

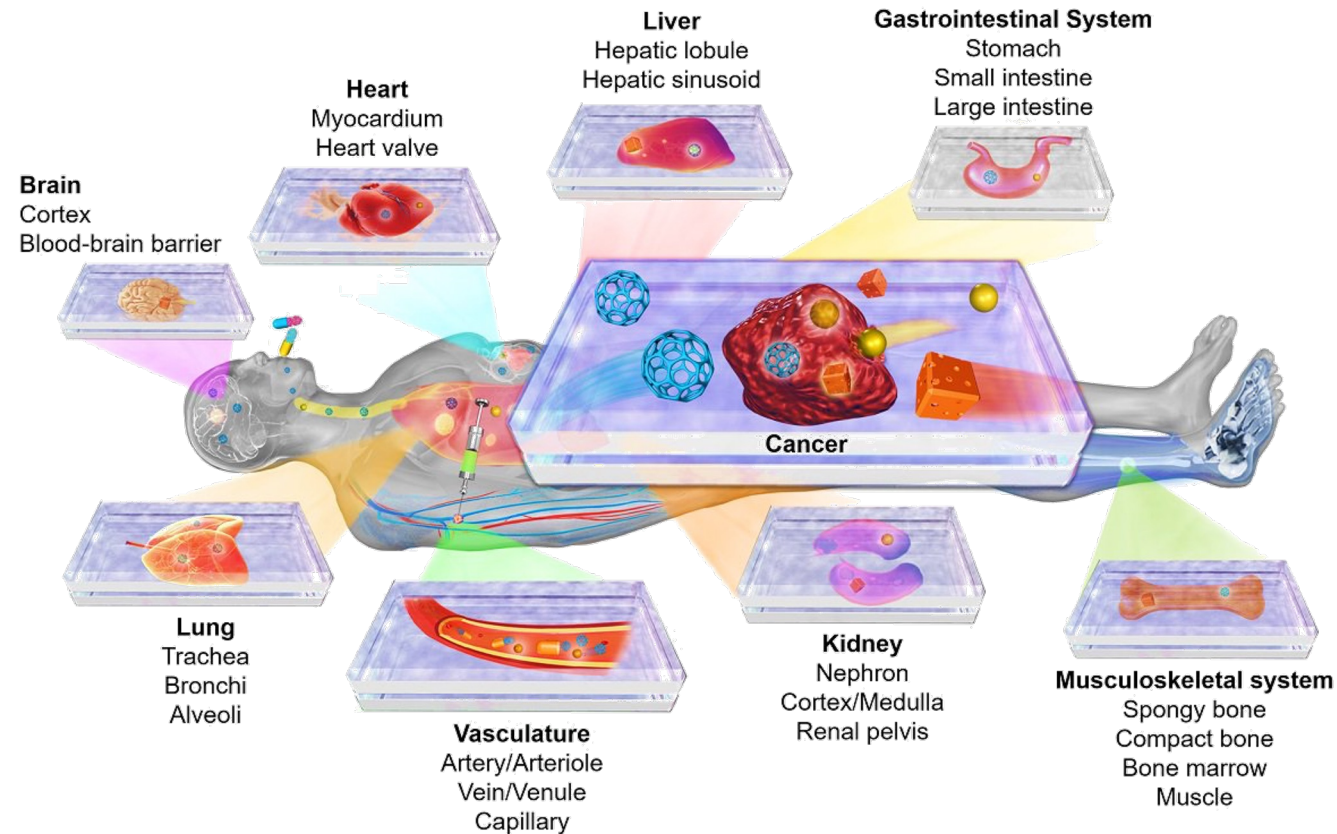
# Biomechanics in Organ-on-Chip Systems

**Dr. Philippe Abdel-Sayed, MER**

*Regenerative Therapy Unit, Department of Musculoskeletal Medicine, CHUV*

*Discovery Learning Laboratory – Bioengineering, EPFL*

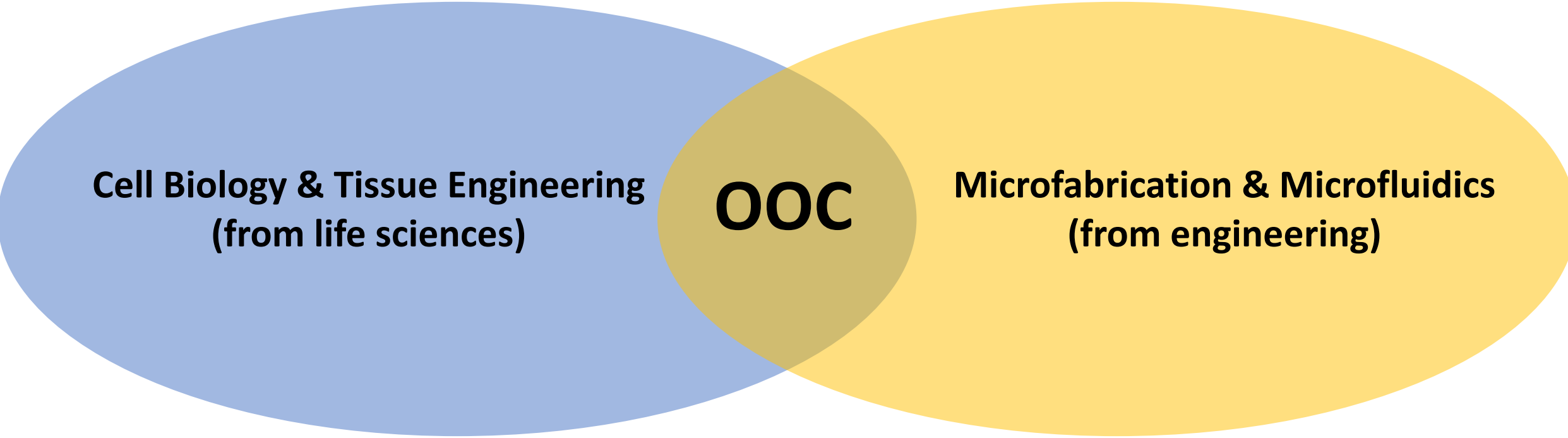
# What are Organ-on-chips (OOC)?



Zhang YS et al. (*Drug Discovery Today*, 2017)

- Microfluidic devices mimicking organs
- Realistic/functional tissue microenvironments

# The OOC is a multidisciplinary field

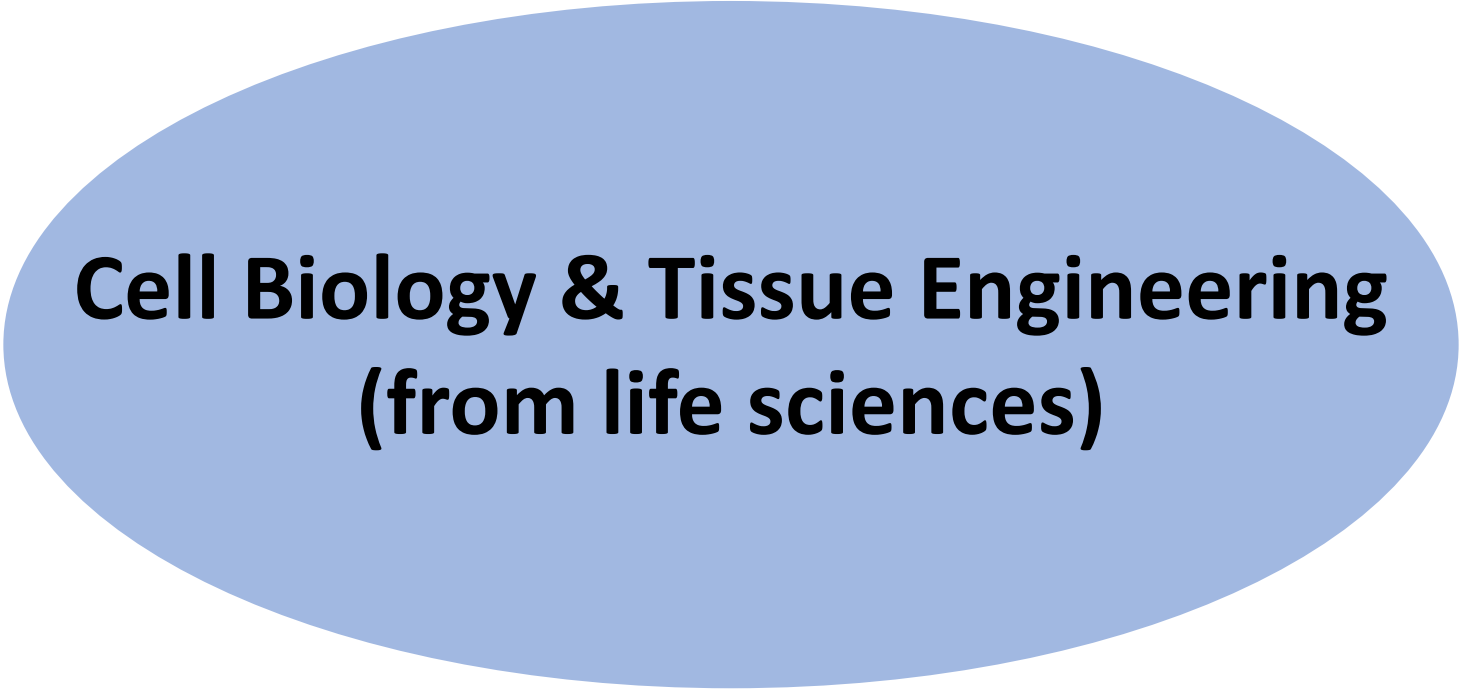


**Cell Biology & Tissue Engineering**  
(from life sciences)

**OOC**

**Microfabrication & Microfluidics**  
(from engineering)

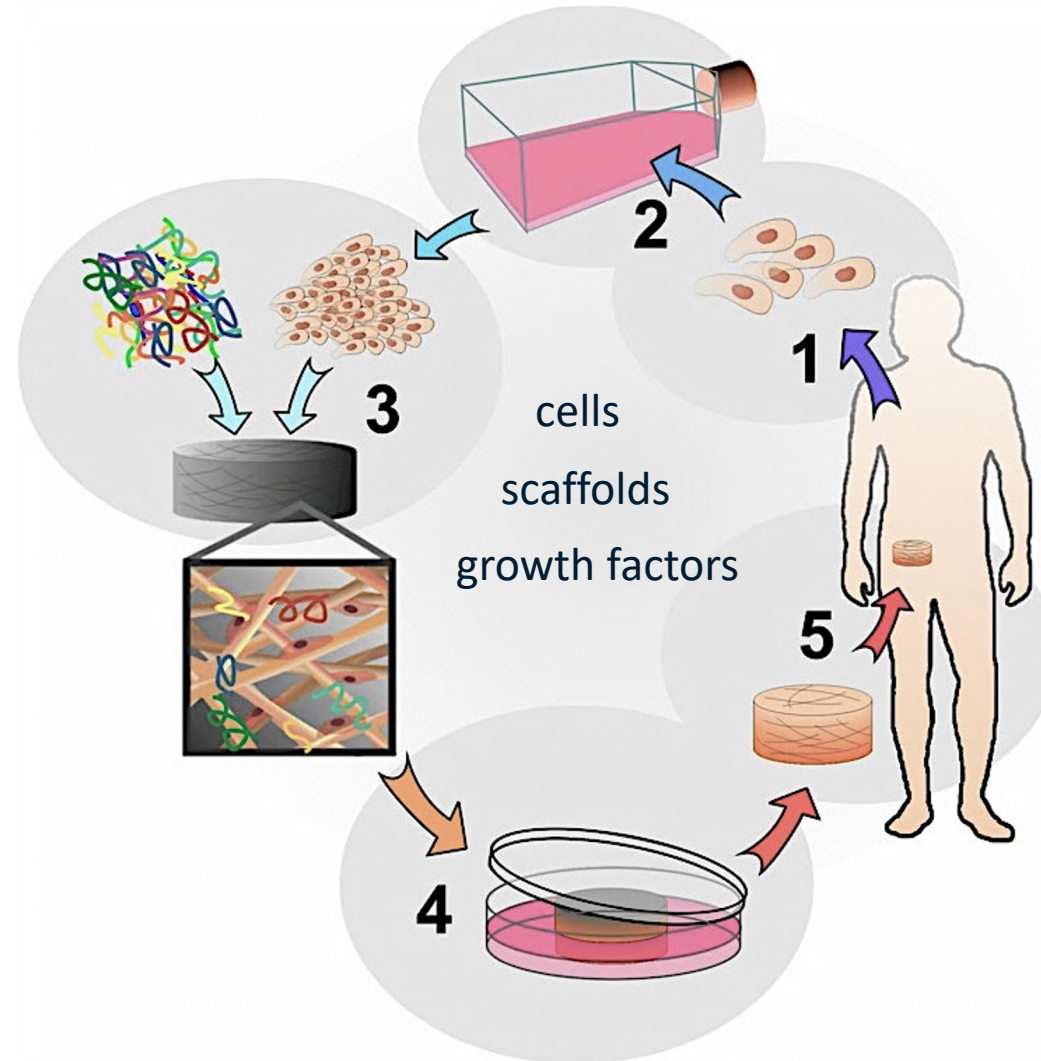
The OOC is a multidisciplinary field



**Cell Biology & Tissue Engineering  
(from life sciences)**

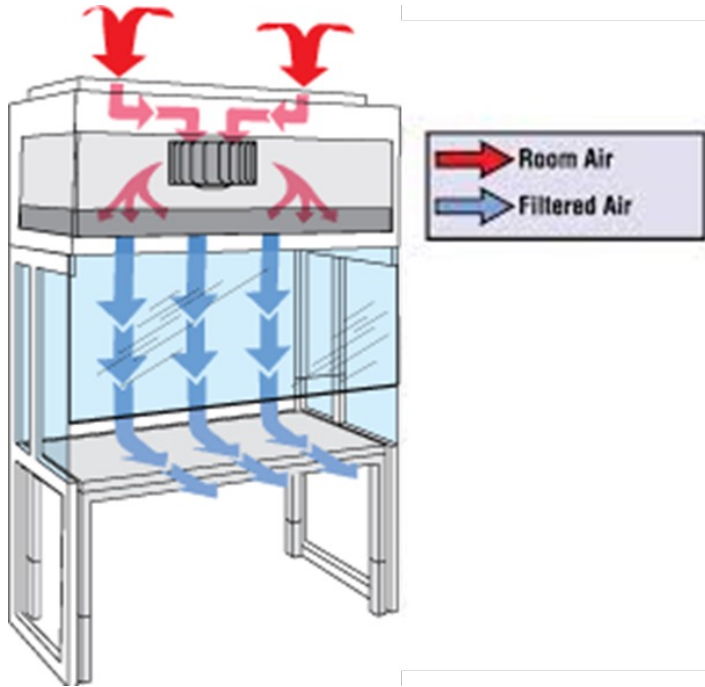


# Tissue engineering concepts



The goal is to restore, maintain, or improve damaged tissue or organs

# Basics of mammalian cells culture



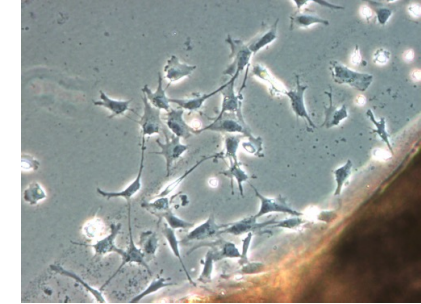
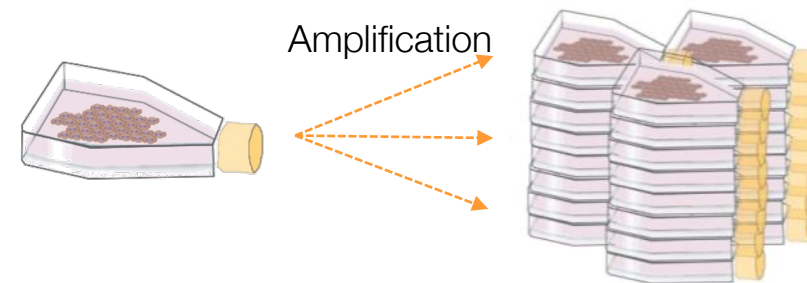
For cell growth



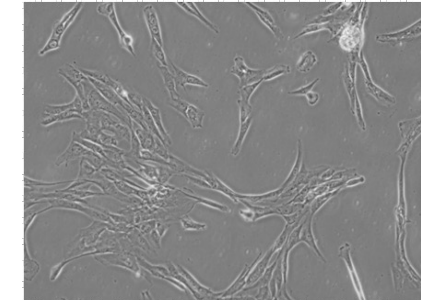
For cell experiments



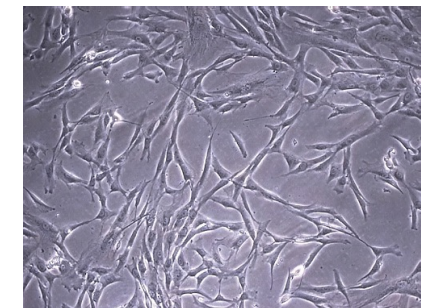
For cell primary explant



Bone

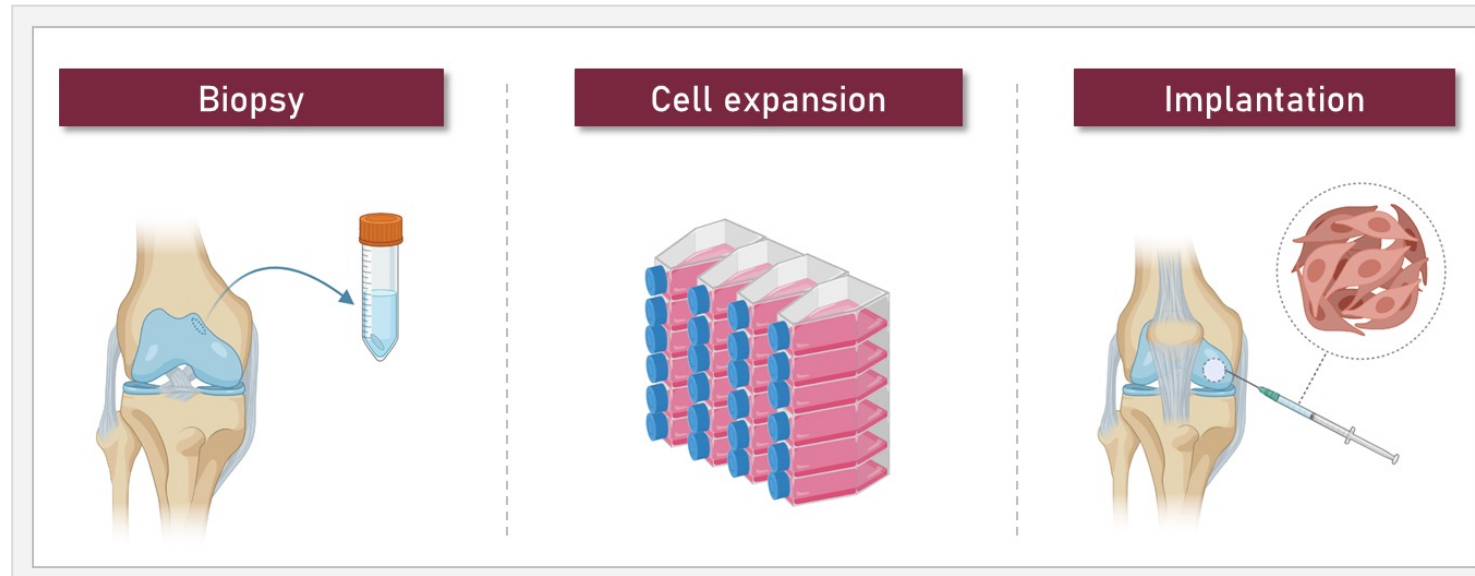
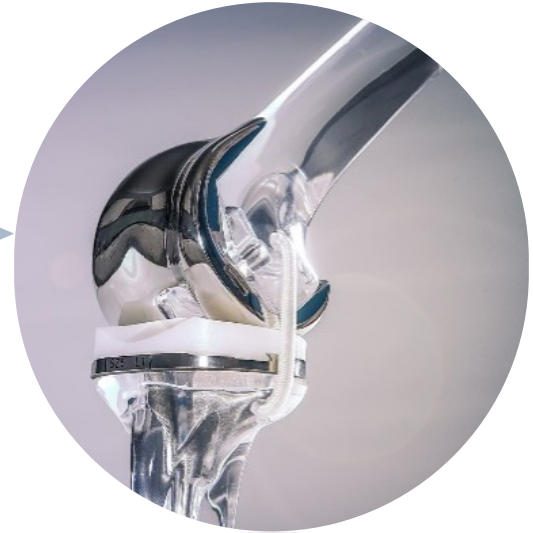
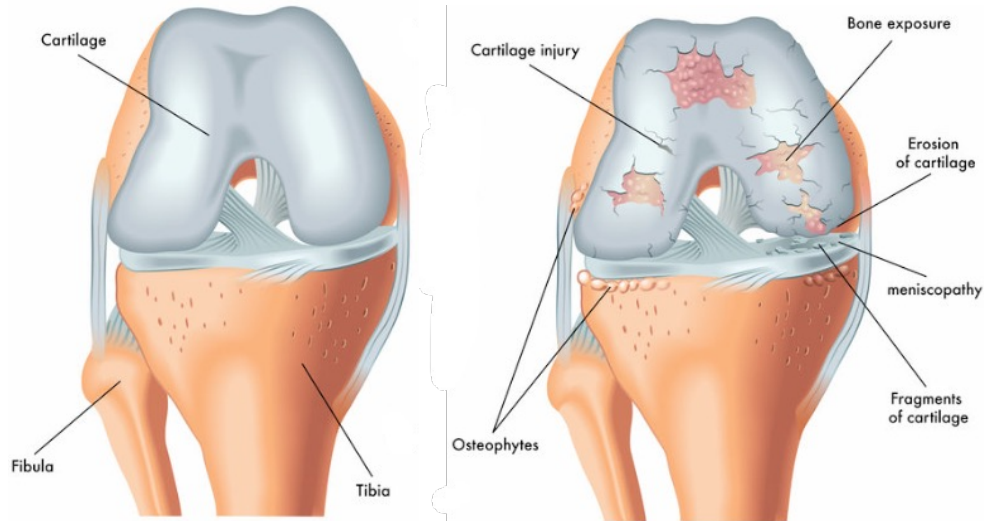


Cartilage

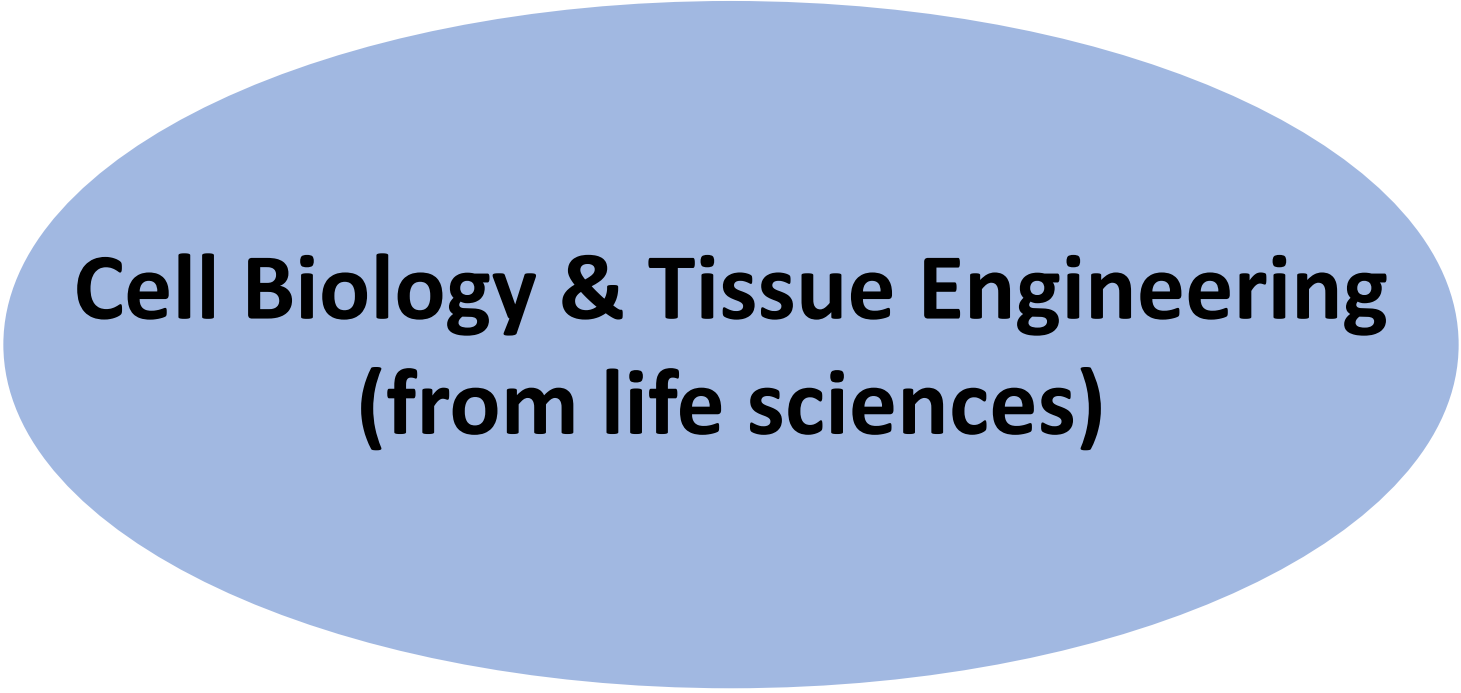


Fibroblasts

# Example of Tissue Engineering: Autologous Chondrocytes Implantation (ACI)



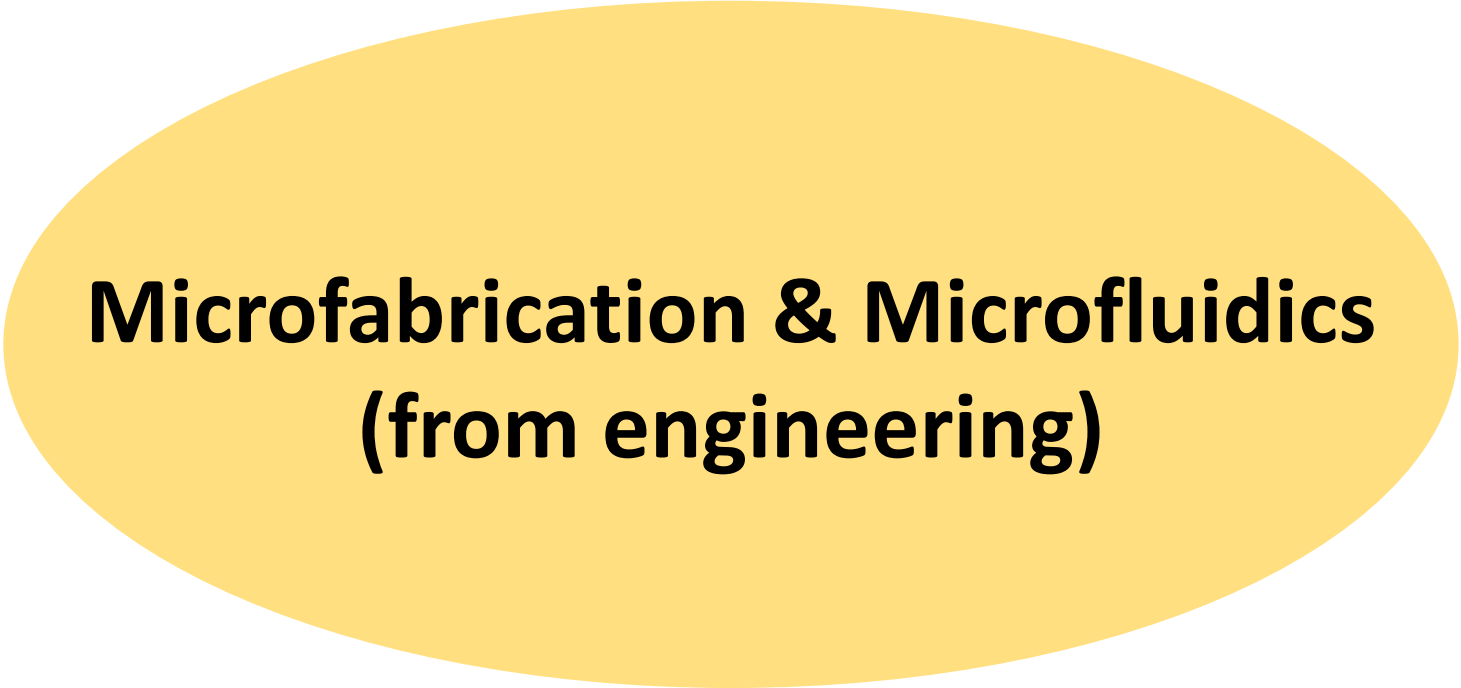
The OOC field originates from the intersection of multiple disciplines



**Cell Biology & Tissue Engineering  
(from life sciences)**



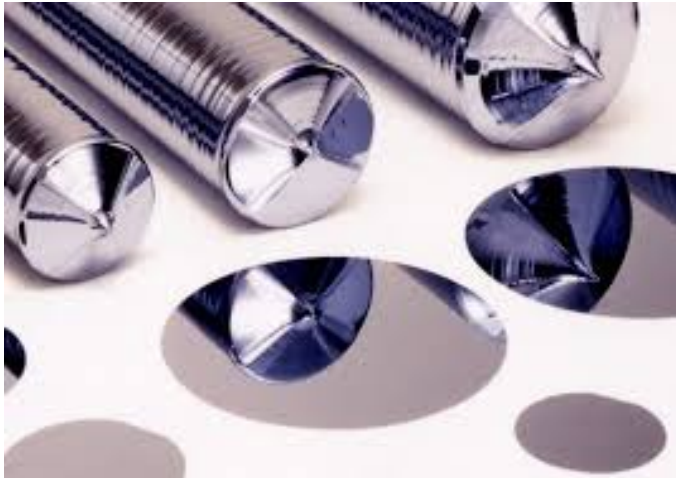
The OOC field originates from the intersection of multiple disciplines



**Microfabrication & Microfluidics  
(from engineering)**

# Lab-on-chips development

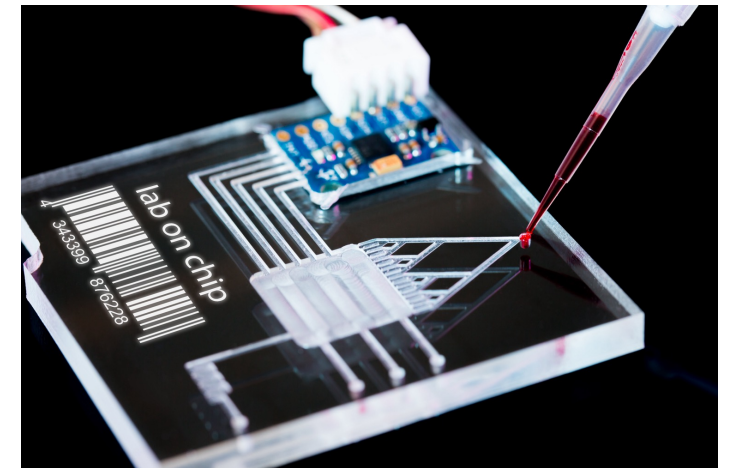
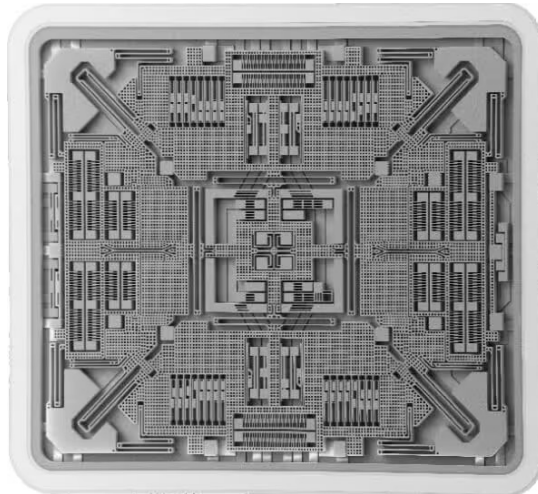
- LOC technology derived from the industry of microelectronics:
  - Use of **microelectronics materials** for which fabrication techniques are available and mature (1980s–2000s)
  - Provided the tools to miniaturize and precisely control fluidic environments at the micrometer scale



Silicon-based 3-12" wafers

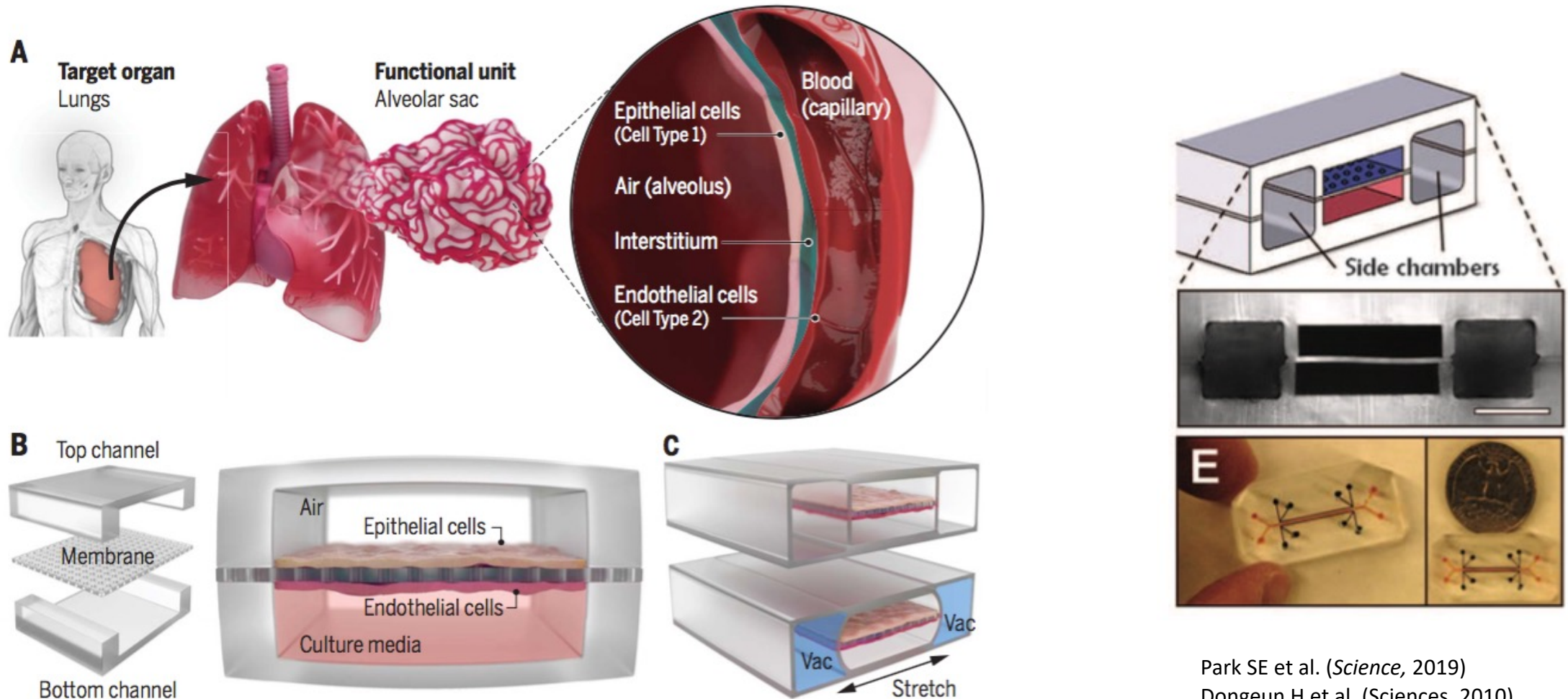


MEMS



Microfluidic systems

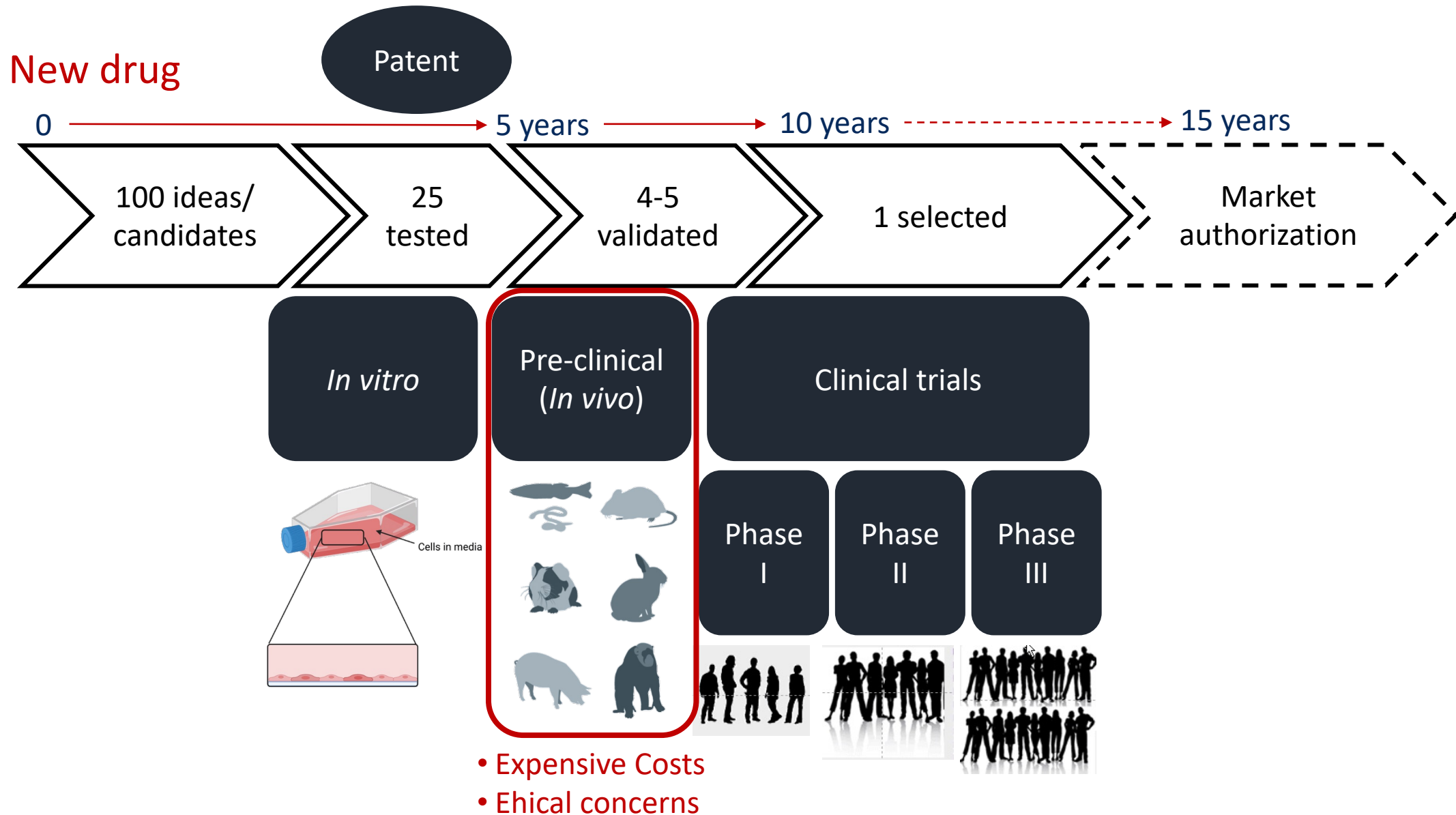
# Why to develop these OOC systems?



Park SE et al. (*Science*, 2019)

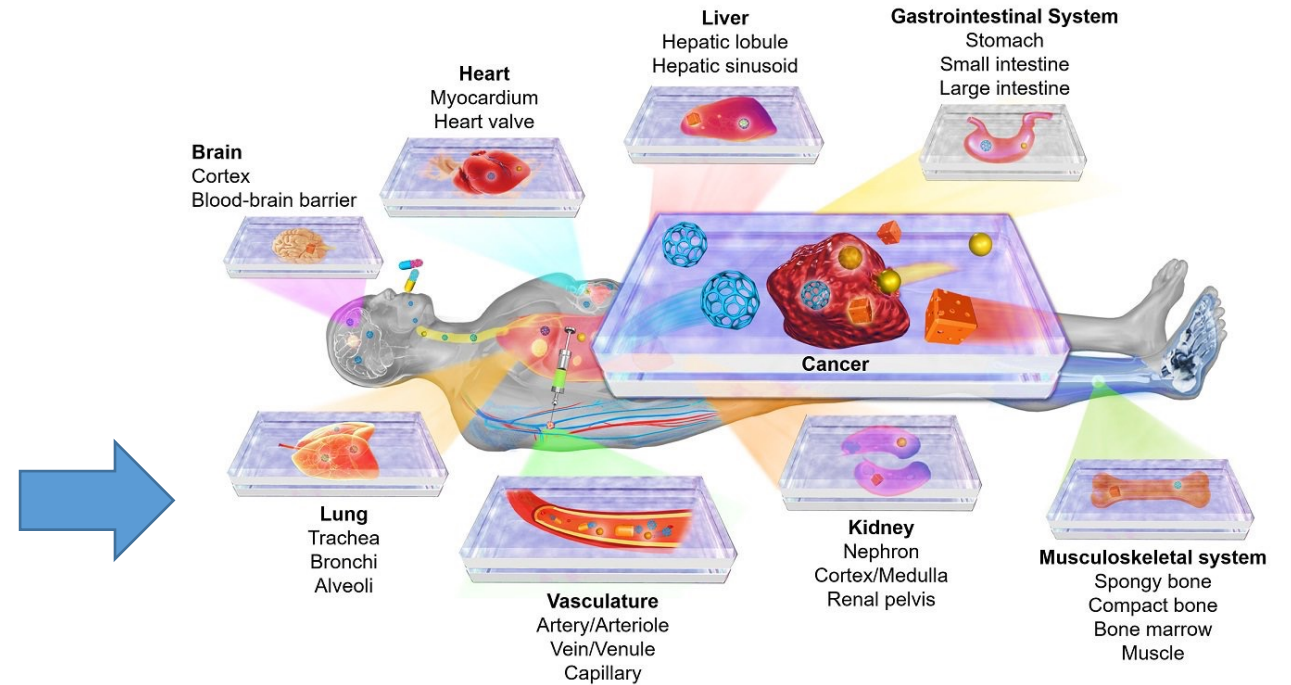
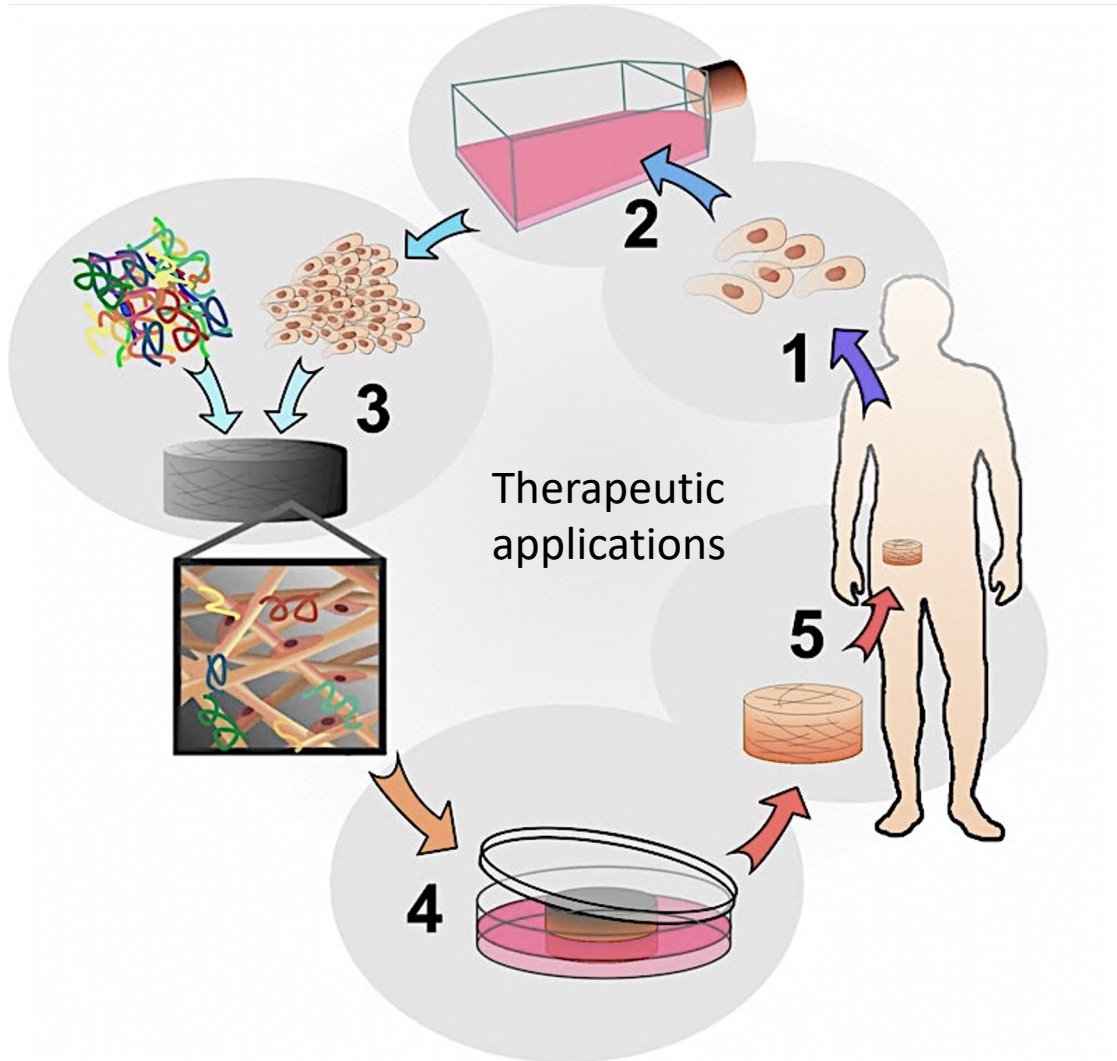
Dongun H et al. (*Sciences*, 2010)

# The pathway of a therapeutic product



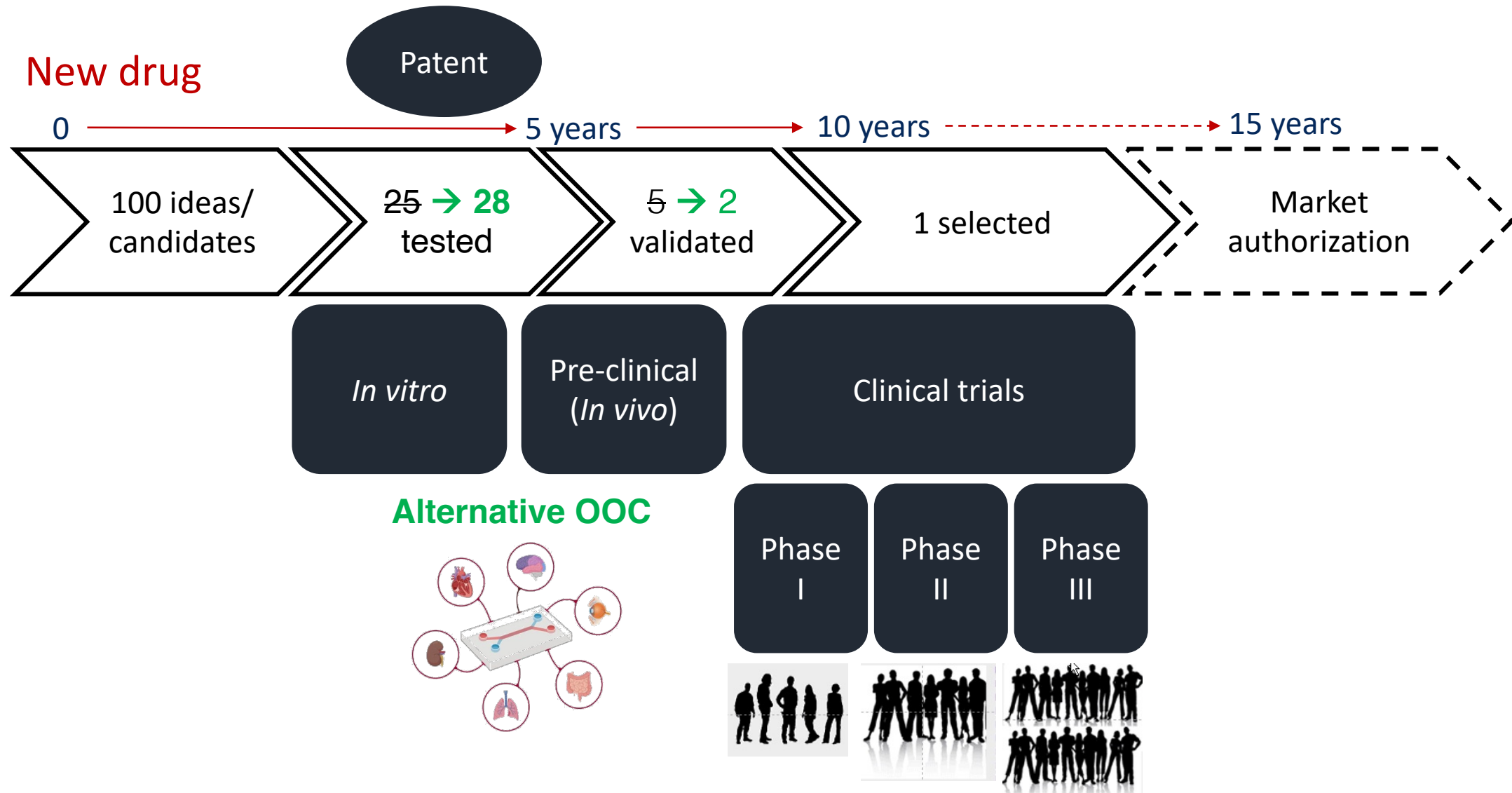


# TE shifting paradigm to organoid models



- Disease modeling (CRISPR gene editing)
- Personalized medicine (e.g. drug screening)

# Alternative to animal experimentation (3R)



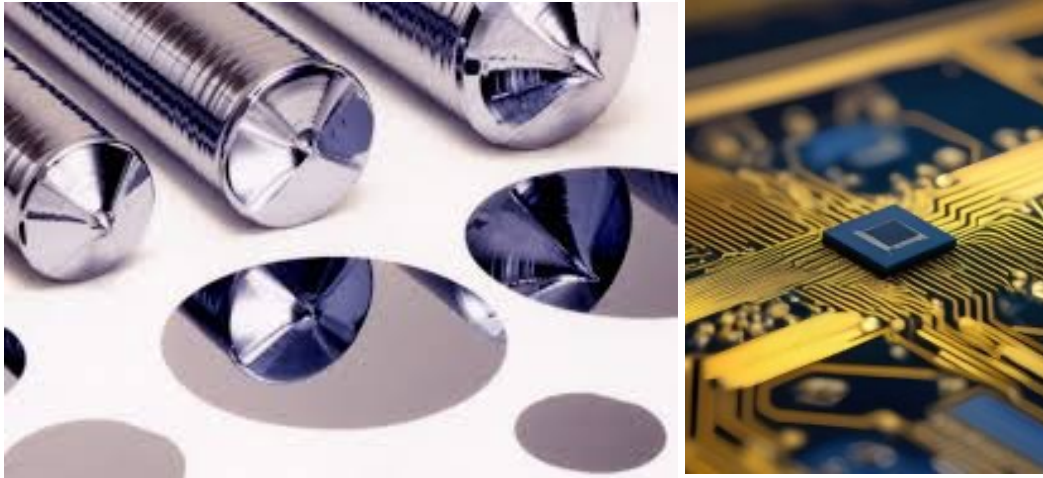
# Main advantages of organ-on-chip systems

- Control over **spatiotemporal organization** of *in vivo*-like tissue architectures
- Ability to precisely control the **amount**, **duration** and **intensity** of the biomechanical or biochemical **cues**
- Useful for initial screening (**3Rs** principle)
- Capability of **monitoring in real time** the effects of applied mechanical forces on cell, tissue and organ functions.

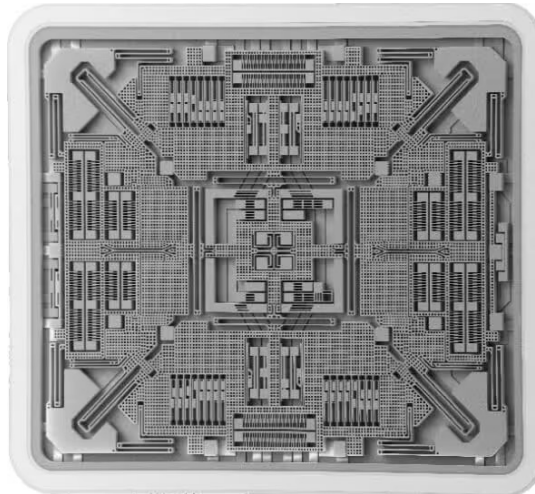
Fabrication methods

# Lab-on-chips development

- LOC technology derived from the industry of microelectronics:
  - Use of **microelectronics materials** for which fabrication techniques were available and mature
  - Well-known physical and chemical **properties** and well-characterized **surface derivatization chemistries**



Silicon-based 3-12" wafers



Clean room



# 1. Photolithography

## Photolithography Process



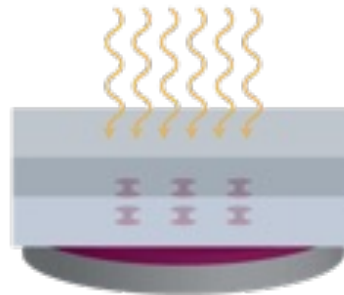
### Silicon wafer

We begin with a clean silicon wafer spin coated with photoresist



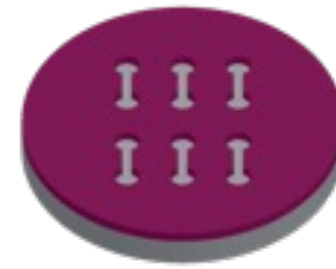
### Photomask

A glass or mylar mask coated with an opaque film defines the features



### Exposure

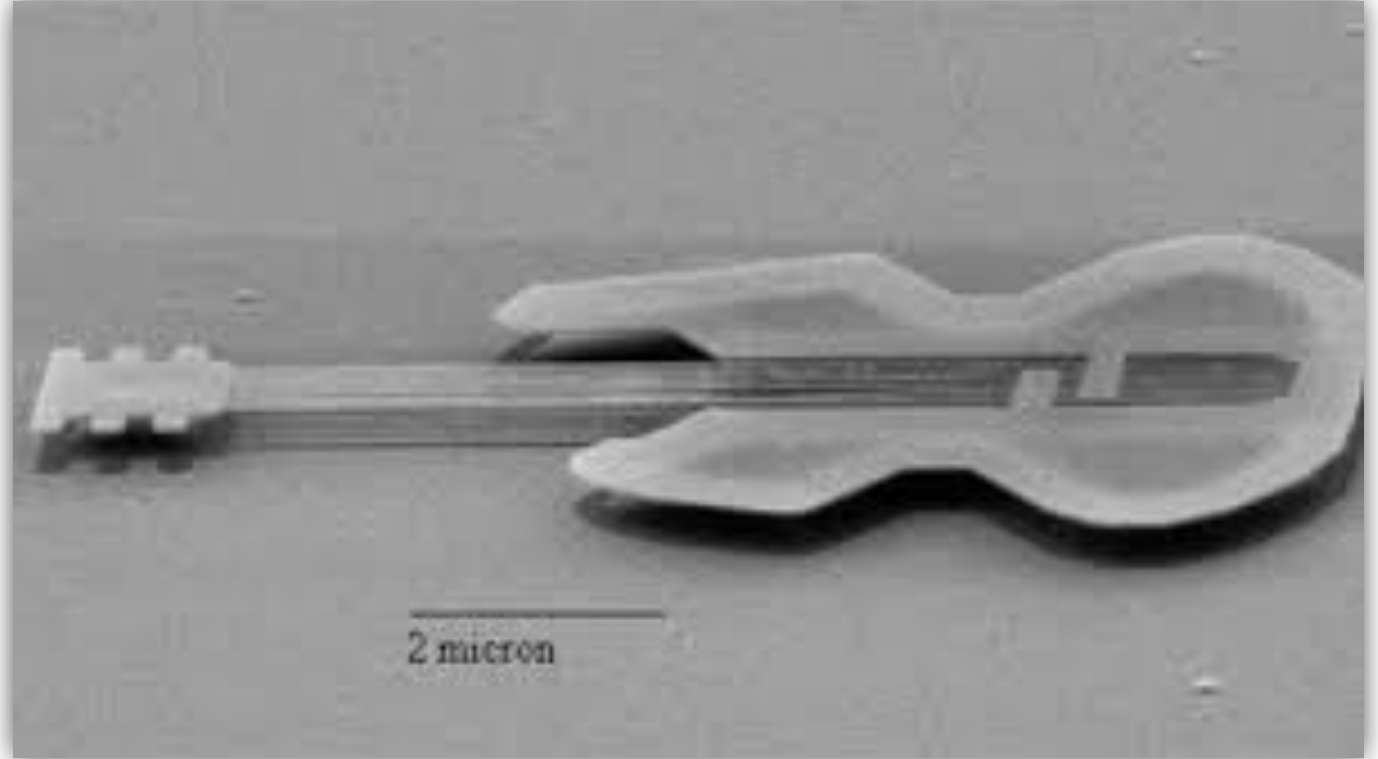
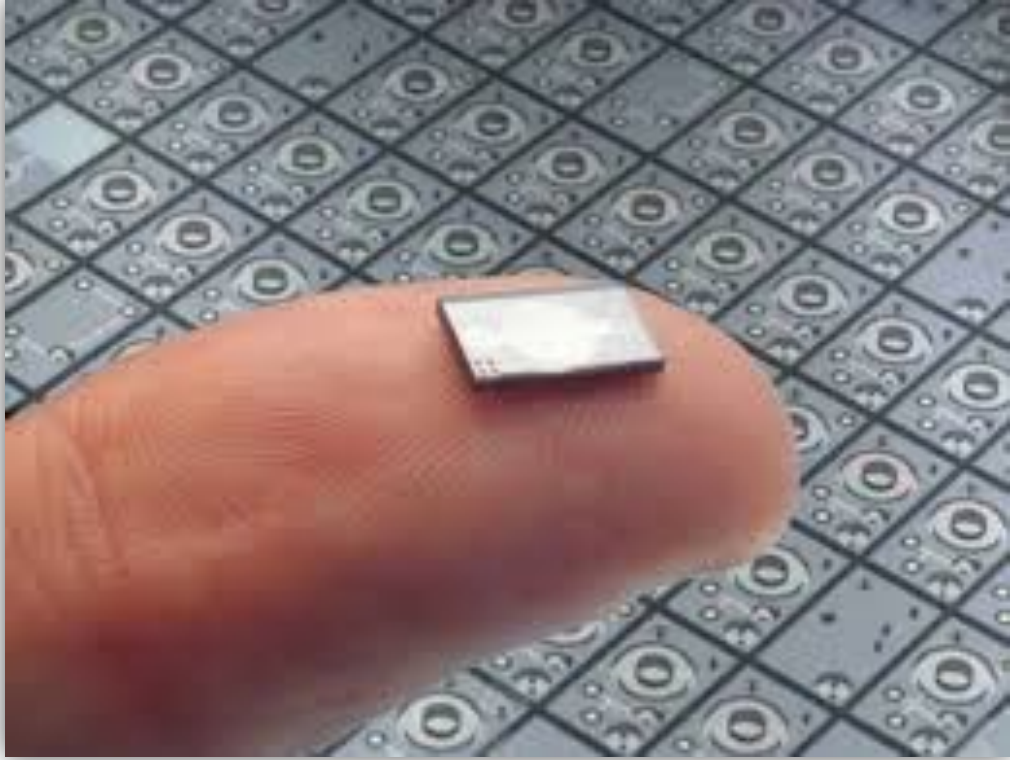
A mask aligner is used to pass UV light through the mask onto the wafer



### Development

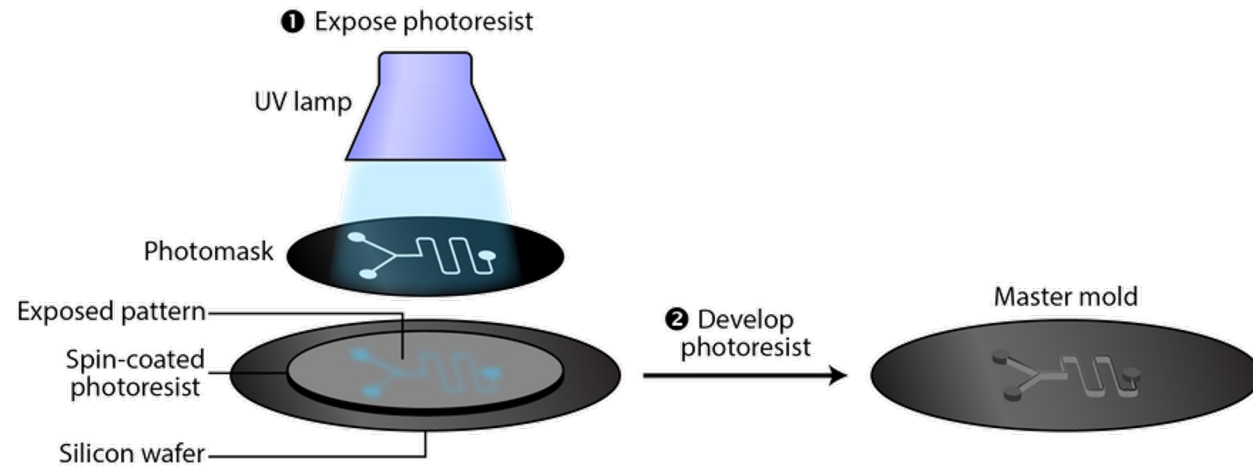
Exposed resist is washed away while unexposed resist remains

# Example

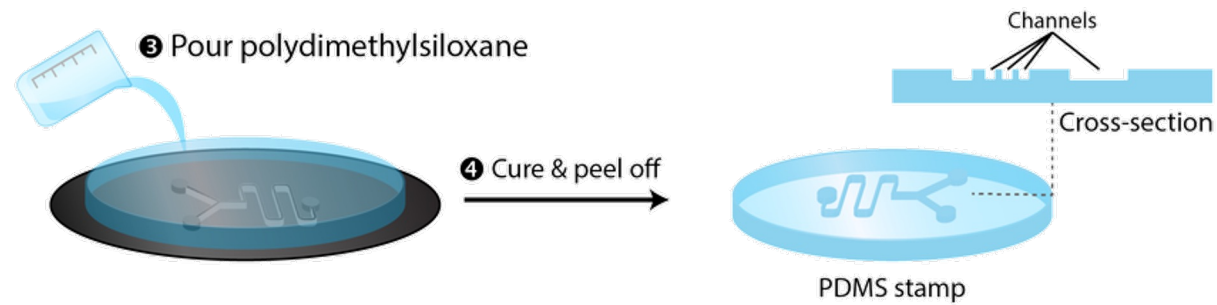


## 2. Soft lithography (Polymer)

photolithography

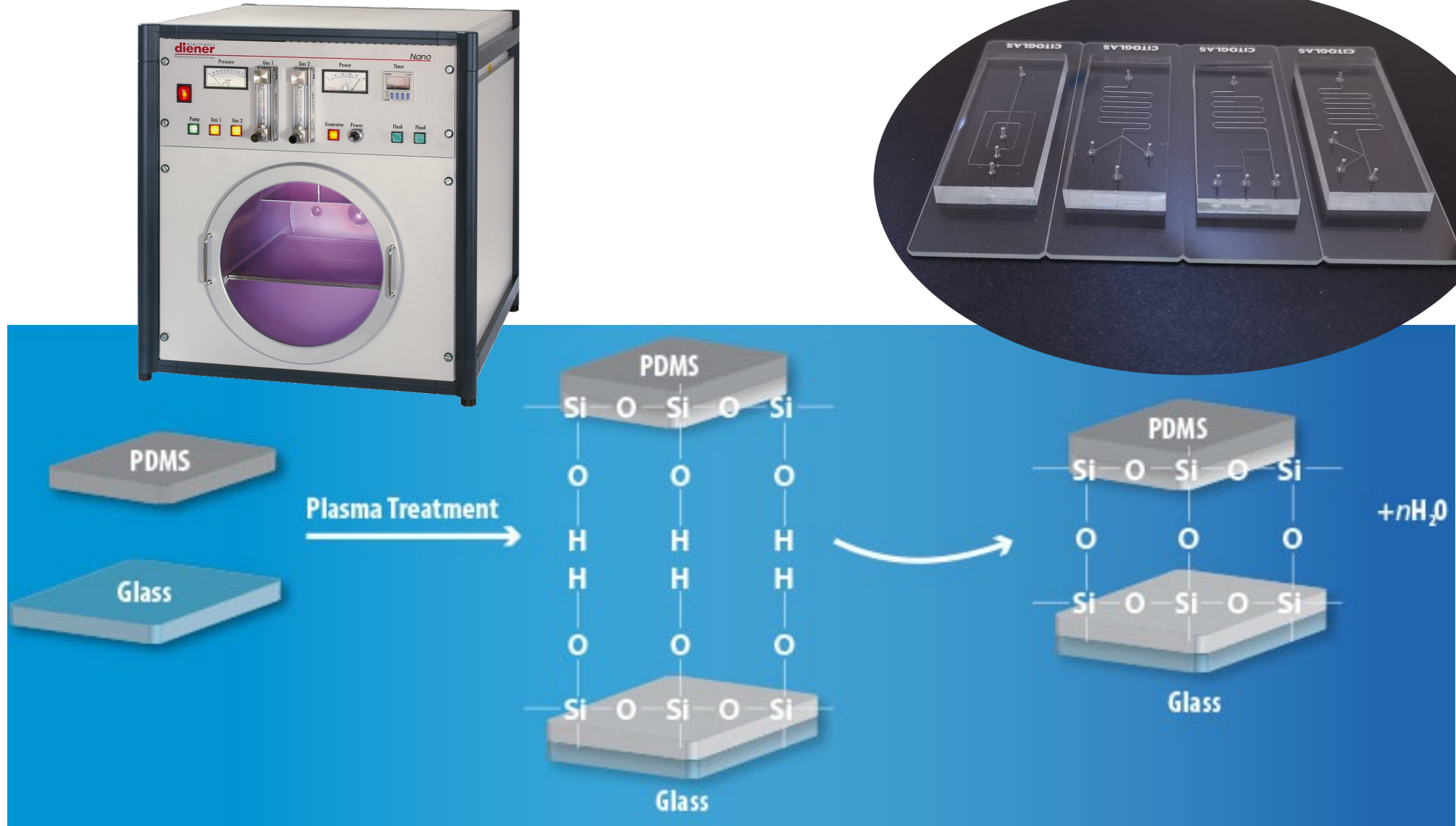


Soft lithography



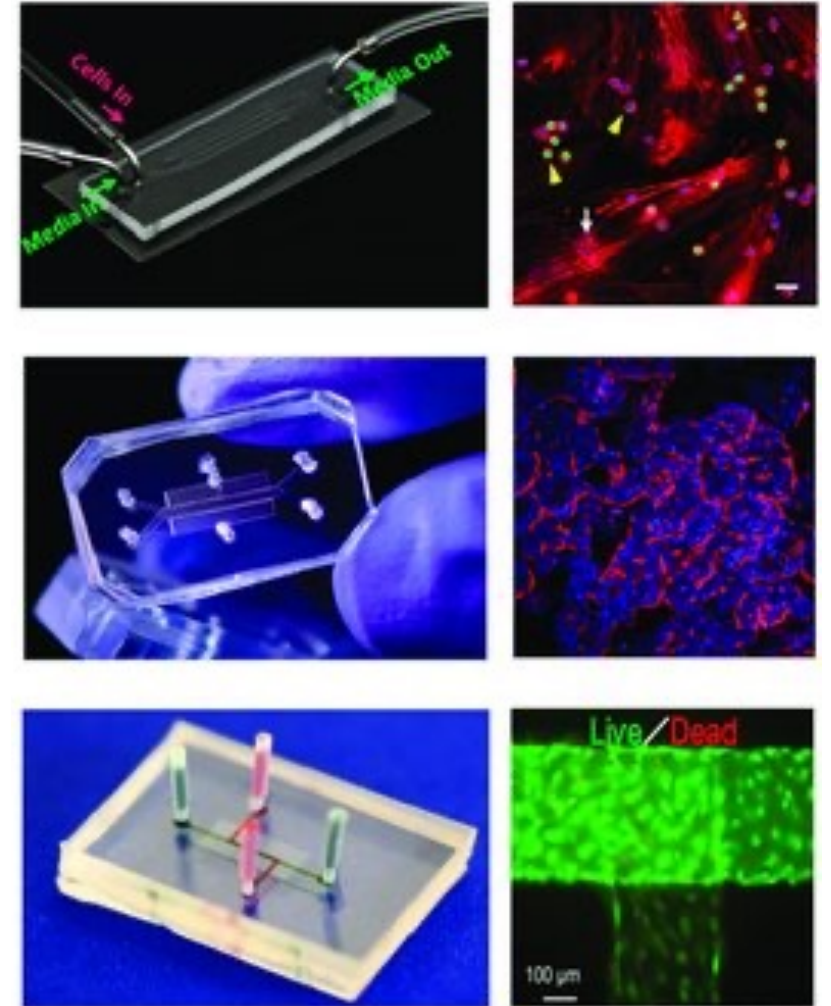


# Plasma treatment

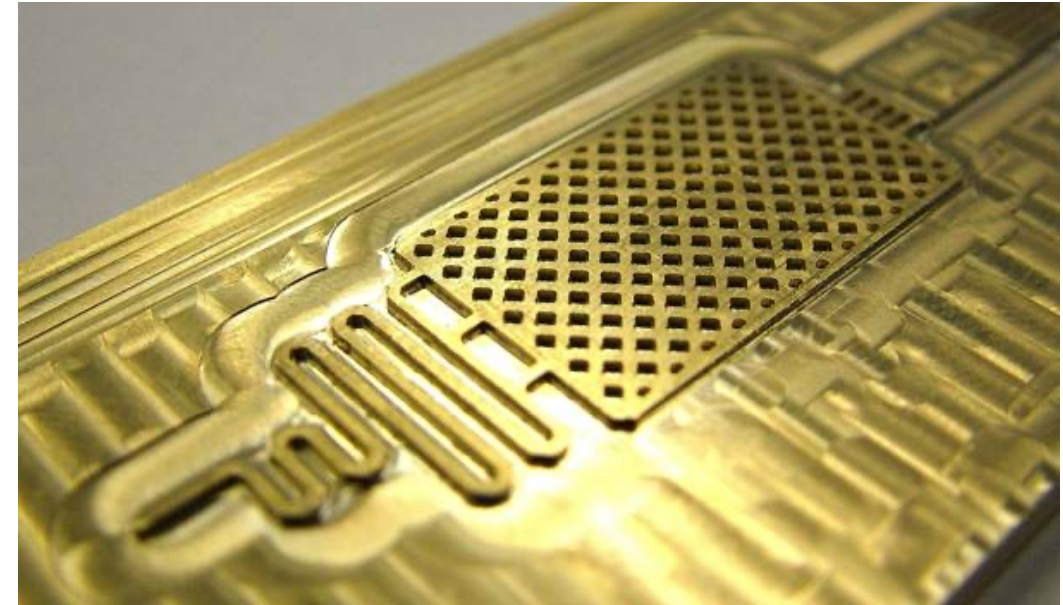
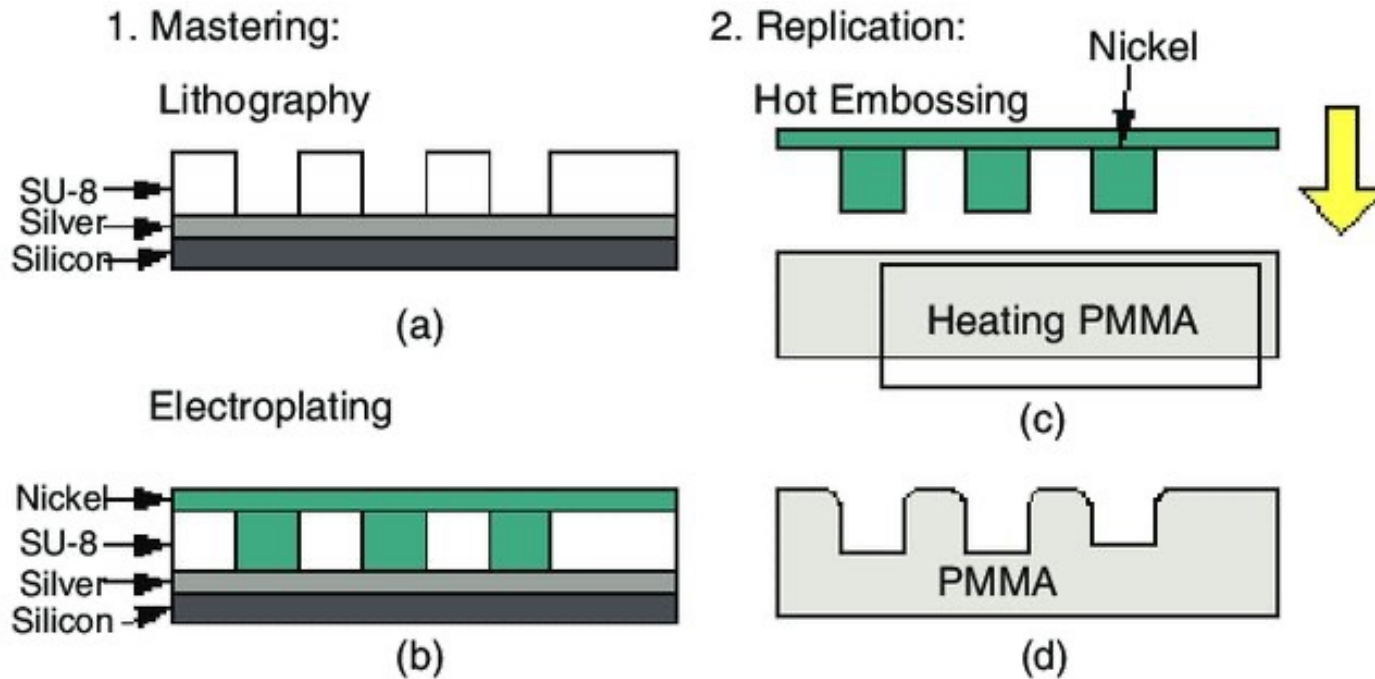


# PDMS: a key polymer for applications in Bio

- Soft lithography  
(no limitation as for clean room)
- Easy and cheap (low production costs)
- Biocompatible and transparent
- Replication accuracy/resolution:  
100  $\mu\text{m}$  (routine) – 10 nm
- Issues?
  - Gas-permeability and hydrophobicity
  - Inertness and extensive adsorption

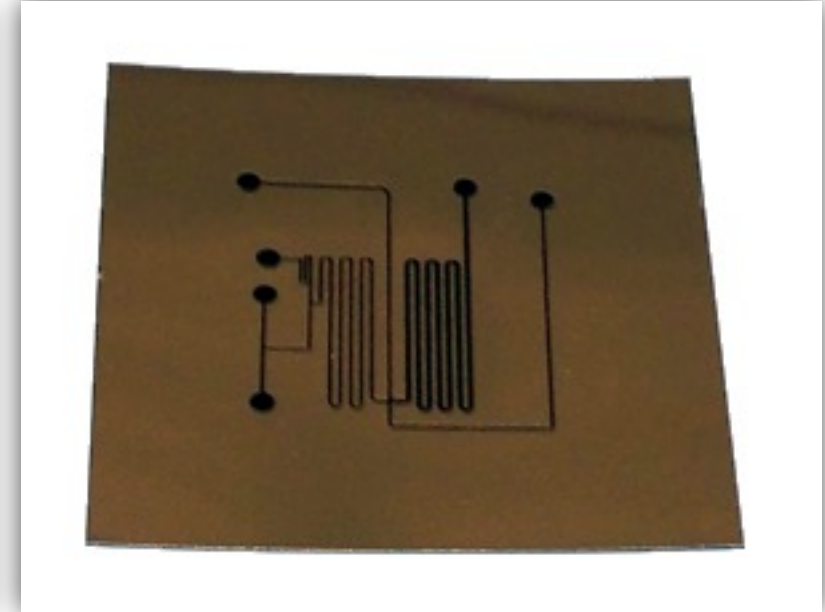
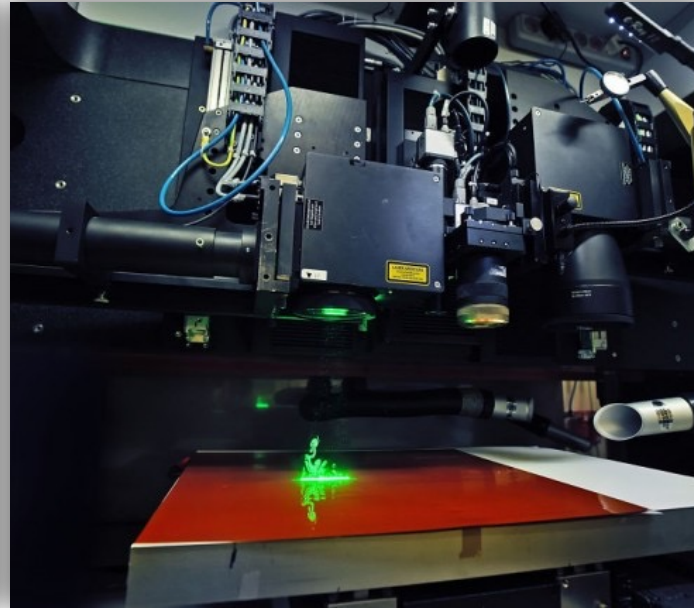
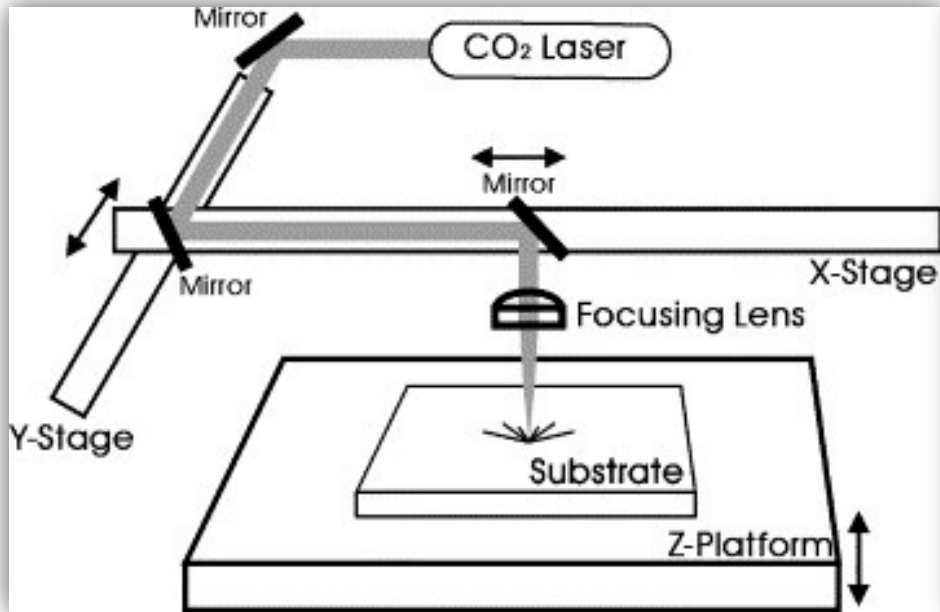


# 3. Hot embossing



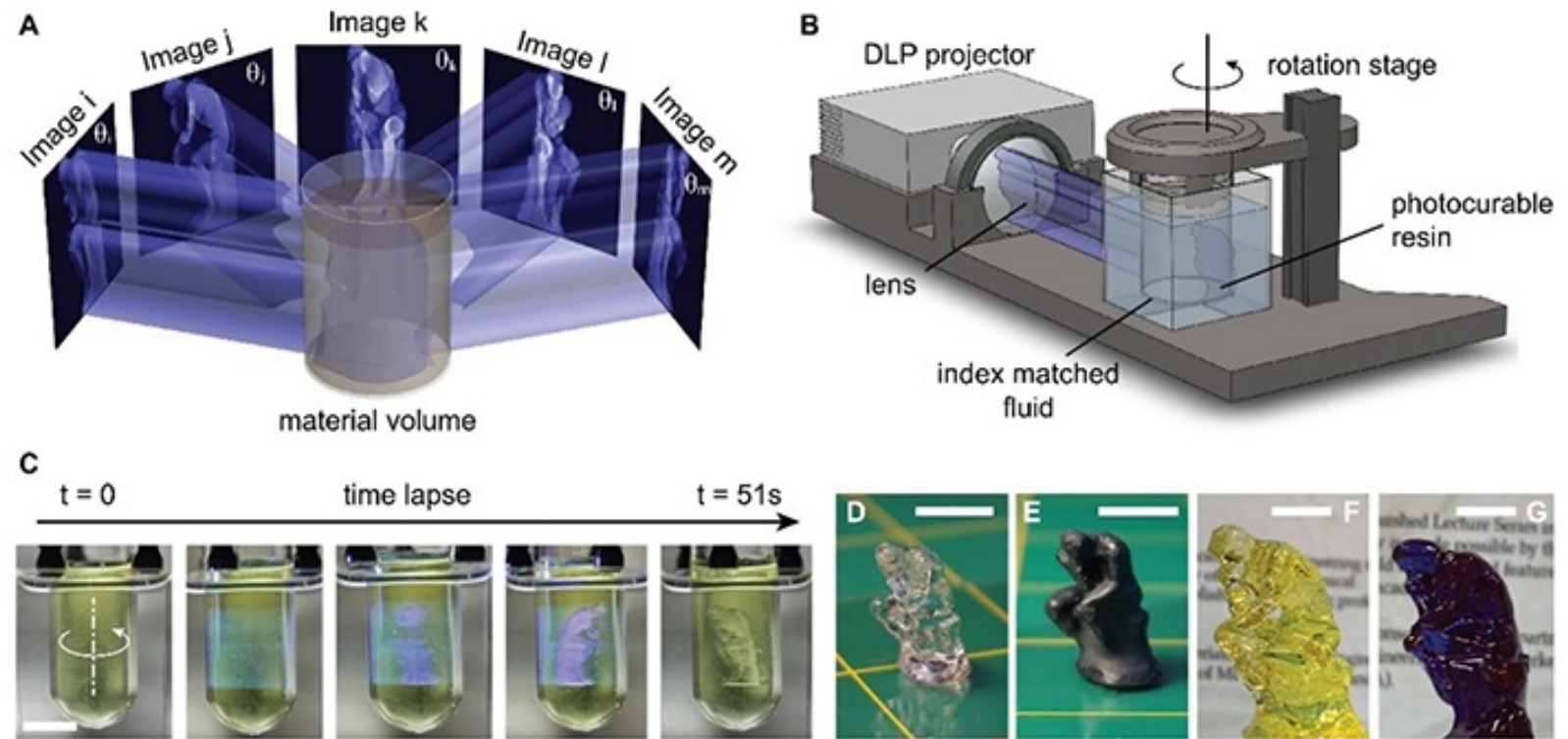


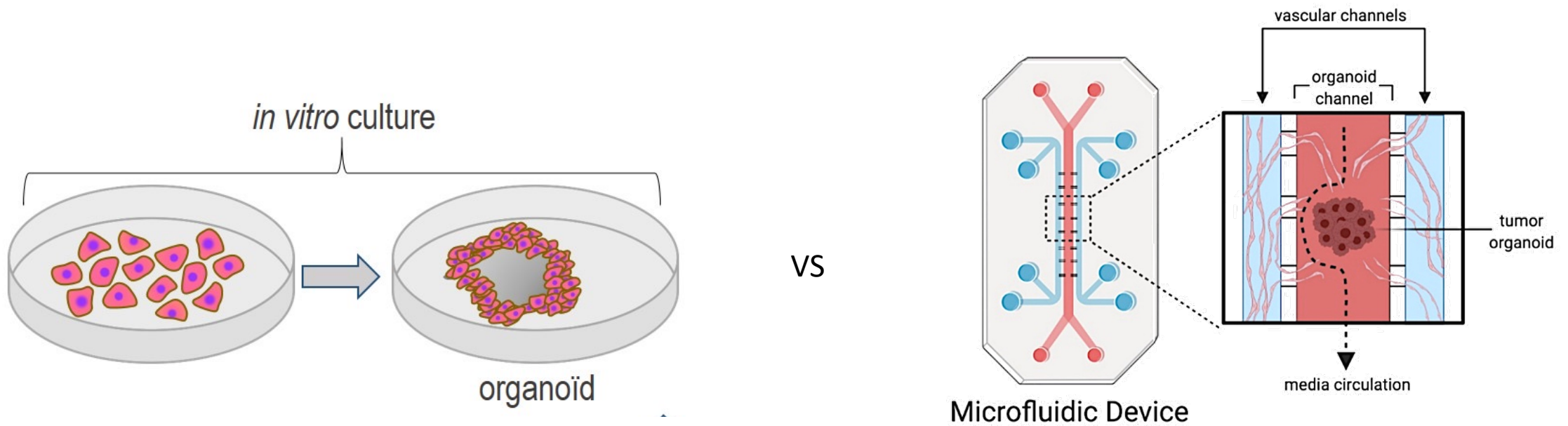
## 4. Laser Machining (rapid prototyping)



# 5. Bioprinting

- Independent of bioink viscosity
- Fast (less than a minute):
  - less photoinitiator;
  - better cell viability;
  - Speed allows for multiple iterations.
- Excellent resolution:
  - approximately  $40\text{ }\mu\text{m}$ , regardless of the size of the object to be printed;
- Minimal contamination risks:
  - Prints on sealed, autoclavable glass vials.
- Suitable for vascular structures





# Why the Micro(fluidic) scale?

10 reasons illustrated by:

- Models/basic physics
- Downscaling/dimensionless numbers
- Examples

# 1. Laminar flow

- In microchannels, flow is laminar
- Reynolds number (Re):
  - ratio inertial/viscous forces
  - Measure for the transition from laminar to turbulent flow
  - Definition:

$$Re = \frac{\rho v D_H}{\mu}$$

$v$  average speed

$D_H$  characteristic length or hydraulic diameter

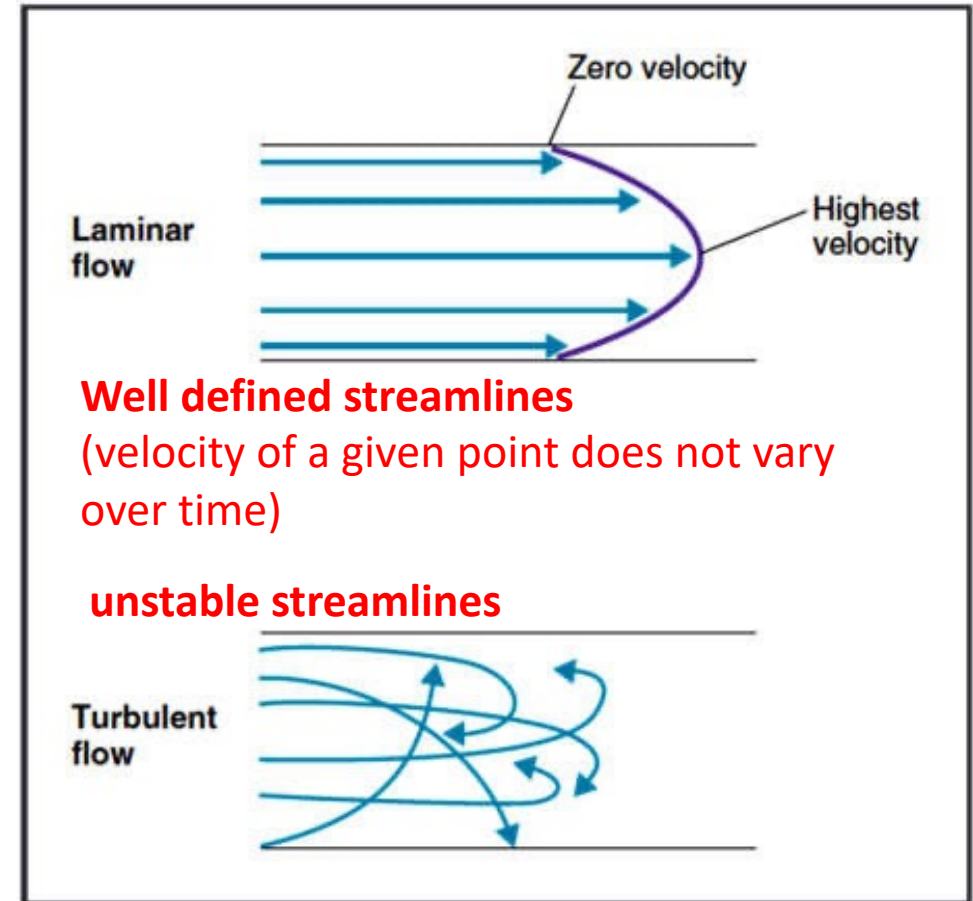
$a$  cross-sectional area

$P$  wetted perimeter

- For a squared ducted:

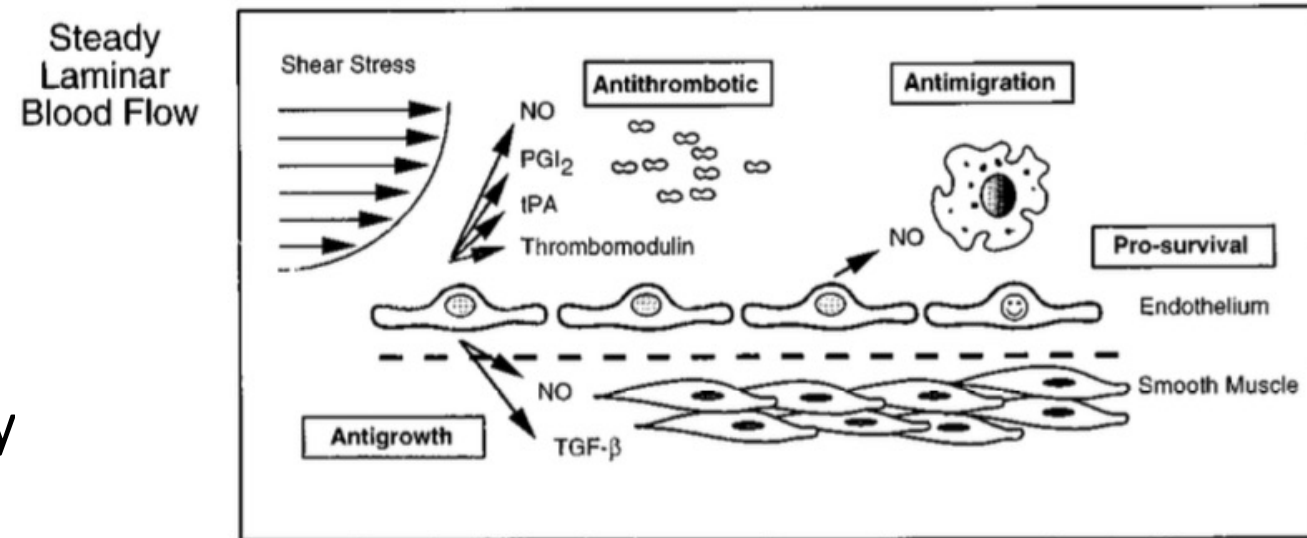
$$D_H = \frac{4 a^2}{4a} = a$$

**Laminar if  $Re < 2000$  and turbulent if  $Re > 4000$**



# Example of laminar flow relevance in Biology

- Controlled shear stress regulates cell behaviour:
  - Steady laminar shear stress** promotes release of **factors** from endothelial cells that inhibit coagulation, migration of leukocytes, and smooth muscle proliferation, while simultaneously promoting endothelial cell survival.
  - no atherosclerosis.





## 2. Diffusion

- Mass transport **by diffusion is a slow process**, but on micrometer scale still fast enough

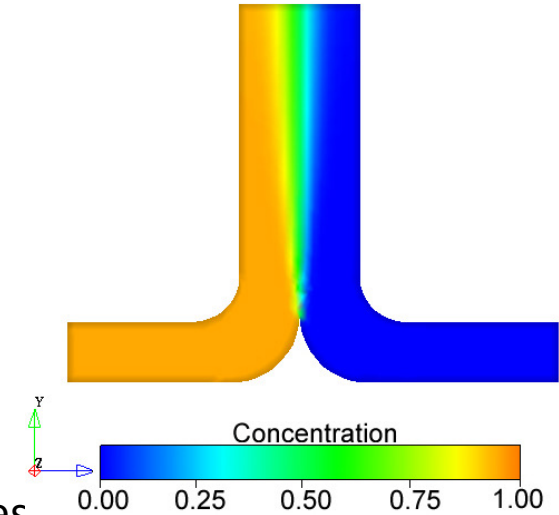
$$d = \sqrt{2 D t}$$

d: distanced travelled by diffusion (m)

D: diffusion coefficient ( $10^{-9} \text{ m}^2/\text{s}$  typical for small molecules,

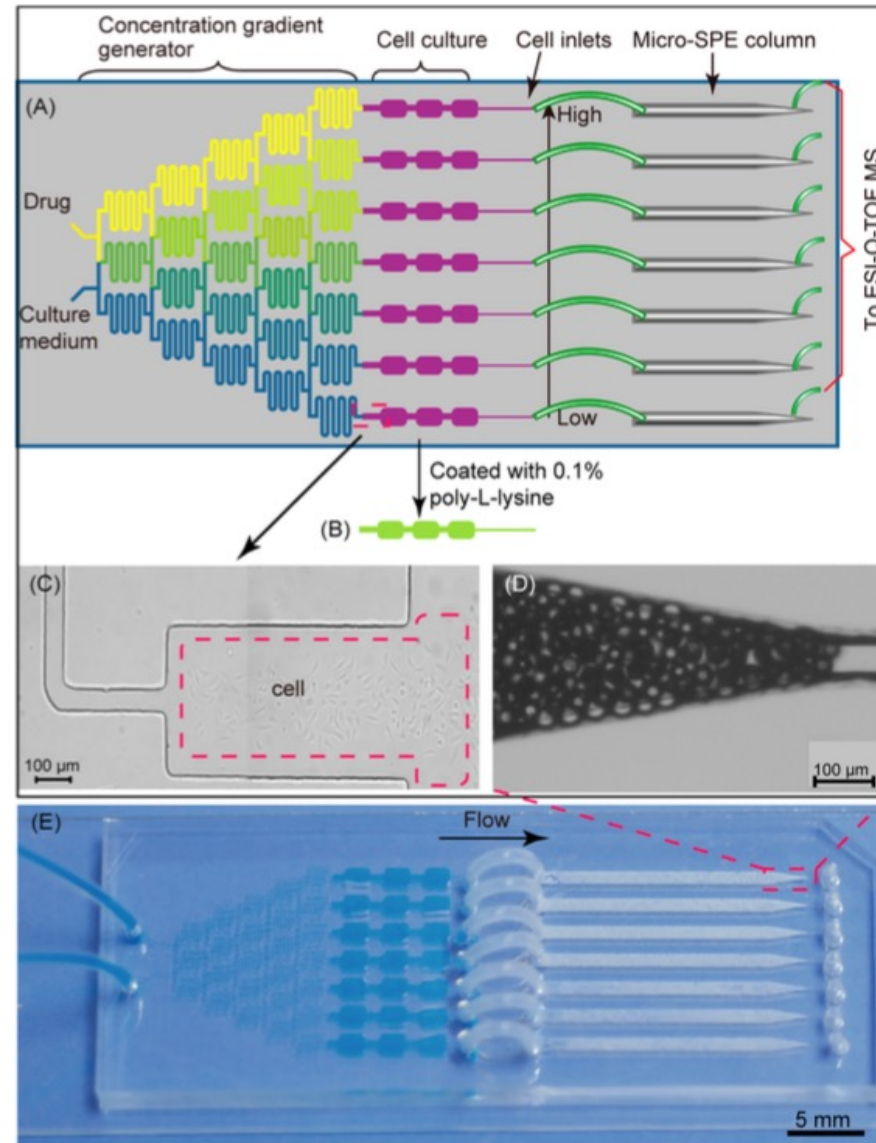
t: time (s)

d	t
45 $\mu\text{m}$	1 s
63 $\mu\text{m}$	2 s
100 $\mu\text{m}$	5 s
500 $\mu\text{m}$	2 min
2.7 mm	1h



Interest: screening of new drug candidates  
Odijk et al. (*Biosensors and Bioelectronics*, 2010)

### 3. High throughput



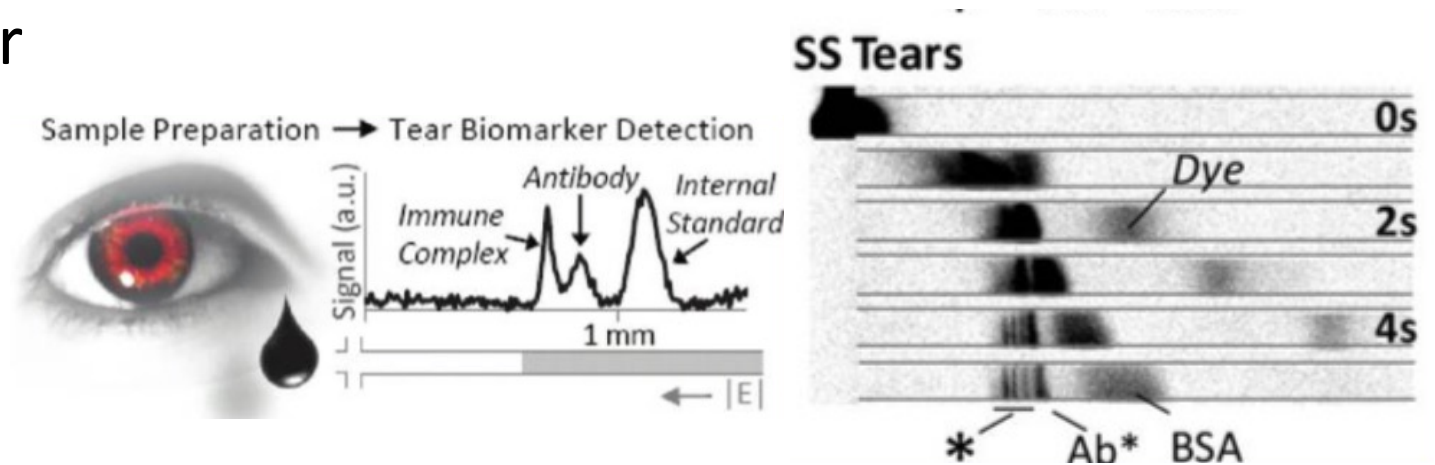
## 4. Less reagent consumption

- Less reagents → less costs
- But also less waste

→ Especially important for

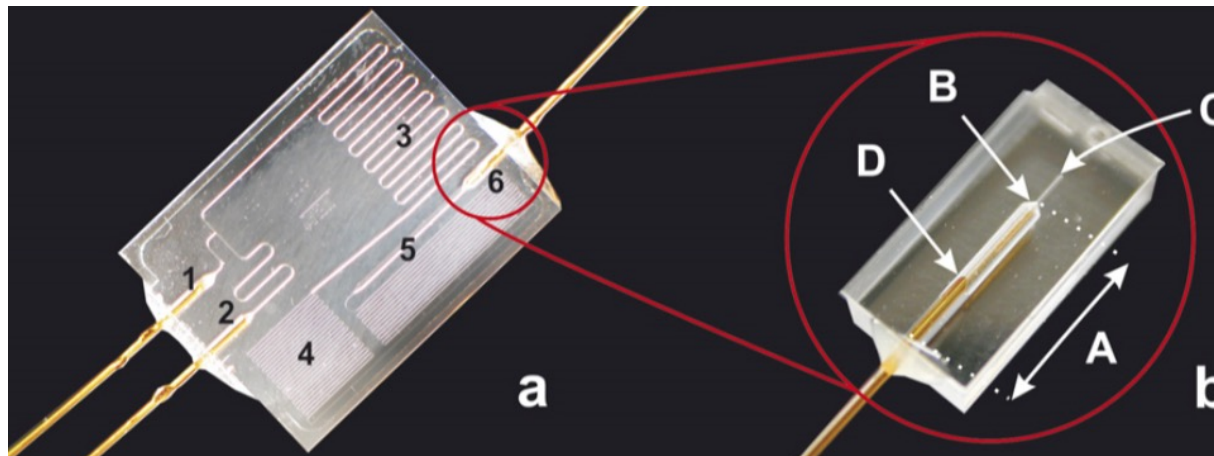
- Expensive samples
- Small volume samples
- Toxic waste products

**Example:** *Lactoferrin (Lf)* is a tear-specific biomarker for *Sjögren's syndrome (SS)*, a serious systemic autoimmune disease currently diagnosed through rudimentary surface chemistry measurements and an invasive lip biopsy.



# 5. Safety

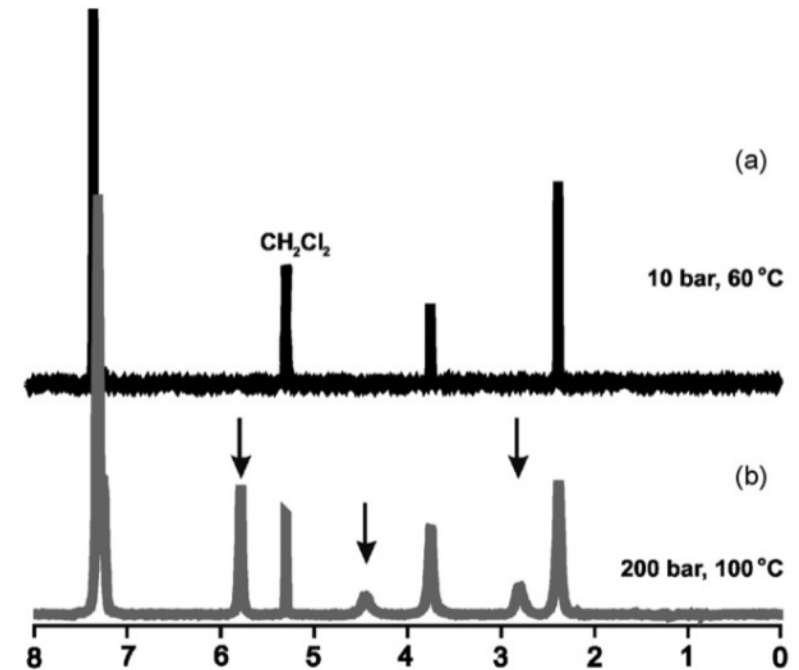
- Enhanced safety because of lower energy stored:
  - At high pressures, a microfluidic platform is only noticed as a small cracking sound
  - When generating explosive reaction products, the volumes involved are too small to cause damage
  - Very toxic compounds are only used in small amounts, so less health risks due to gases, etc.



Tiggelaar RM et al. (*Chemical Engineering Journal*, 2007)

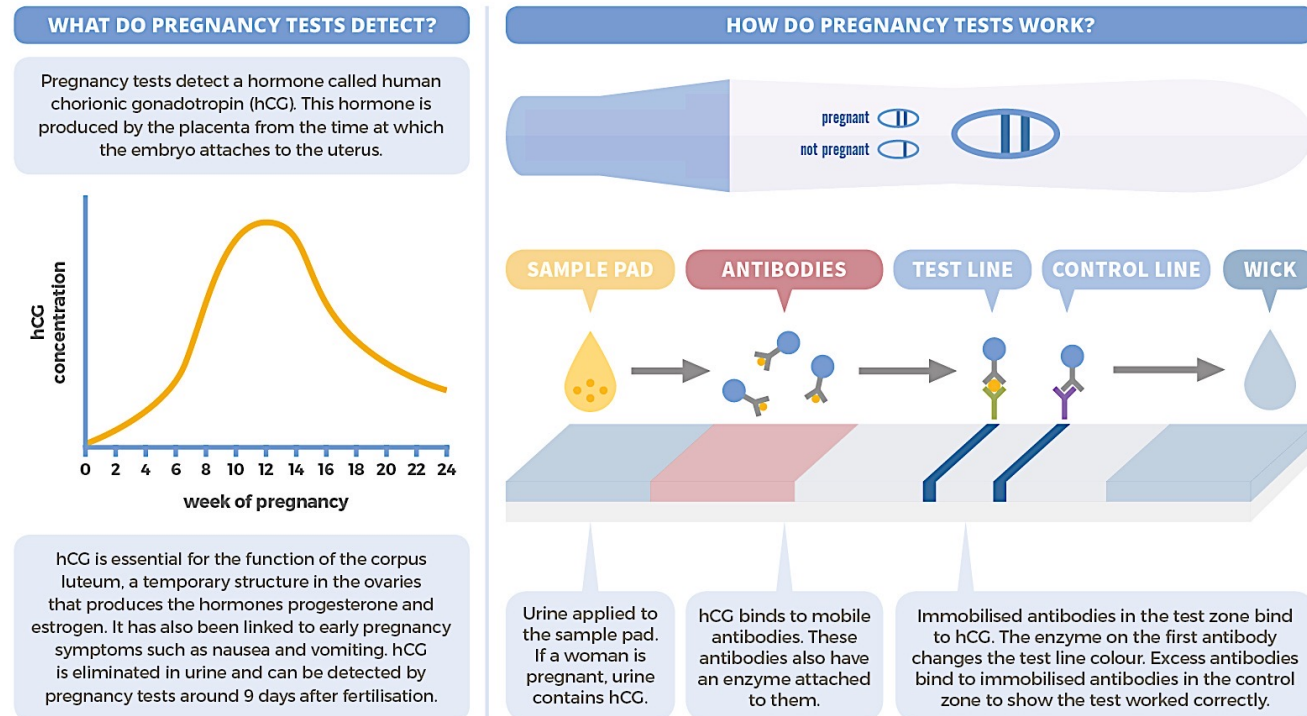


Carbamic acid formation by reaction of *N*-benzyl methanamine ( $\alpha$ ) and  $\text{CO}_2$  ( $\beta$ ).

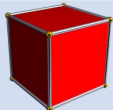


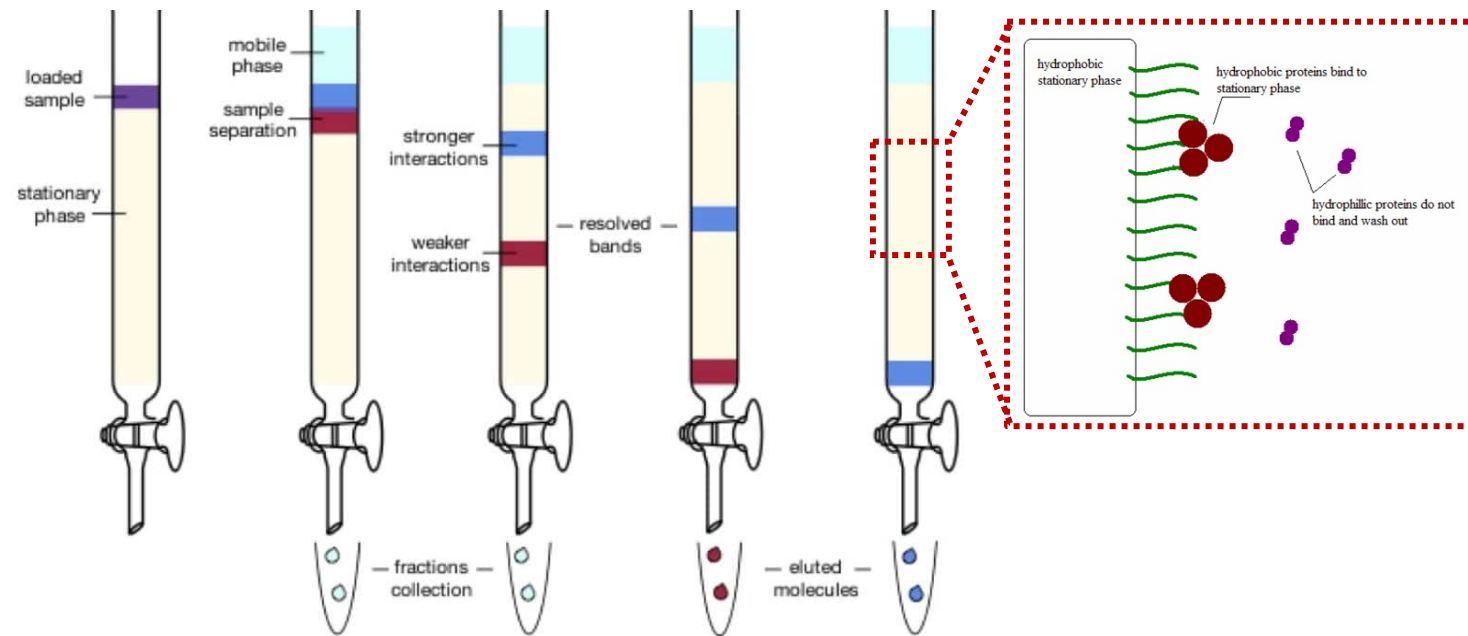
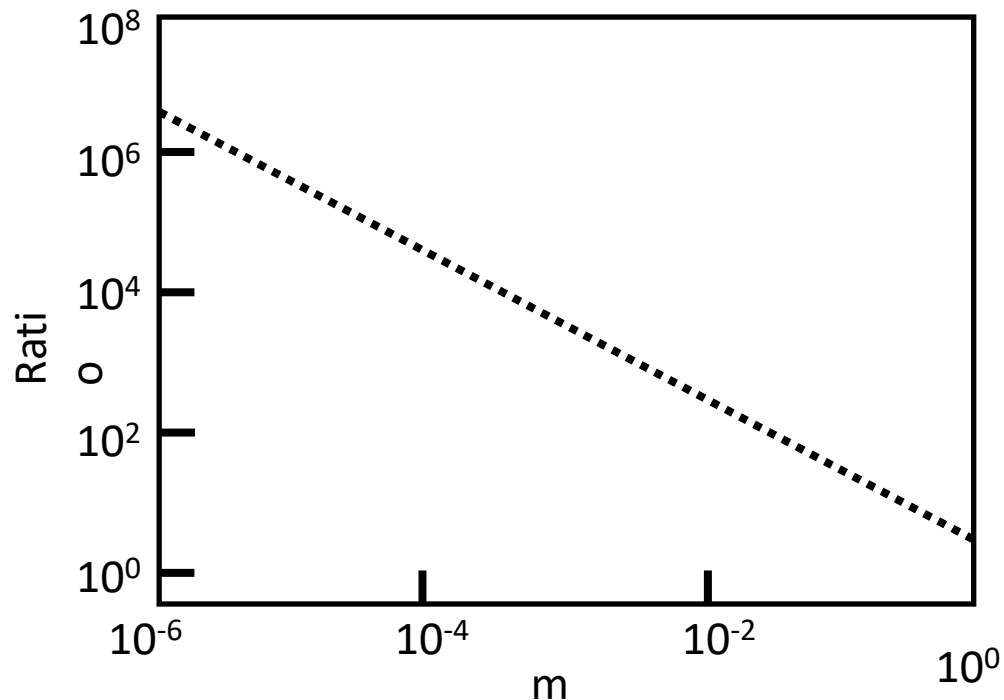
## 6. Portability and disposability

- Disposability: if the chip is only few CHF there is no need for expensive cleaning after measurement  
→ Important in the medical applications for contaminations of other patients



# 7. High surface-to-volume ratio

Shape		Characteristic length $a$	Surface area	Volume	Ratio
Cube		side	$6a^2$	$a^3$	$6/a$

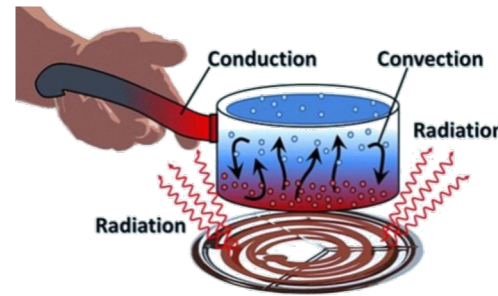


→ A higher ratio implies more interactions with a channel walls

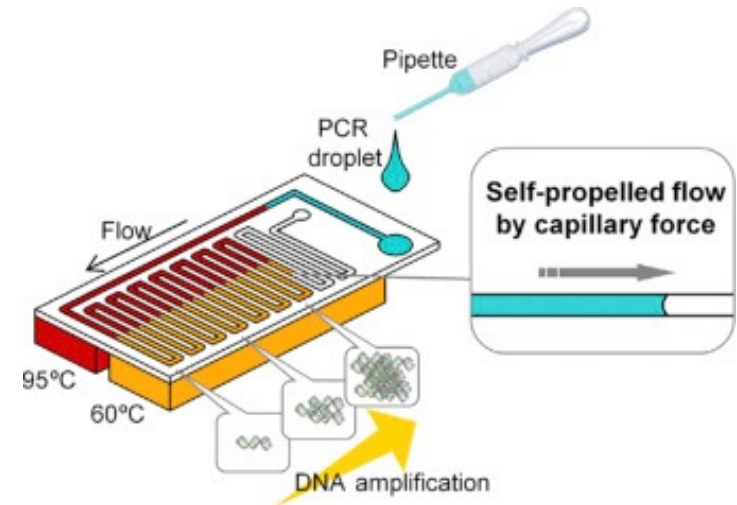


## 8. Better and faster temperature control

- Heat transfer by 3 processes:
  - Conduction
  - Convection
  - Radiation
- In microfluidic platforms, heat is mainly transferred by **conduction**, and this is a fast process due to small dimensions



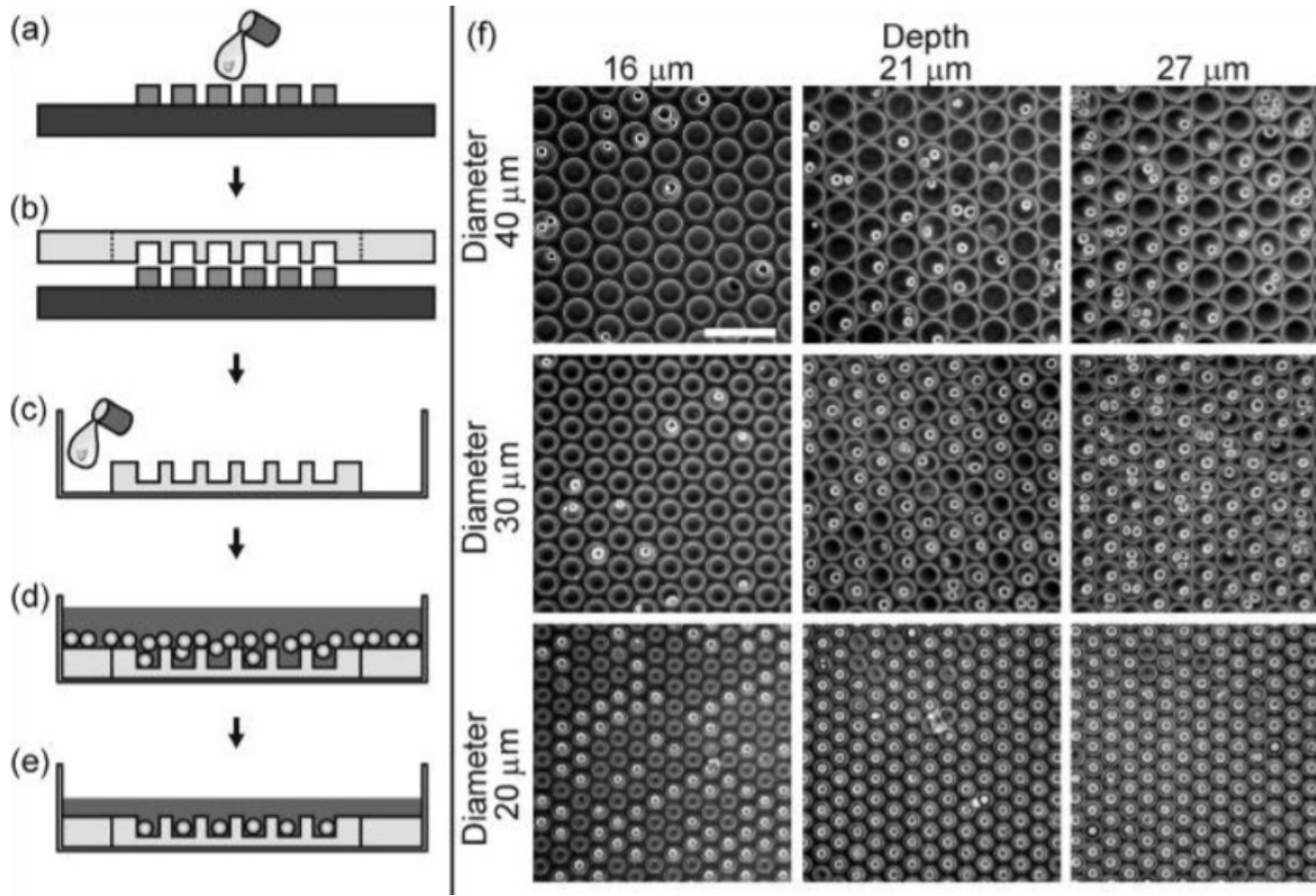
### Example of microfluidic PCR



Ali Shahid et al. (Bioelectronics and Medical Devices, 2019)

$$\frac{\Delta T}{R_{tot}} = \frac{\Delta Q}{\Delta t} \quad R_{tot} = 2 \frac{d_{gl}}{k_{gl}A} + \frac{d_{air}}{k_{air}A}$$
A diagram showing a cross-section of a microfluidic device. It consists of two blue vertical bars labeled 'Glass' and a central grey vertical bar labeled 'Air'. A red line represents the temperature profile, starting at 'T1' on the left glass bar, dipping into the air gap, and rising to 'T2' on the right glass bar.

# 9. Single Cell Analysis



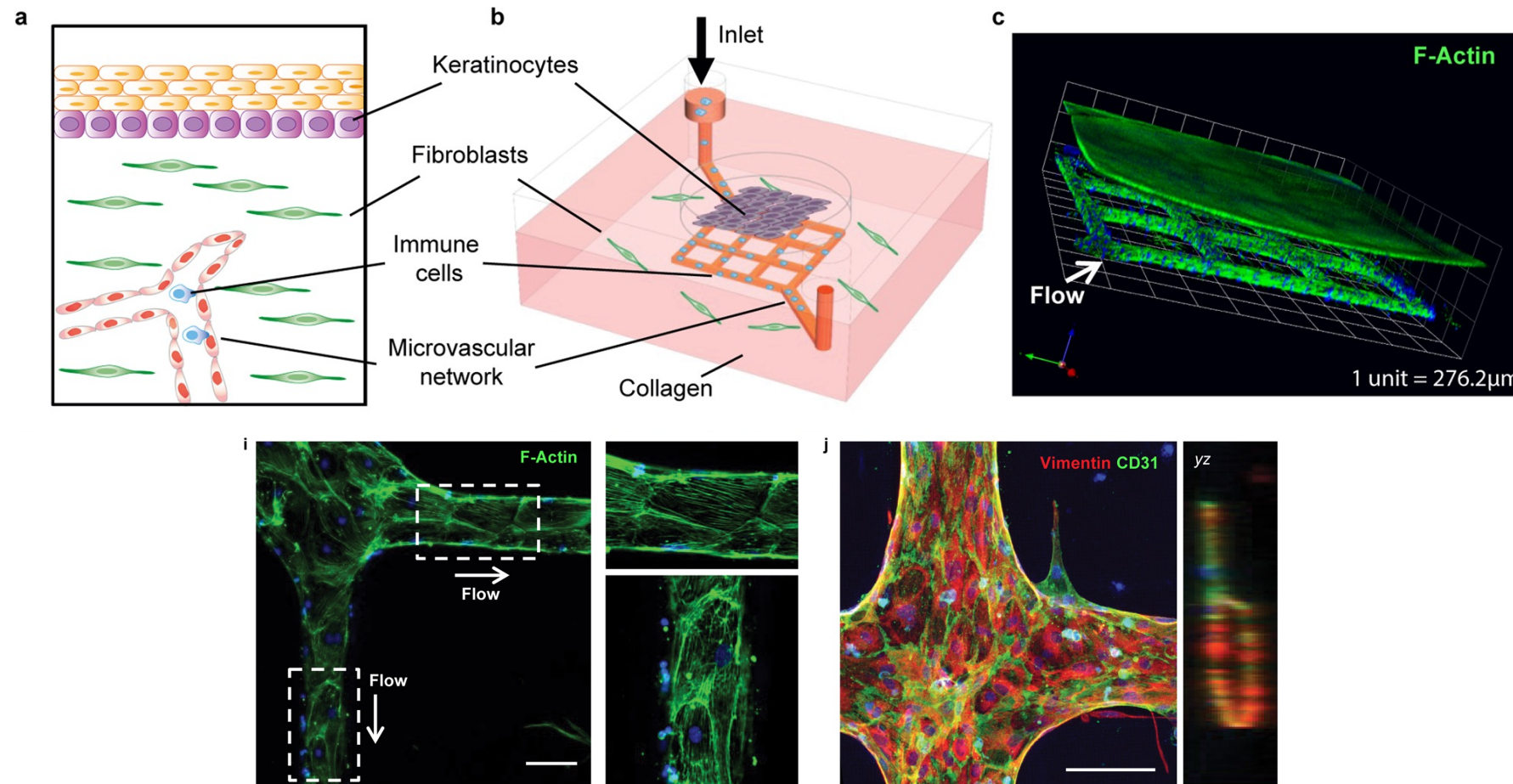
Rettig et al. (*Analytical Chemistry*, 2005)

- Track the changes (missed by bulk sequencing)
- Example: Study the genetic evolution of cancer, as cancer cells are constantly mutating; heterogeneity of cell populations can be observed using single cell sequencing



# 10. Complex tissue organization

«Skin-on-chip» mimicking a stratified epidermis with a dermis perfused by a microvascular network



# Outline

- Part 1
  - What is an organ-on-chip system, its origin and advantages
  - Fabrication methods
  - Why the microfluidic scale?
- Part 2
  - Relevance of mechanobiology
  - Biomechanics in microchip systems
  - Cell response and Analysis (quantification: western blotting, immunochemistry)

# Questions?

End of Part 1