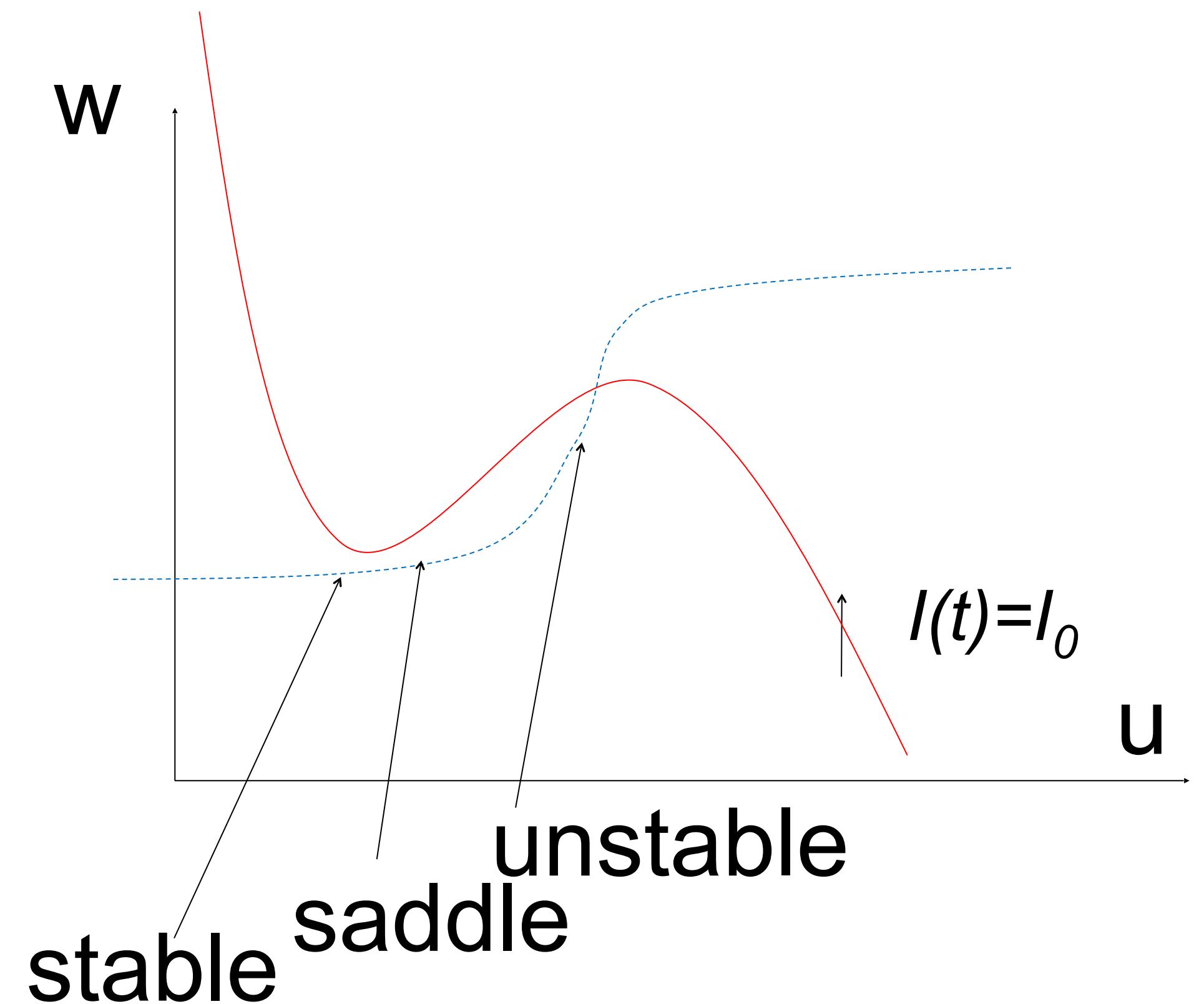
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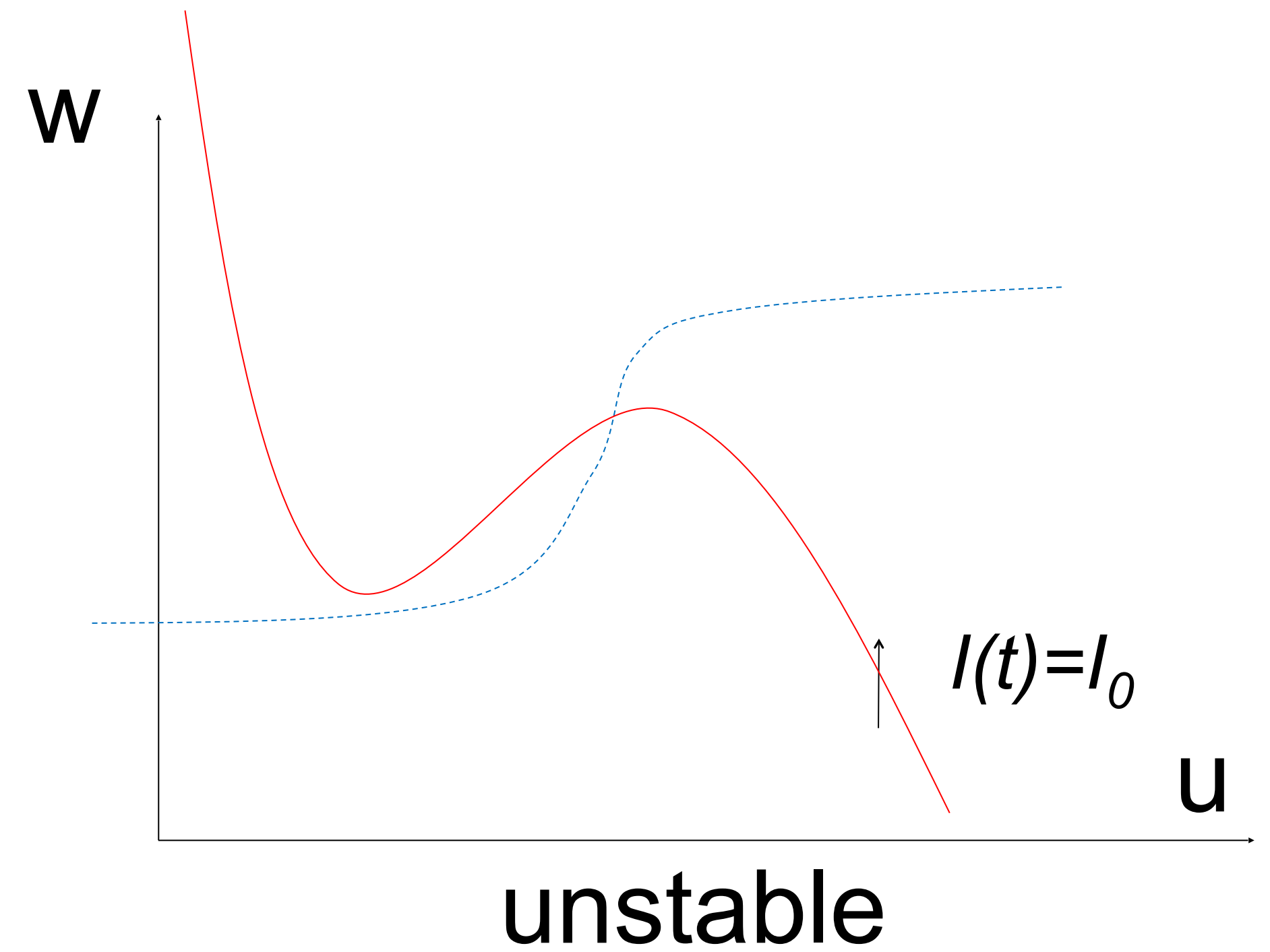
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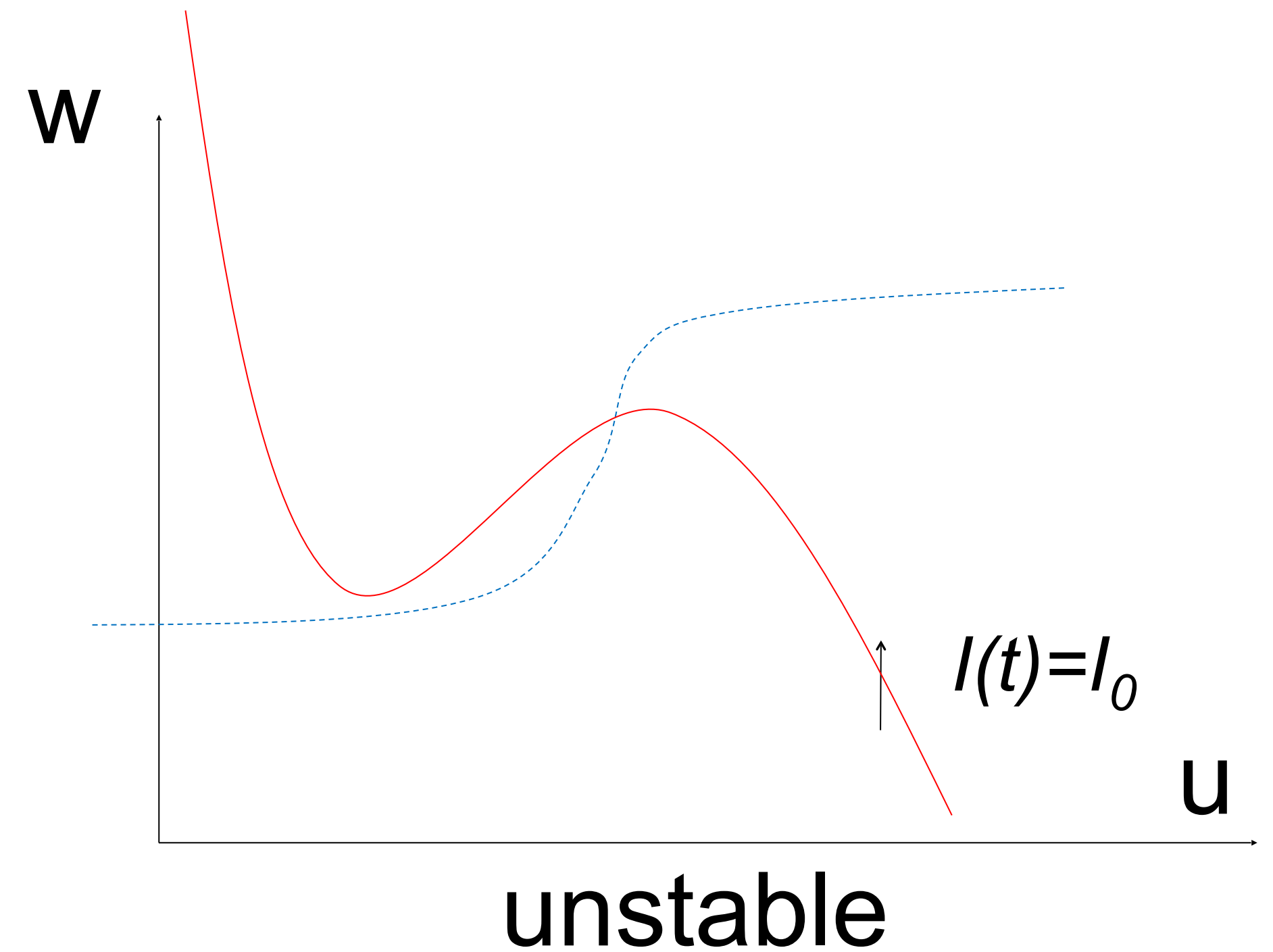
stimulus



$+RI(t)$

constant input

- flow arrows,
- ghost/ruins



## 4.2. Type I and II Neuron Models

2-dimensional equation

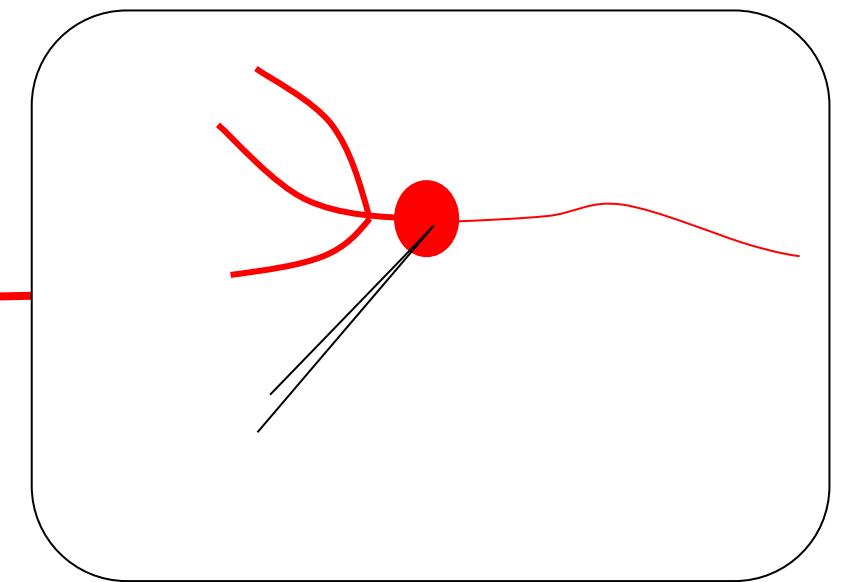
stimulus



ramp input/  
constant input



neuron



Enables graphical analysis!

Type I and type II models

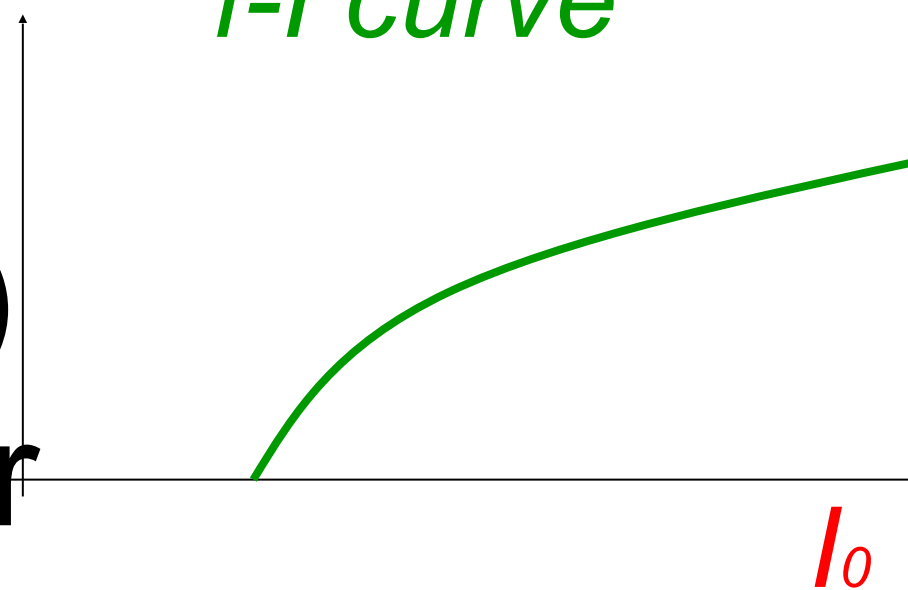
Constant input

→ repetitive firing (or not)

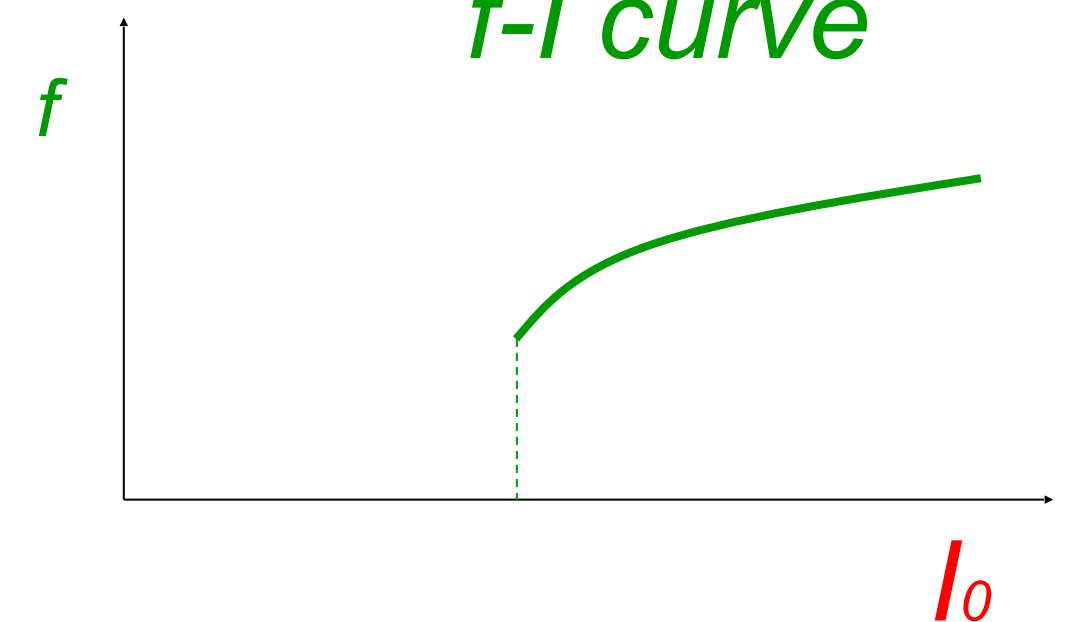
→ limit cycle (or

not)

*f-I curve*



*f-I curve*





# Neuronal Dynamics – Quiz 4.1.

## A. 2-dimensional neuron model with (supercritical) saddle-node-onto-limit cycle bifurcation

☐ The neuron model is of type II, because there is a jump in the f-I curve

☐ The neuron model is of type I, because the f-I curve is continuous

☐ The neuron model is of type I, if the limit cycle passes through a regime where the flow is very slow.

## B. Threshold in a 2-dimensional neuron model with subcritical Hopf bifurcation

☐ The neuron model is of type II, because there is a jump in the f-I curve

☐ The neuron model is of type I, because the f-I curve is continuous


☐ in the regime below the Hopf bifurcation, bistability between regular firing and rest state is possible.

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- ☒ [x] The neuron model is of type I, because the f-I curve is continuous
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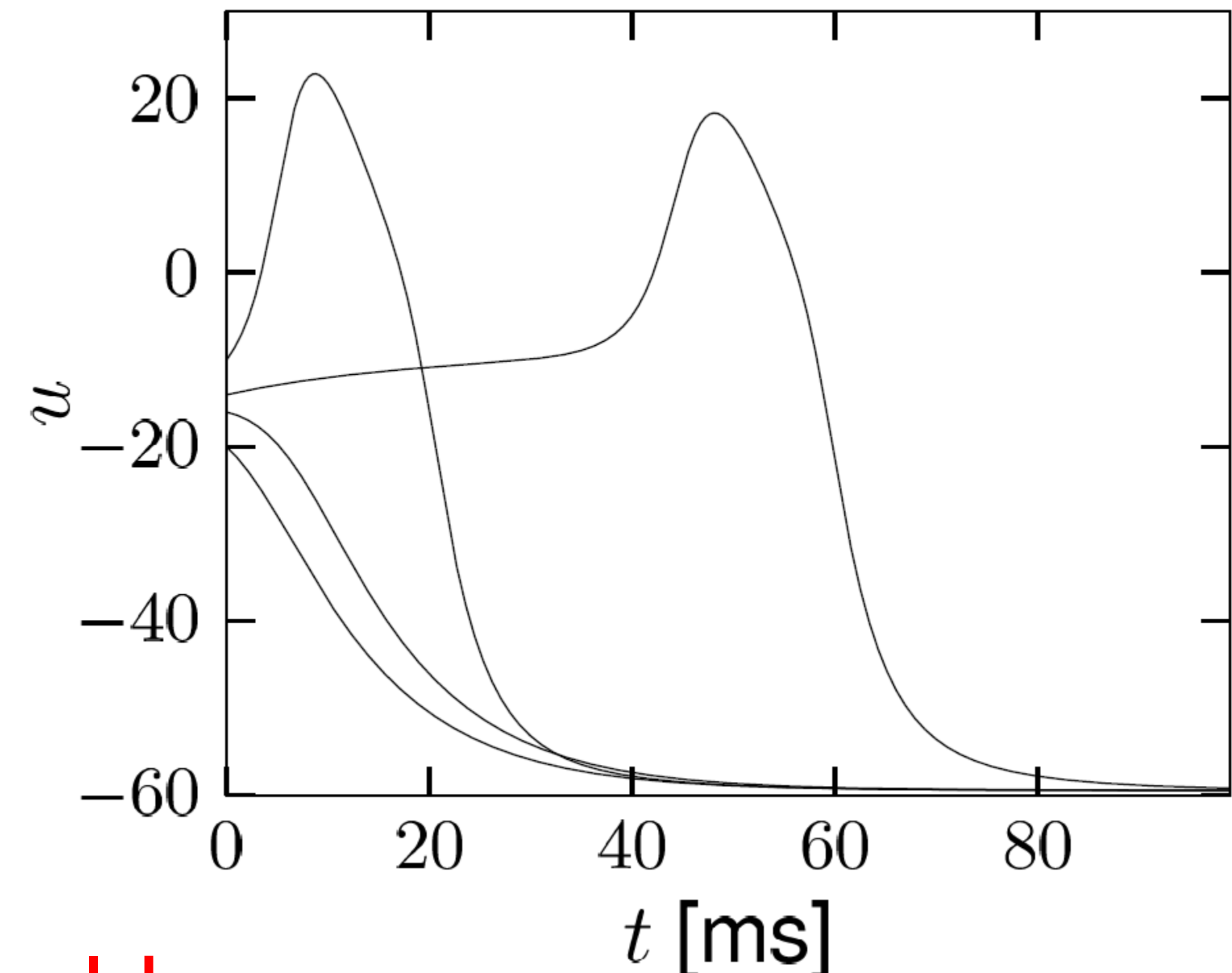
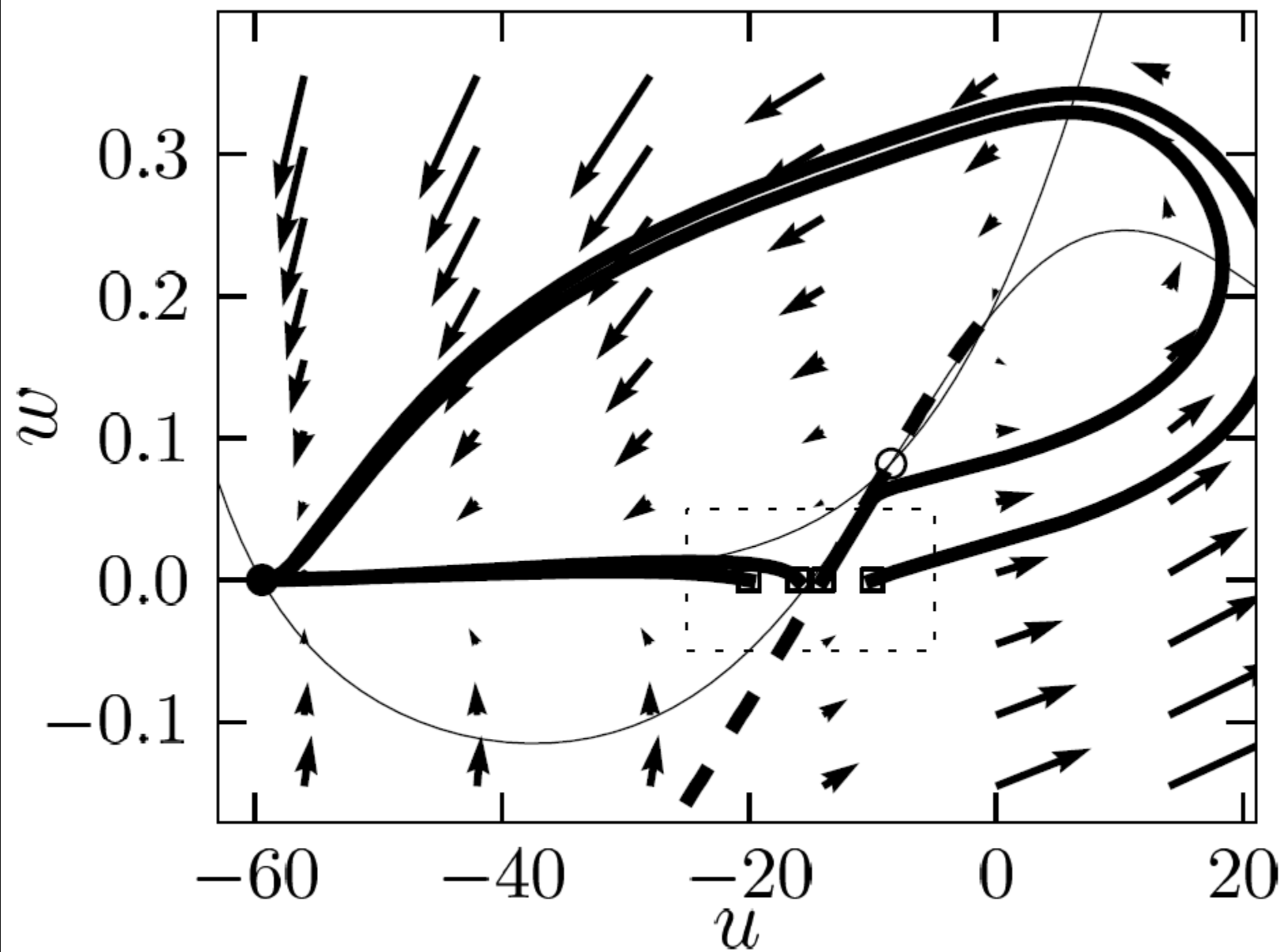
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- ☐ [ ] The neuron model is of type I, because the f-I curve is continuous
- ☒ [X] in the regime below the Hopf bifurcation, bistability between regular firing and rest state is possible.

## 4.2. Summary: Limit cycles and neuron models

- 1) In 2 dimensions we have a powerful theorem: if we can find a bounding box around an unstable fixed such that all flow arrows point inside the box, then there must be a limit cycle.
- 2) We can change the stability of the fixed point(s) by a constant input.
- 3) The limit cycle MAY appear at the moment when the fixed point loses stability. In this case it would often be a limit cycle of small amplitude in the neighborhood of the fixed point.
- 4) But we can also observe bistability between the stable fixed point and a limit cycle.
- 5) Neuron models can be classified according to the bifurcation type that makes a limit cycle appear. Type 1 neuron models have a smooth f-I curve and are always linked to a saddle-node-onto limit cycle bifurcation.
- 6) Type 2 models can have various origins; an example is the subcritical Hopf-bifurcation



## 4.3 Type I model: Delayed spike initiation for Pulse input

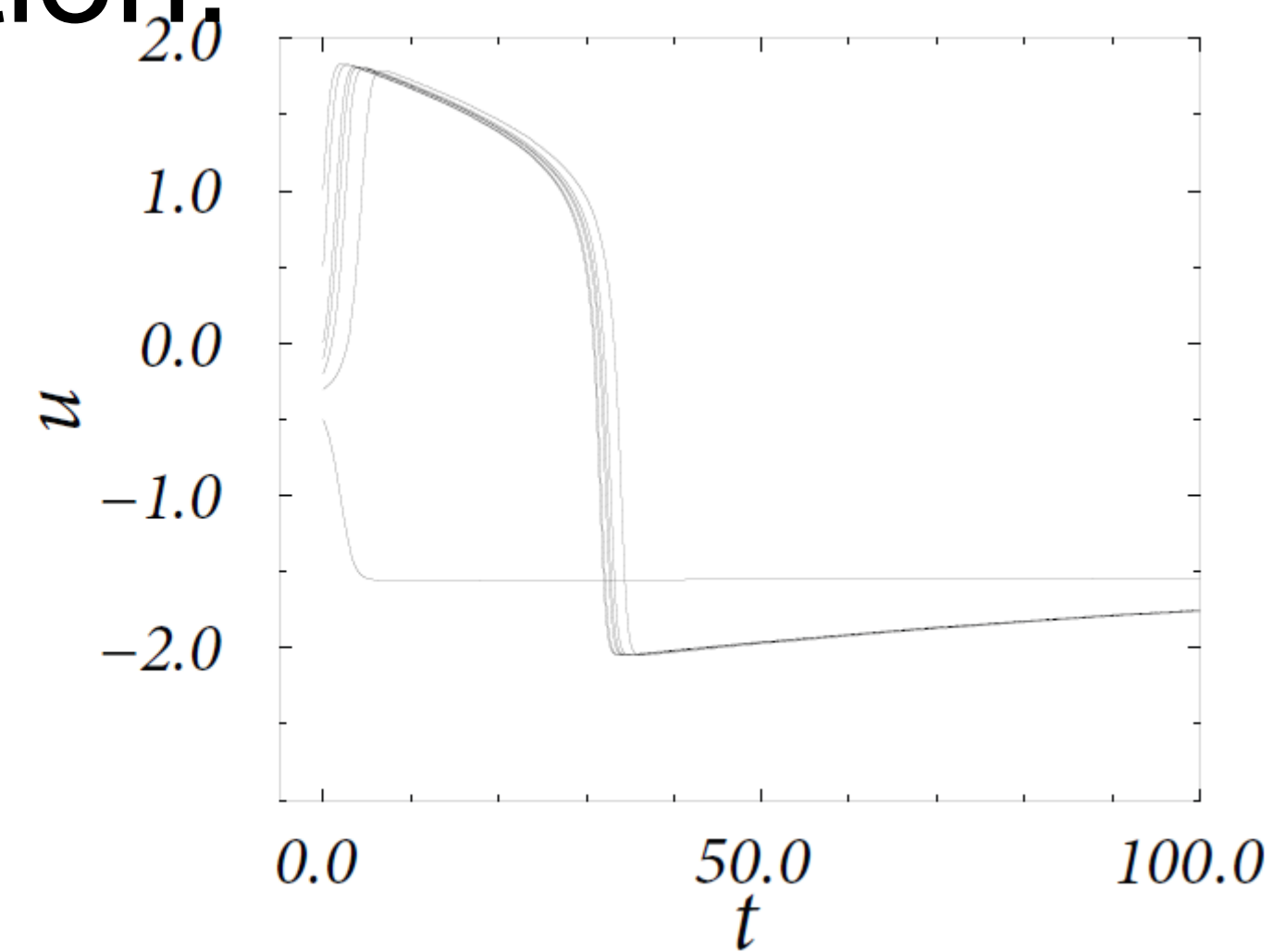
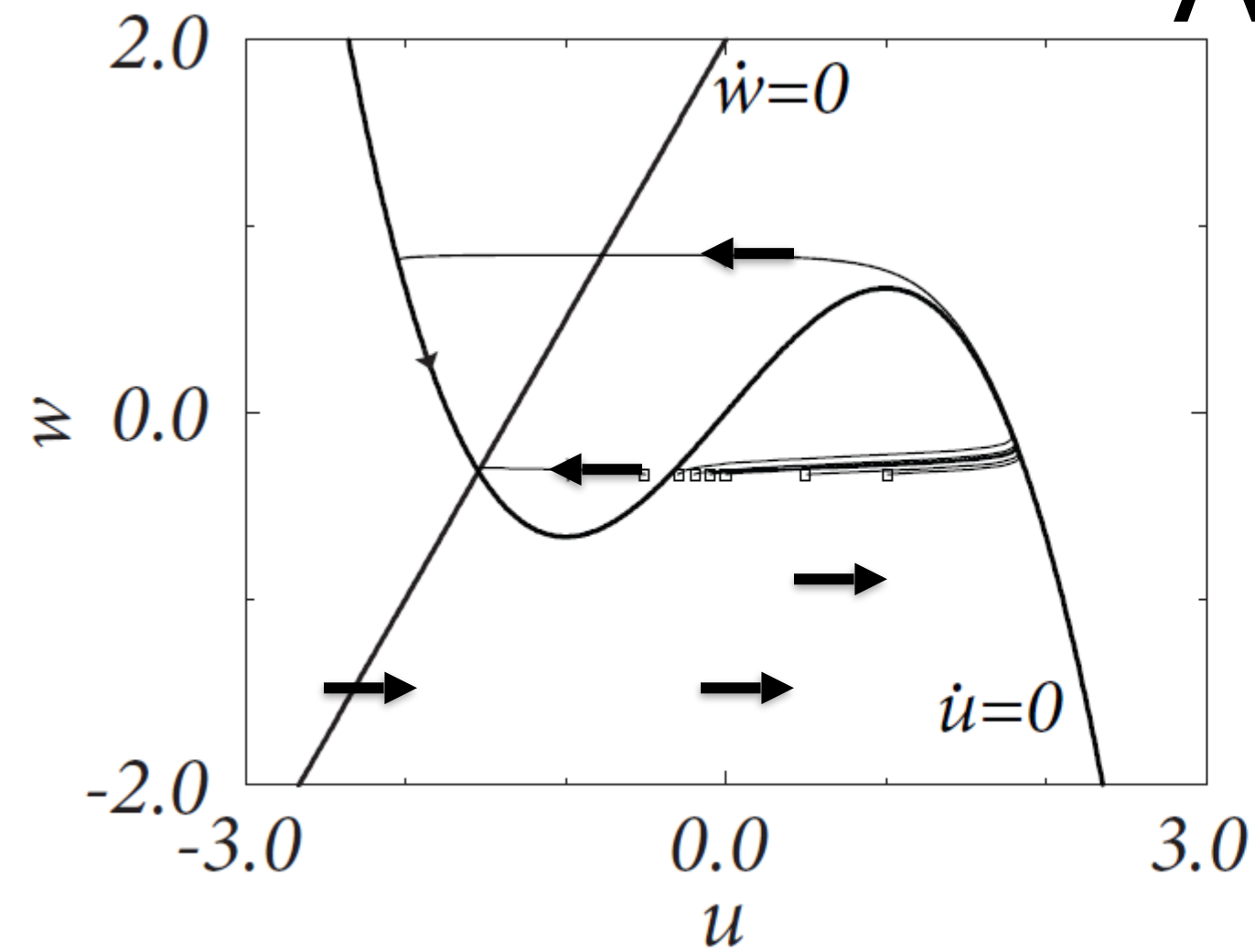


- Stable manifold plays role of threshold for pulse input
- Delayed spike initiation close to 'Threshold' (for pulse input)

*Image: Neuronal Dynamics,  
Gerstner et al.,  
Cambridge Univ. Press (2014)*

## 4.3 FitzHugh-Nagumo model: Threshold for Pulse input

Assumption;



Middle branch of  $u$ -nullcline  
plays role of  
'Threshold' (for pulse input)

*Image: Neuronal Dynamics,  
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Cambridge Univ. Press (2014)*

## Week 4– Quiz 4.2.

### A. Threshold in a 2-dimensional neuron model with saddle-node bifurcation

[ ] The voltage threshold for repetitive firing is always the same as the voltage threshold for pulse input.

[ ] in the regime below the saddle-node bifurcation, the voltage threshold for **repetitive firing** is given by the stable manifold of the saddle.

[ ] in the regime below the saddle-node bifurcation, the voltage threshold for **action potential firing in response to a short pulse input** is given by the stable manifold of the saddle point.

## Week 4– Quiz 4.2.

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- ☒ ☐ in the regime below the saddle-node bifurcation, the voltage threshold for **action potential firing in response to a short pulse input** is given by the stable manifold of the saddle point.



## Week 4– Quiz 4.3.

### B. Threshold in a 2-dimensional neuron model with subcritical Hopf bifurcation

[ ] in the regime below the Hopf bifurcation, the voltage threshold for firing of an isolated action potential in response to a short pulse input is the middle branch of the u-nullcline.

[ ] in the regime below the bifurcation, a voltage threshold for firing of an isolated action potential in response to a short pulse input exists only if

# Week 4– Quiz 4.3.

## B. Threshold in a 2-dimensional neuron model with subcritical Hopf bifurcation

- [ ] [ ] in the regime below the Hopf bifurcation, the voltage threshold for firing of an isolated action potential firing in response to a short pulse input is the middle branch of the u-nullcline.
- [x] [ ] in the regime below the bifurcation, a voltage threshold for firing of an isolated action potential f in response to a short pulse input exists only if

## 4.3. Summary: Pulse input and thresholds

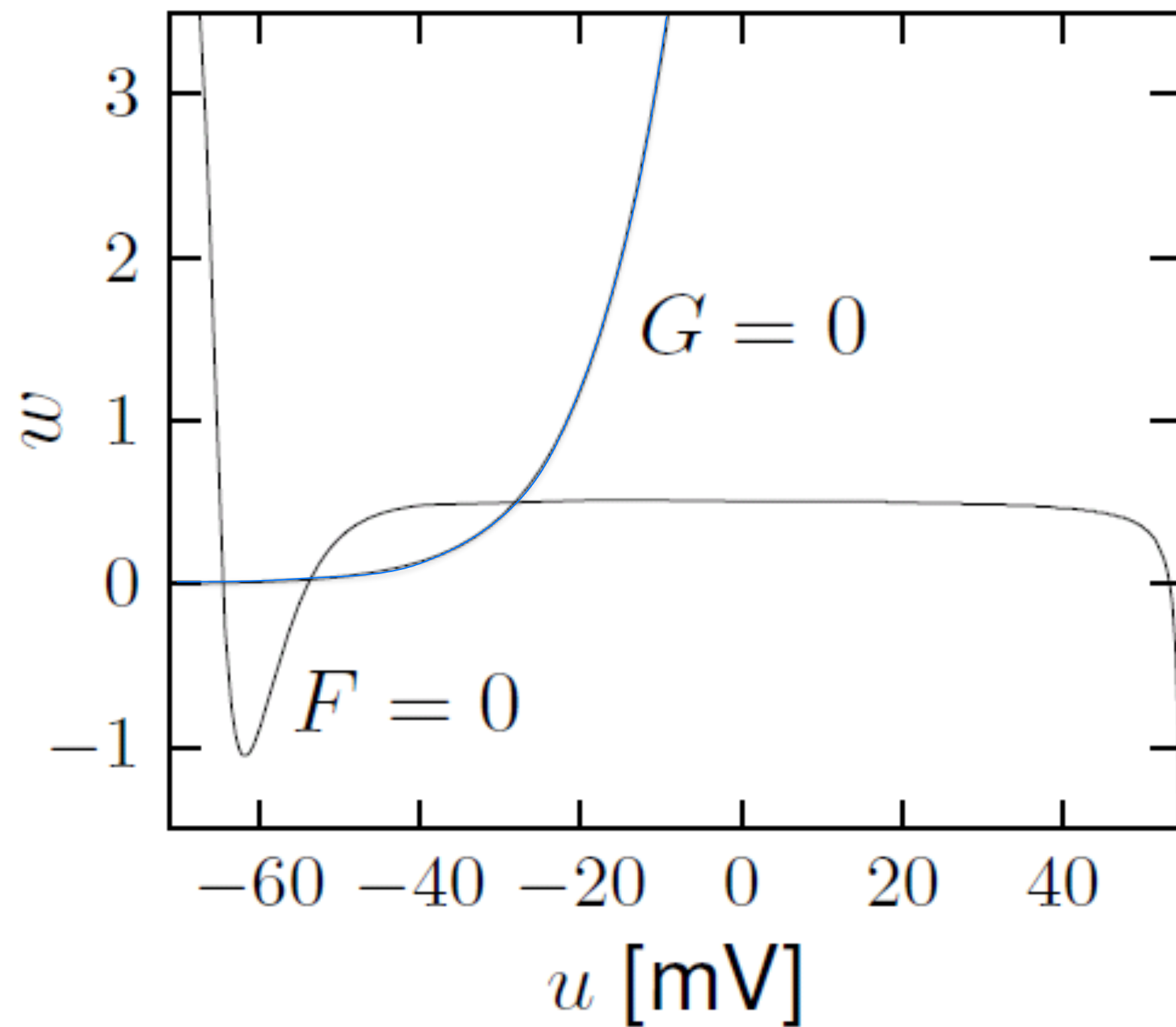
Neuron models with Saddle-node-onto limit cycle bifurcation have

- a smooth f-I curve
- a well-defined threshold for pulse input: either an AP occurs or not.
- Transition from subthreshold to superthreshold happens via an AP with very large delay.

Neuron models with subcritical Hopf-bifurcation have

- a non-smooth f-I curve
- not a well-defined threshold: there is a small regime where an AP transforms smoothly into non-AP
- However, together with a separation of time scale, the middle branch of the  $u$ -nullcline acts as a voltage threshold.

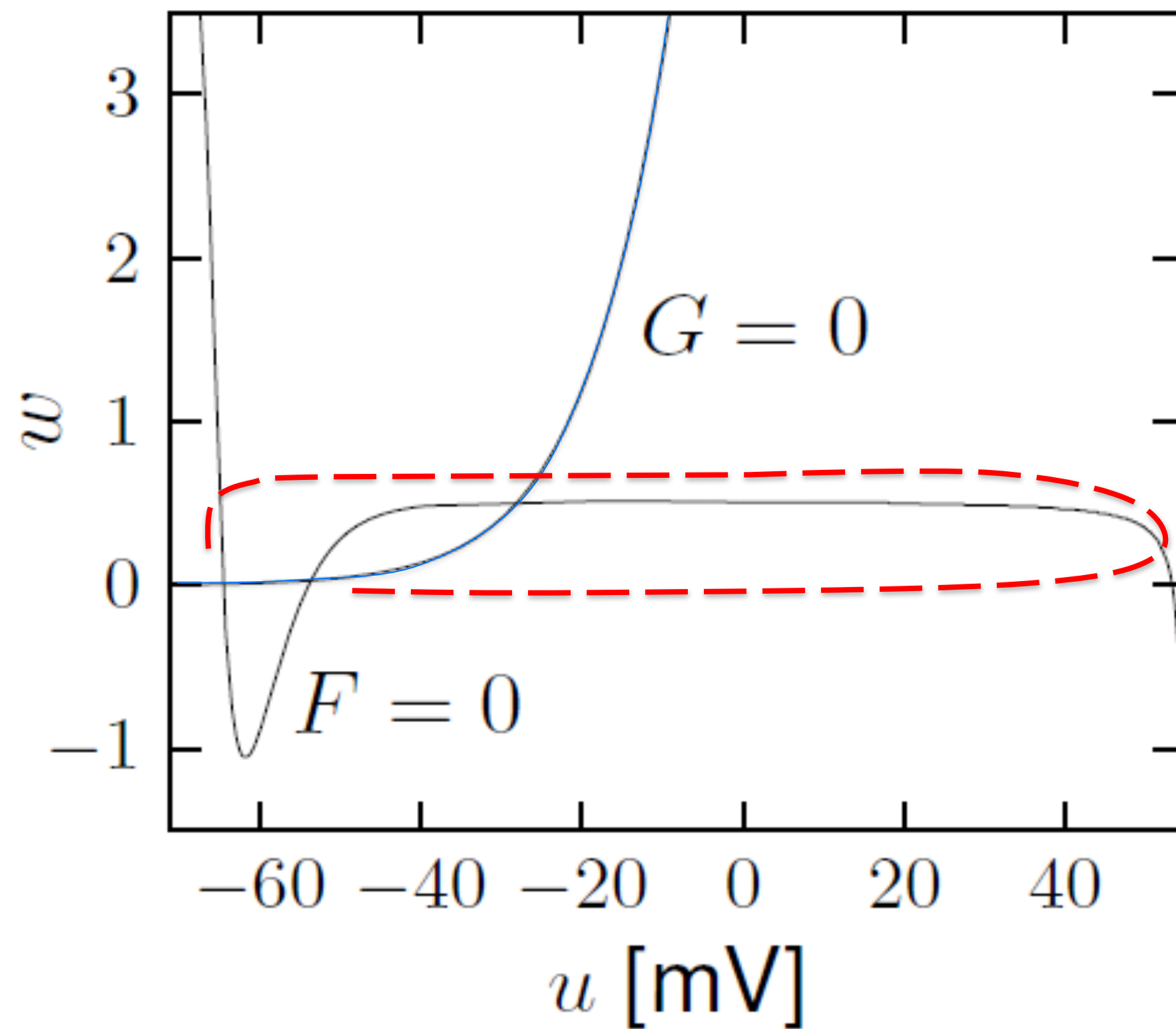
## 4.4. 2D model, after spike initiation



2-dimensional equation

Separation of time scales:  
 $w$  is constant (if not firing)

## 4.4. 2D model, after spike initiation

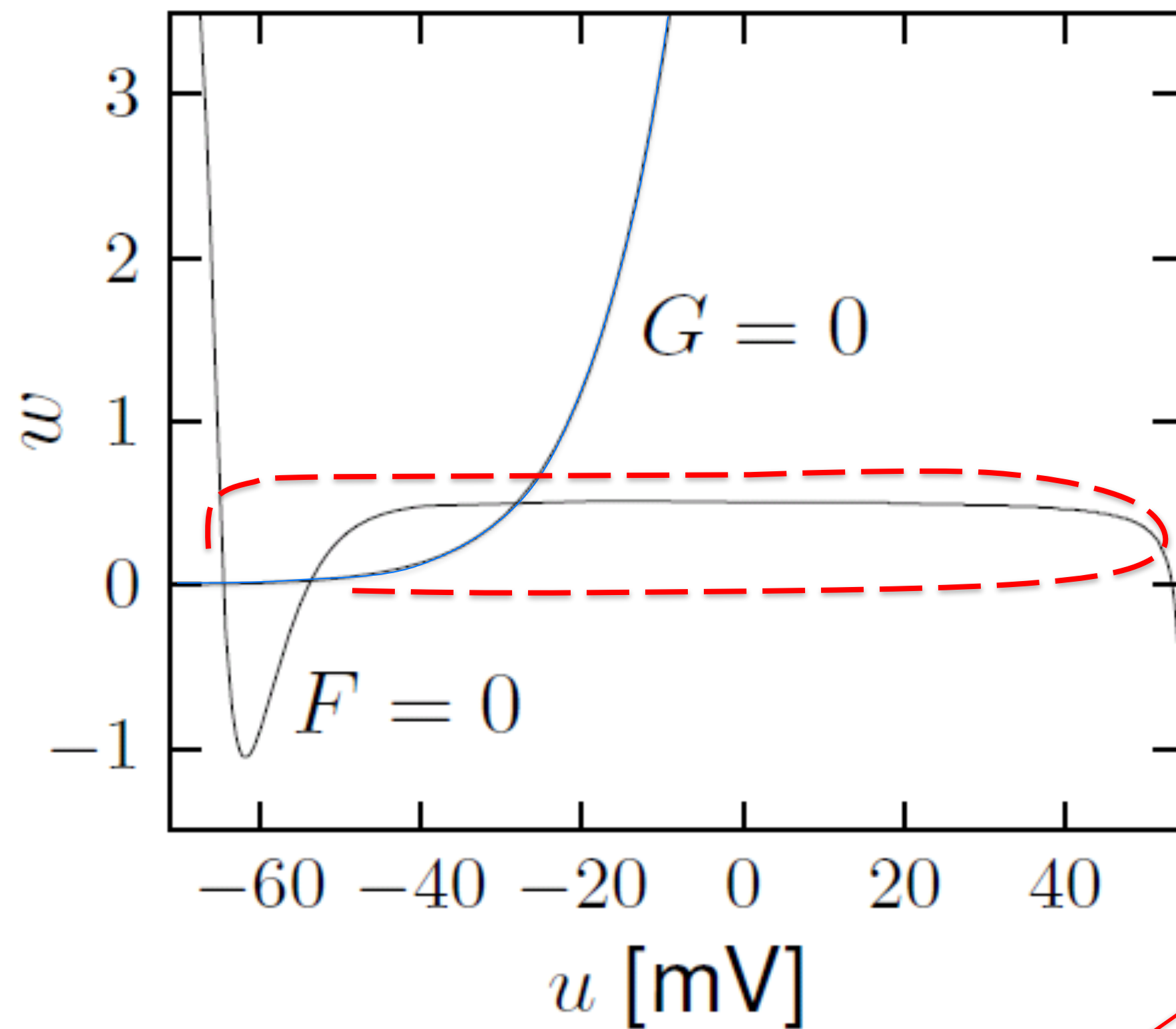


2-dimensional equation

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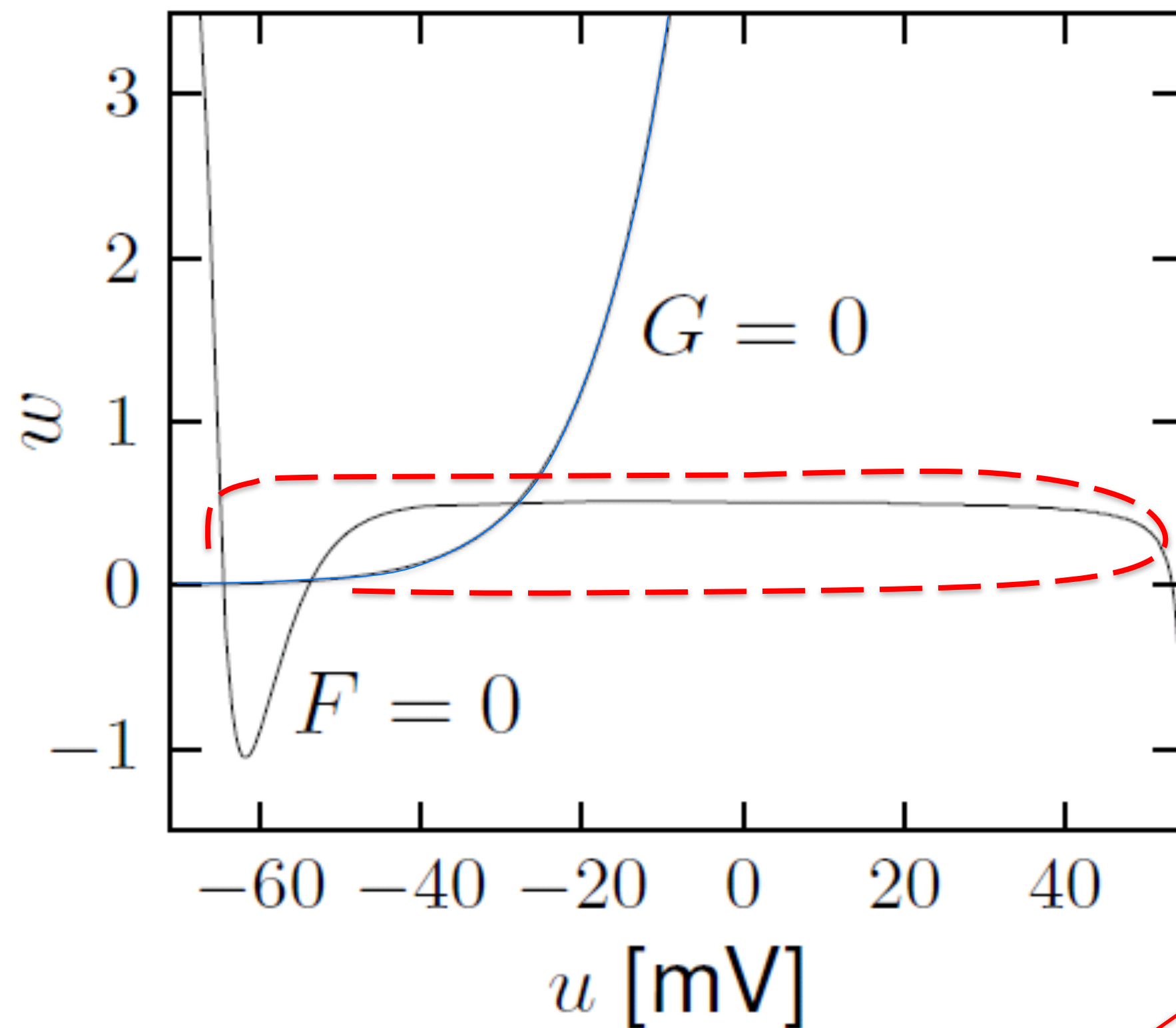


2-dimensional equation

Separation of time scales:  
 $w$  is constant (if not firing)

Relevant during spike  
and immediately  
after downswing of AP

## 4.4. 2D model, after spike initiation



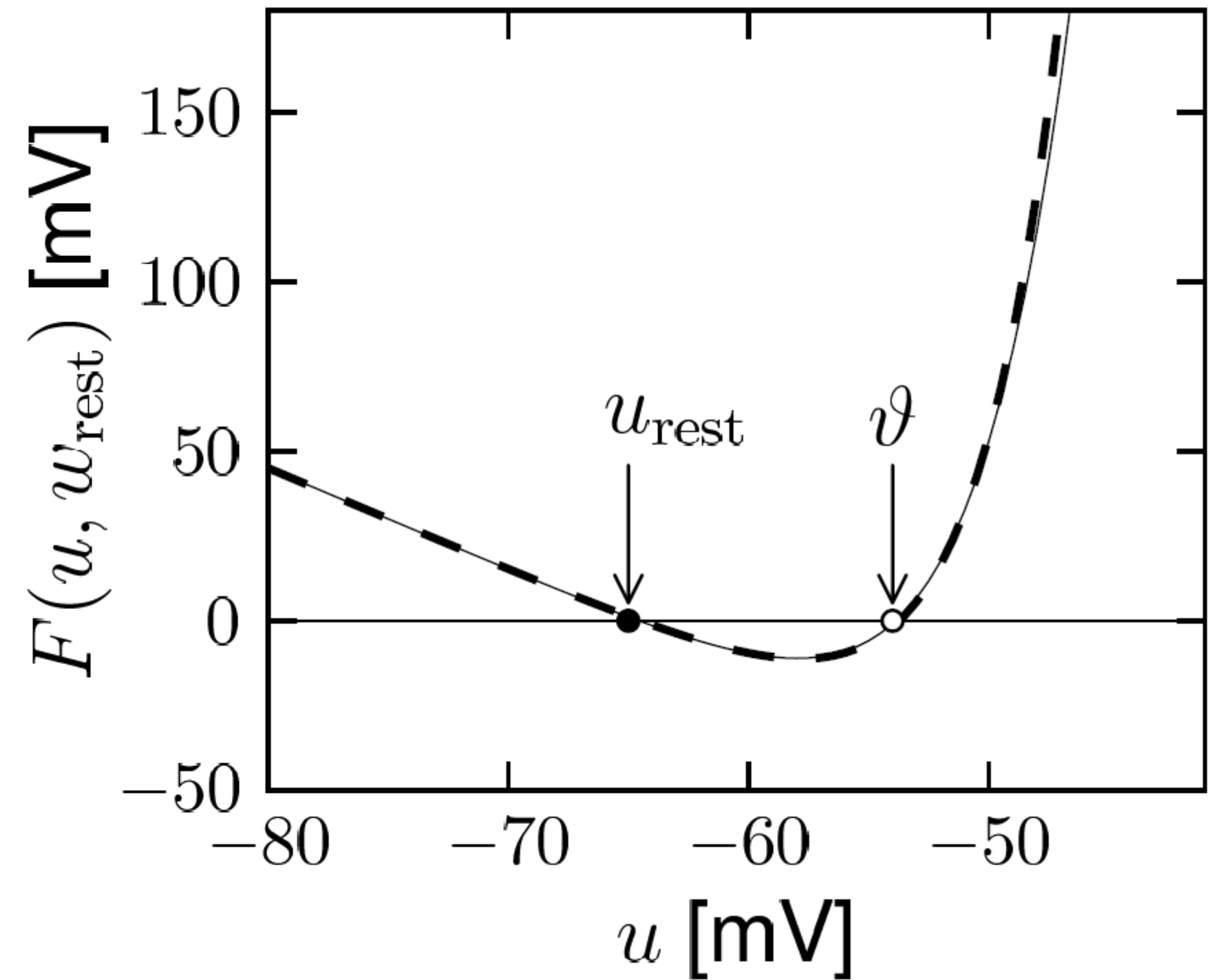
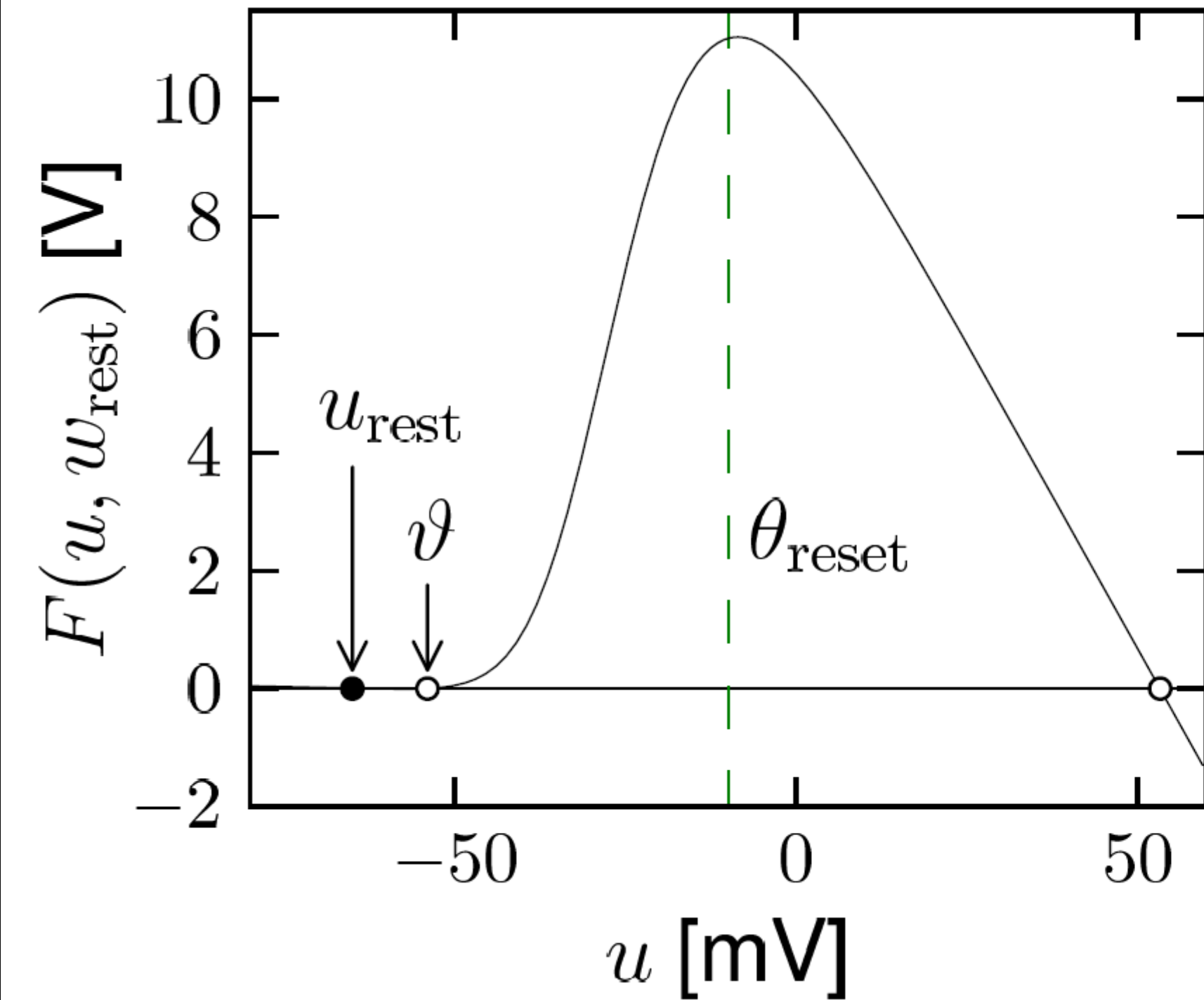
2-dimensional equation

Separation of time scales:  
 $w$  is constant (if not firing)

Relevant during spike  
and immediately  
after downswing of AP

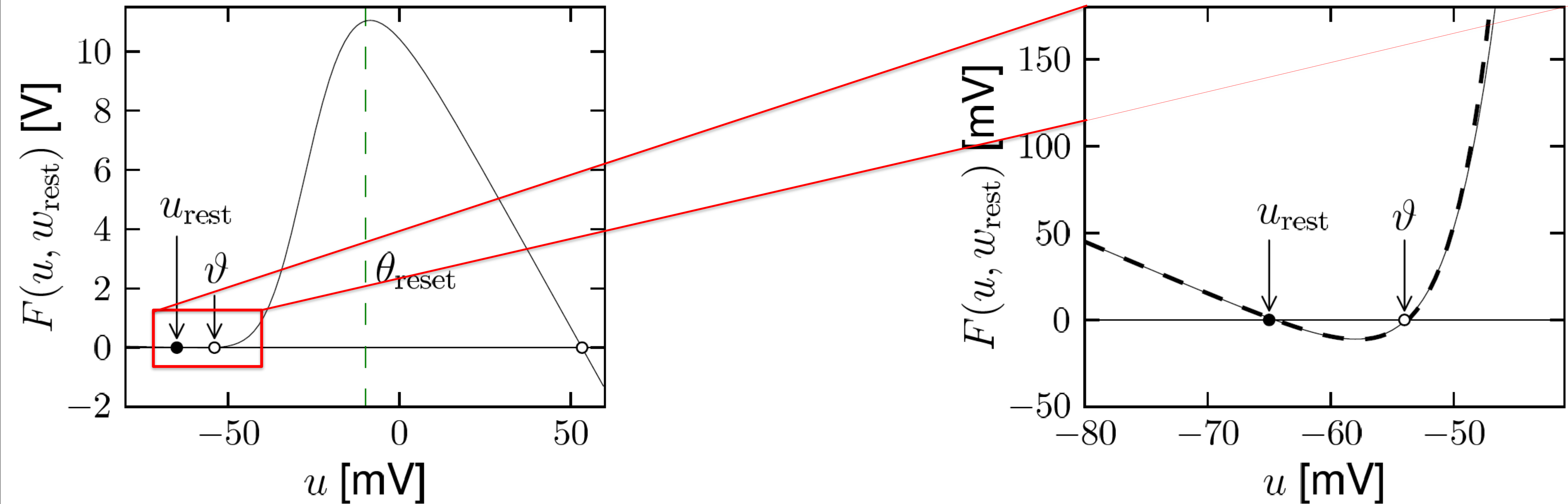
Integrate-and-fire:  
threshold+reset for AP

## 4.4. Spike initiation: Nonlinear Integrate-and-Fire Model



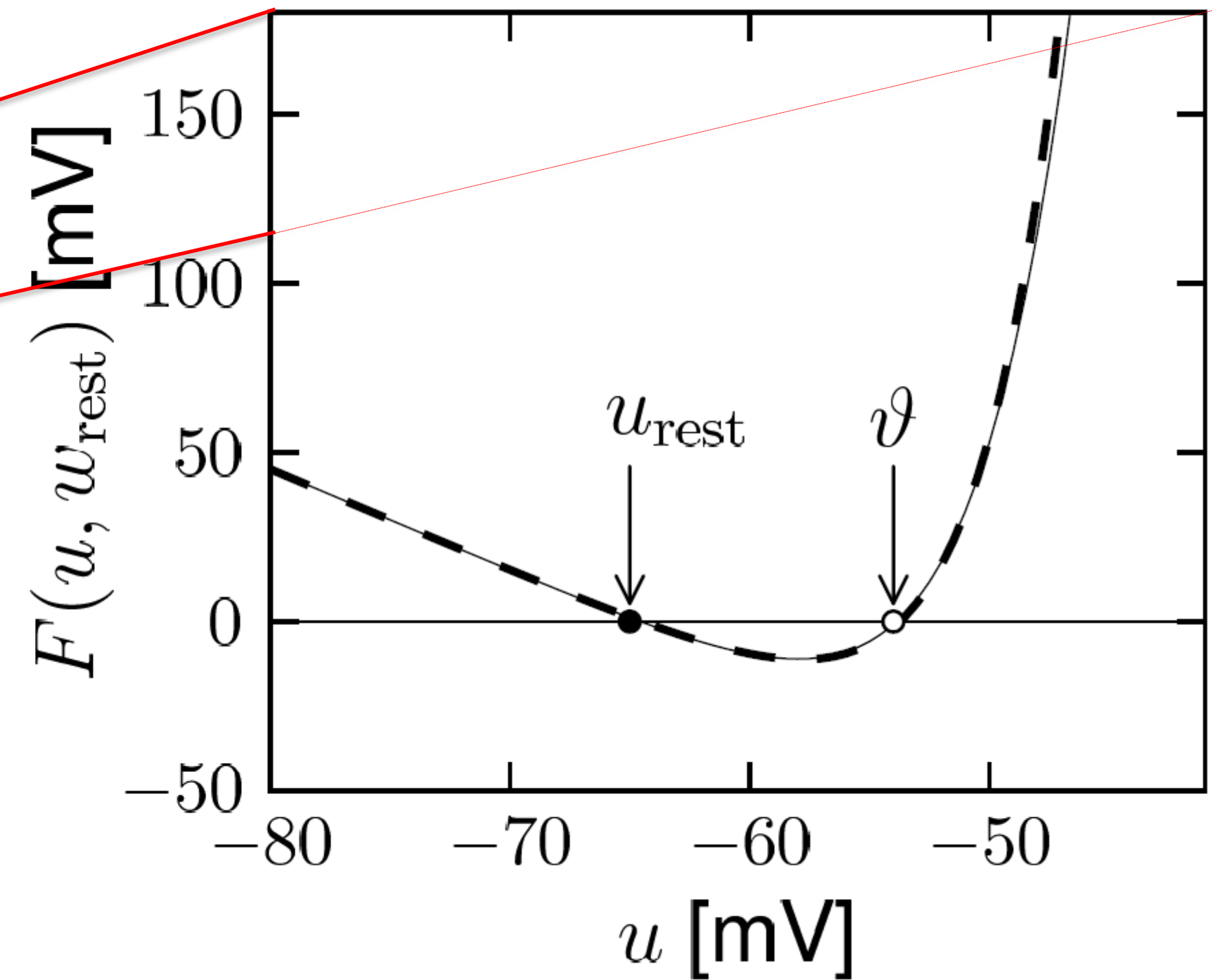
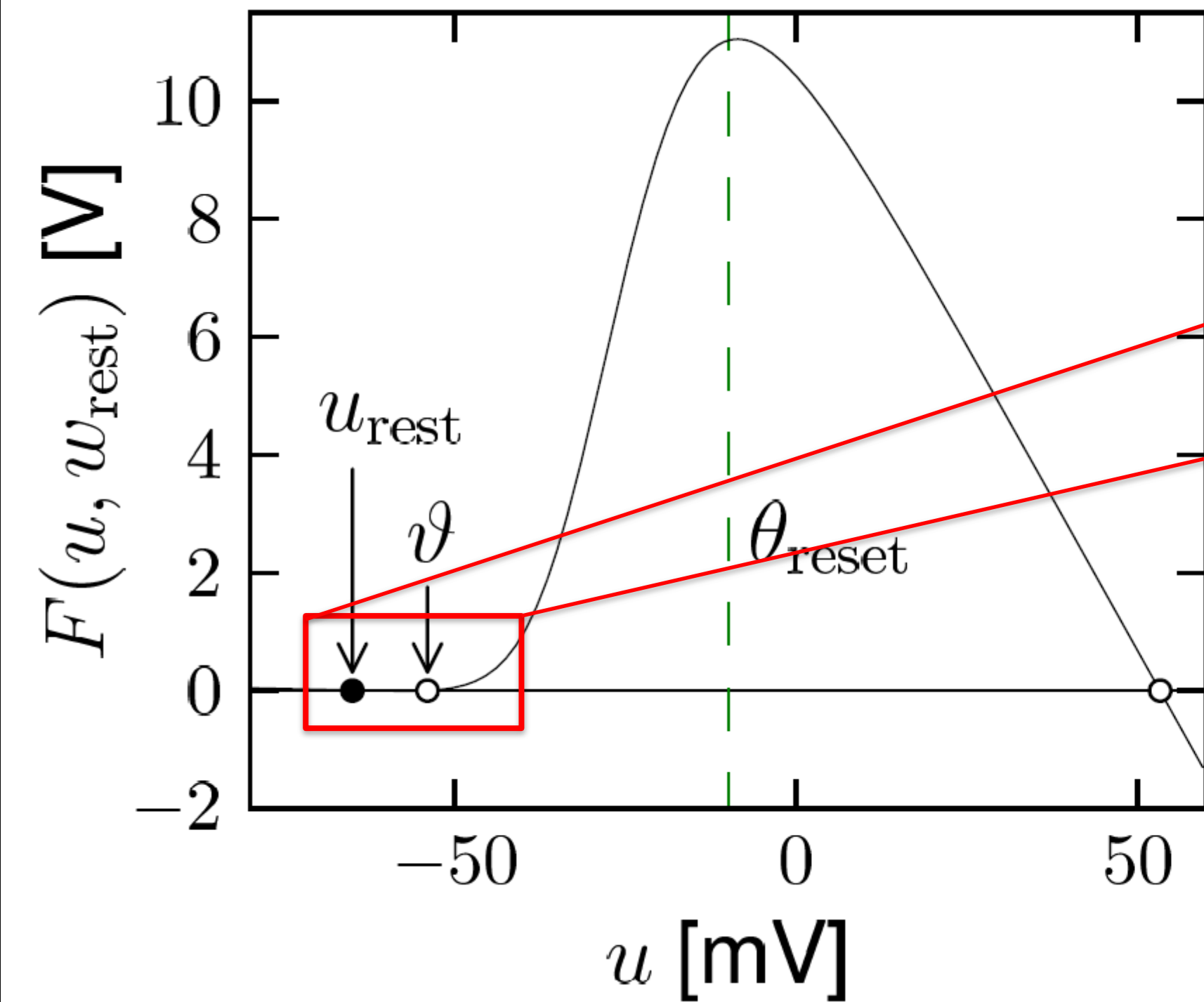
*Image: Neuronal Dynamics,  
Gerstner et al.,  
Cambridge Univ. Press (2014)*

## 4.4. Spike initiation: Nonlinear Integrate-and-Fire Model



*Image: Neuronal Dynamics,  
Gerstner et al.,  
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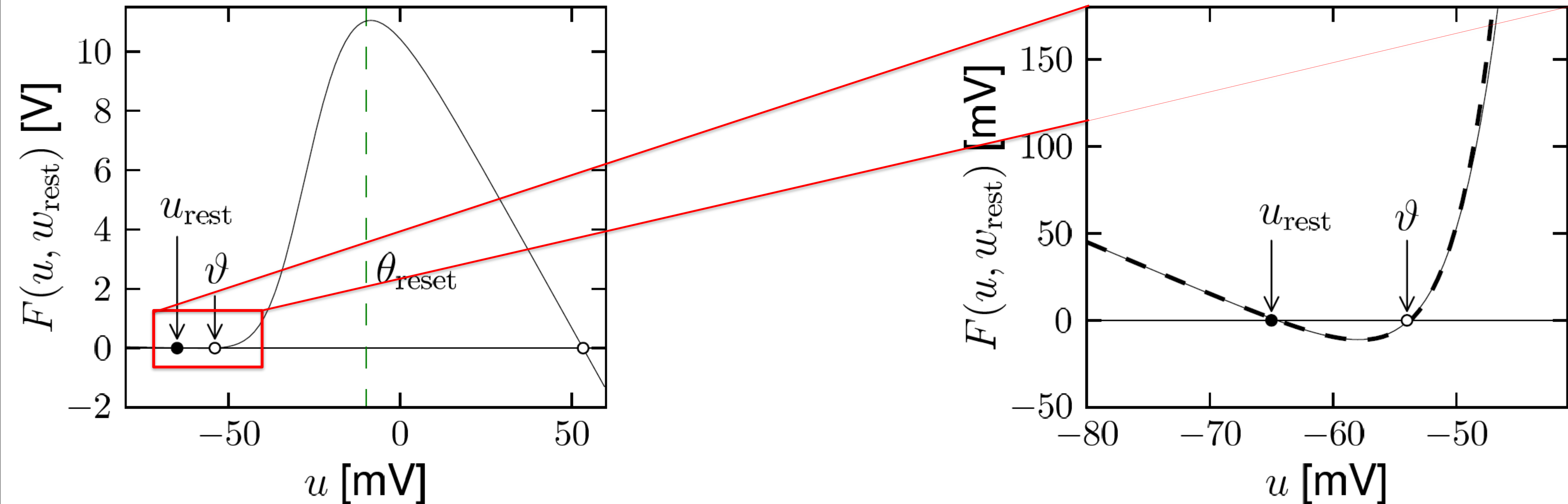
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→ Nonlinear I&F (see week 1!)

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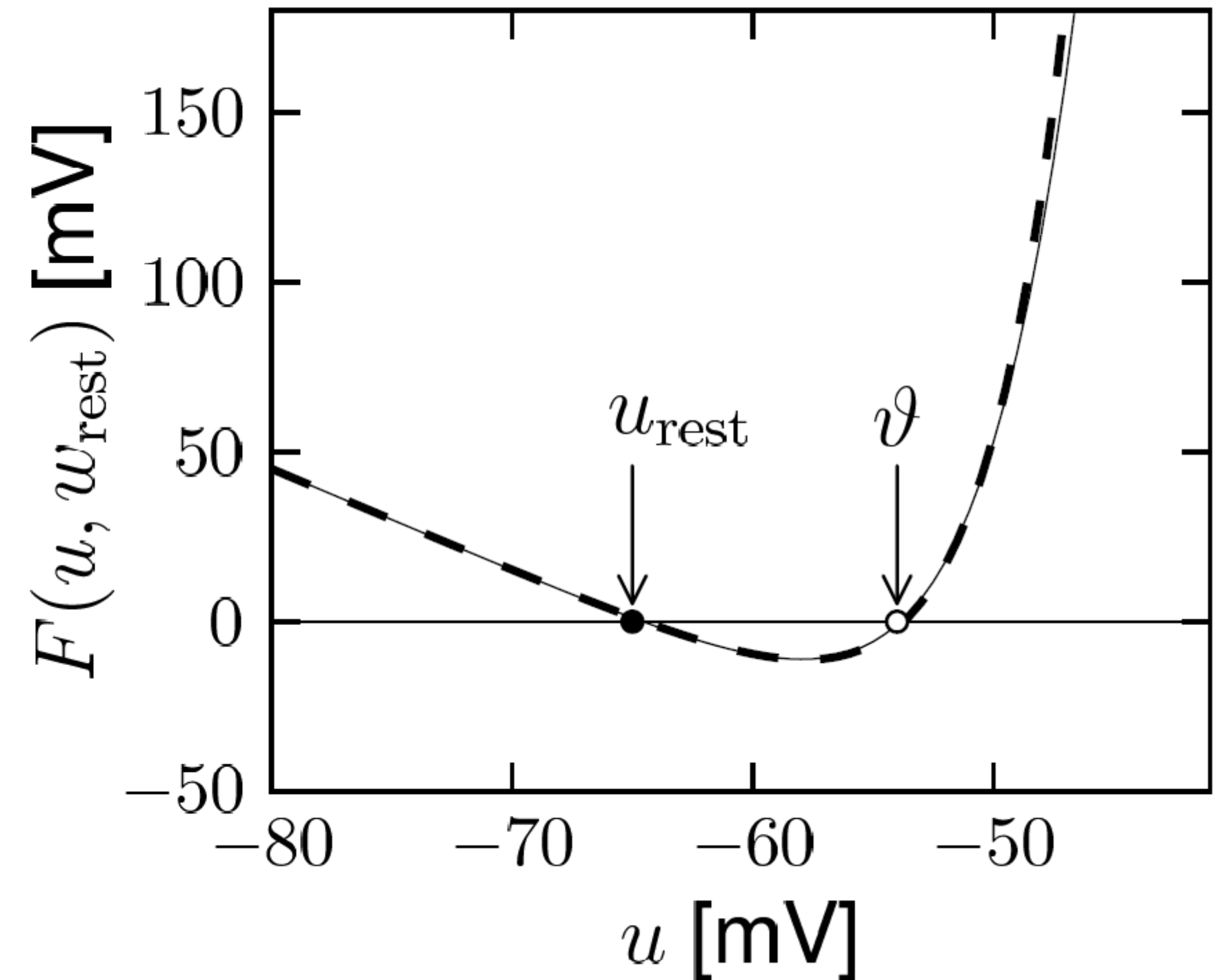
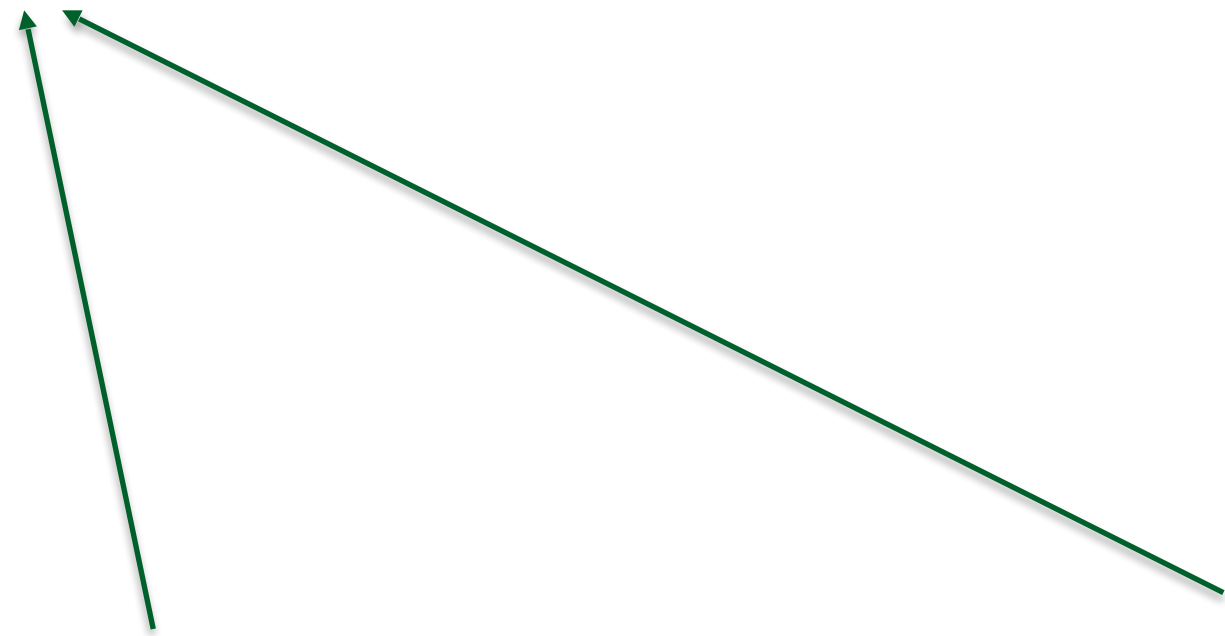
→ **Nonlinear I&F (see week 1!)**

During spike initiation, the 2D models with separation of time scales can be reduced to a 1D model equivalent to nonlinear integrate-and-fire



## 4.3. Exponential Integrate-and-Fire Model

Exponential integrate-and-fire model  
(EIF)



*Image: Neuronal Dynamics,  
Gerstner et al.,  
Cambridge Univ. Press (2014)*

→ Nonlinear I&F (see week 1!)

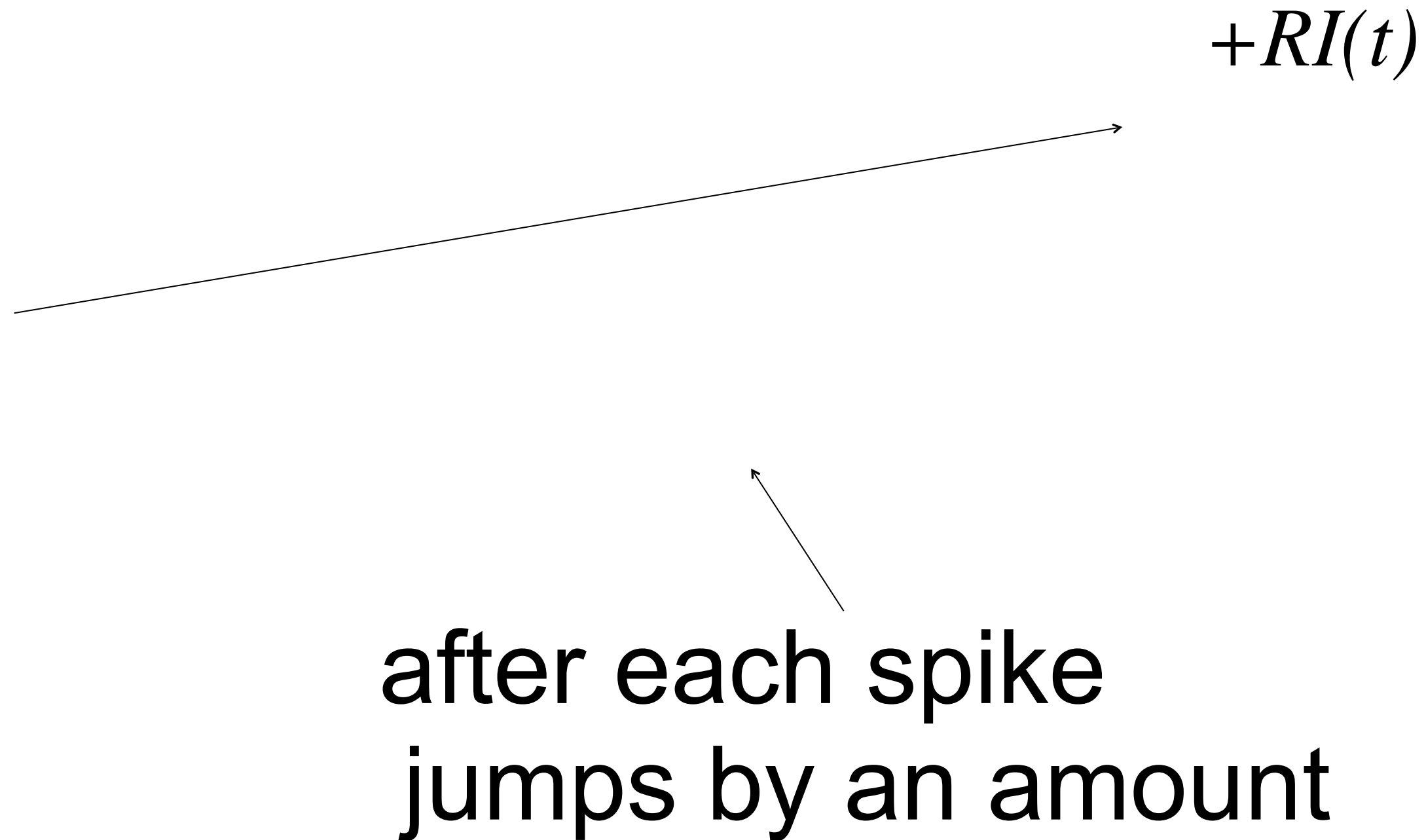
## 4.4 Extension to Adaptive Exponential I&F

Add adaptation variables:

$$+RI(t)$$

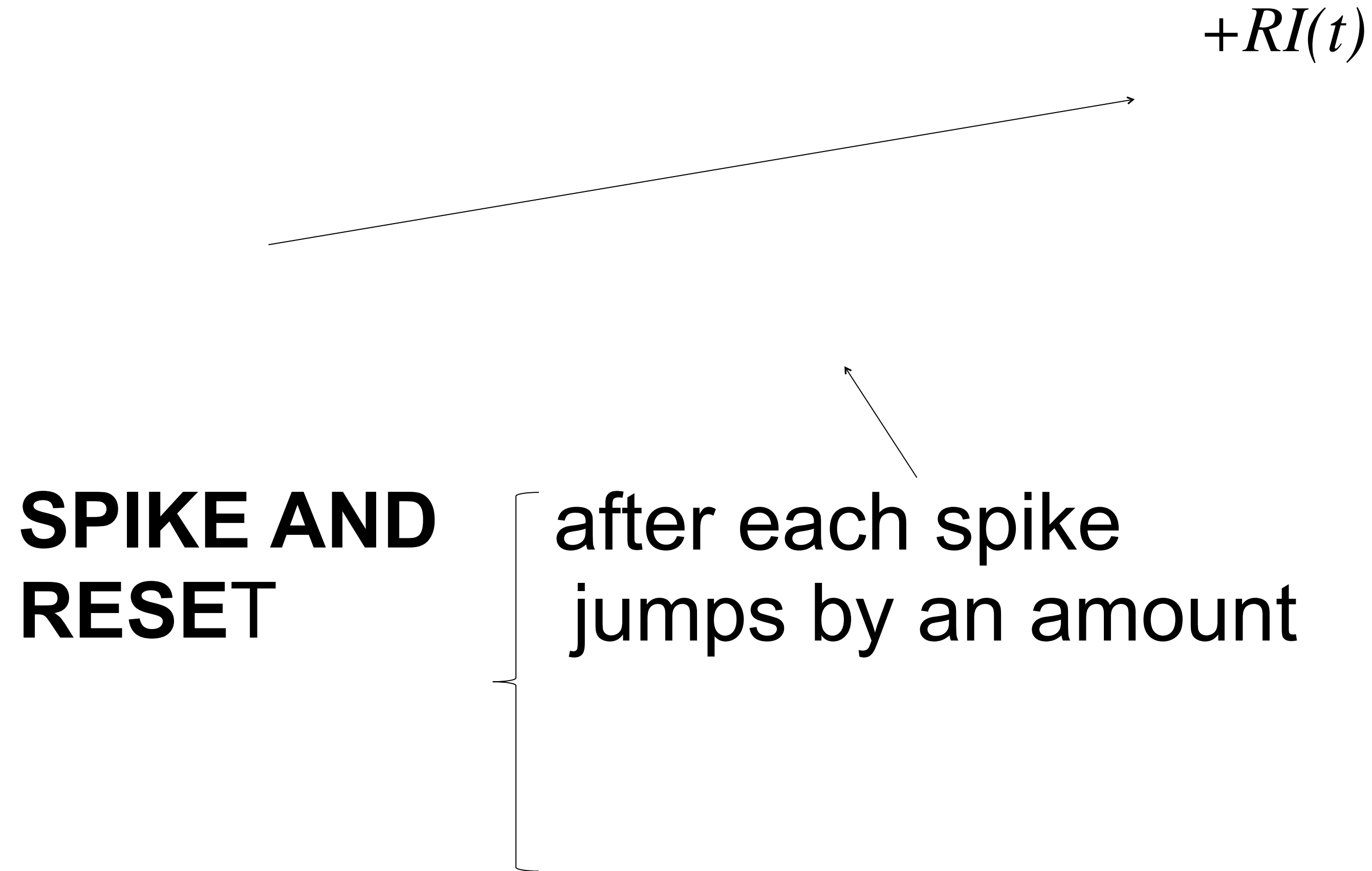
## 4.4 Extension to Adaptive Exponential I&F

Add adaptation variables:



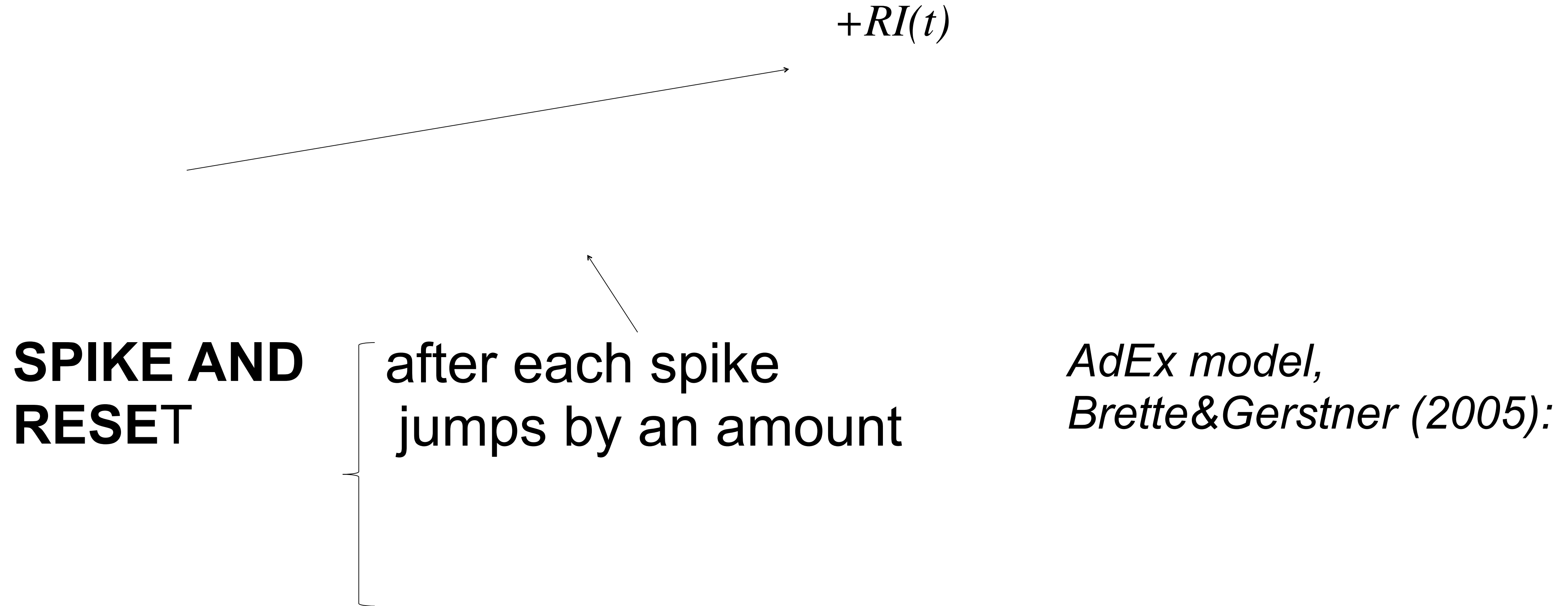
## 4.4 Extension to Adaptive Exponential I&F

Add adaptation variables:



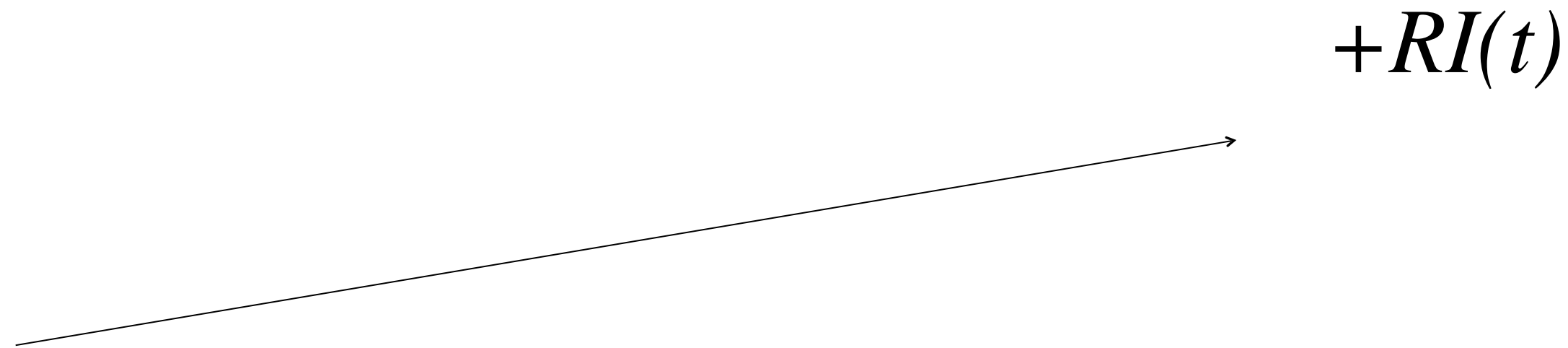
## 4.4 Extension to Adaptive Exponential I&F

Add adaptation variables:



## 4.4 Extension to Adaptive Exponential I&F

Add adaptation variables:



Exponential I&F  
+ 1 adaptation var.  
= AdEx

**SPIKE AND  
RESET**

after each spike  
jumps by an amount

*AdEx model,  
Brette&Gerstner (2005):*



## 4.4. Summary: from HH to generalized integrate-and-fire

- The **reduction of the Hodgkin-Huxley (HH) model** from 4 to 2 dimensions generates nonlinear nullclines with several intersections.
- If we zoom in on the two left-most intersections the u-nullcline looks similar to a superposition of a linear and an exponential term
- Between (rare) spike events, the w-variable has always time to go back to resting potential. Hence during spike-initiation we can consider the w-variable as constant.
- This gives rise to the **exponential integrate-and-fire model**
- **Adaptation** means that for constant input the interspike intervals increase over time
- The standard HH-model shows no (or very little) adaptation
- More complicated Hodgkin-Huxley type models would have additional variables (describing other ion channels) that cause adaptation
- In integrate-and-fire models, these additional adaptation variables can often be approximated by a linear dynamics for new variables  $w_k$

# Computational Neuroscience: Neuronal Dynamics

## Part I: Single Neurons, deterministic. Week 1-4

*Week 1:* A first simple neuron model/  
neurons and mathematics

*Week 2:* Hodgkin-Huxley models and  
biophysical modeling

*Week 3:* Two-dimensional models and  
phase plane analysis

*Week 4:* Two-dimensional models,  
type I and type II models  
transition to IF models

## LEARNING OUTCOMES

- Solve linear one-dimensional differential equations
- Analyze two-dimensional models in the phase plane
- Develop a simplified model by separation of time scales
- Analyze connected networks in the mean-field limit
- Formulate stochastic models of biological phenomena
- Formalize biological facts into math
- Prove stability and convergence
- Apply model concepts in simulations
- Predict outcome of dynamics
- Describe neuronal phenomena

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