



NIBS and multimodal imaging

Prof. Dr. med. Friedhelm Hummel

Defitech Chair for Clinical Neuroengineering,
Neuro-X Institute (INX) & Brain Mind Institute (BMI)
Ecole Federale Polytechnique de Lausanne (EPFL)

Department of Clinical Neuroscience, University Hospital of Geneva



What are the potential benefits of multimodal imaging combined with neuromodulation?

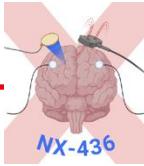


Recording of brain activity simultaneously

- focally and at the network level
- adds to mechanistic understanding
- safety monitoring
- state dependent close-loop applications

Online interference with brain activity

- causal understanding
- network vs. local effects
- state dependent close-loop applications



What are the disadvantages and challenges of
multimodal imaging combined with neuromodulation?

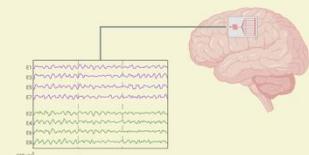
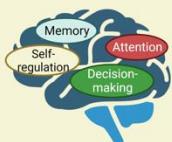


Challenges

- temporal, spatial resolution
- safety
- artefacts
- feasibility
- accessibility, clinical translation
- cost

**INVASIVE****NON-INVASIVE****Neurosensing/ Neuro-monitoring
"READ"**

Monitors electrical/BOLD activity in the central nervous system



eCoG, iEEG



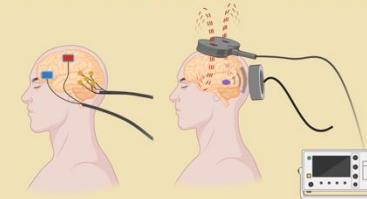
EEG, MEG, fMRI

**Neuromodulation
"WRITE"**

Targets and improves functions such as motor, attention, memory, decision-making, self-regulation either electrically, magnetically or via ultrasound



DBS



TMS, tES, TUS

**Combinatory (bidirectional)
"READ + WRITE"**

Monitors and reacts to brain states with prosthetics, robotics, brain stimulation



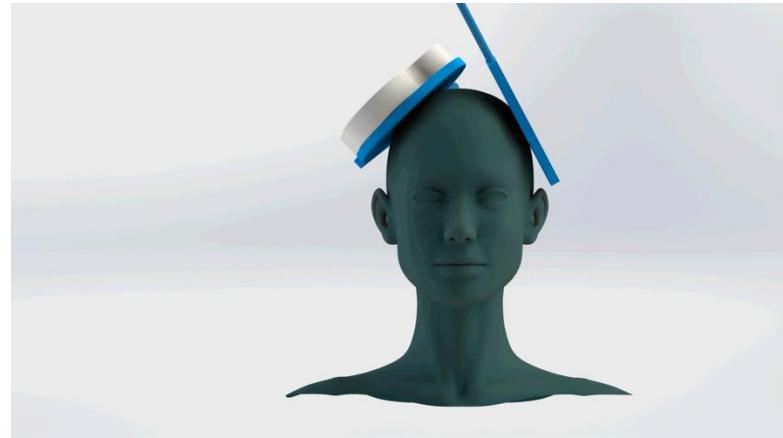
Closed-loop DBS



BCI, BBI, ...



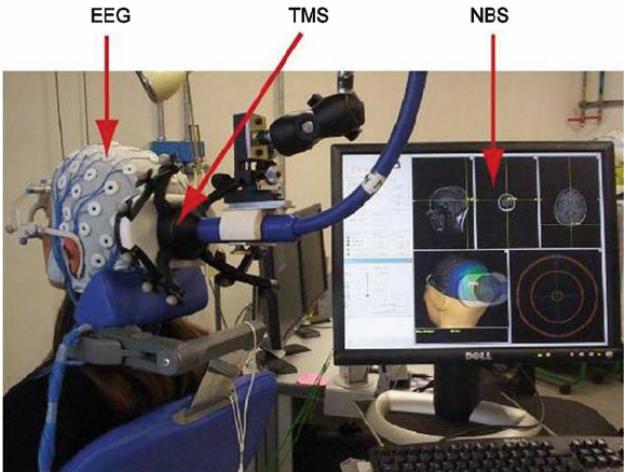
WHITE: TMS coil (stimulation)
NX-436



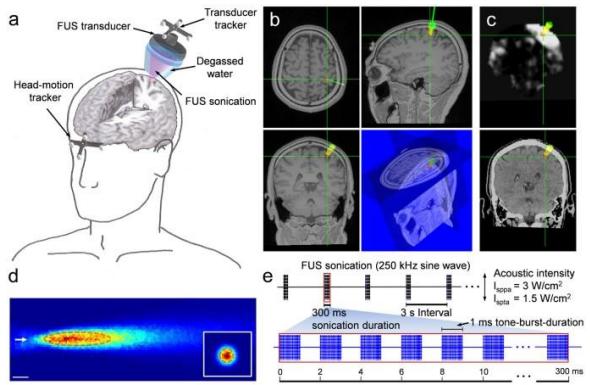


Friedhelm C. Hummel

TMS-EEG



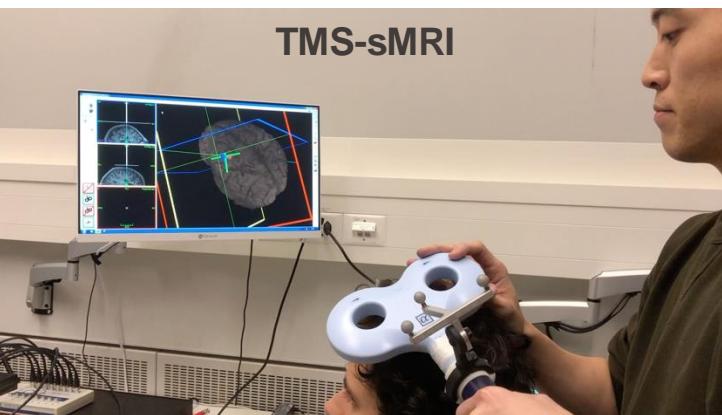
fUS-TMS/EEG/MRI



TMS-fMRI

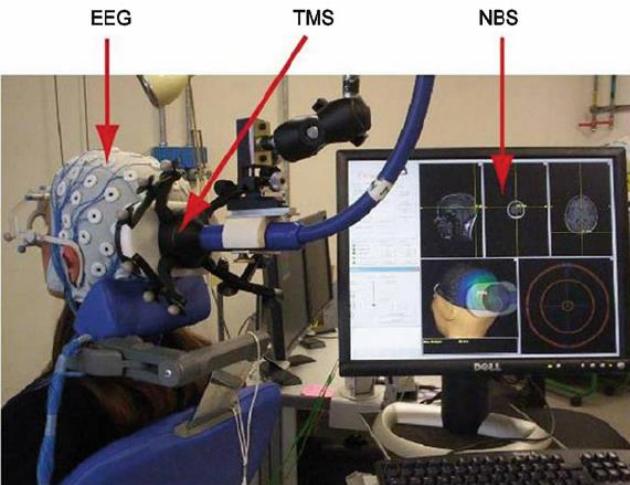
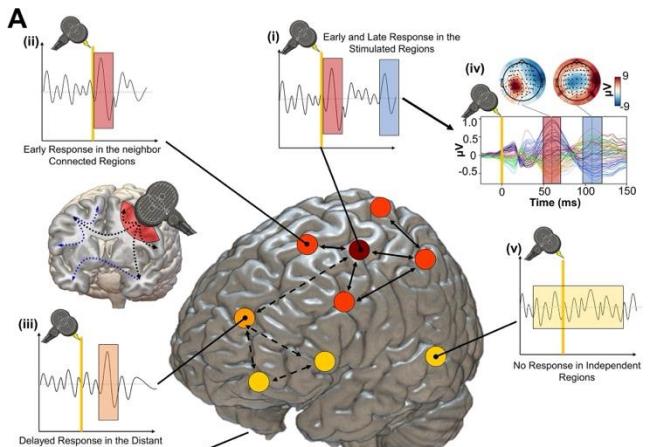


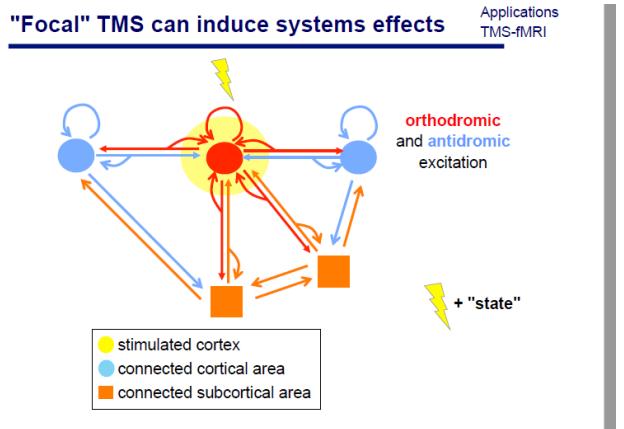
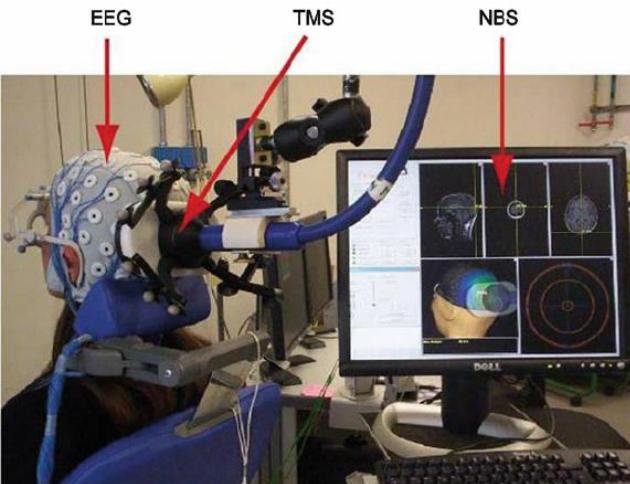
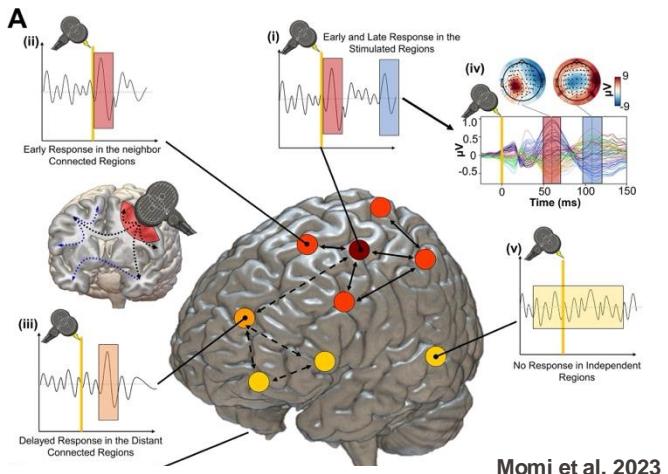
TMS-sMRI



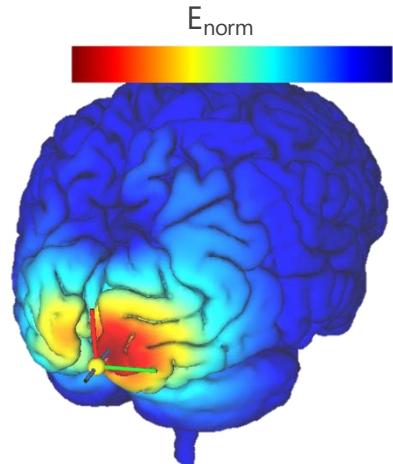
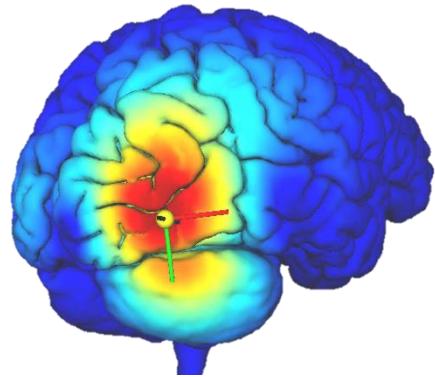
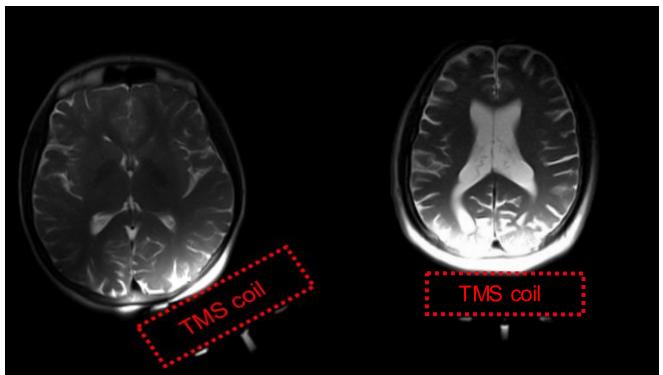


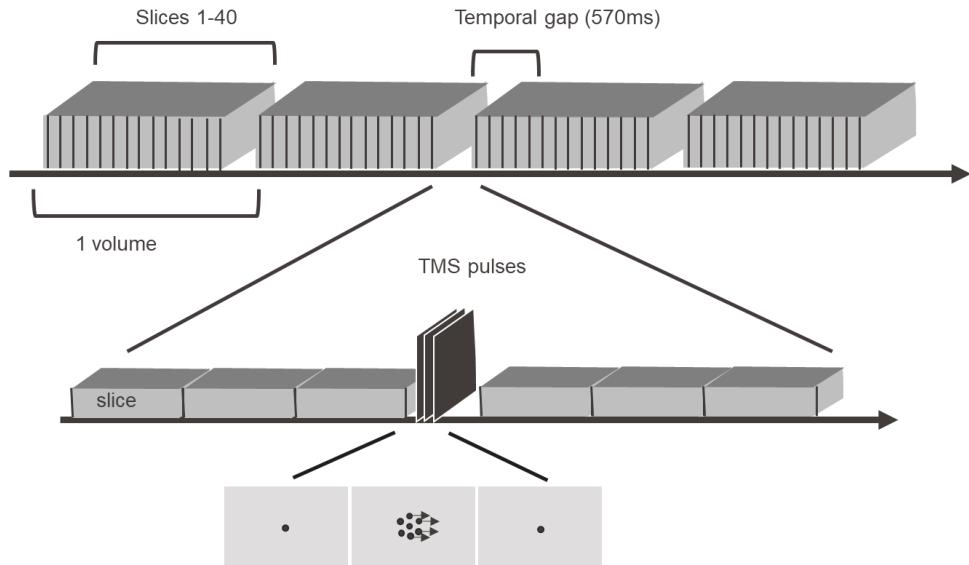
Friedhelm C. Hämmerle







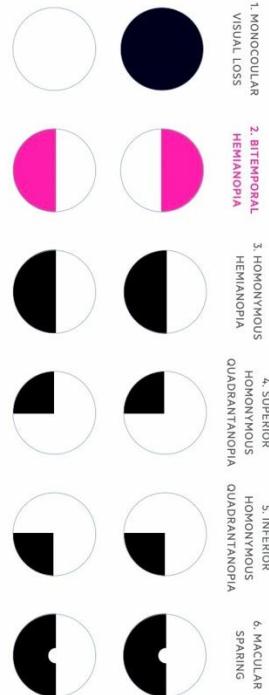
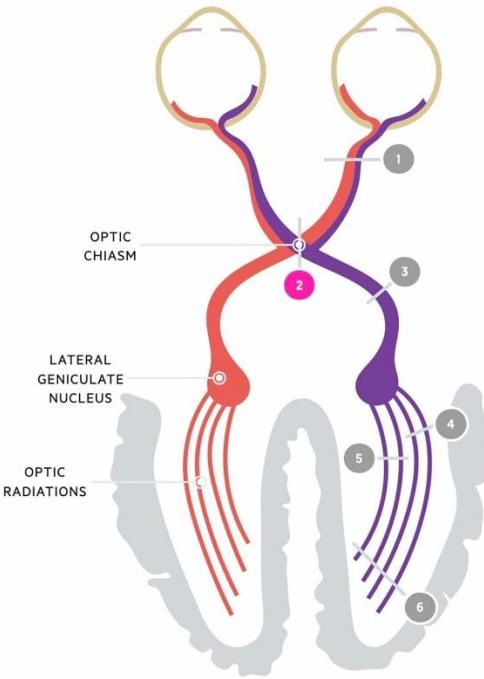
TMS_(V1)TMS_(MT)

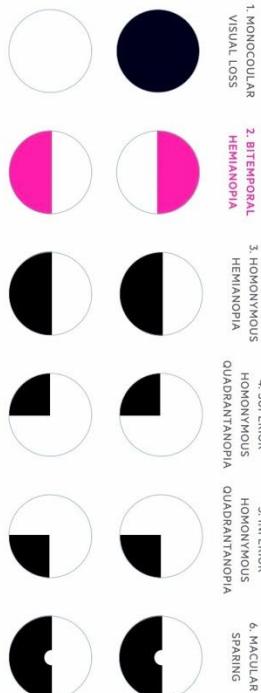
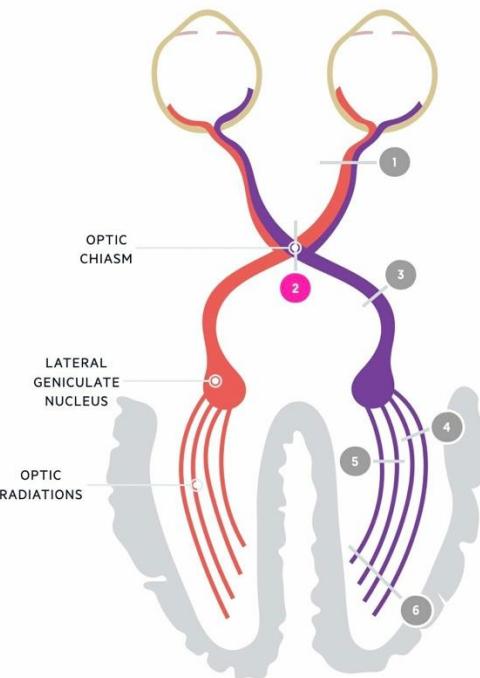
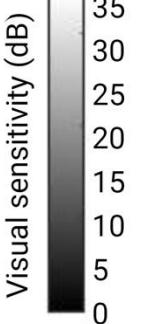
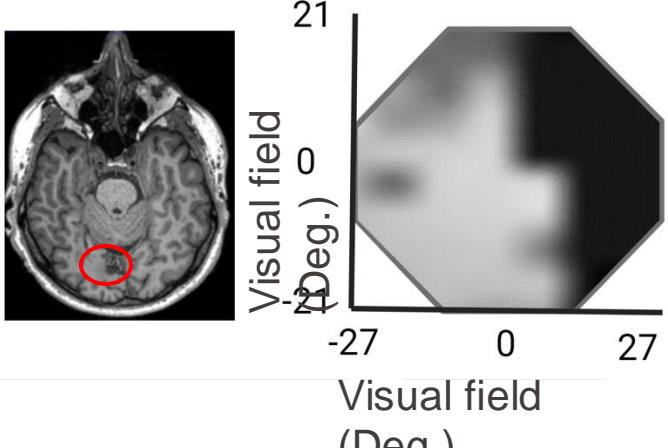


Visual field defects

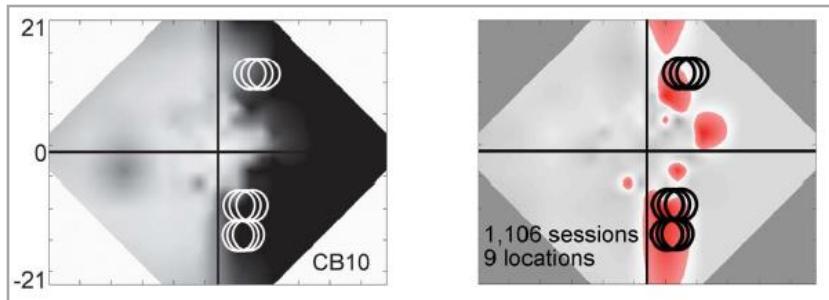
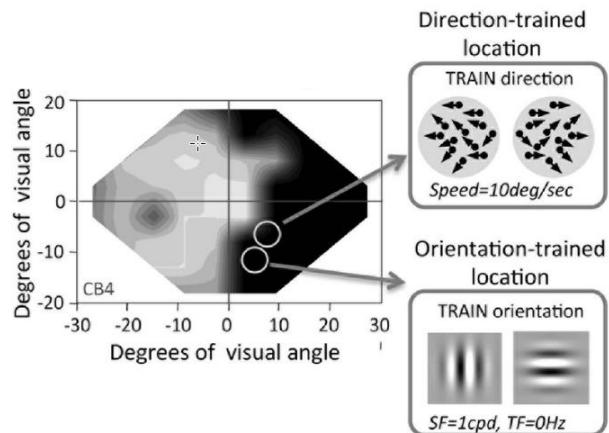




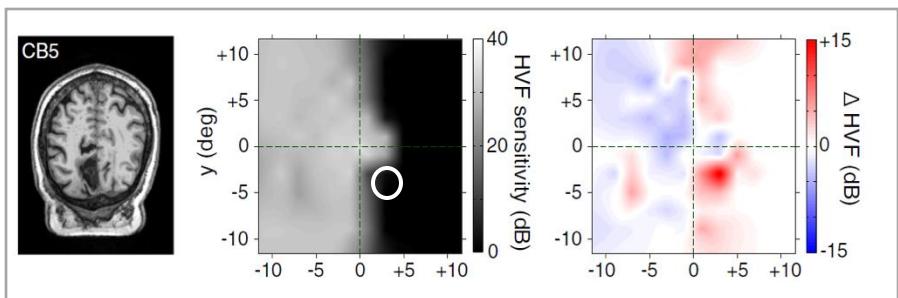




Visuo-attentional training

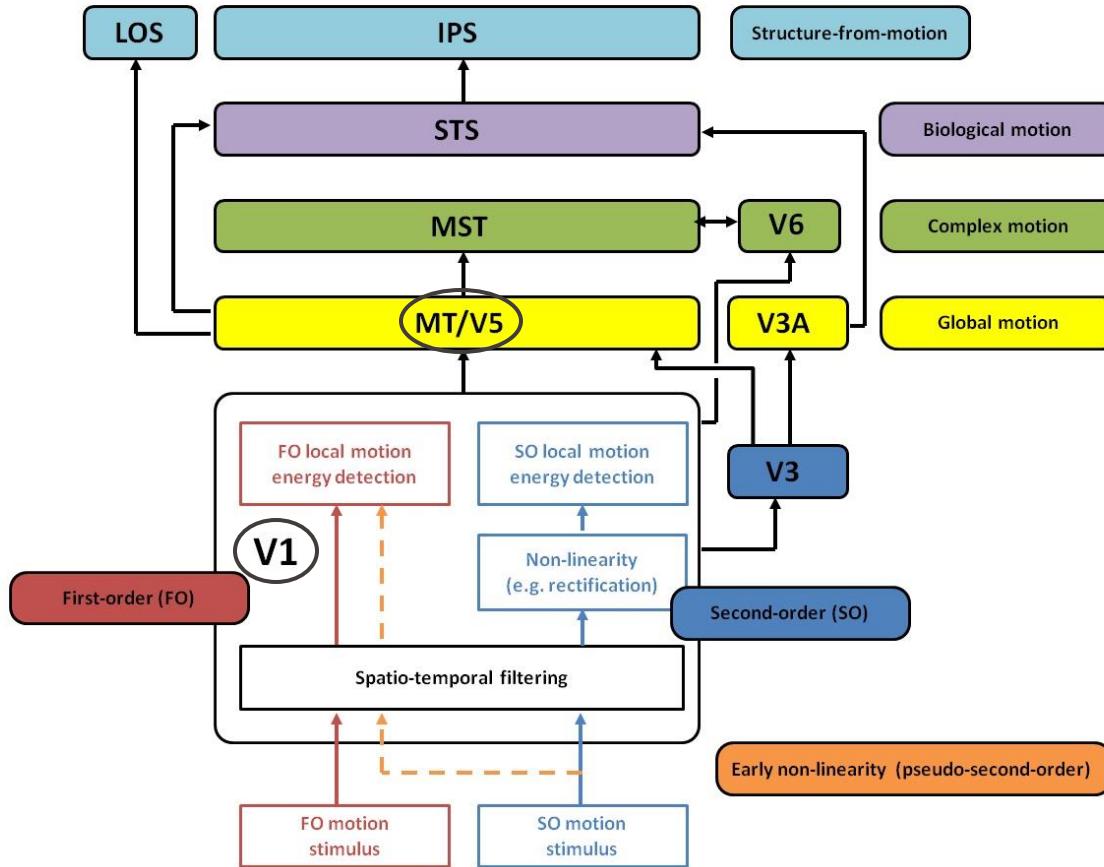


Cavaunaugh and Huxlin *et al.*, 2017, *Neurology*



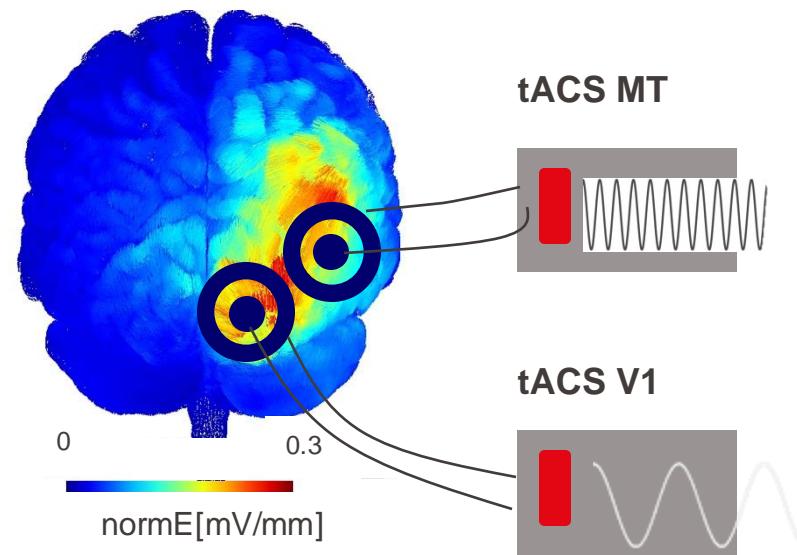
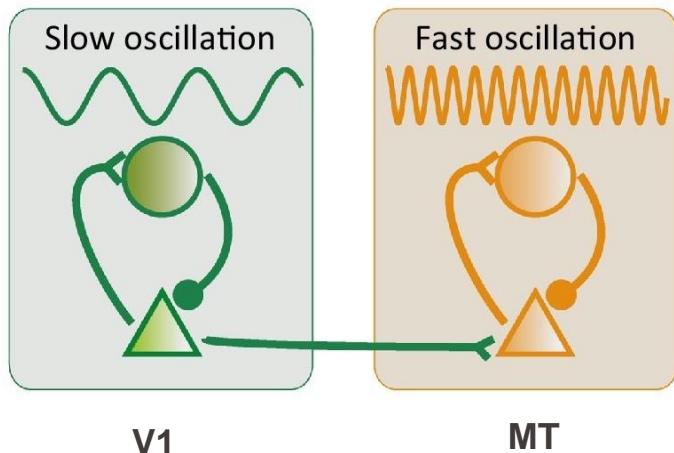
Barbot *et al.*, 2021, *J Neurosci*.

The motion processing hierarchy

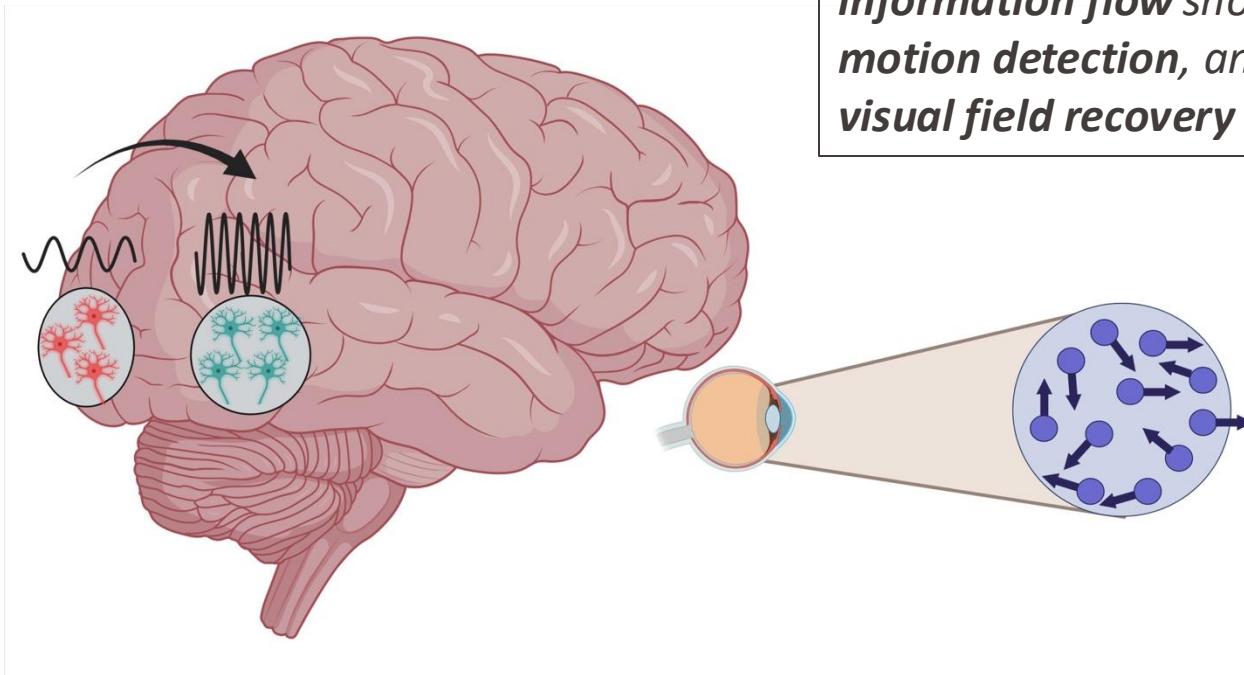


How to promote inter-areal communication?

Inter-regional Phase-Amplitude Coupling (PAC)
reflects **unidirectional coupling**

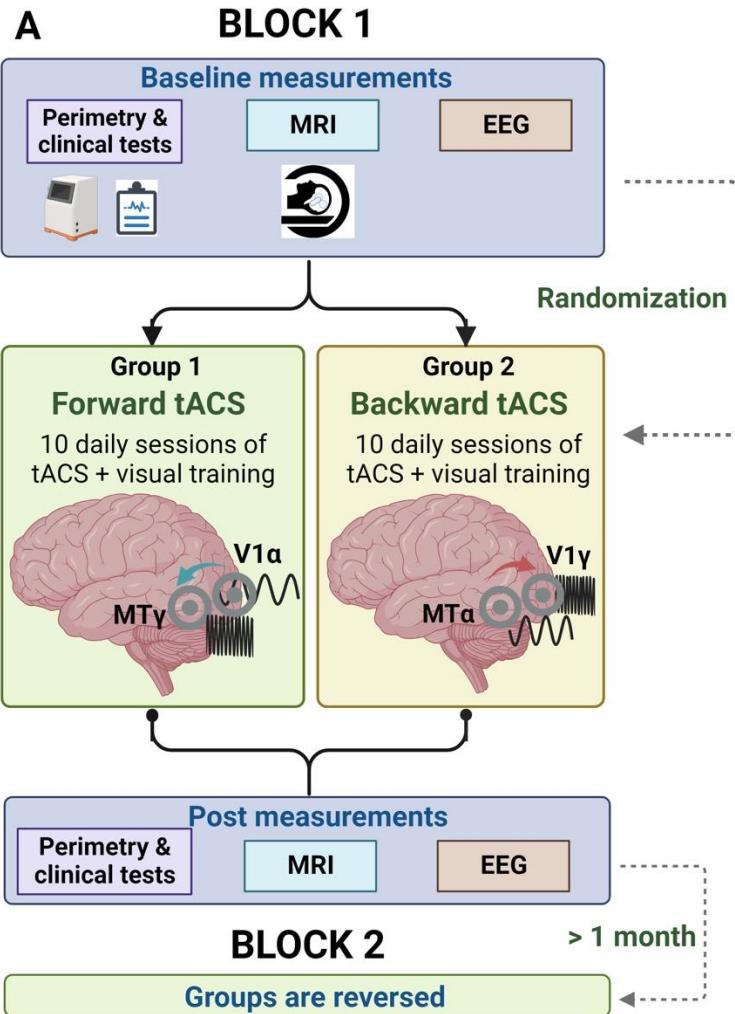


Hypothesis



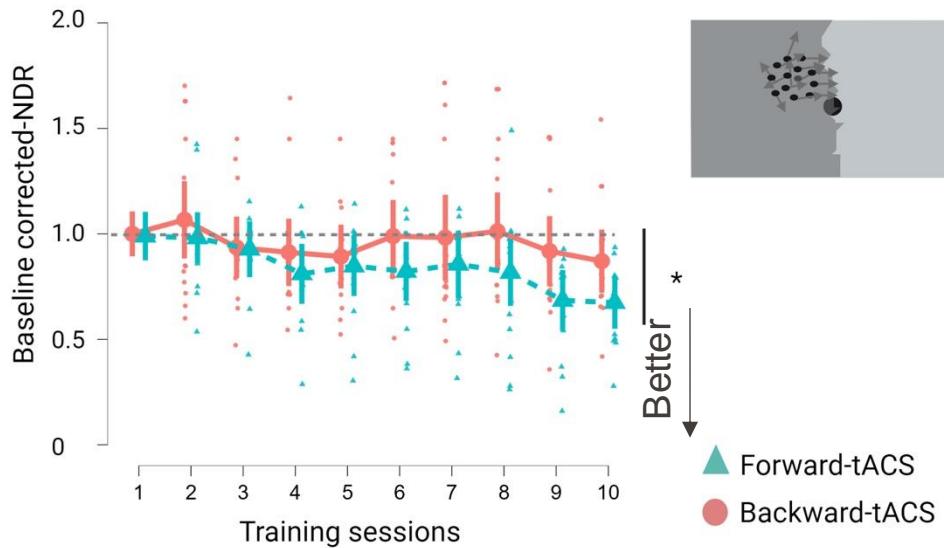
Promoting bottom-up direction of information flow should facilitate motion detection, and in turn, boost visual field recovery

Experimental design

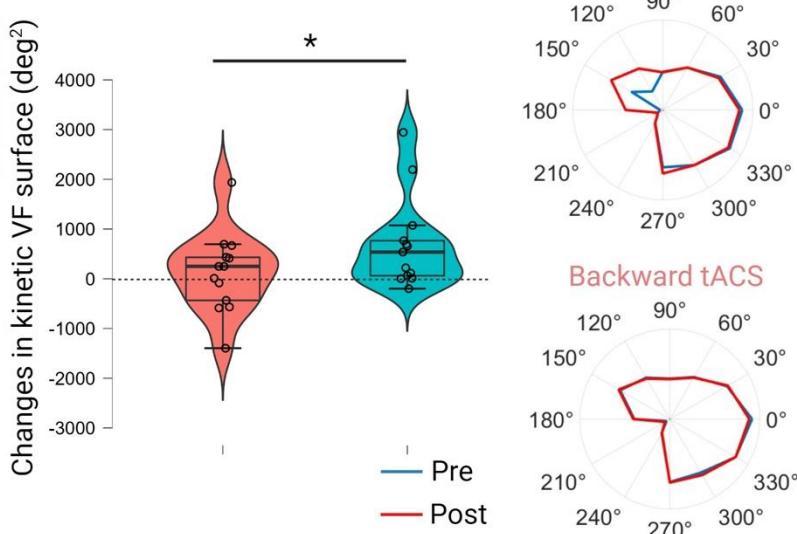


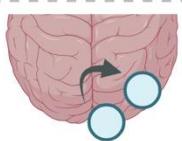
Results

A. Daily motion discrimination performances

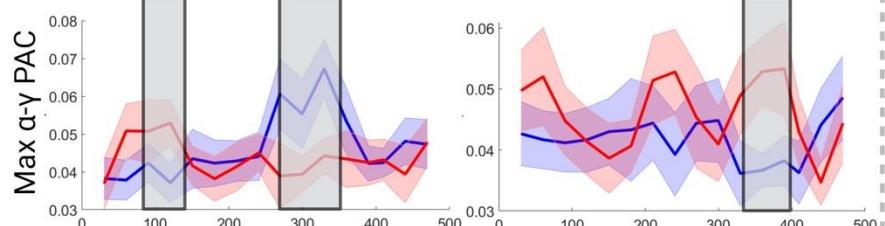
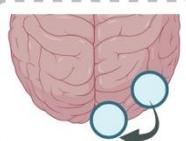
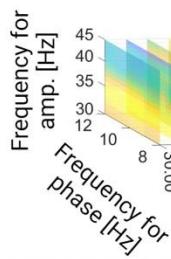
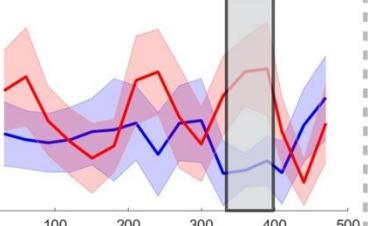


B. Kinetic visual field maps

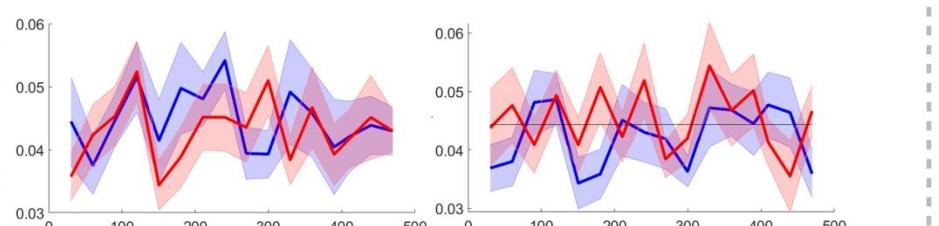
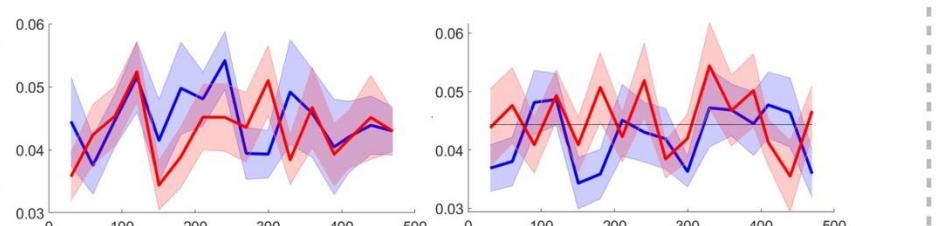




Forward tACS

V1 α phase-MT γ amplMT α phase-V1 γ ampl

Backward tACS

V1 α phase-MT γ amplMT α phase-V1 γ ampl

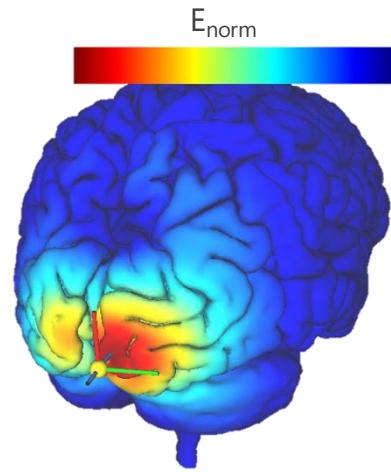
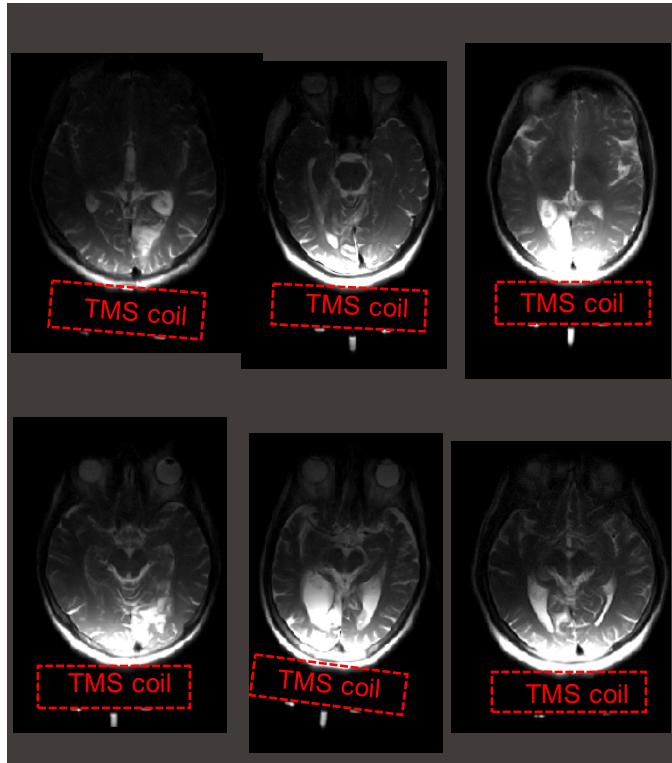
Pre
Post

Post-Pre differences
Modulation index

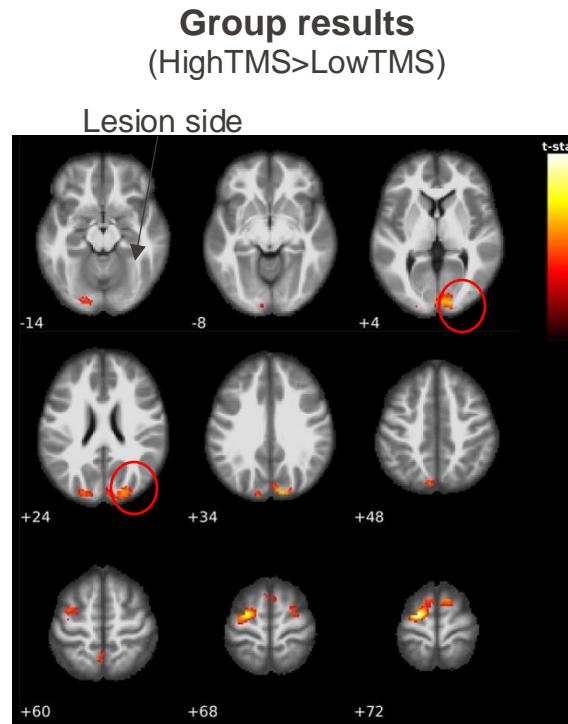
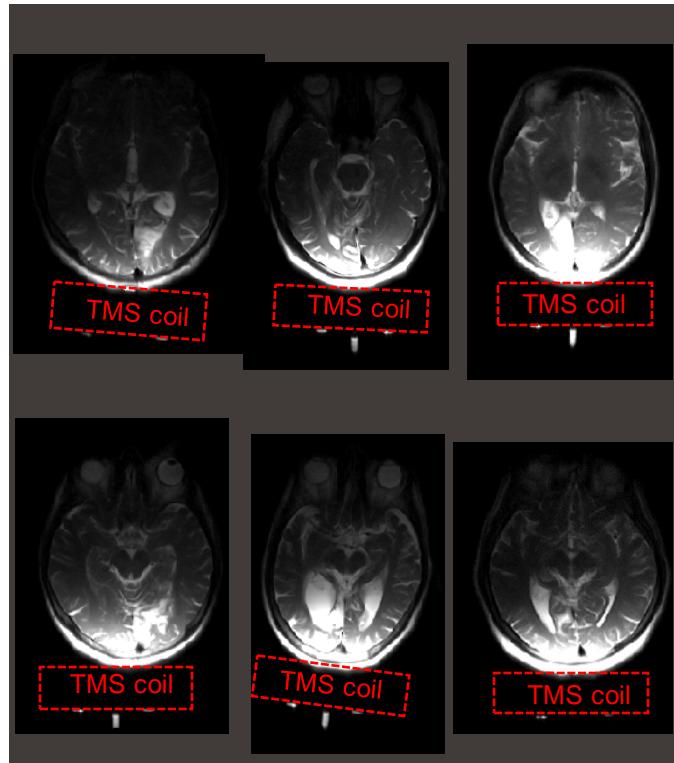
Does V1 reactivity predict recovery?



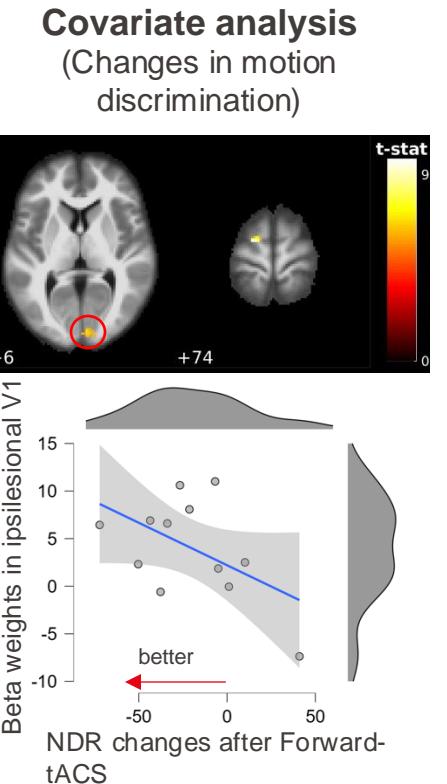
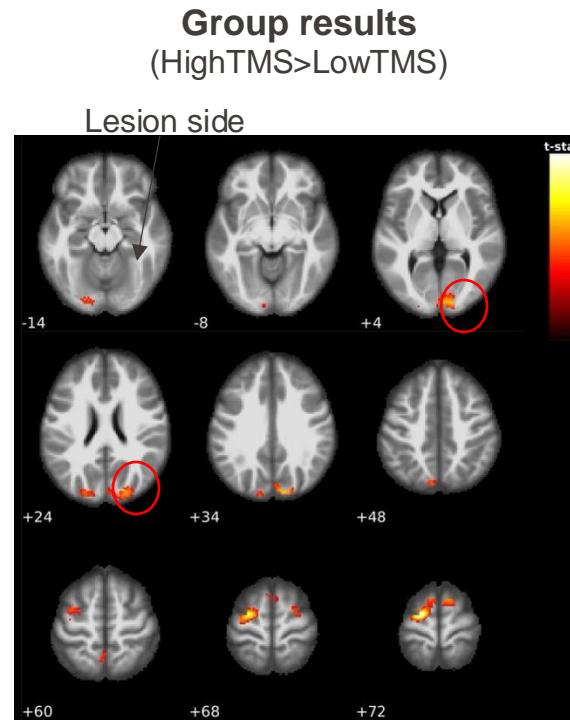
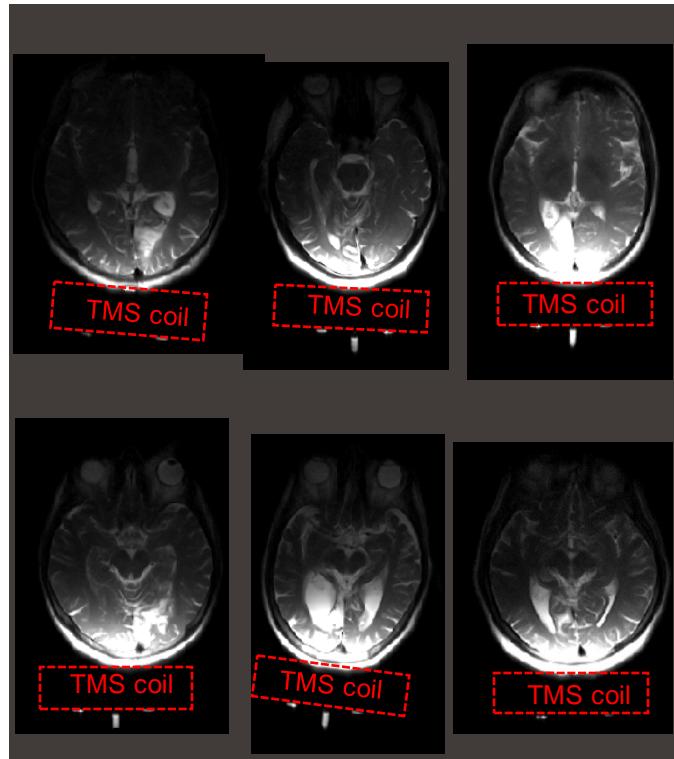
Does V1 reactivity predict recovery?



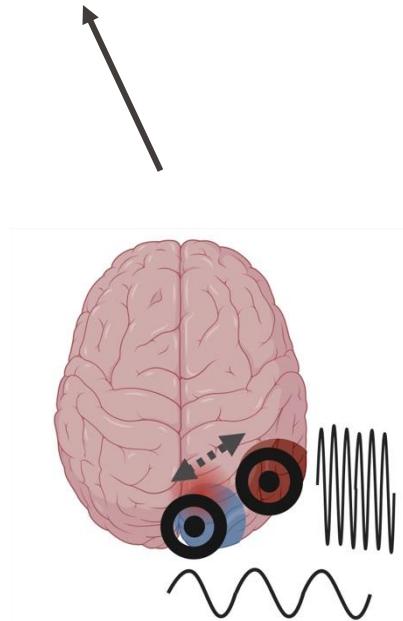
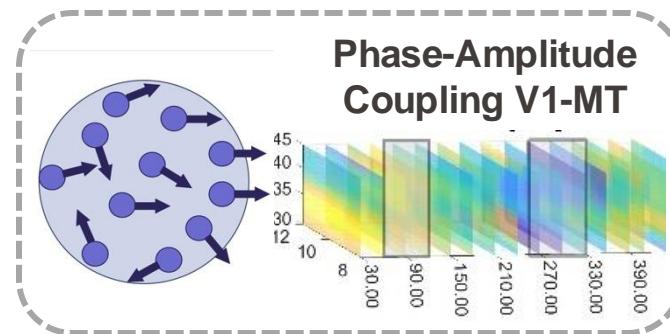
Does V1 reactivity predict recovery?



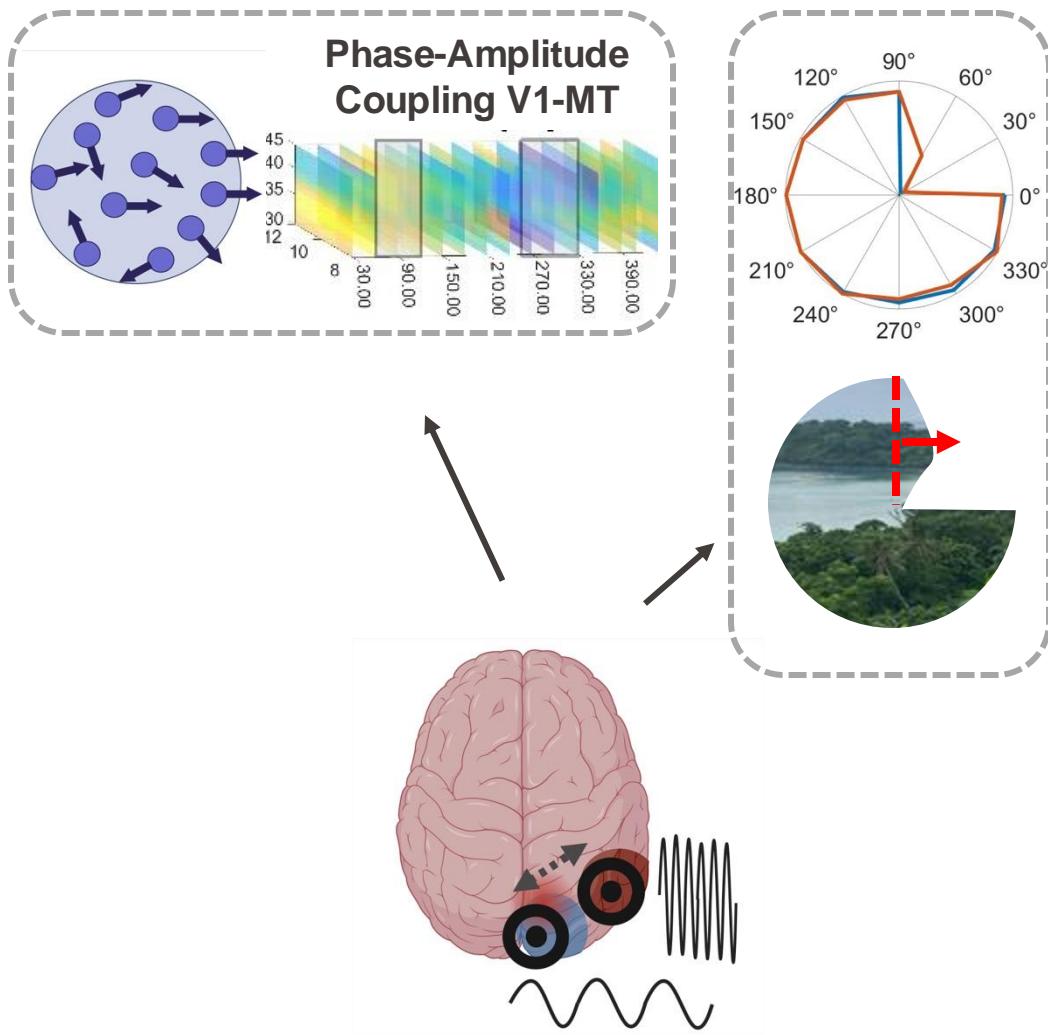
Does V1 reactivity predict recovery?



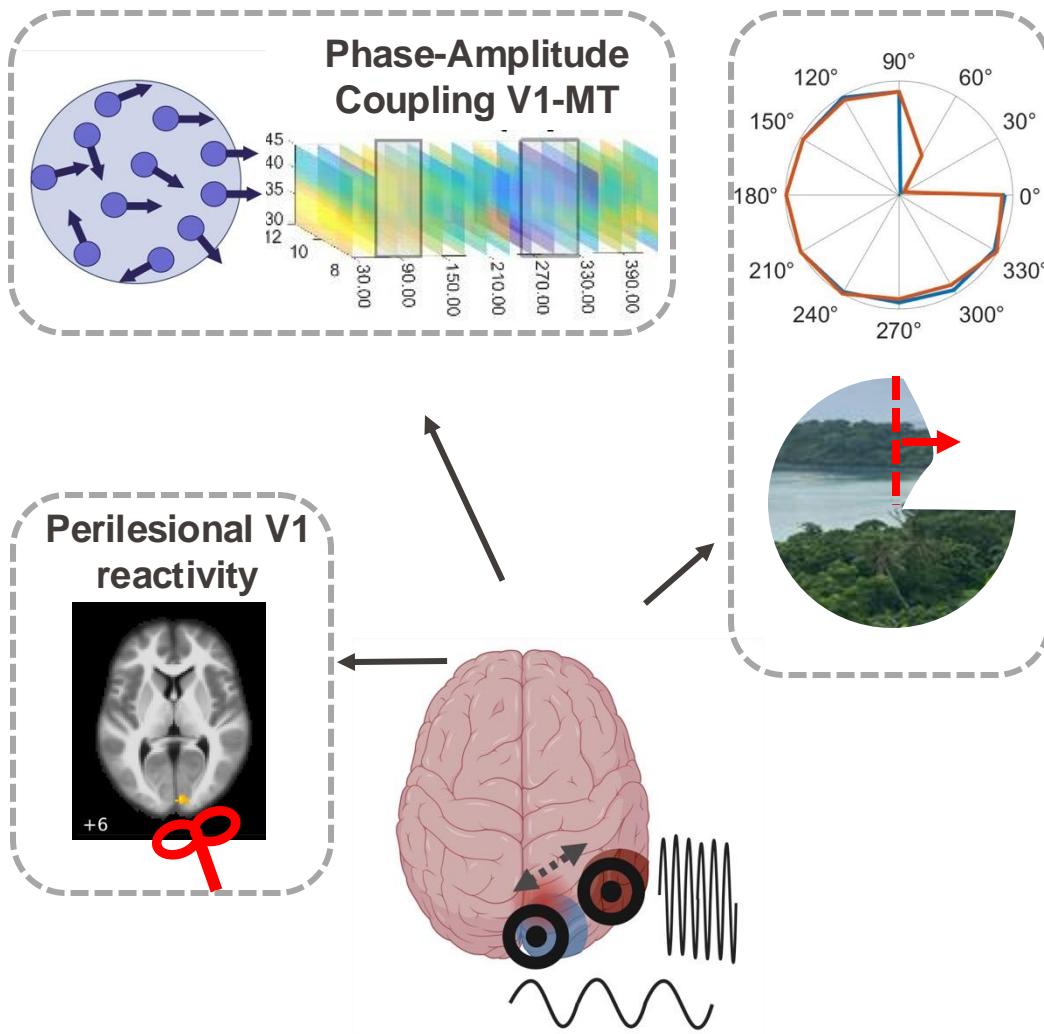
- The pathway and direction-dependent tACS protocol **improves motion processing in the blind field**
 - Changes in bi-directional cross-frequency V1-MT interactions
 - More efficient pathway-dependent processing

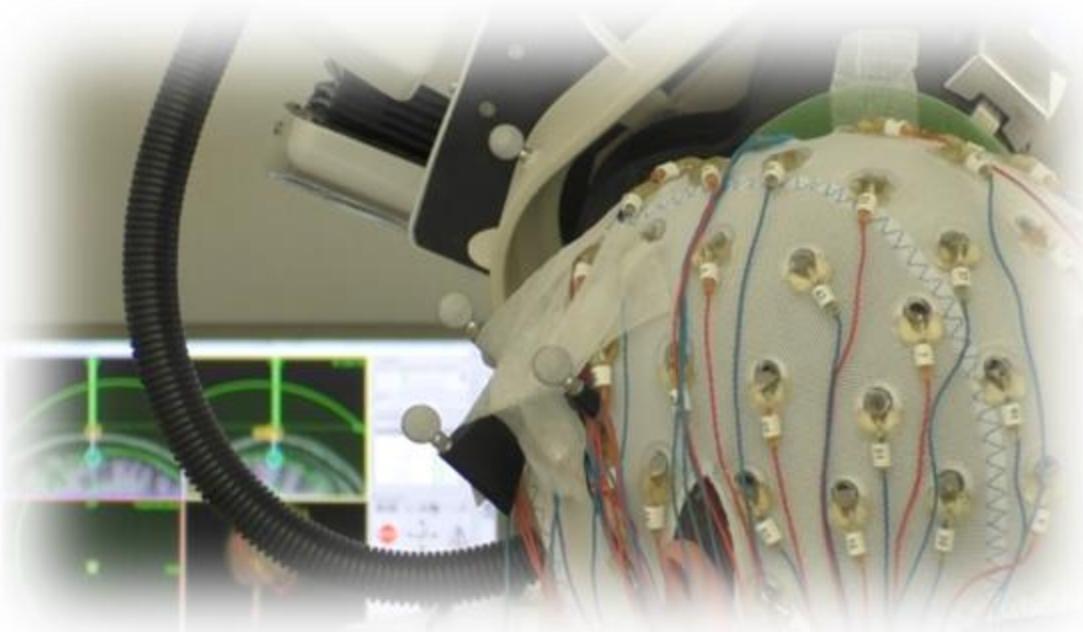
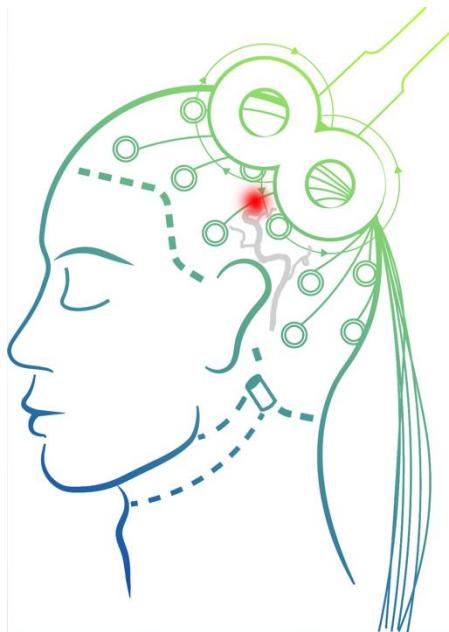


- The pathway and direction-dependent tACS protocol **improves motion processing in the blind field**
 - Changes in bi-directional cross-frequency V1-MT interactions
 - More efficient pathway-dependent processing
- and **enlarges visual field borders**



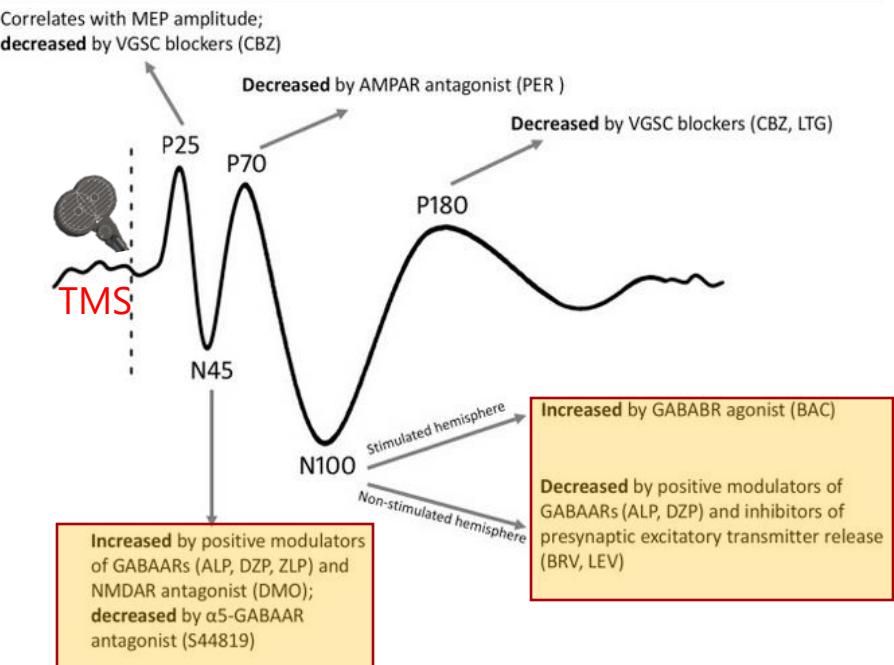
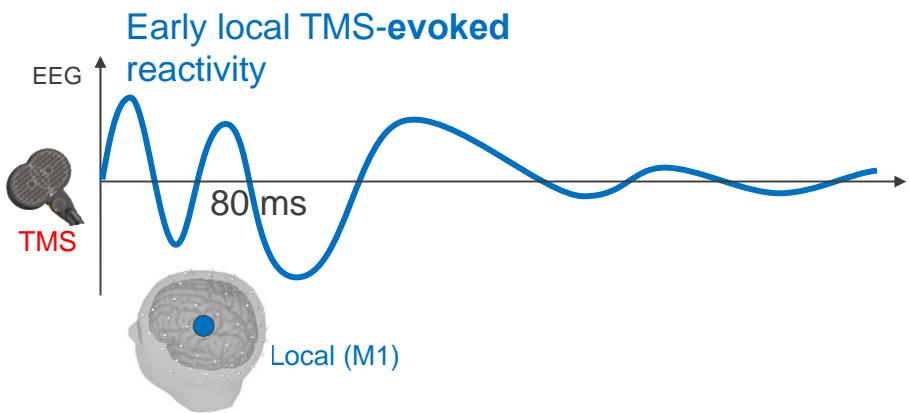
- The pathway and direction-dependent tACS protocol **improves motion processing in the blind field**
 - Changes in bi-directional cross-frequency V1-MT interactions
 - More efficient pathway-dependent processing
- and **enlarges visual field borders**
- was predicted by **more perilesional V1 activity** in response to TMS at baseline

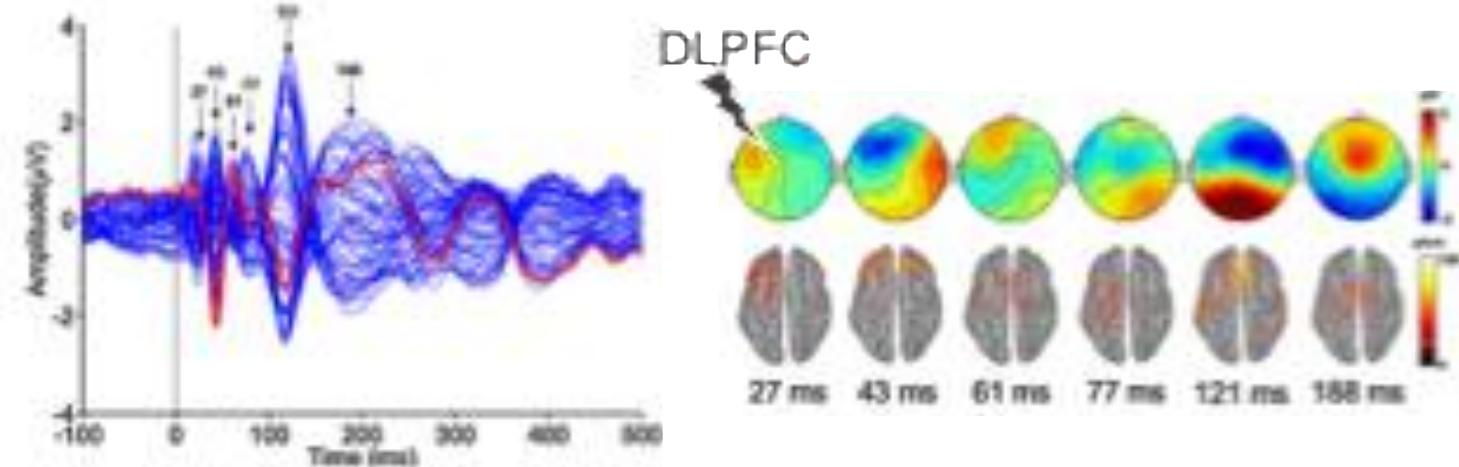




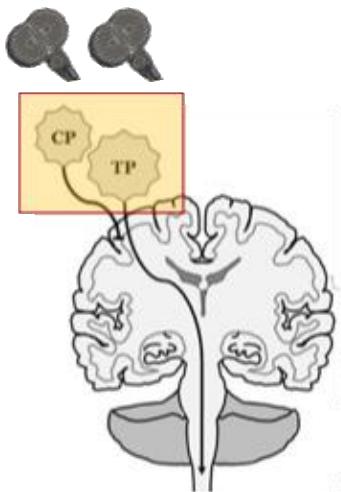


Friedhelm C. Hämmerle

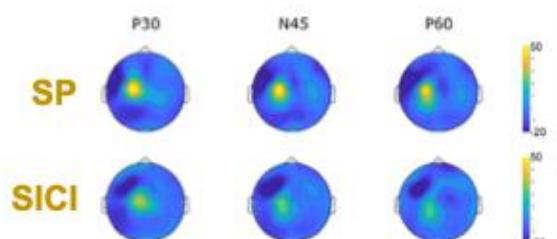
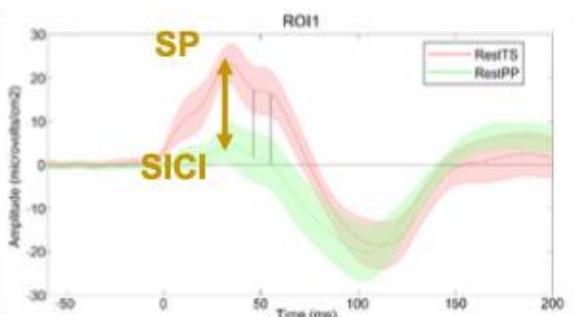




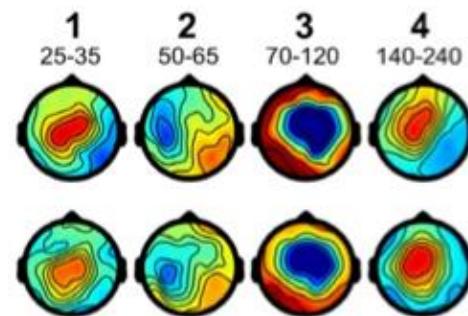
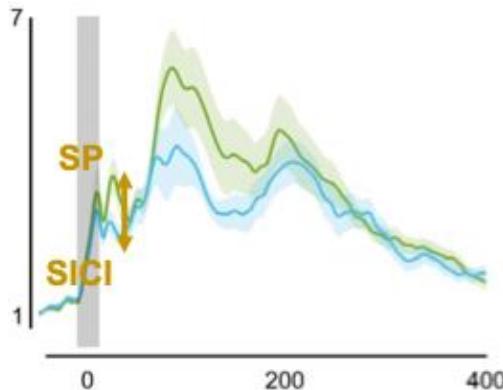
TEPs = local activity + remote connectivity



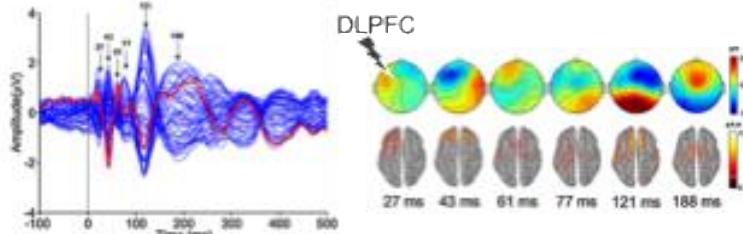
Short-Interval Cortical inhibition (SICI)



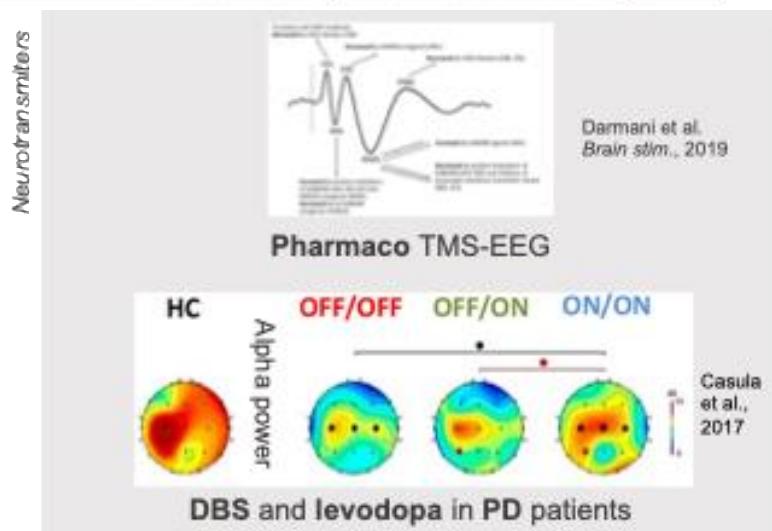
Leodori *et al.*, 2019



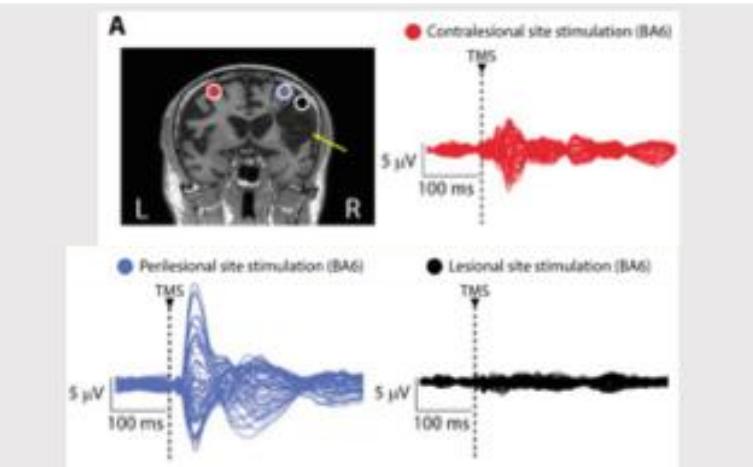
Raffin & Harquel *et al.*, 2020



TEPs = local activity + remote connectivity

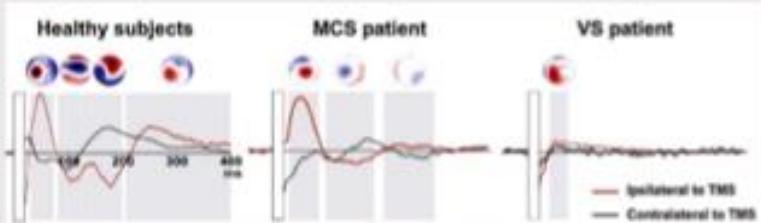


Clinical



Cortical reactivity after focal injury

Sarasso et al., *Brain*, 2020



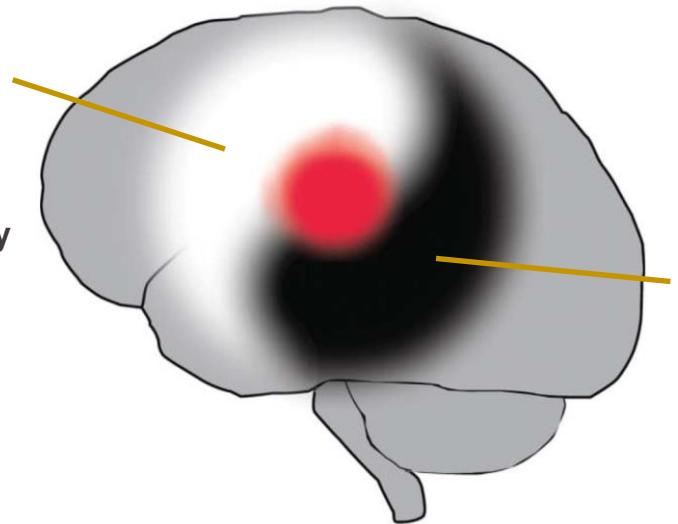
Impairment of reactivity and connectivity in vegetative state patients

Ragazzoni et al., *PLOS One*, 2013

Animal Models

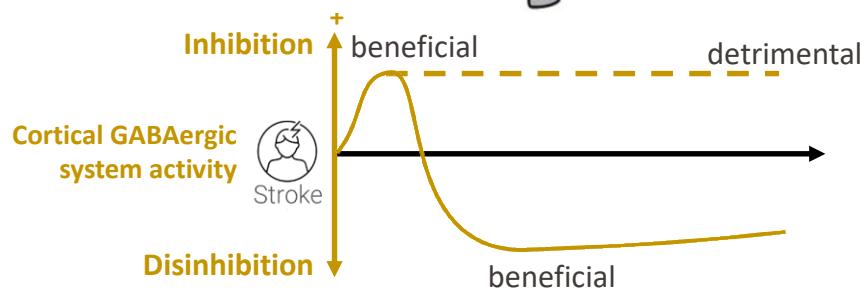
- Tonic Hyperinhibition
- Low excitability

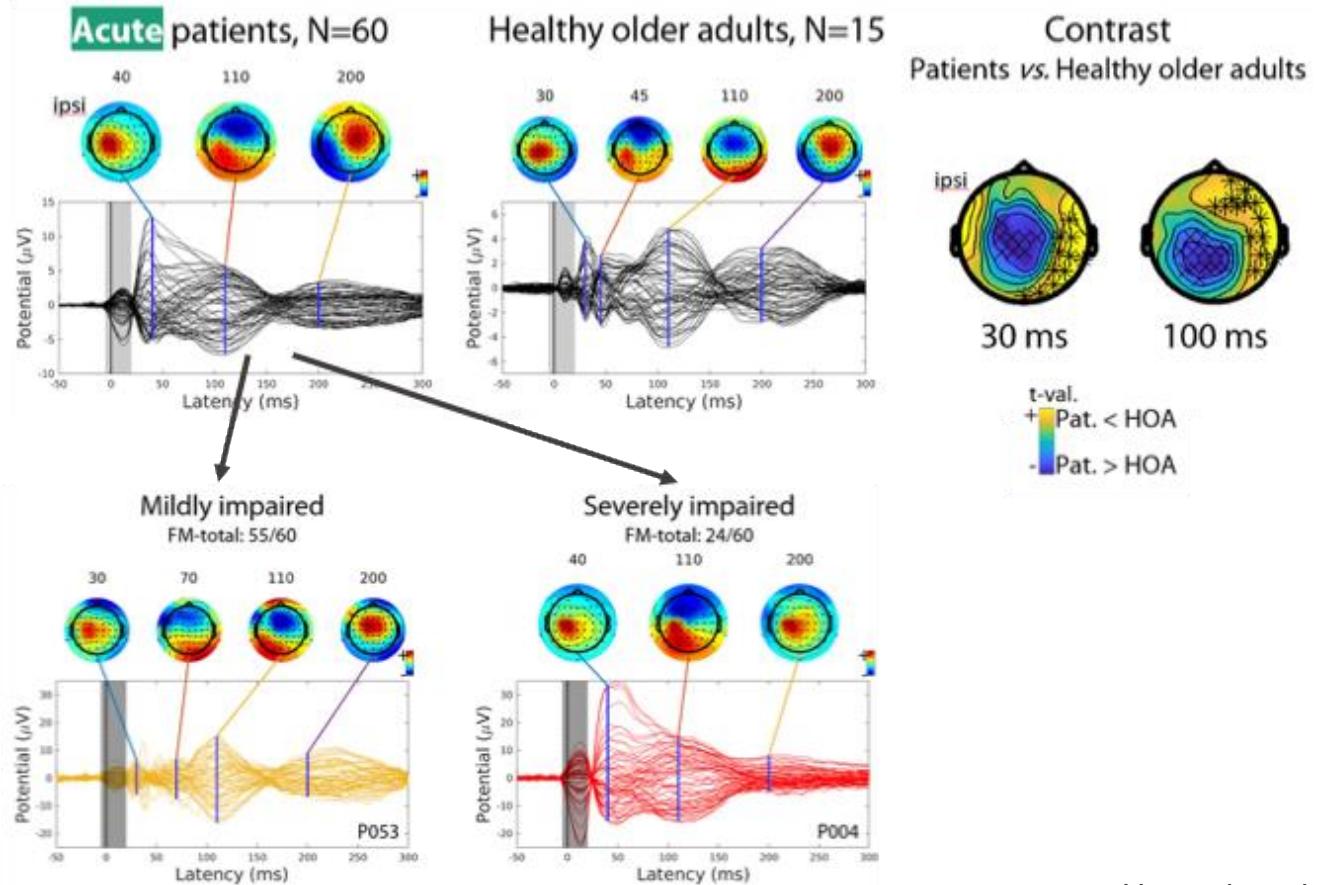
-> **Beneficial** for preventing **excitotoxicity**



- Hyperexcitability
- Decrease of tonic inhibition

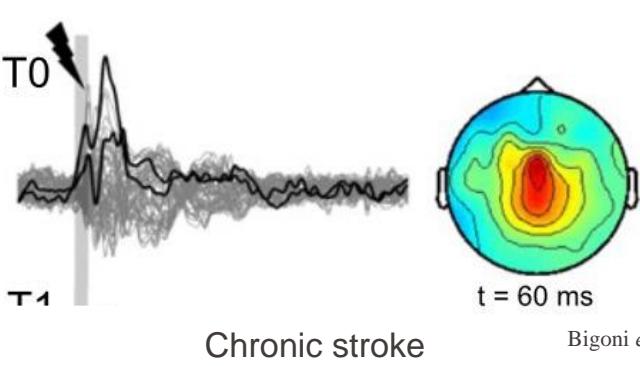
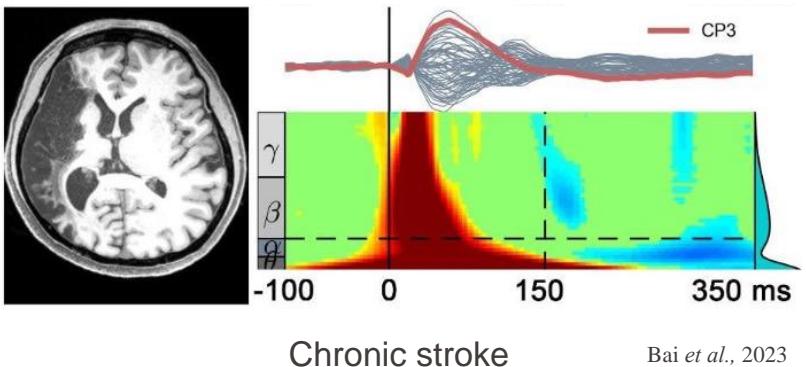
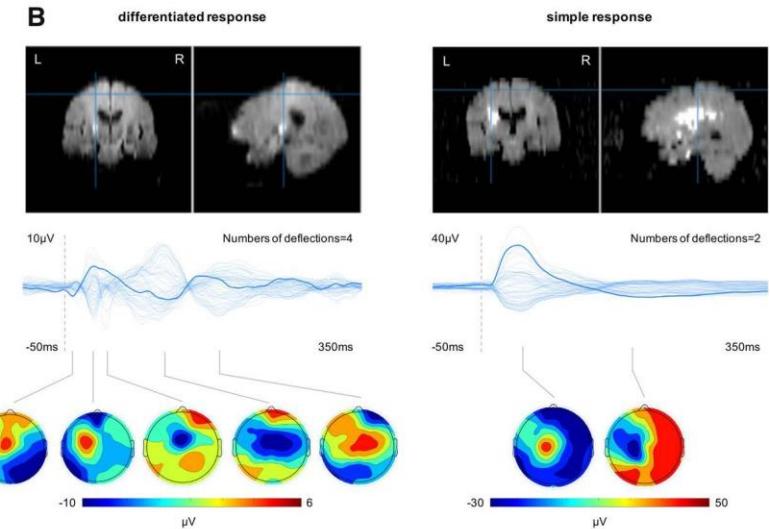
-> **Beneficial** for **plasticity**

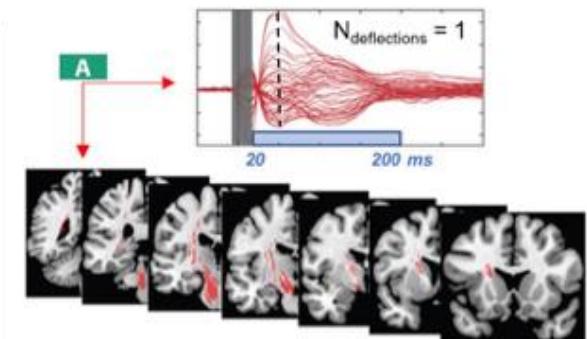




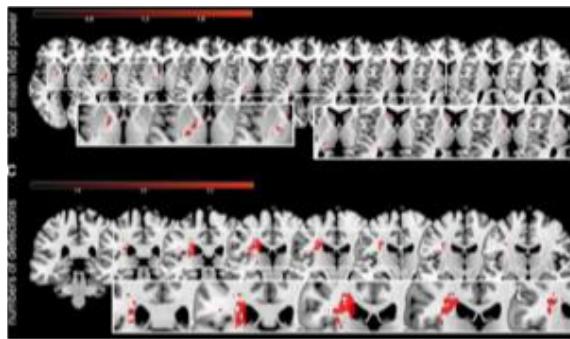


Stroke Patients

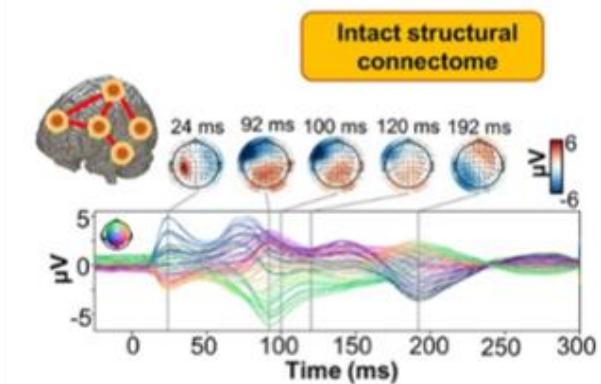




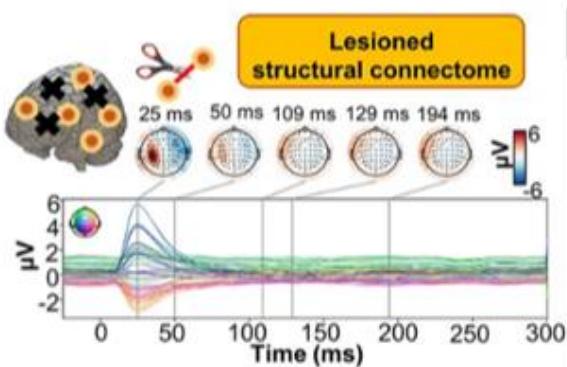
Internal capsule (TiMeS)

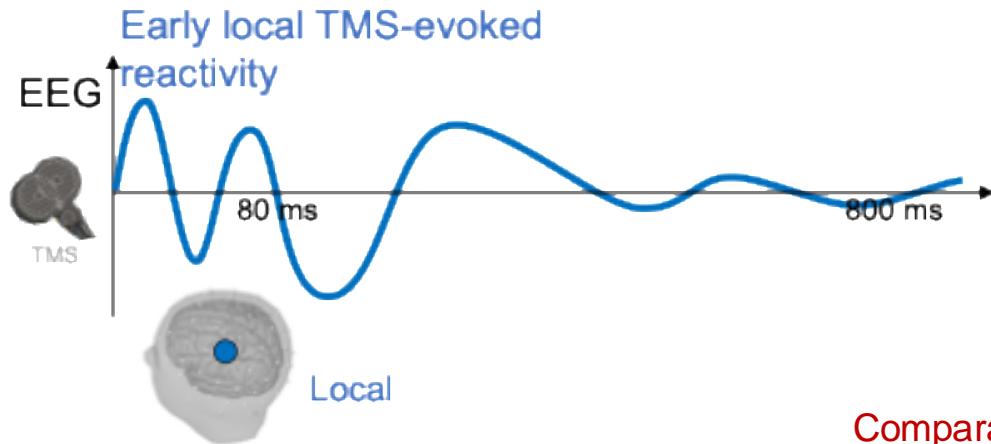


Internal capsule, caudate nucleus
(Tscherpel *et al.*, 2020)

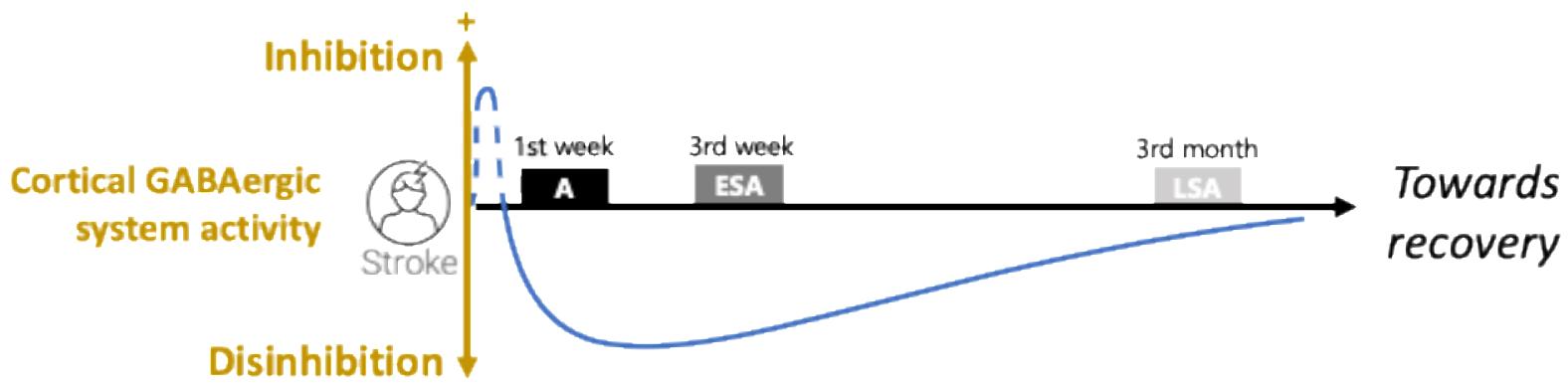


Computational modelling (Momi *et al.*, 2023)





Comparable to animal work





ELSEVIER

Contents lists available at [ScienceDirect](#)

Clinical Neurophysiology

journal homepage: www.elsevier.com/locate/clinph

Review

Clinical utility and prospective of TMS-EEG

Sara Tremblay ^{a,b,*}, Nigel C. Rogasch ^c, Isabella Premoli ^d, Daniel M. Blumberger ^a,
Silvia Casarotto ^e, Robert Chen ^f, Vincenzo Di Lazzaro ^g, Faranak Farzan ^h, Fabio Ferrarelli ⁱ,
Paul B. Fitzgerald ^{j,k}, Jeanette Hui ^a, Risto J. Ilmoniemi ^l, Vasilios K. Kimiskidis ^m,
Dimitris Kugiumtzis ⁿ, Pantelis Lioumis ^a, Alvaro Pascual-Leone ^o, Maria Concetta Pellicciari ^p,
Tarek Rajji ^a, Gregor Thut ^q, Reza Zomorrodi ^a, Ulf Ziemann ^r, Zafiris J. Daskalakis ^a





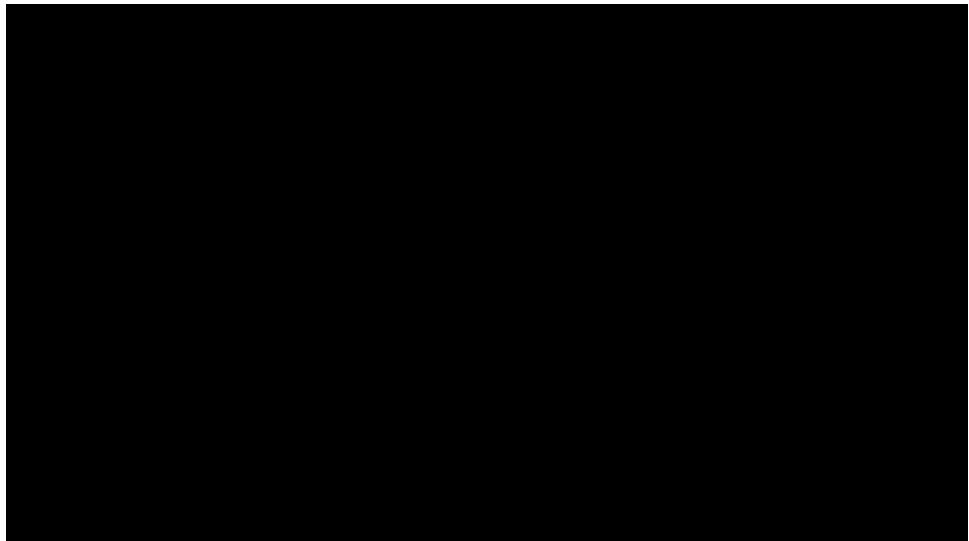
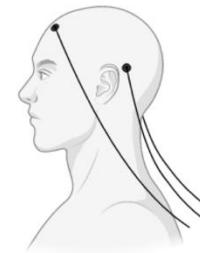
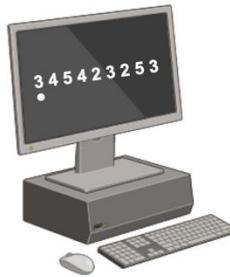
nature neuroscience

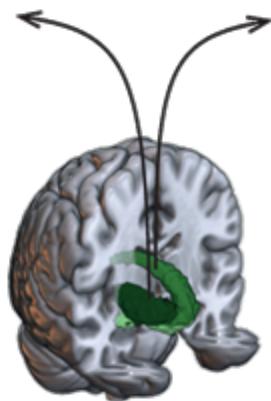
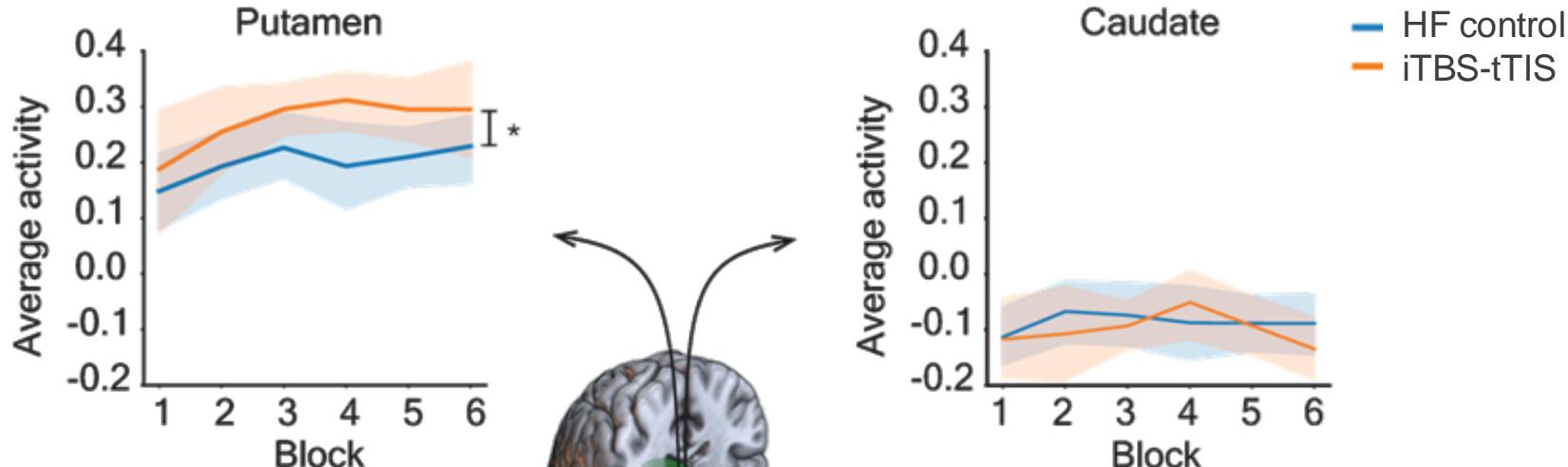
a

Article

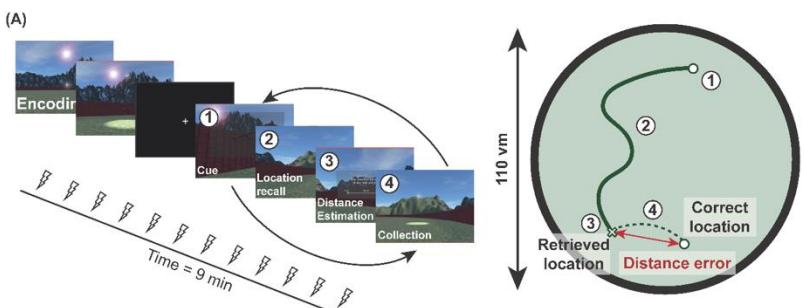
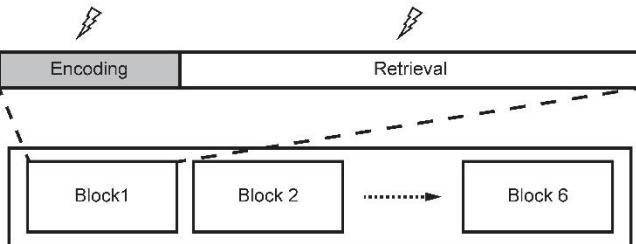
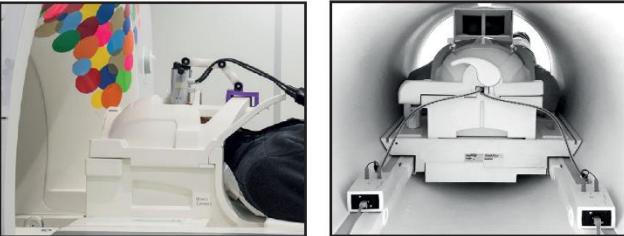
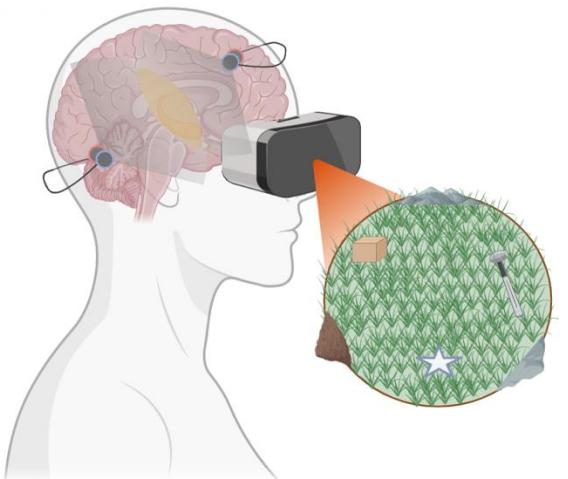
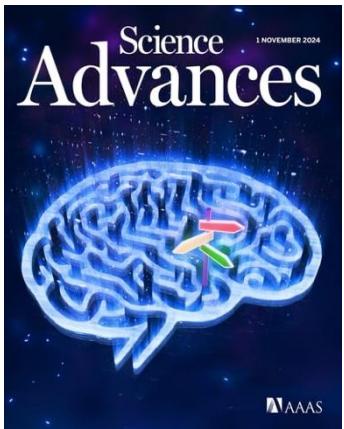
<https://doi.org/10.1038/s41593-023-01457-7>

Noninvasive theta-burst stimulation of the human striatum enhances striatal activity and motor skill learning

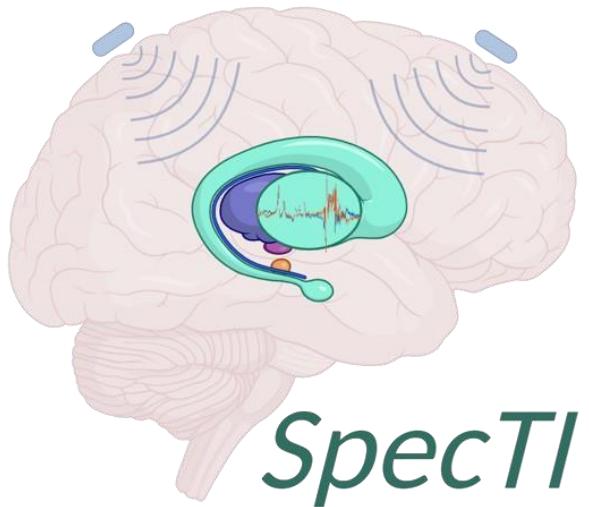
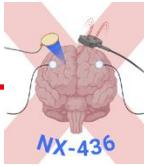
Wessel, Beanato *et al.* 2023



Stimulation effects are specific to the subregion already involved in the task

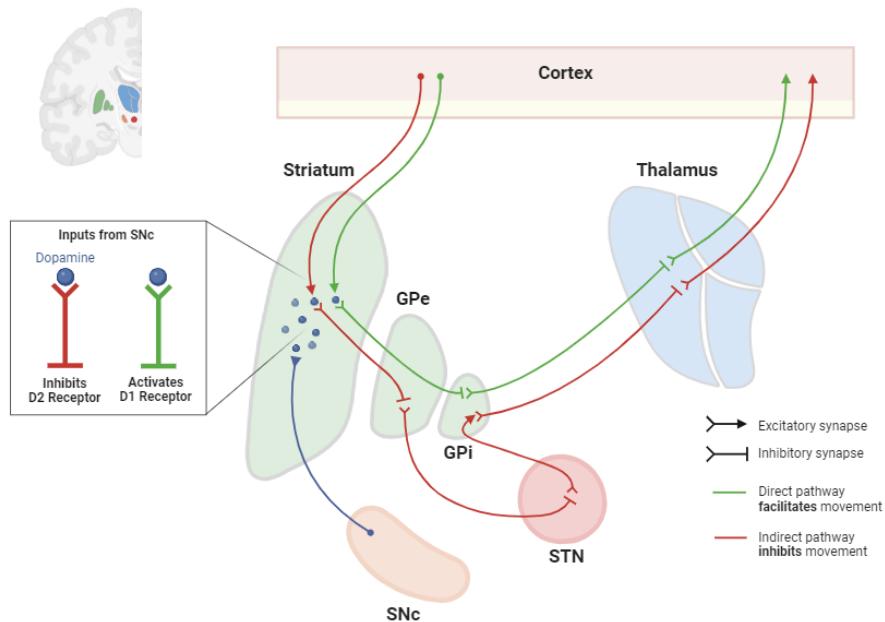
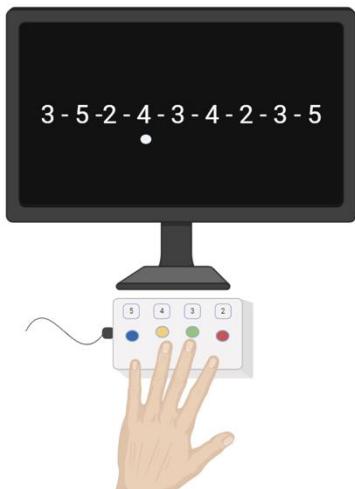


Beanato, Moon et al. 2024. *Science Advances*



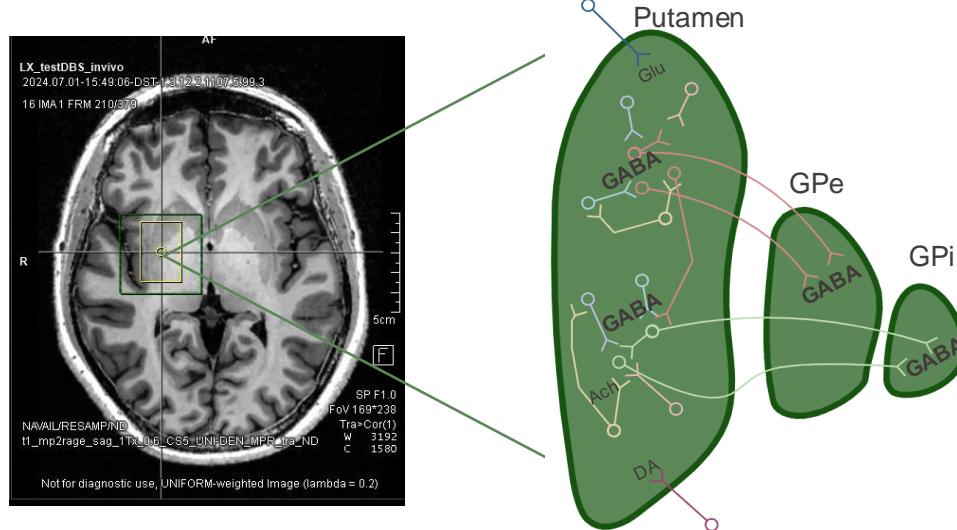


- How does striatal tTIS modulate neuromodulator levels in the putamen?
- How does this differ when performing a motor learning task?



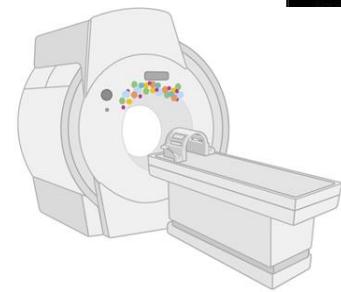
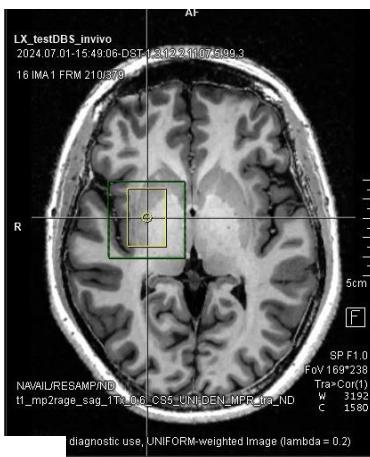


- Majority of neurons in Putamen are GABAergic
 - Medium spiny projection neurons
 - GABAergic Interneurons

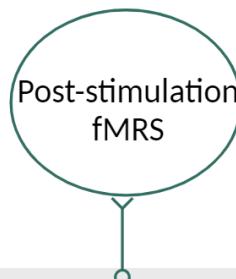
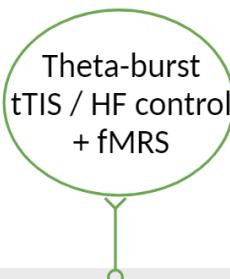
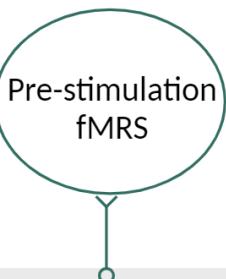




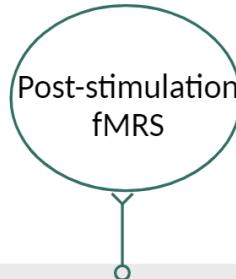
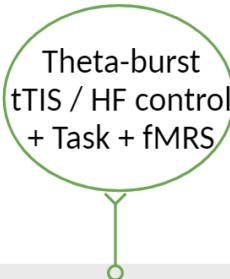
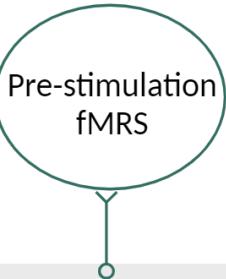
- Record functional MR spectroscopy of the Putamen at 7T

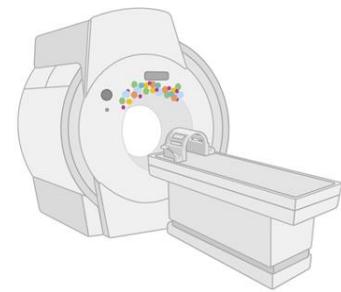
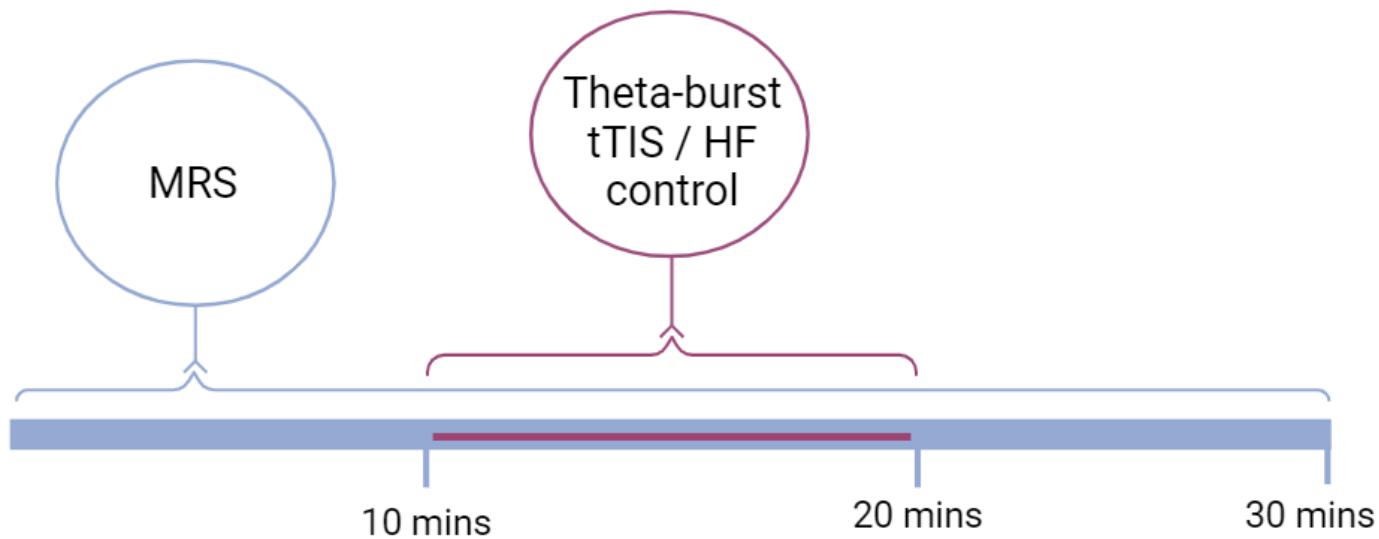


Resting state



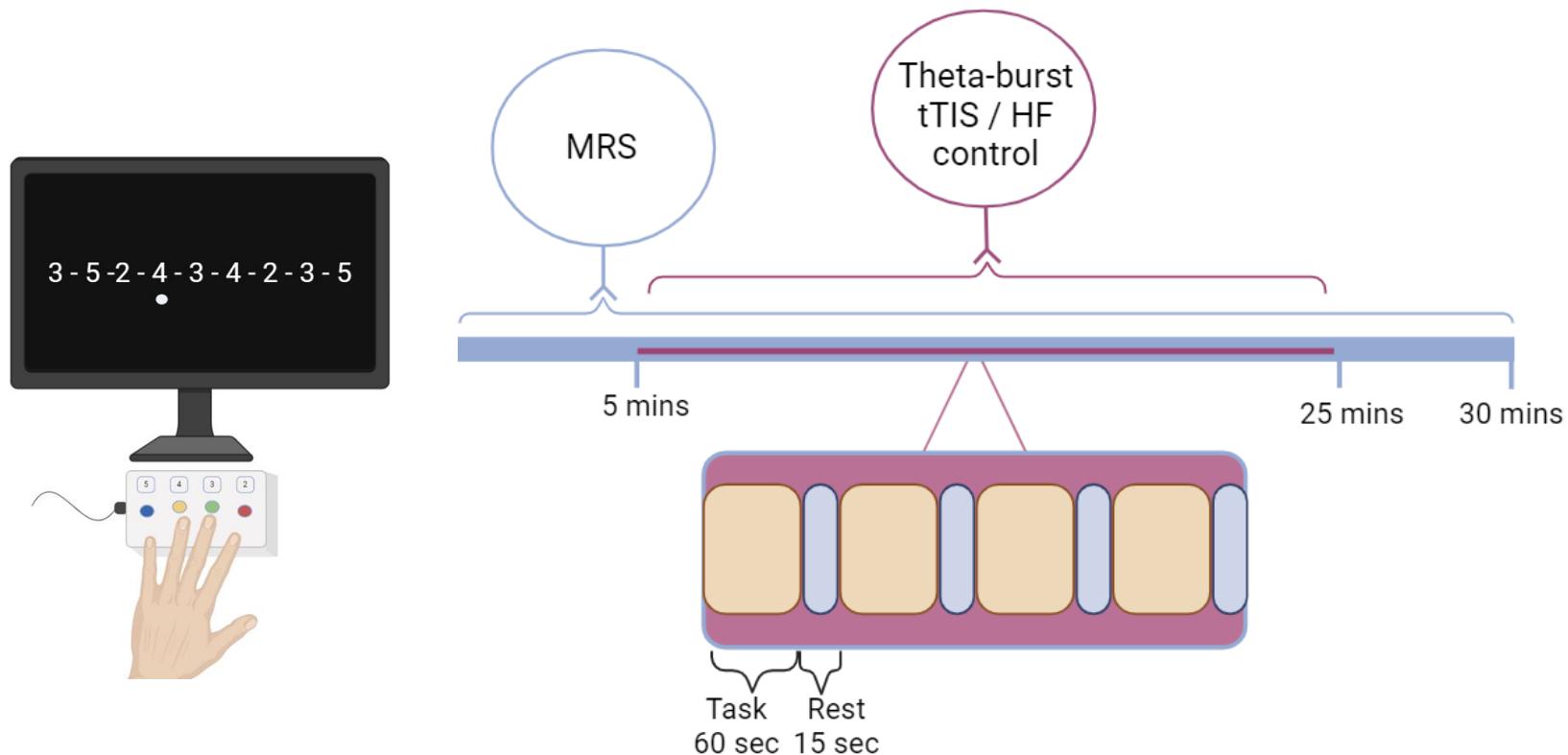
Task-based

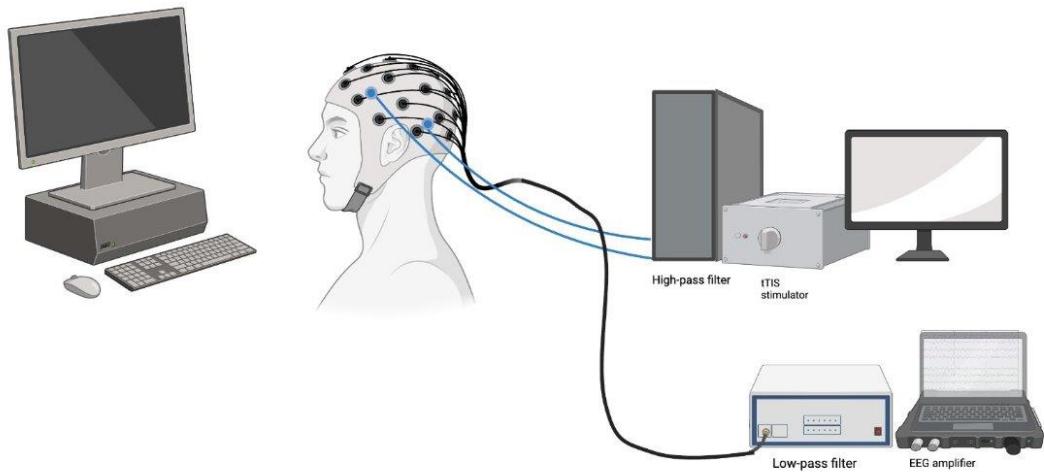


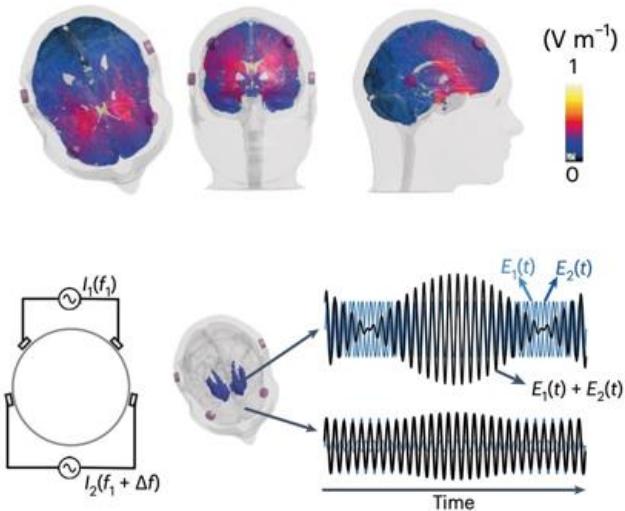




- Sequential finger tapping task to motor learning







Temporal Interference (TI) Stimulation uses two electric fields at frequencies f_1 and f_2 to stimulate the brain at the difference frequency ($|f_1-f_2|=\Delta f$), which lies within the range of brain activity, non-invasively.

'Pulsed Temporal Interference' uses two electric fields at frequencies, f_1 and f_2 , and periodically switch a particular field to $f_2 + \Delta f$ in a timed, pulsed manner (i.e. in bursts).

Each electric field is generated by a constant current sources

Electric field modeling with striatal montage
Maximilian J. Wessel, Elena Beanato et al. 2023



What is the current hypothesis of how tTIS modulates brain activity?

Subthreshold stimulation that requires behavioral co-activation of the brain area of focus (rs- fMRI vs. task-based fMRI)

(Wessel, Beanato et al. 2023, Violante et al. 2023)

Disruptive effect on the underlying network oscillation pattern when applied in a continuous and not in a pulsed-stimulation pattern (it is not phase locked to the underlying oscillatory rhythm or the continuous stimulation masks the underlying network activity)

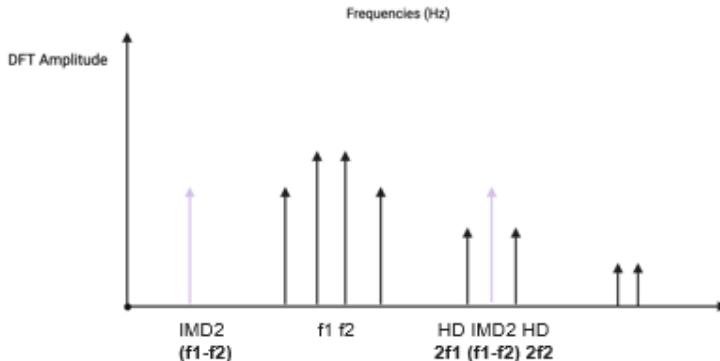
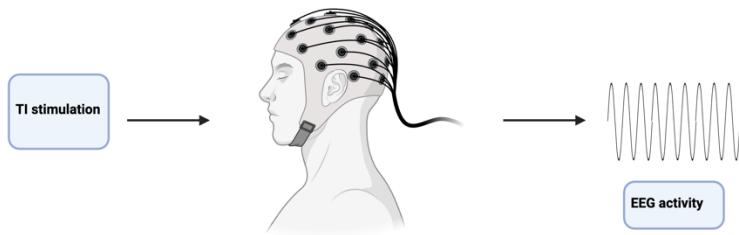
(Vassiliadis et al. 2024, Viera et al. 2024, Chenhao Yang et al. 2024)

At a cellular level, neuron can mix the high carrier frequencies and produces non-linear mixed products – new frequencies -

(Mirzakhalili et al. 2020)

Neuron is mixing exogenous and endogenous subthreshold membrane potential oscillations to create new oscillatory frequencies (Kinetics of voltage-gated sodium channels are non-linear)

(Luff et al. 2024)



Concurrent TI-EEG recording:

Advantages

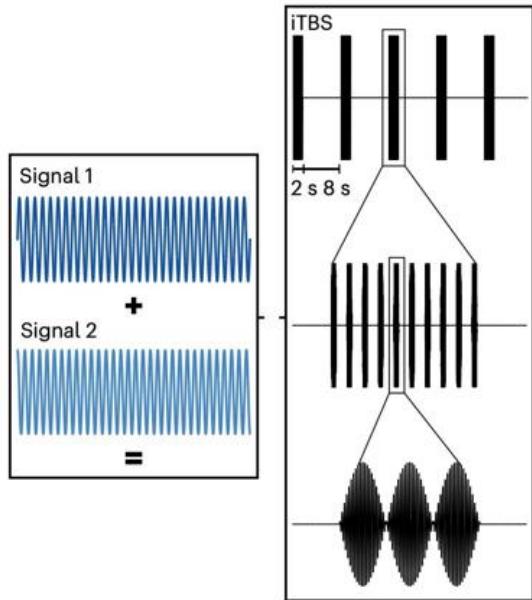
Continuous EEG recording during and after tTIS:

- Mechanistic understanding of tTIS effects on brain circuits with high temporal resolution
- Reveal sustained effects of tTIS during and after the experiment

Technical challenges

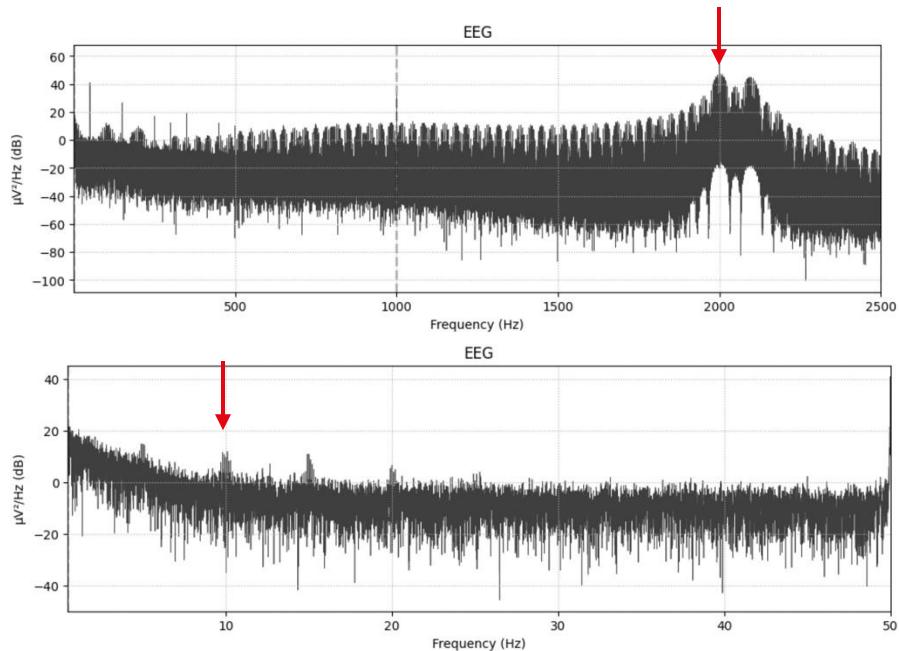
tTIS creates voltage potential that is above the limits of commercially available EEG amplifiers: **non-linear system**

EEG recording will be distorted by non-linear artefacts, as a result of the tTIS



Intermittent theta burst stimulation pattern
Maximilian J. Wessel, Elena Beanato et al. 2023

Example of stimulation artefacts



Red arrows: Carrier TI frequencies (2kHz, 2.1kHz), TI stimulation artefact at 5Hz (FFT)



Stimulation artefacts can be approximated by Taylor expansion:

Is an infinite sum of terms which represent an approximation of a function around a specific point on the function.

It allows any function (including non-linear ones, as long as it is infinitely differentiable) to be represented as the sum of terms scaled by the function's derivatives at a specific point (with approximation accuracy reducing the further one gets from the specified point)

A Maclaurin Series is the same thing as a Taylor Series but with the specified point around which to approximate defined as zero:

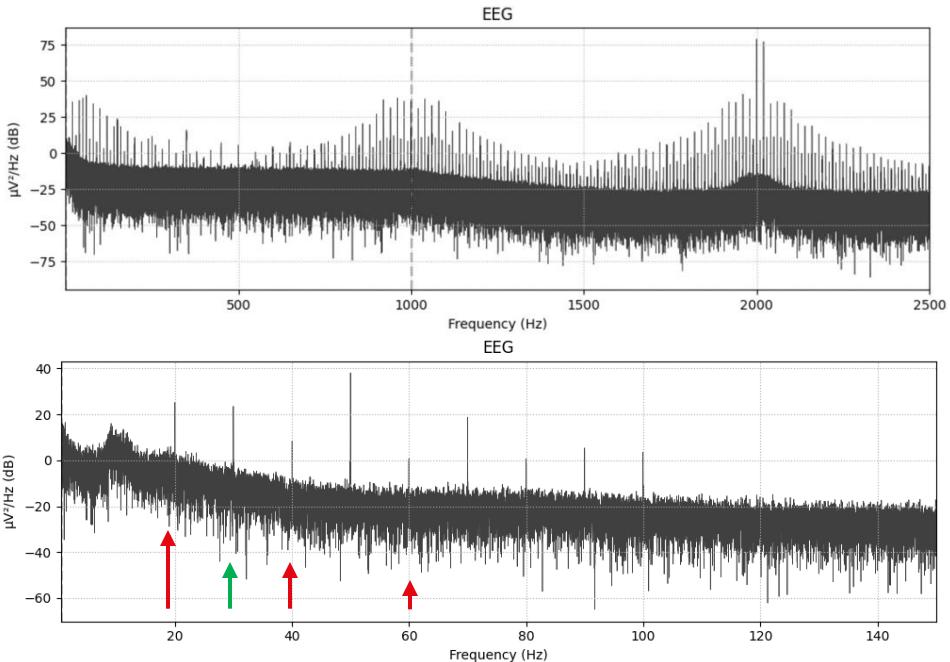
$$f(0) + \frac{f'(0)}{1!}x + \frac{f''(0)}{2!}x^2 + \frac{f'''(0)}{3!}x^3 + \dots = \sum_{n=0}^{\infty} \frac{f^{(n)}(0)}{n!} x^n$$

Linear

Non-Linear



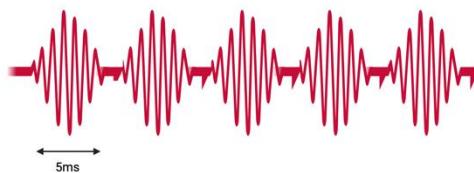
Example of stimulation artefacts with continuous TI stimulation, beat frequency at 20Hz



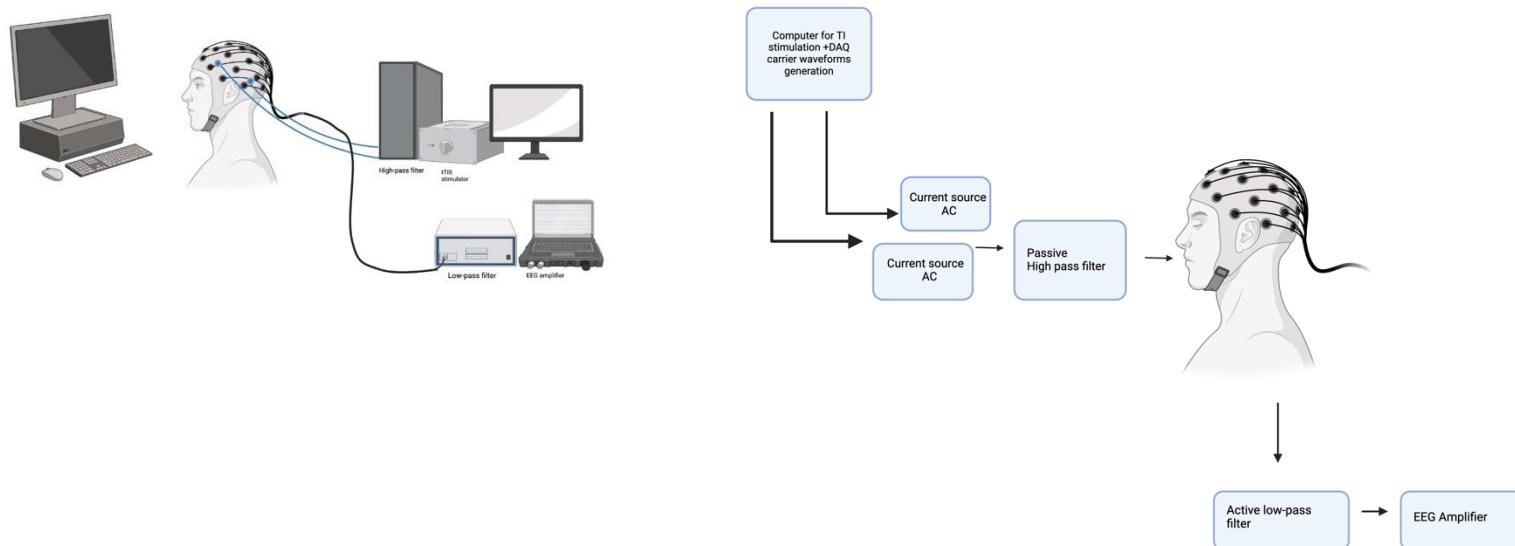
Carrier TI frequencies (2kHz, 2.02kHz)

Red arrows: TI stimulation artefact at 20Hz and its harmonics (FFT)

Green arrows: TI stimulation artefact at 30Hz (mixing with power line noise)



TI stimulation, beat frequency 20Hz (enveloppe graphical representation)



TI-EEG set up configuration:

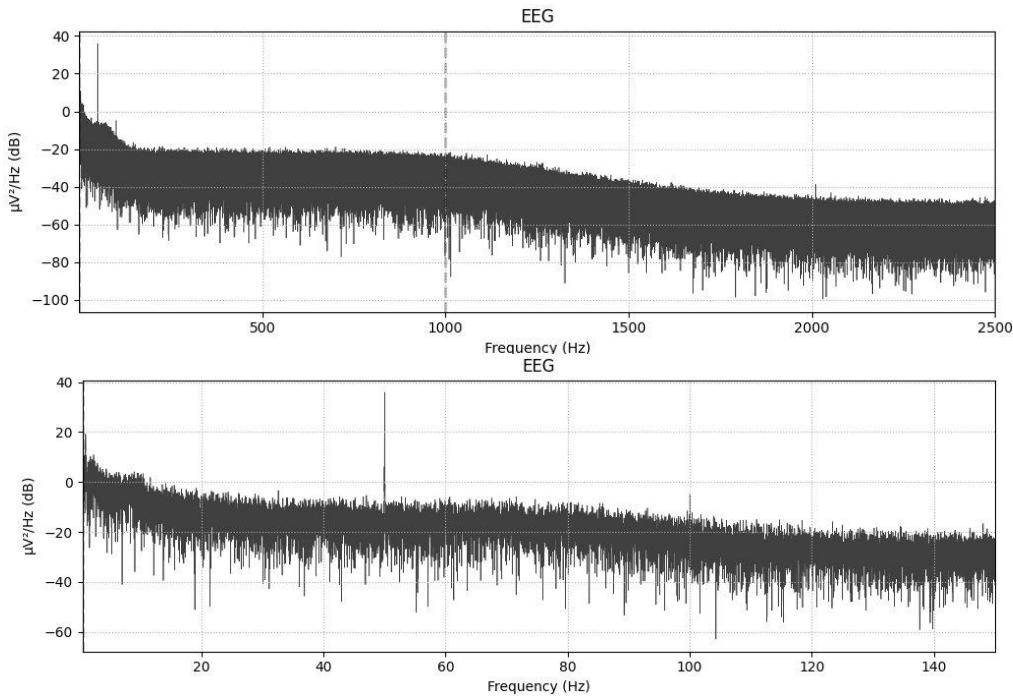
Passive high-pass filter: allows only the high carrier frequencies to pass, after the TI stimulators

Active low-pass filter: allows only the frequencies below 100Hz to pass, eliminating the carrier frequencies before reaching the EEG amplifier

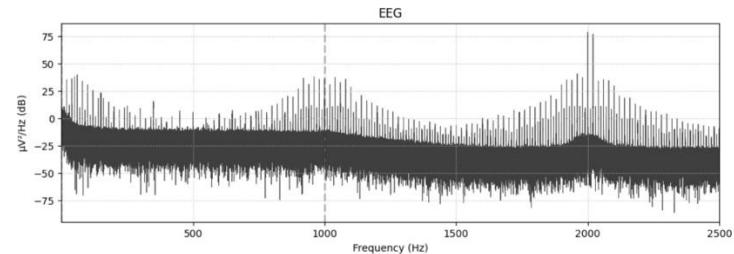


Hardware filters, tTIS 2kHz, Beat frequency 20Hz

EEG recording with hardware filters, no artefacts for all the EEG channels



Without hardware filters:

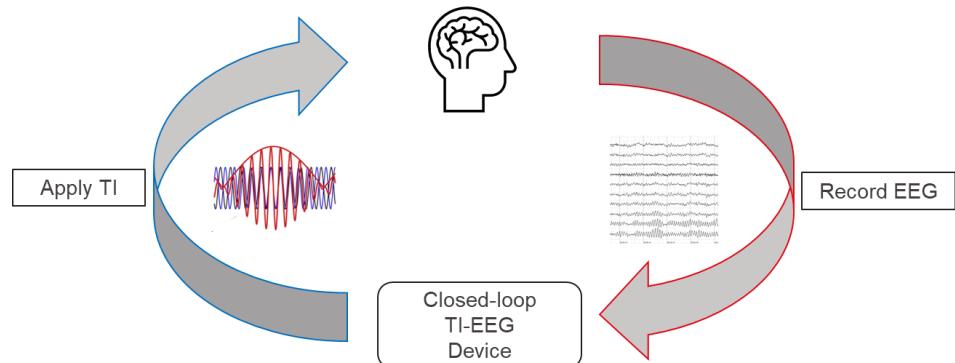




Applications with tTIS-EEG recording and possible technological developments:

Closed-loop application based on neurofeedback and/or behavioral performance:

1. Optimize tTIS (beat frequency, pattern) based on cortical output EEG activity
2. Deliver pulsed-pattern stimulation, locked to endogenous cortical EEG activity
3. Enhance or disturb reinforcement learning, closed-loop with changes in cortical EEG recording
4. Modeling striatal sEEG activity in correlation with EEG cortical activity:
adjust online envelope focus, beat frequency to endogenous rhythm, for example in Parkinson's disease
5. Phase-locking tTIS





Applications with tTIS-EEG recording:

Hippocampus TI stimulation and EEG cortical output:

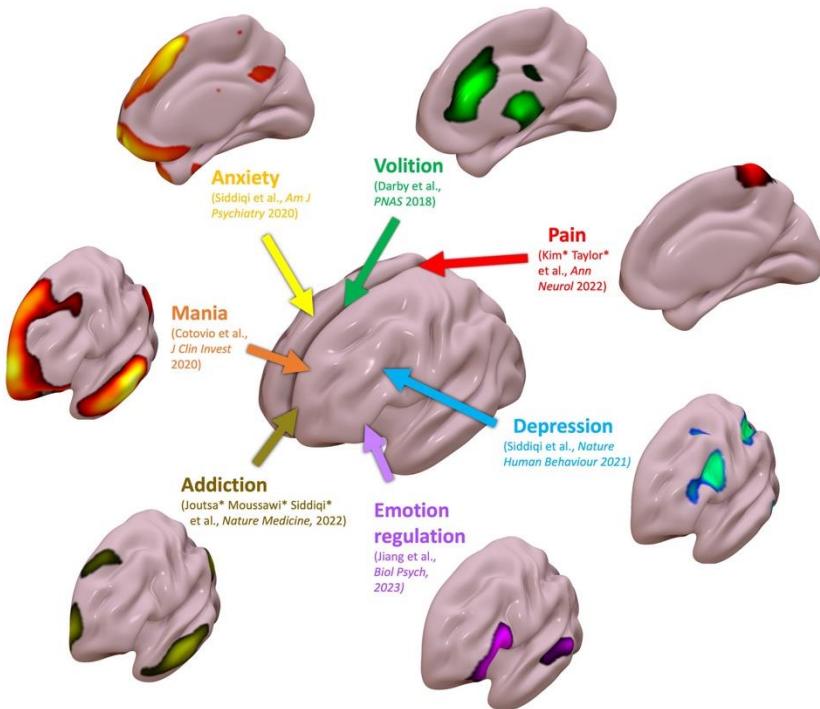
Alzheimer's disease (AD):

- Establish physiological rhythm patterns in DMN and FPN
- Cortical biomarkers of response to TI stimulation

Striatum TI stimulation and EEG cortical output:

Parkinson's disease (PD):

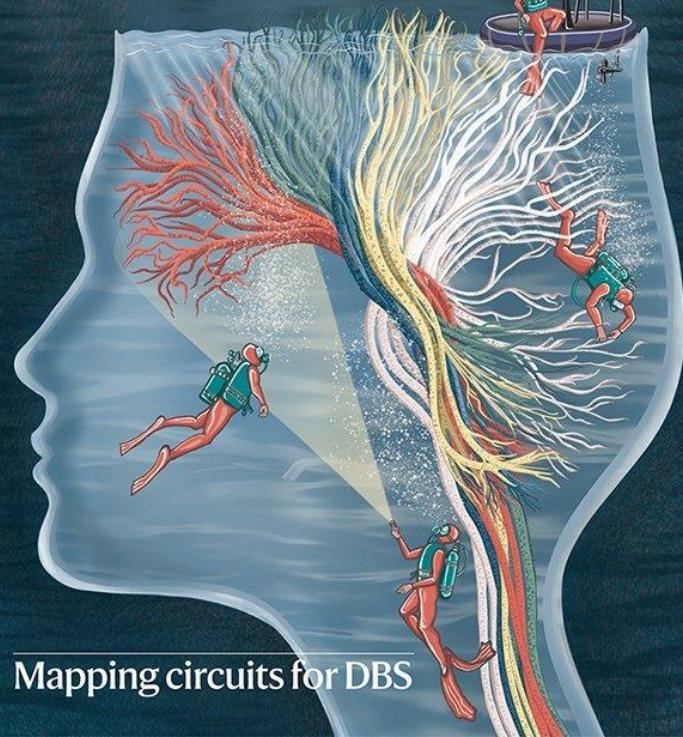
- Establish physiological rhythm patterns in cortico-basal ganglia loop, targeting pathological beta activity
- PD apathetic patients and targeting altered EEG alpha and theta oscillations



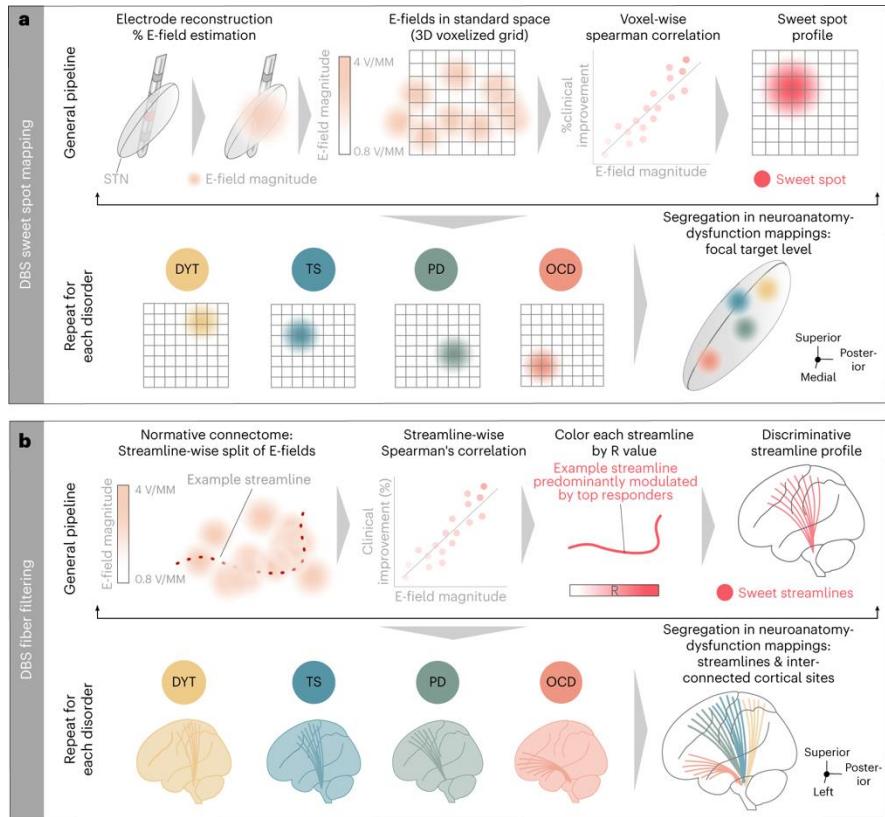


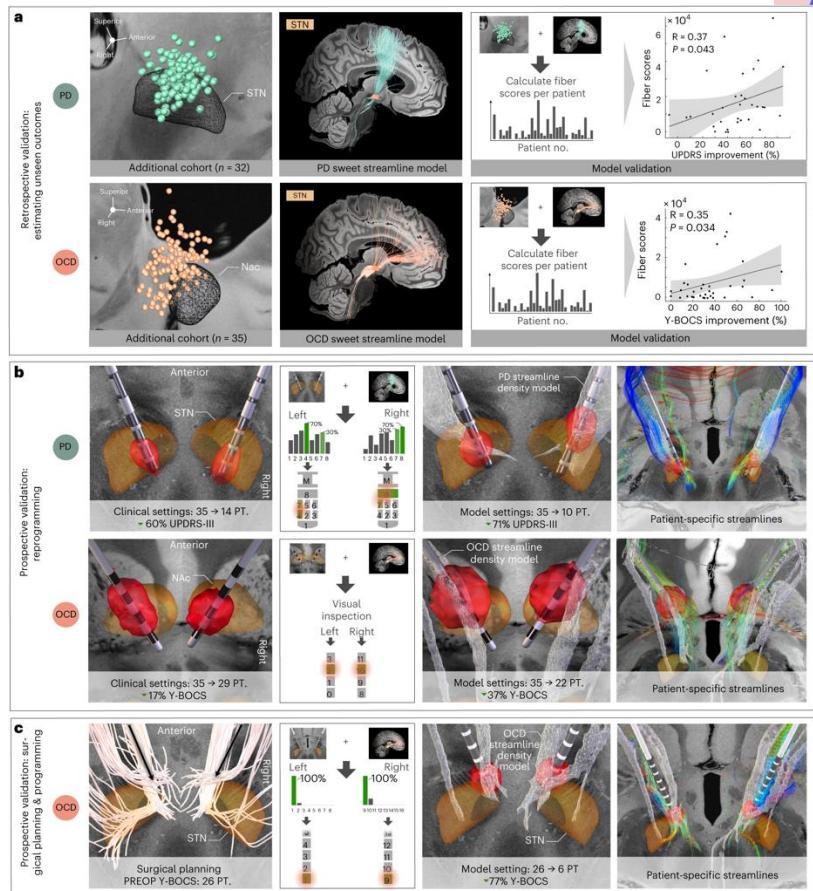
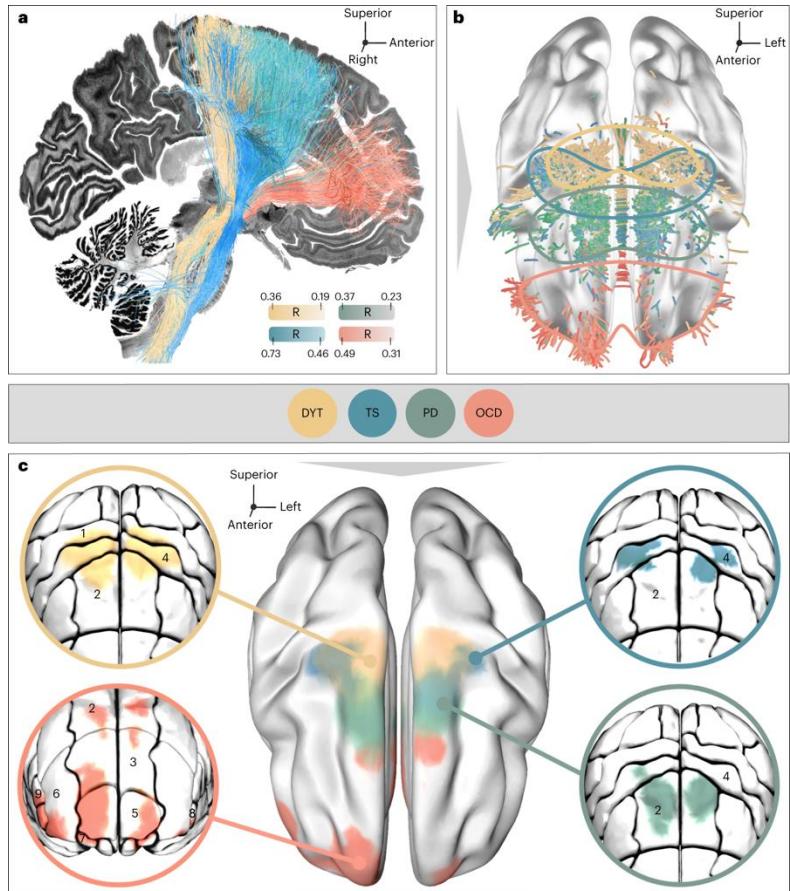
www.nature.com/neo/March 2024 Vol. 27 No. 3

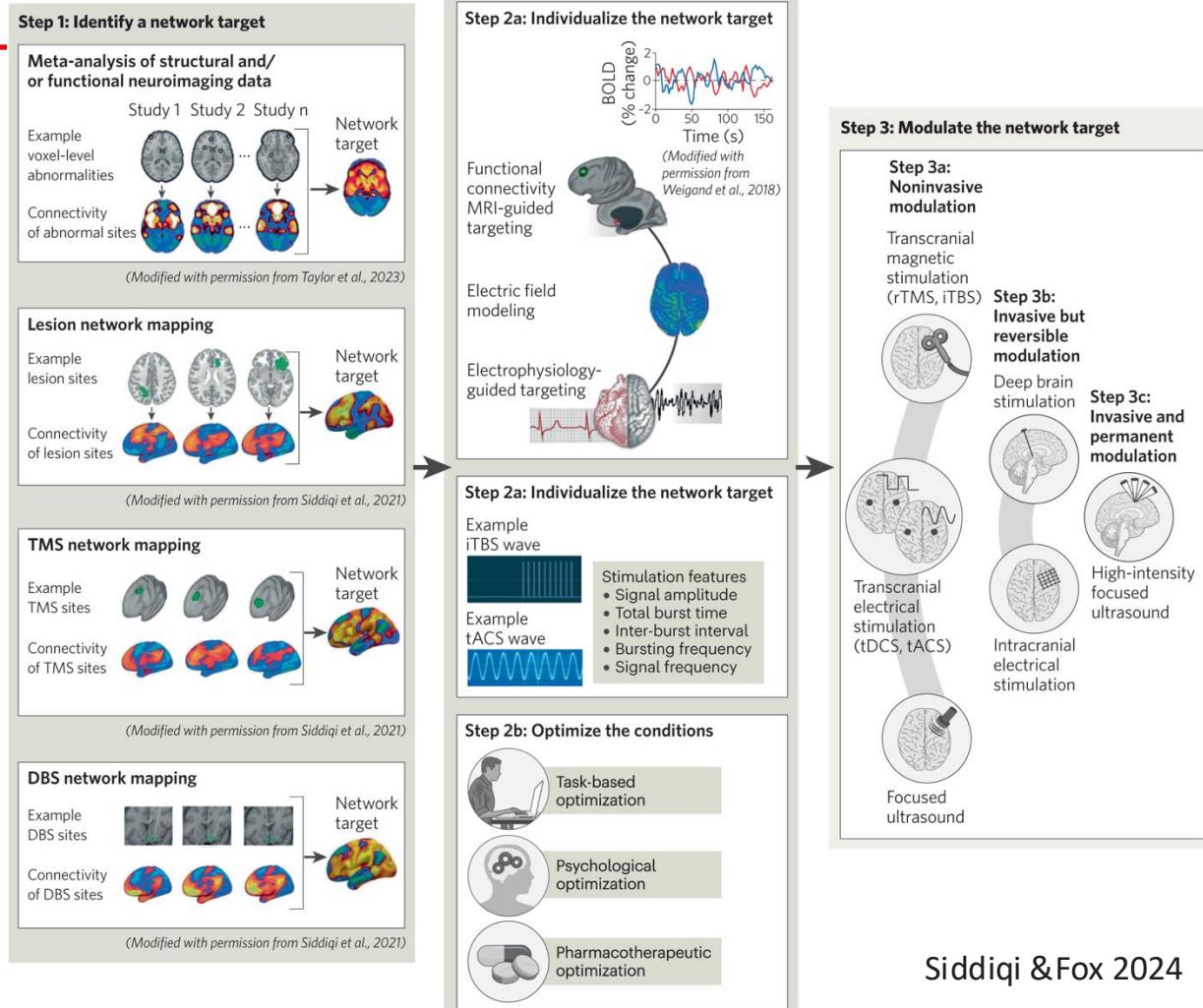
nature neuroscience

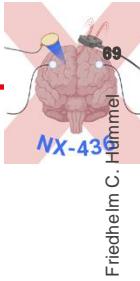


Mapping circuits for DBS









Recording of brain activity simultaneously

- focally and at the network level
- adds to mechanistic understanding
- safety monitoring
- state dependent close-loop applications

Challenges

- safety
- artefacts
- feasibility
- accessibility, clinical translation
- cost

Online interference with brain activity

- causal understanding
- network vs. local effects
- state dependent close-loop applications

Selection of method

- local vs network activity
- oscillatory vs. activation
- artefact profile