

**Series 9 – Solutions**

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**Chapter 20: Wave Travel and Velocity****Exercise 20.1 – Solution**

If  $\Delta t$  is the mean duration of a cardiac cycle and  $c_0$  is the propagation speed of the pressure wave, the wavelength  $\lambda$  is given by:

$$\lambda = c_0 \cdot \Delta t \quad (1)$$

Using the values from the course notes we obtain:

$$\lambda = 4 \frac{\text{m}}{\text{sec}} \cdot 0.86 \text{ sec} = 3.44 \text{ m} \quad (2)$$

If we compare the pressure wavelength to the length of the arterial system (typically  $\approx 1.7$  m), we observe that the pressure wave created during a cardiac cycle spans the whole arterial tree excluding the interference of a cardiac beat with the next one.

The factors that can modify the value of  $\lambda$  are the propagation speed and the heart rate.

**Exercise 20.2 – Solution**

1) At normal myogenic tone (green curve) and mean pressure  $p_1 = 100$  mmHg (13.33 kPa) the inner diameter is:

$$D_{i,1} = 0.595 \text{ mm} \quad (1)$$

and the lumen area is:

$$A_1 = \frac{\pi D_{i,1}^2}{4} = \frac{\pi \cdot 0.595^2}{4} \text{ mm}^2 \quad (2)$$

The tangent  $\left( \frac{\Delta D_i}{\Delta p} \right)_1$  of the curve at this point is calculated using a central difference:

$$\left( \frac{\Delta D_i}{\Delta p} \right)_1 = \frac{0.6 - 0.58}{14 - 13} = 0.02 \frac{\text{mm}}{\text{kPa}} \quad (3)$$

The area compliance  $C_{A,1}$  at this point is calculated by:

$$C_{A,1} = \frac{\pi D_{i,1}}{2} \left( \frac{\Delta D_i}{\Delta p} \right)_1 = \frac{\pi \cdot 0.595}{2} 0.02 \frac{\text{mm}^2}{\text{kPa}} \quad (4)$$

And finally, taking the blood density  $\rho = 1050 \text{ kgr/m}^3$  the pulse wave velocity  $c_1$  is calculated by the Newton-Young equation:

$$c_1 = \sqrt{\frac{A_1}{\rho C_{A,1}}} = \sqrt{\frac{\frac{\pi \cdot 0.595^2}{4} \text{ mm}^2}{1050 \frac{\text{kgr}}{\text{m}^3} \frac{\pi \cdot 0.595}{2} 0.02 \frac{\text{mm}^2}{\text{kPa}} \frac{1}{1000} \frac{\text{kPa} \cdot \text{m} \cdot \text{sec}^2}{\text{kgr}}}} = 3.764 \frac{\text{m}}{\text{sec}} \quad (5)$$

2) After a strong dose of norepinephrine (still green curve) the mean pressure is raised to  $p_2 = 150 \text{ mmHg}$  (20 kPa) and the inner diameter becomes:

$$D_{i,2} = 0.655 \text{ mm} \quad (6)$$

and the lumen area is:

$$A_2 = \frac{\pi D_{i,2}^2}{4} = \frac{\pi \cdot 0.655^2}{4} \text{ mm}^2 \quad (7)$$

The tangent  $\left( \frac{\Delta D_i}{\Delta p} \right)_2$  of the curve at this point is calculated using a central difference:

$$\left( \frac{\Delta D_i}{\Delta p} \right)_2 = \frac{0.665 - 0.645}{21 - 19} = 0.01 \frac{\text{mm}}{\text{kPa}} \quad (8)$$

The area compliance  $C_{A,2}$  at this point is calculated by:

$$C_{A,2} = \frac{\pi D_{i,2}}{2} \left( \frac{\Delta D_i}{\Delta p} \right)_2 = \frac{\pi \cdot 0.655}{2} 0.01 \frac{\text{mm}^2}{\text{kPa}} \quad (9)$$

And finally, taking the blood density  $\rho = 1050 \text{ kgr/m}^3$  the new value of the pulse wave velocity  $c_2$  is calculated by the Newton-Young equation:

$$c_2 = \sqrt{\frac{A_2}{\rho C_{A,2}}} = \sqrt{\frac{\frac{\pi \cdot 0.655^2}{4} \text{ mm}^2}{1050 \frac{\text{kgr}}{\text{m}^3} \frac{\pi \cdot 0.655}{2} 0.01 \frac{\text{mm}^2}{\text{kPa}} \frac{1}{1000} \frac{\text{kPa} \cdot \text{m} \cdot \text{sec}^2}{\text{kgr}}}} = 5.585 \frac{\text{m}}{\text{sec}} \quad (10)$$

So we observe that an increase in pressure due to a strong dose of norepinephrine decreases the compliance of the arterial wall ( $C_{A,2} < C_{A,1}$ ) and this in turn results in a higher pulse wave velocity ( $c_2 > c_1$ ).

3) Following the increase in pressure to  $p_2 = 150$  mmHg (20 kPa) the artery develops very strong myogenic tone and reaches maximal contraction (red curve). The inner diameter becomes:

$$D_{i,3} = 0.630 \text{ mm} \quad (11)$$

and the lumen area is:

$$A_3 = \frac{\pi D_{i,3}^2}{4} = \frac{\pi \cdot 0.630^2}{4} \text{ mm}^2 \quad (12)$$

The tangent  $\left( \frac{\Delta D_i}{\Delta p} \right)_3$  of the curve at this point is calculated using a central difference:

$$\left( \frac{\Delta D_i}{\Delta p} \right)_3 = \frac{0.640 - 0.605}{21 - 19} = 0.0175 \frac{\text{mm}}{\text{kPa}} \quad (13)$$

The area compliance  $C_{A,3}$  at this point is calculated by:

$$C_{A,3} = \frac{\pi D_{i,3}}{2} \left( \frac{\Delta D_i}{\Delta p} \right)_3 = \frac{\pi \cdot 0.630}{2} 0.0175 \frac{\text{mm}^2}{\text{kPa}} \quad (14)$$

And finally, taking the blood density  $\rho = 1050 \text{ kgr/m}^3$  the new value of the pulse wave velocity  $c_3$  is calculated by the Newton-Young equation:

$$c_3 = \sqrt{\frac{A_3}{\rho C_{A,3}}} = \sqrt{\frac{\frac{\pi \cdot 0.630^2}{4} \text{ mm}^2}{1050 \frac{\text{kgr}}{\text{m}^3} \frac{\pi \cdot 0.630}{2} 0.0175 \frac{\text{mm}^2}{\text{kPa}} \frac{1}{1000} \frac{\text{kPa} \cdot \text{m} \cdot \text{sec}^2}{\text{kgr}}}} = 4.140 \frac{\text{m}}{\text{sec}} \quad (15)$$

So we observe that an increase in myogenic tone under constant pressure increases the compliance of the arterial wall ( $C_{A,3} > C_{A,2}$ ) and this in turn results in a lower pulse wave velocity ( $c_3 < c_2$ ).

4a) The incremental elastic modulus  $E_{inc,1}$  under normal myogenic tone (green curve) and mean pressure  $p_1 = 100$  mmHg (13.33 kPa) is calculated by the Moens-Korteweg equation:

$$E_{inc,1} = \frac{c_1^2 \rho}{\frac{h_1}{D_{i,1}}} = \frac{3.764^2 \frac{\text{m}^2}{\text{sec}^2} 1050 \frac{\text{kgr}}{\text{m}^3} \frac{1}{1000} \frac{\text{kPa} \cdot \text{m} \cdot \text{sec}^2}{\text{kgr}}}{\frac{1}{10}} = 148.761 \text{ kPa} \quad (16)$$

where  $h_1$  is the thickness of the arterial wall under these conditions. The outer diameter is:

$$D_{o,1} = D_{i,1} + 2h_1 = D_{i,1} + 2D_{i,1}/10 = 0.595 + 2 \cdot 0.595/10 = 0.714 \text{ mm} \quad (17)$$

4b) We employ the incompressibility condition (conservation of cross-sectional area) to calculate the outer diameter  $D_{o,2}$  under normal myogenic tone (green curve) and mean pressure  $p_2 = 150 \text{ mmHg}$  (20 kPa):

$$\begin{aligned} \frac{\pi}{4}(D_{o,2}^2 - D_{i,2}^2) &= \frac{\pi}{4}(D_{o,1}^2 - D_{i,1}^2) \Rightarrow \\ \Rightarrow D_{o,2} &= \sqrt{D_{i,2}^2 + D_{o,1}^2 - D_{i,1}^2} = \sqrt{0.655^2 + 0.714^2 - 0.595^2} = 0.765 \text{ mm} \end{aligned} \quad (18)$$

The ratio of thickness to diameter then becomes:

$$\frac{h_2}{D_{i,2}} = \frac{D_{o,2} - D_{i,2}}{2D_{i,2}} = \frac{0.765 - 0.655}{2 \cdot 0.655} = 0.084 \quad (19)$$

The new value of incremental elastic modulus  $E_{inc,2}$  is calculated by the Moens-Korteweg equation:

$$E_{inc,2} = \frac{c_2^2 \rho}{\frac{h_2}{D_{i,2}}} = \frac{5.585^2 \frac{\text{m}^2}{\text{sec}^2} 1050 \frac{\text{kg}}{\text{m}^3} \frac{1}{1000} \frac{\text{kPa} \cdot \text{m} \cdot \text{sec}^2}{\text{kg}}}{0.084} = 389.903 \text{ kPa} \quad (20)$$

4c) We employ the incompressibility condition (conservation of cross-sectional area) to calculate the outer diameter  $D_{o,3}$  under maximal contraction (red curve) and mean pressure  $p_2 = 150 \text{ mmHg}$  (20 kPa):

$$\begin{aligned} \frac{\pi}{4}(D_{o,3}^2 - D_{i,3}^2) &= \frac{\pi}{4}(D_{o,1}^2 - D_{i,1}^2) \Rightarrow \\ \Rightarrow D_{o,3} &= \sqrt{D_{i,3}^2 + D_{o,1}^2 - D_{i,1}^2} = \sqrt{0.630^2 + 0.714^2 - 0.595^2} = 0.743 \text{ mm} \end{aligned} \quad (21)$$

The ratio of thickness to diameter then becomes:

$$\frac{h_3}{D_{i,3}} = \frac{D_{o,3} - D_{i,3}}{2D_{i,3}} = \frac{0.743 - 0.630}{2 \cdot 0.630} = 0.090 \quad (22)$$

The new value of incremental elastic modulus  $E_{inc,3}$  is calculated by the Moens-Korteweg equation:

$$E_{inc,3} = \frac{c_3^2 \rho}{\frac{h_3}{D_{i,3}}} = \frac{4.140^2 \frac{\text{m}^2}{\text{sec}^2} 1050 \frac{\text{kg}}{\text{m}^3} \frac{1}{1000} \frac{\text{kPa} \cdot \text{m} \cdot \text{sec}^2}{\text{kg}}}{0.090} = 199.962 \text{ kPa} \quad (23)$$