

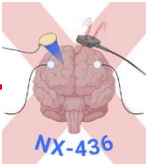


# NIBS and multimodal imaging II

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Ecole Federale Polytechnique de Lausanne (EPFL)

Department of Clinical Neuroscience, University Hospital of Geneva



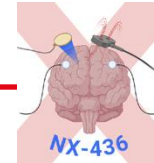
Why combining neuroimaging with brain stimulation?

Why simultaneous NIBS and neuroimaging?

Challenges and Opportunities

Safety

Examples of application

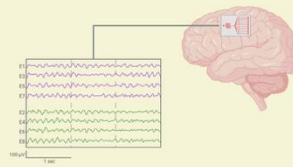


## INVASIVE

## NON-INVASIVE

**Neurosensing/ Neuro-monitoring  
"READ"**

Monitors electrical/BOLD activity in the central nervous system



eCoG, iEEG



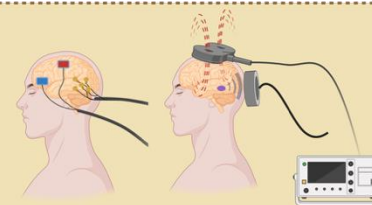
EEG, MEG, fMRI

**Neuromodulation  
"WRITE"**

Targets and improves functions such as motor, attention, memory, decision-making, self-regulation either electrically, magnetically or via ultrasound



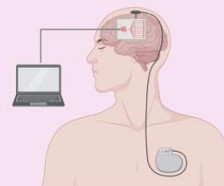
DBS



TMS, tES, TUS

**Combinatory (bidirectional)  
"READ + WRITE"**

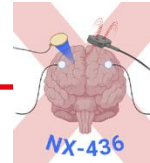
Monitors and reacts to brain states with prosthetics, robotics, brain stimulation



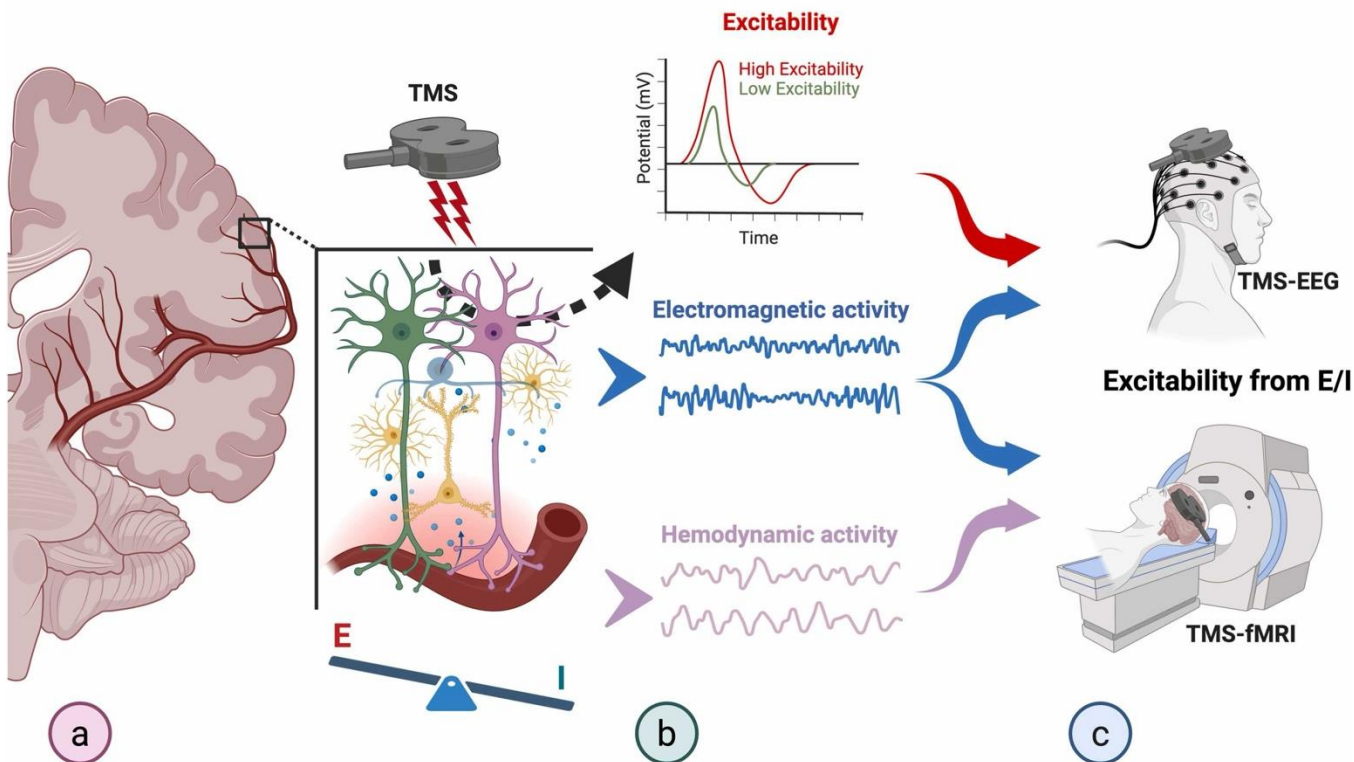
Closed-loop DBS



BCI, BBI, ...

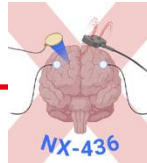


## Physiological Proxies for Excitability





What are the potential benefits of multimodal imaging combined with neuromodulation?



## **Recording of brain activity simultaneously**

- target validation (especially relevant for nDBS)
- understanding of topographic specificity
- focally and at the network level
- adds to mechanistic understanding
- safety monitoring
- state dependent close-loop applications

## **Online interference with brain activity**

- causal understanding
- network vs. local effects
- state dependent close-loop applications

## **Target selection for brain stimulation**

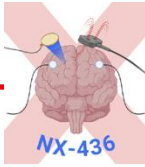
- personalization

## **Parameter selection for brain stimulation**

- personalization

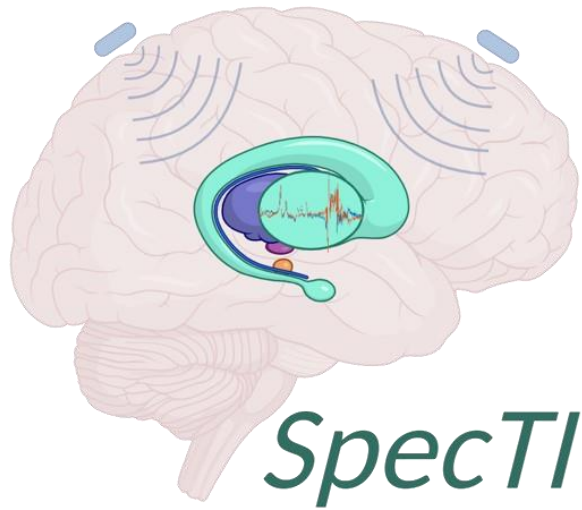


What are the disadvantages and challenges of multimodal imaging combined with neuromodulation?

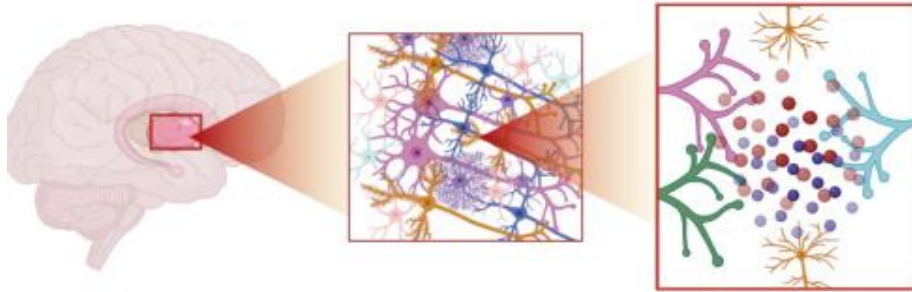
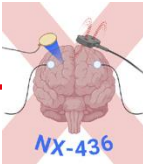


## Disadvantages and Challenges

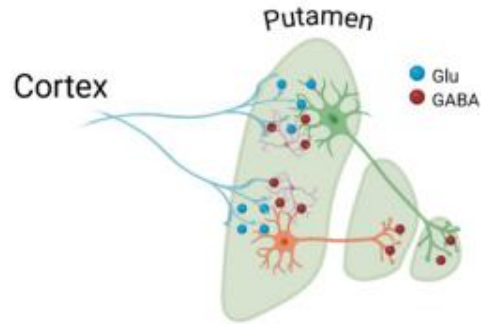
- technologically challenging
- temporal, spatial resolution
- safety
- artefacts
- feasibility
- accessibility, clinical translation
- cost
- reporting



- Provides information about neurotransmitter levels, e.g. GABA, Glutamate
- Predefined volume, whole brain analyses not possible
- Temporal resolution low (minutes)
- Usually performed in resting state
- Task-related evaluation challenging due to low temporal resolution
- Accessibility limited
- Costly



- Measure the concentrations of neurotransmitters in a given region

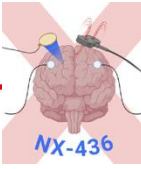


- Striatal circuits are largely GABAergic with cortical Glutamatergic inputs

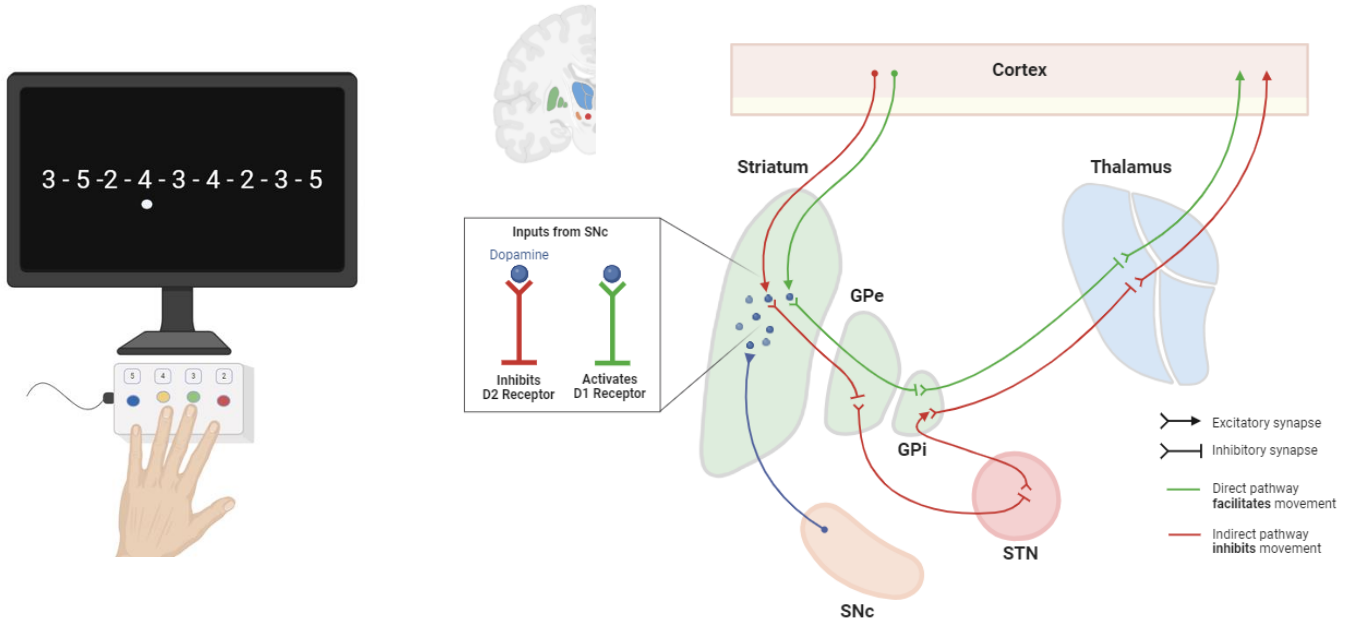


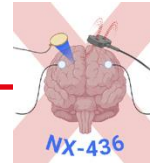
**How does striatal tTIS modulate these circuits to enhance motor learning?**



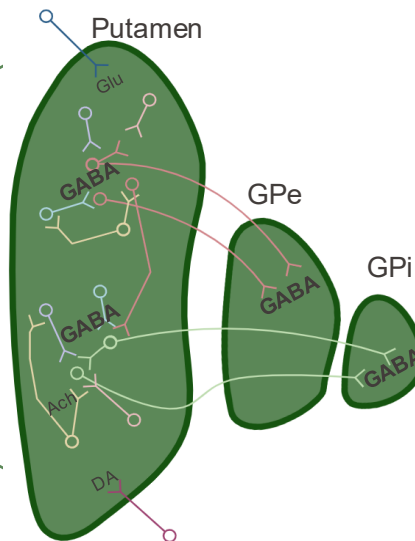
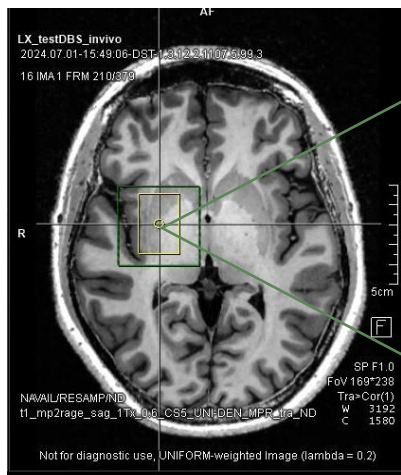


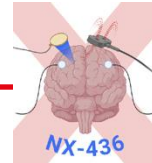
- How does striatal tTIS modulate neuromodulator levels in the putamen?
- How does this differ when performing a motor learning task?



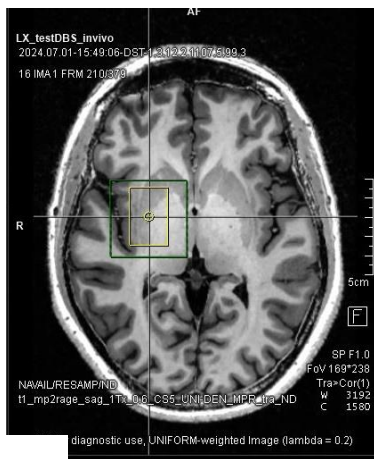


- Majority of neurons in Putamen are GABAergic
  - Medium spiny projection neurons
  - GABAergic Interneurons
  - Glutamate-ergic cortical inputs





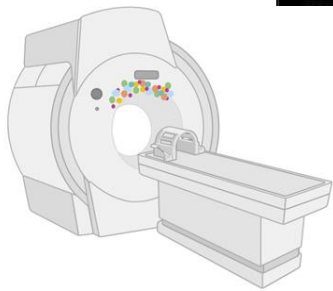
- Record functional MR spectroscopy of the Putamen at 7T

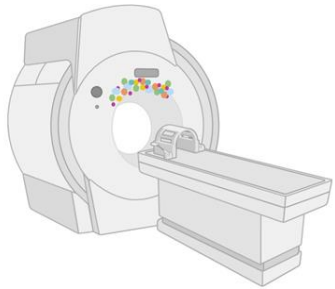
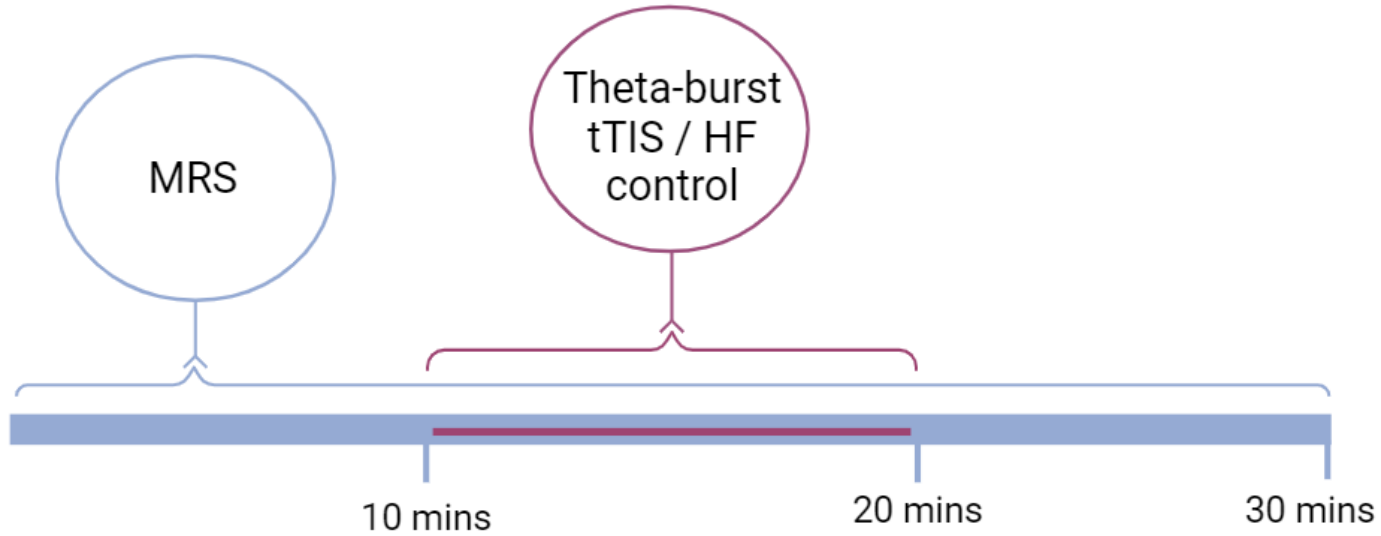
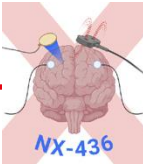


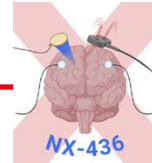
Resting state

Pre-stimulation  
fMRSTheta-burst  
tTIS / HF control  
+ fMRSPost-stimulation  
fMRS

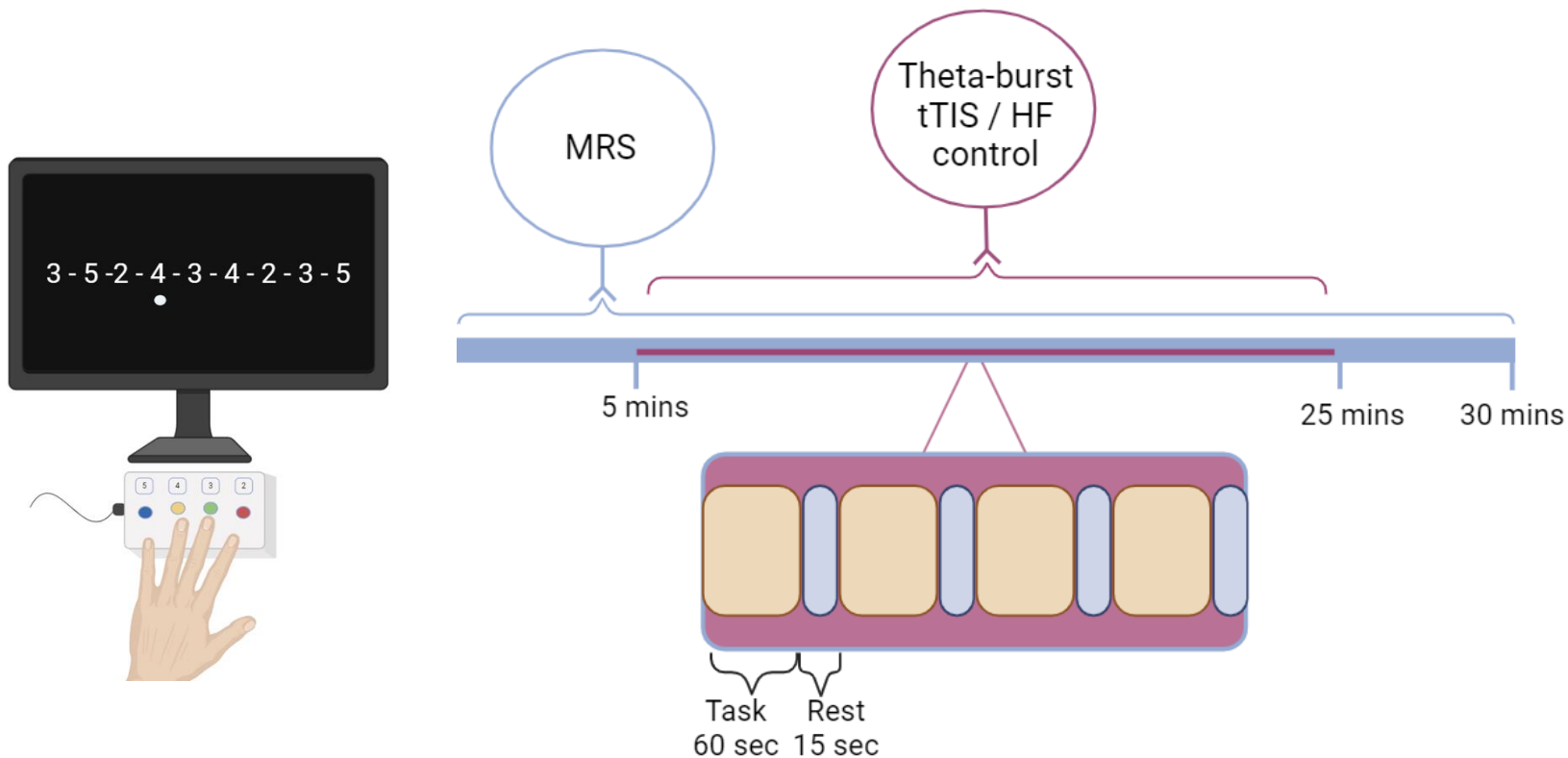
Task-based

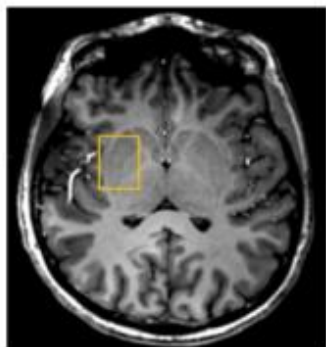
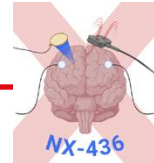
Pre-stimulation  
fMRSTheta-burst  
tTIS / HF control  
+ Task + fMRSPost-stimulation  
fMRS





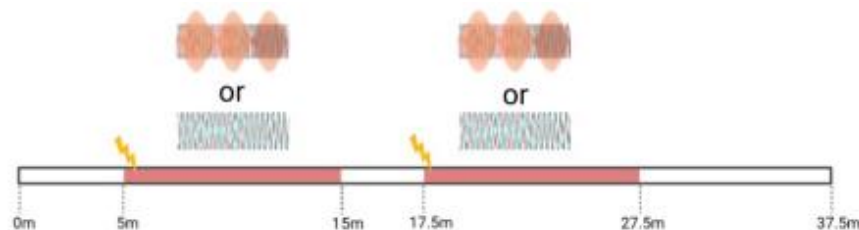
- Sequential finger tapping task to motor learning





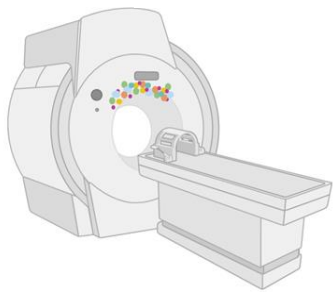
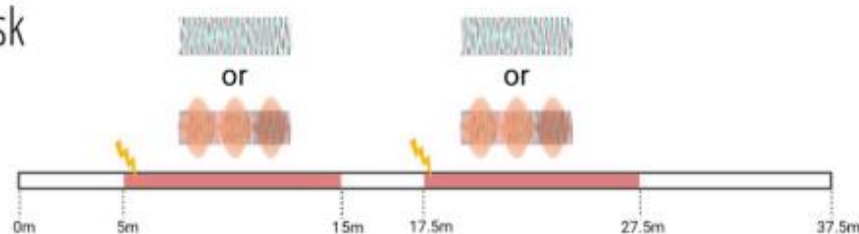
Resting state

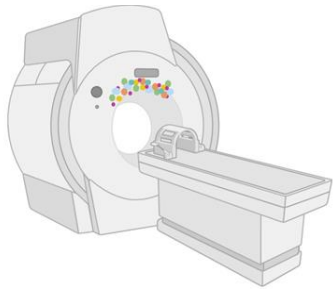
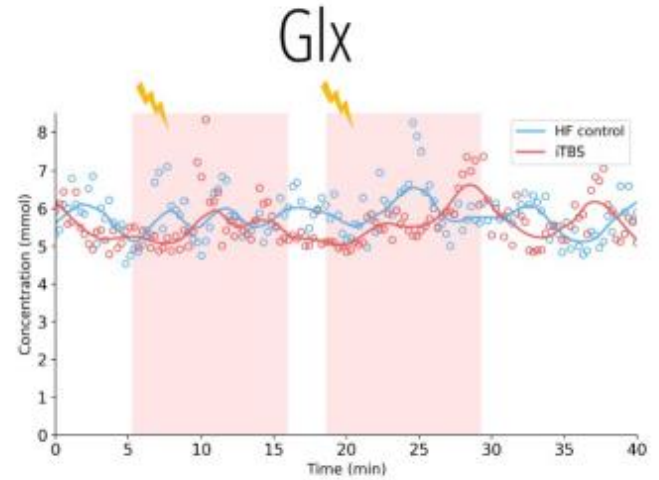
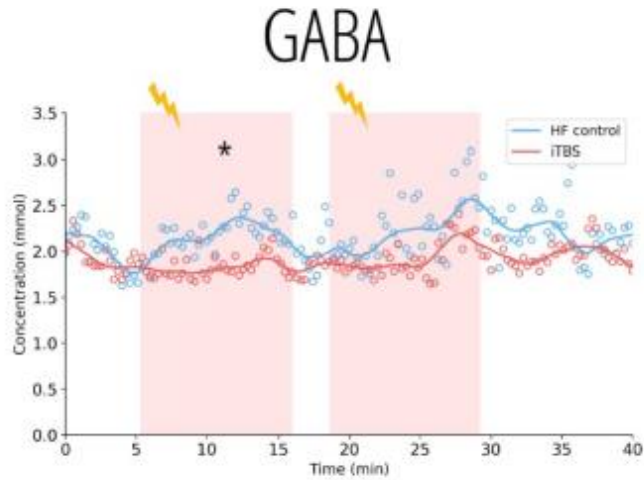
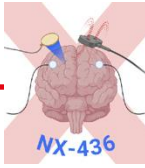
x2

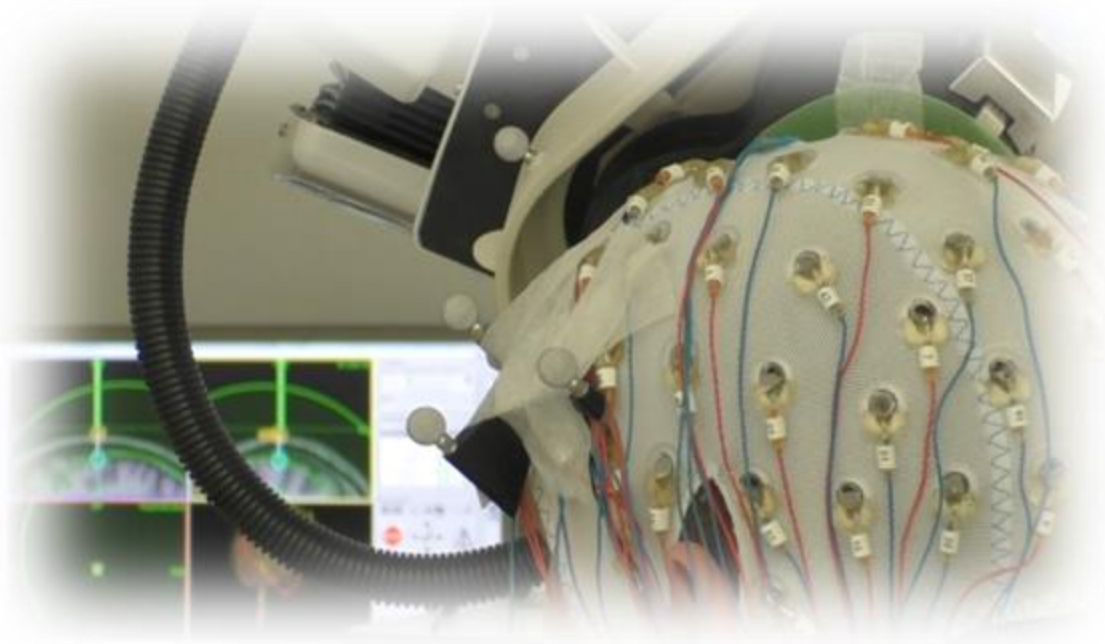
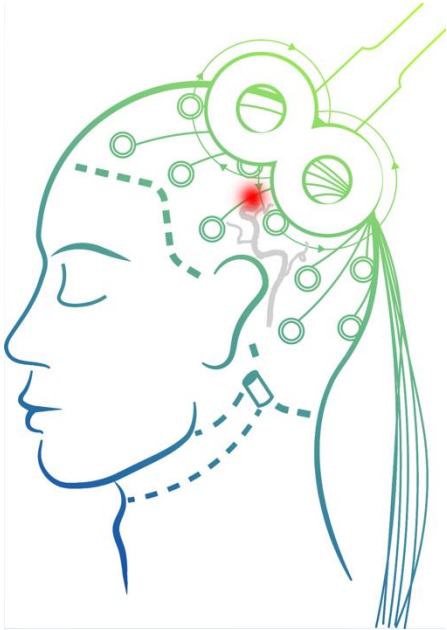
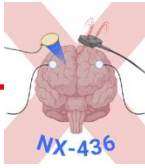


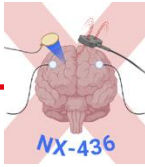
Motor learning task

x2









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## Clinical Neurophysiology

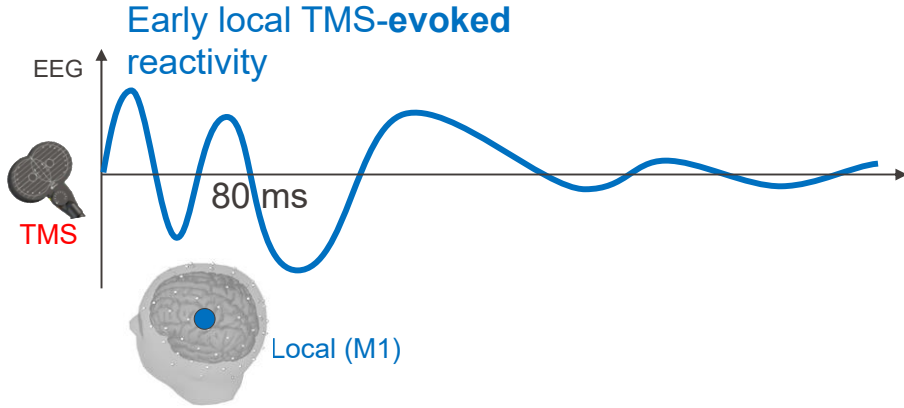
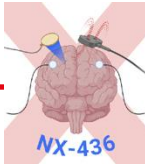
journal homepage: [www.elsevier.com/locate/clinph](http://www.elsevier.com/locate/clinph)

Review

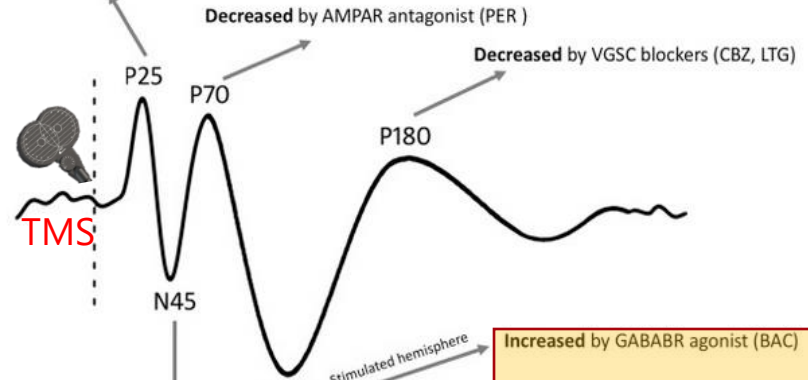
### Clinical utility and prospective of TMS–EEG

Sara Tremblay<sup>a,b,\*</sup>, Nigel C. Rogasch<sup>c</sup>, Isabella Premoli<sup>d</sup>, Daniel M. Blumberger<sup>a</sup>,  
Silvia Casarotto<sup>e</sup>, Robert Chen<sup>f</sup>, Vincenzo Di Lazzaro<sup>g</sup>, Faranak Farzan<sup>h</sup>, Fabio Ferrarelli<sup>i</sup>,  
Paul B. Fitzgerald<sup>j,k</sup>, Jeanette Hui<sup>a</sup>, Risto J. Ilmoniemi<sup>l</sup>, Vasilios K. Kimiskidis<sup>m</sup>,  
Dimitris Kugiumtzis<sup>n</sup>, Pantelis Lioumis<sup>a</sup>, Alvaro Pascual-Leone<sup>o</sup>, Maria Concetta Pellicciari<sup>p</sup>,  
Tarek Rajji<sup>a</sup>, Gregor Thut<sup>q</sup>, Reza Zomorodi<sup>a</sup>, Ulf Ziemann<sup>r</sup>, Zafiris J. Daskalakis<sup>a</sup>





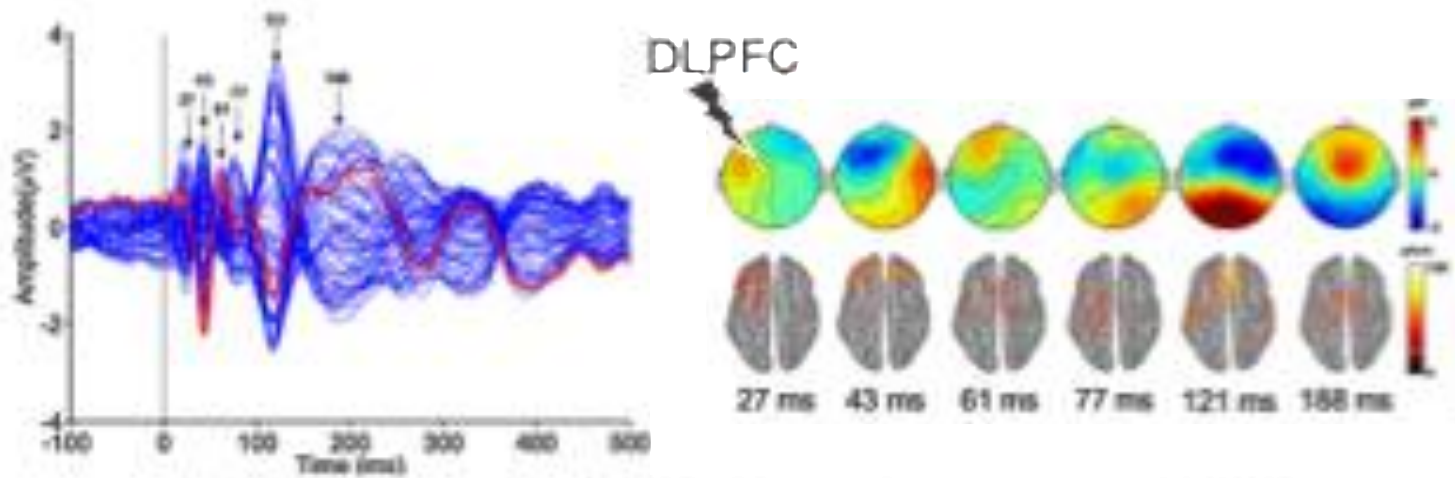
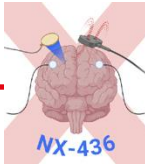
Correlates with MEP amplitude;  
**decreased** by VGSC blockers (CBZ)



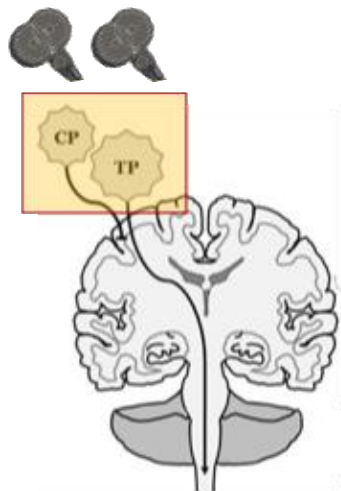
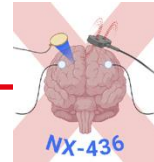
**Increased** by positive modulators of GABAARs (ALP, DZP, ZLP) and NMDAR antagonist (DMO);  
**decreased** by  $\alpha 5$ -GABAAR antagonist (S44819)

**Increased** by GABABR agonist (BAC)

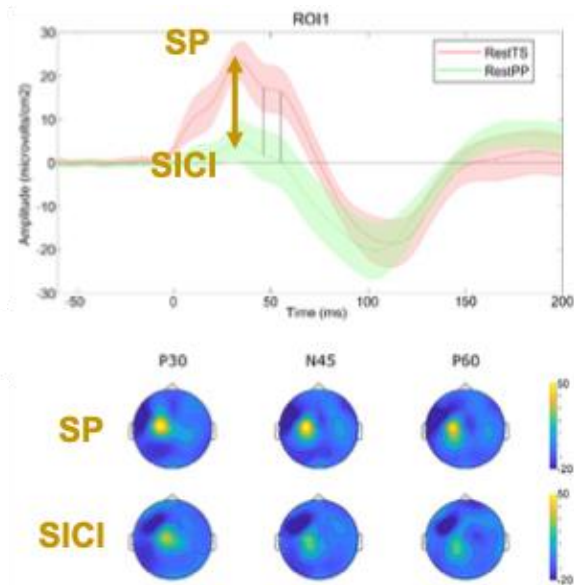
**Decreased** by positive modulators of GABAARs (ALP, DZP) and inhibitors of presynaptic excitatory transmitter release (BRV, LEV)



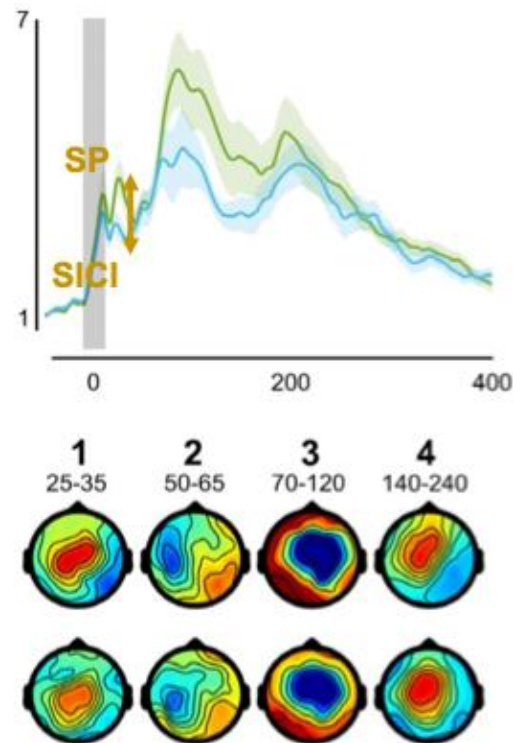
TEPs = local activity + remote connectivity



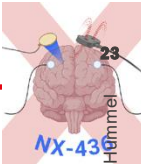
Short-Interval Cortical  
inhibition (SICI)



Leodori *et al.*, 2019



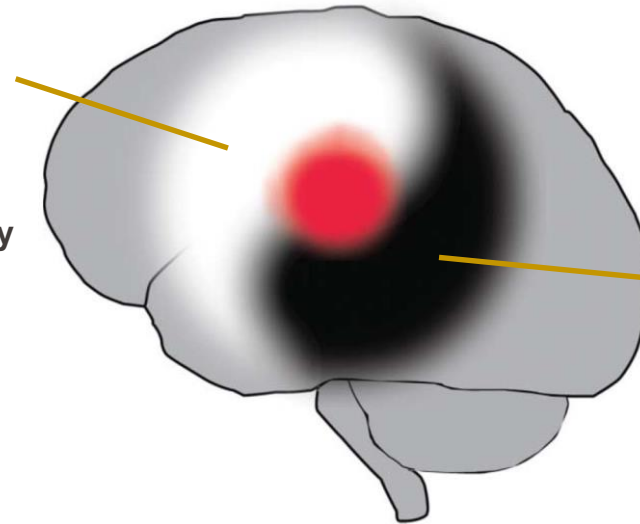
Raffin & Harquel *et al.*, 2020



## Animal Models

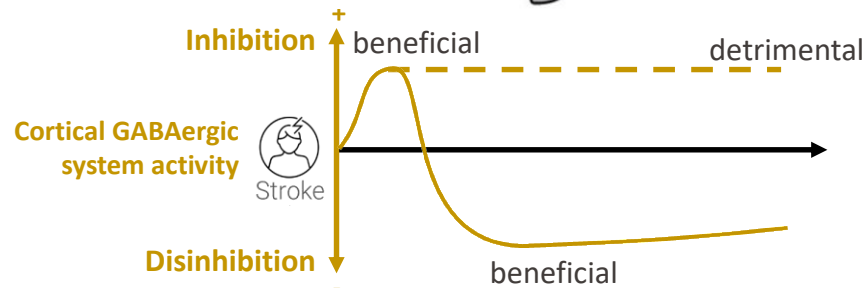
- Tonic Hyperinhibition
- Low excitability

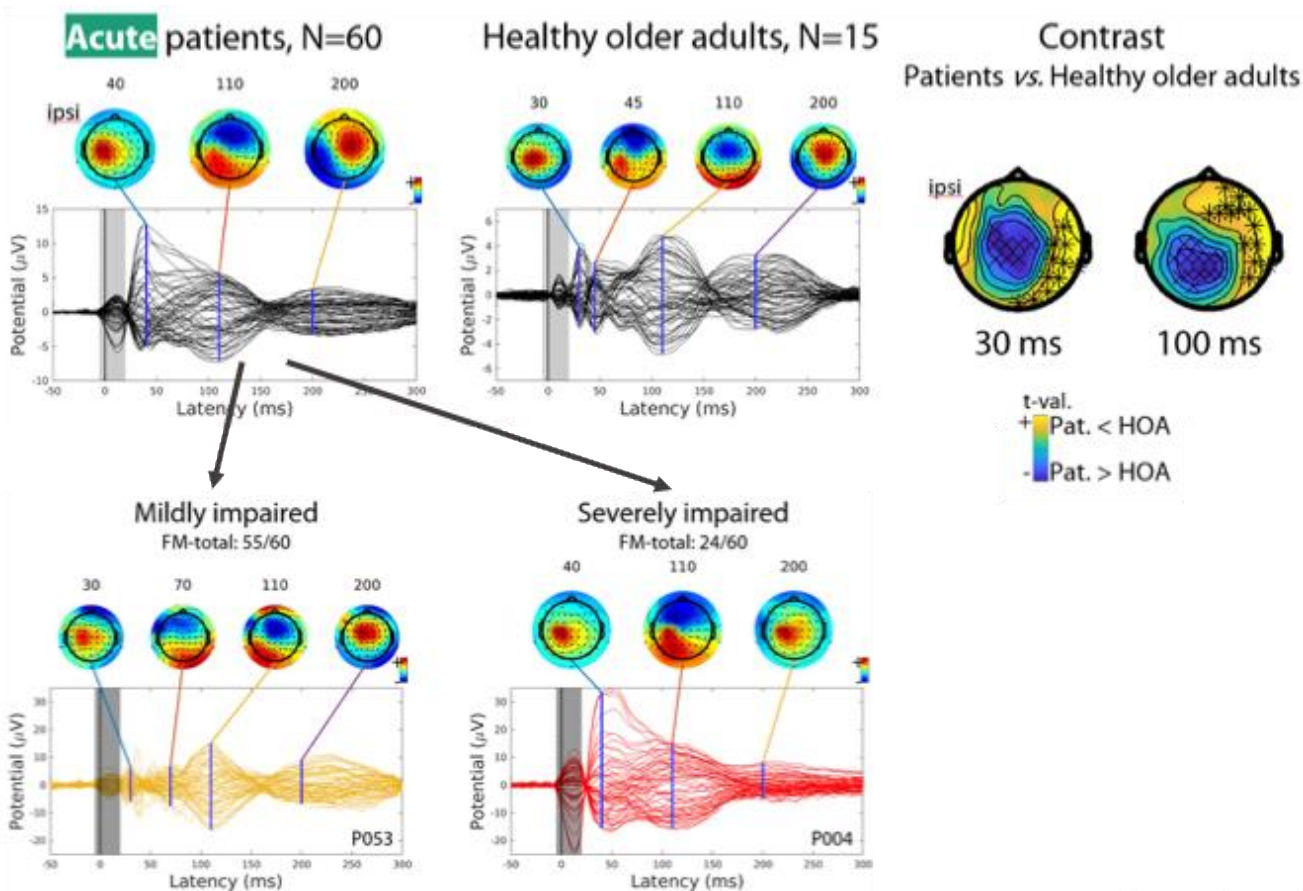
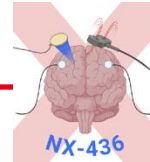
-> **Beneficial** for preventing **excitotoxicity**

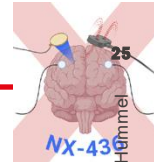


- Hyperexcitability
- Decrease of tonic inhibition

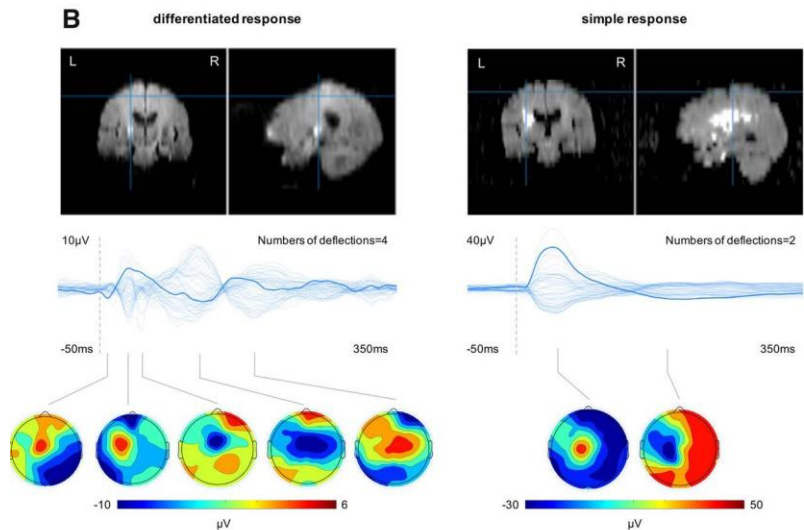
-> **Beneficial** for **plasticity**





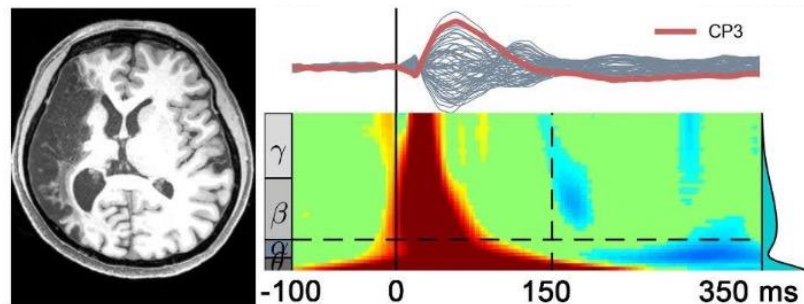


## Stroke Patients



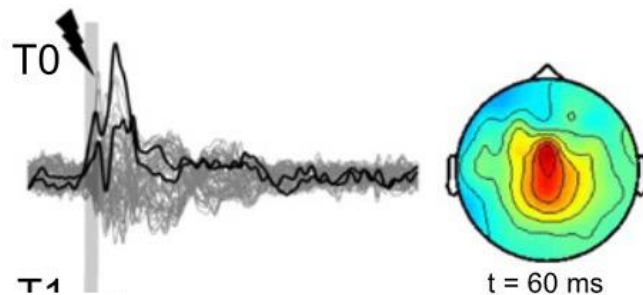
Tscherpel *et al.*, 2020

Acute stroke



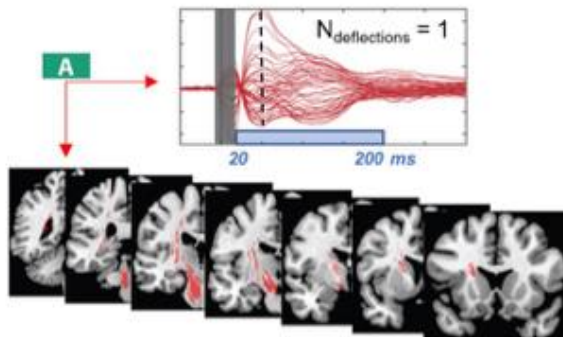
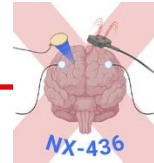
Chronic stroke

Bai *et al.*, 2023

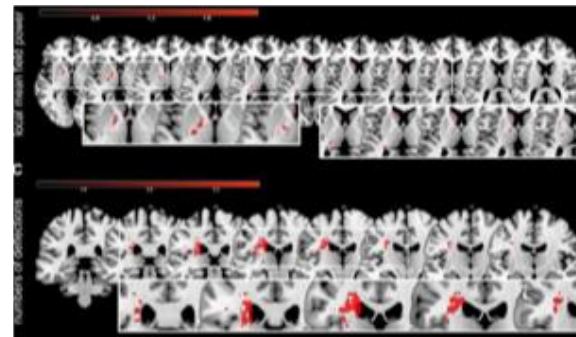
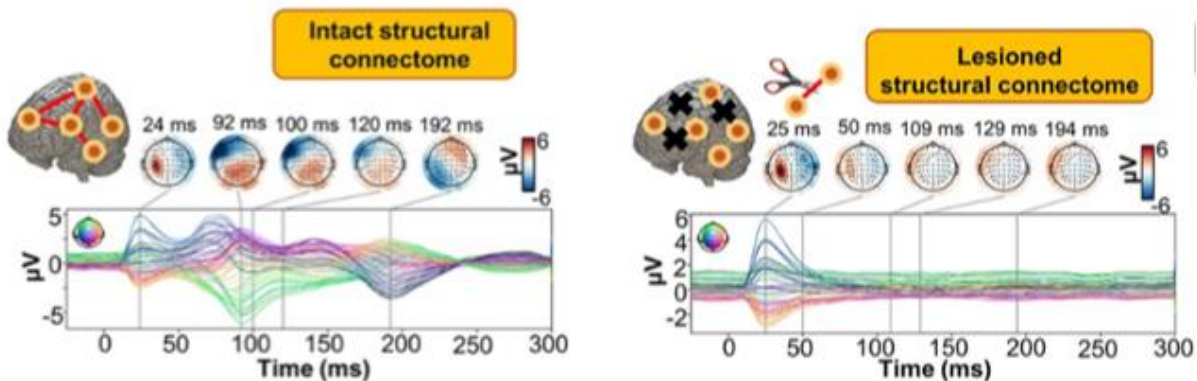


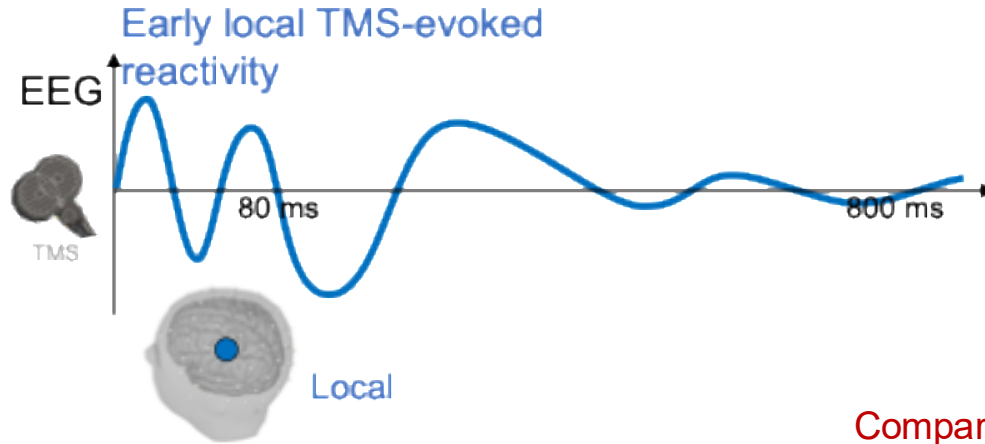
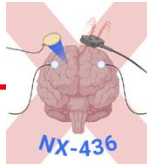
Chronic stroke

Bigoni *et al.*, 2023

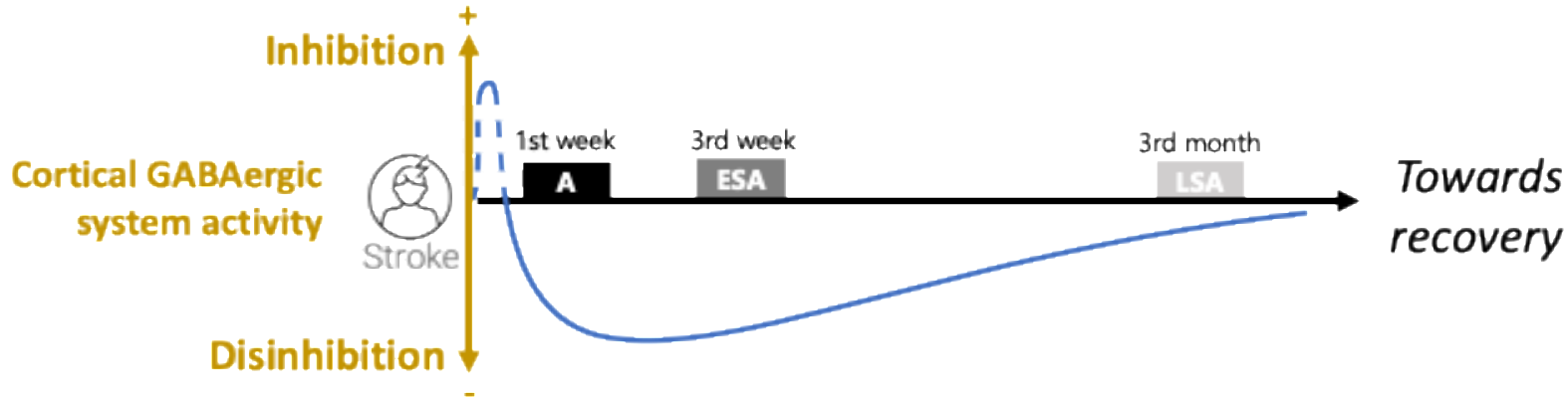
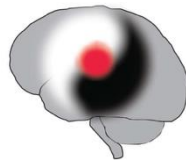


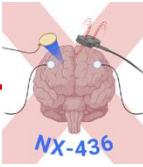
Internal capsule (TiMeS)

Internal capsule, caudate nucleus  
(Tscherpel *et al.*, 2020)Computational modelling (Momi *et al.*, 2023)

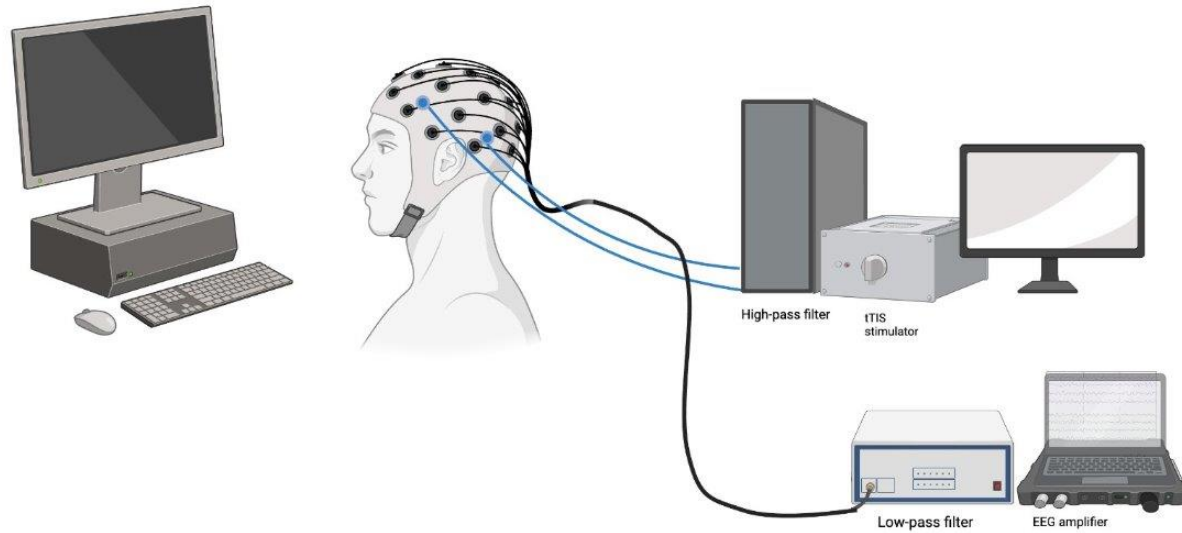
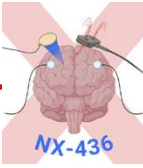


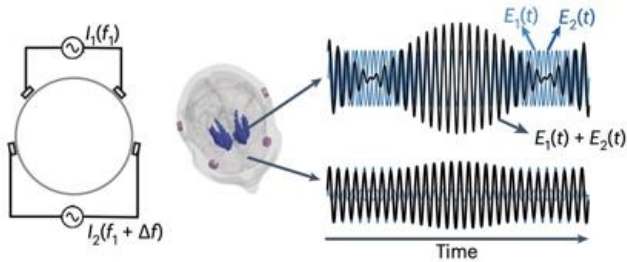
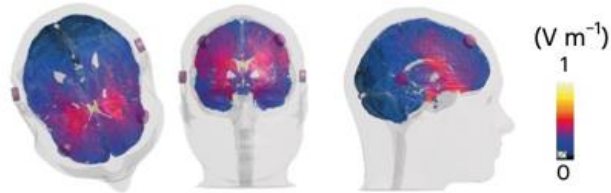
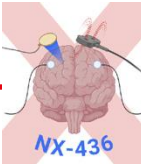
Comparable to animal work





- whole brain activity
- with excellent temporal resolution
- sufficient topographic resolution
- provides information about the activated network by the TMS pulse
- activation can be well standardized and therefore comparable
- provides information about underlying transmitter systems
- well accessible and clinically translatable
- state dependent close-loop applications



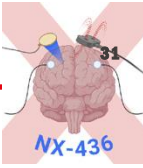


Electric field modeling with striatal montage  
Maximilian J. Wessel, Elena Beanato et al. 2023

**Temporal Interference (TI) Stimulation** uses two electric fields at frequencies  $f_1$  and  $f_2$  to stimulate the brain at the difference frequency ( $|f_1 - f_2| = \Delta f$ ), which lies within the range of brain activity, non-invasively.

**'Pulsed Temporal Interference'** uses two electric fields at frequencies,  $f_1$  and  $f_2$ , and periodically switch a particular field to  $f_2 + \Delta f$  in a timed, pulsed manner (i.e. in bursts).

Each electric field is generated by a constant current sources



## What are the current hypotheses of how tTIS modulates brain activity?

Subthreshold stimulation that requires behavioral co-activation of the brain area of focus (rs- fMRI vs. task-based fMRI)

(Wessel, Beanato et al. 2023, Violante et al. 2023)

Disruptive effect on the underlying network oscillation pattern when applied in a continuous and not in a pulsed -stimulation pattern (it is not phase locked to the underlying oscillatory rhythm or the continuous stimulation masks the underlying network activity)

(Vassiliadis et al. 2024, Viera et al. 2024, Chenhao Yang et al. 2024)

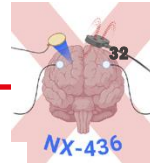
At a cellular level, neuron can mix the high carrier frequencies and produces non-linear mixed products – new frequencies -

(Mirzakhilili et al. 2020 )

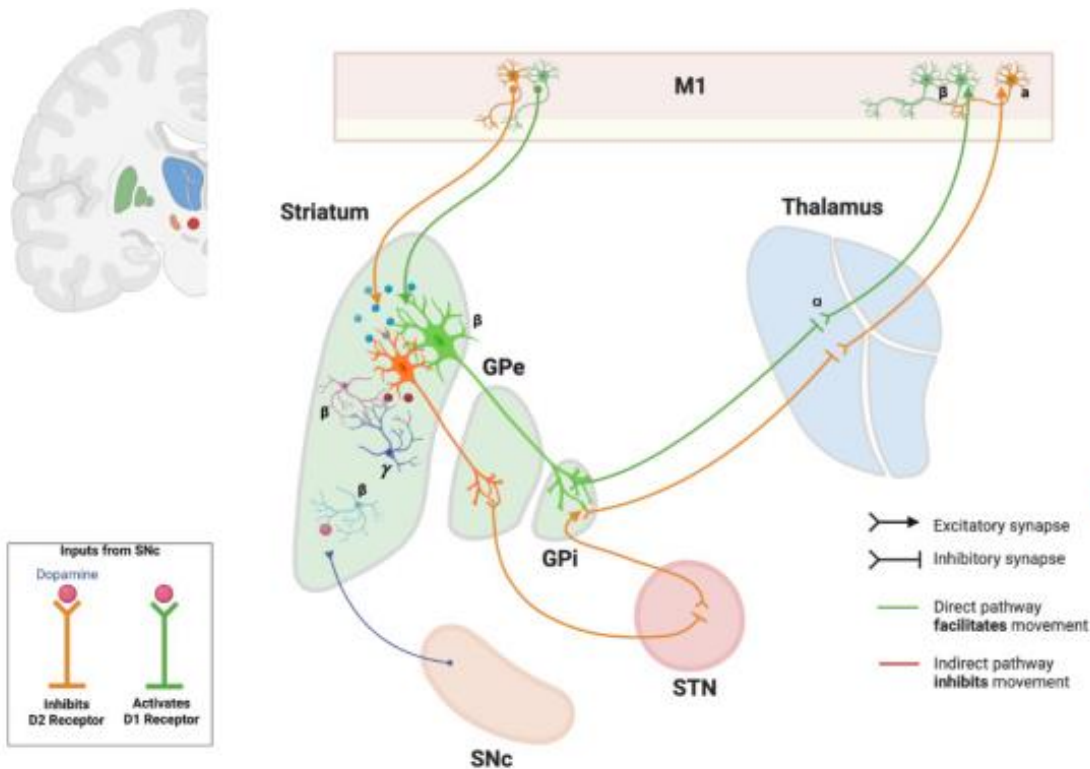
Neuron is mixing exogenous and endogenous subthreshold membrane potential oscillations to create new oscillatory frequencies (Kinetics of voltage-gated sodium channels are non-linear)

(Luff et al. 2024)

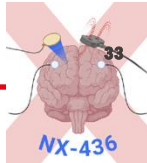
**tTIS-EEG concurrent recording will allow to add to the mechanistic understanding**



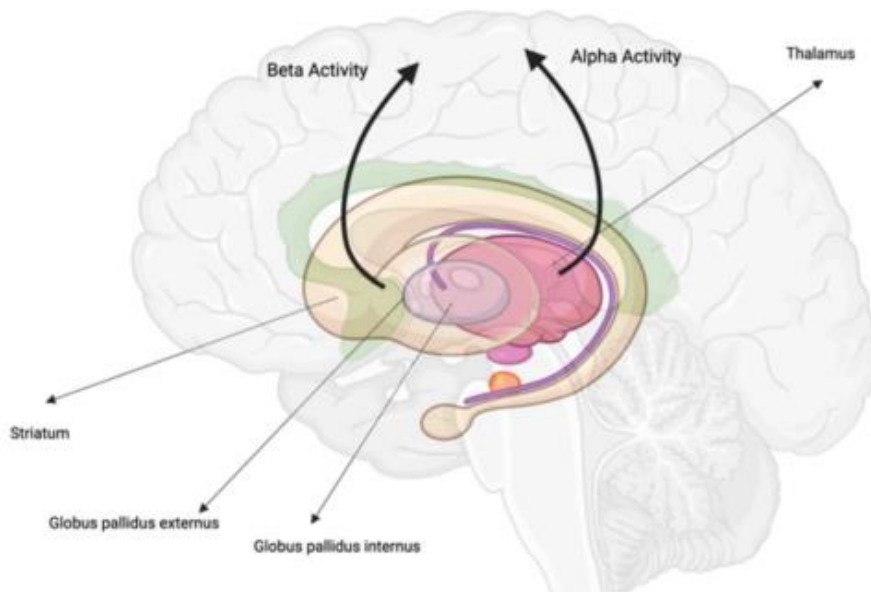
## Neuronal networks of cortico-striatal interactions



**➔ Beta and mu activity modulation in M1**

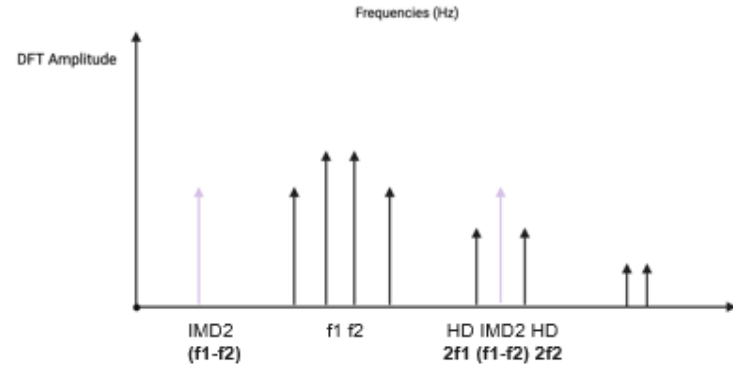
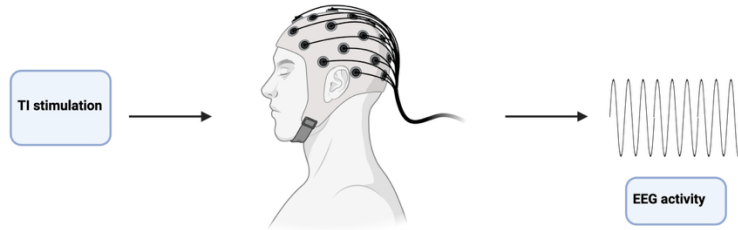
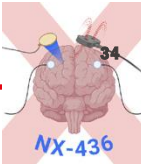


## Electrophysiological correlates of Motor Learning



### Sensorimotor oscillatory activity:

- Mu oscillations
  - **Thalamic nuclei** -> cortical cells
- Beta oscillations
  - **Striatal nuclei** -> cortical cells
- Modulation by motor activity during learning:  
Desynchronisation during movement ↓



## Concurrent TI-EEG recording:

### Advantages

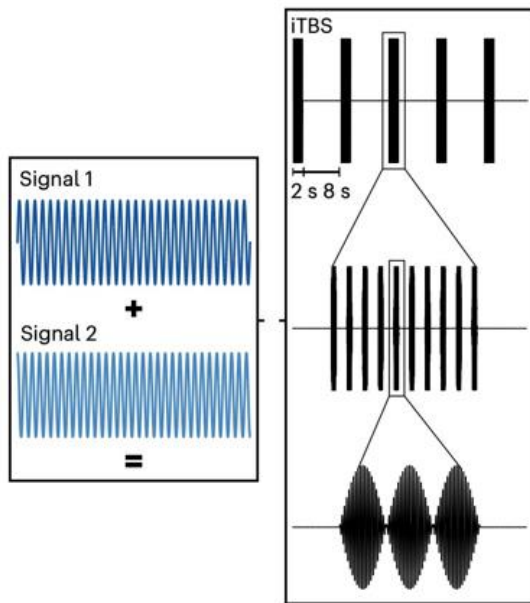
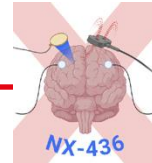
Continuous EEG recording during and after tTIS:

- Mechanistic understudying of tTIS effects on brain circuits with high temporal resolution
- Reveal sustained effects of tTIS during and after the experiment

### Technical challenges

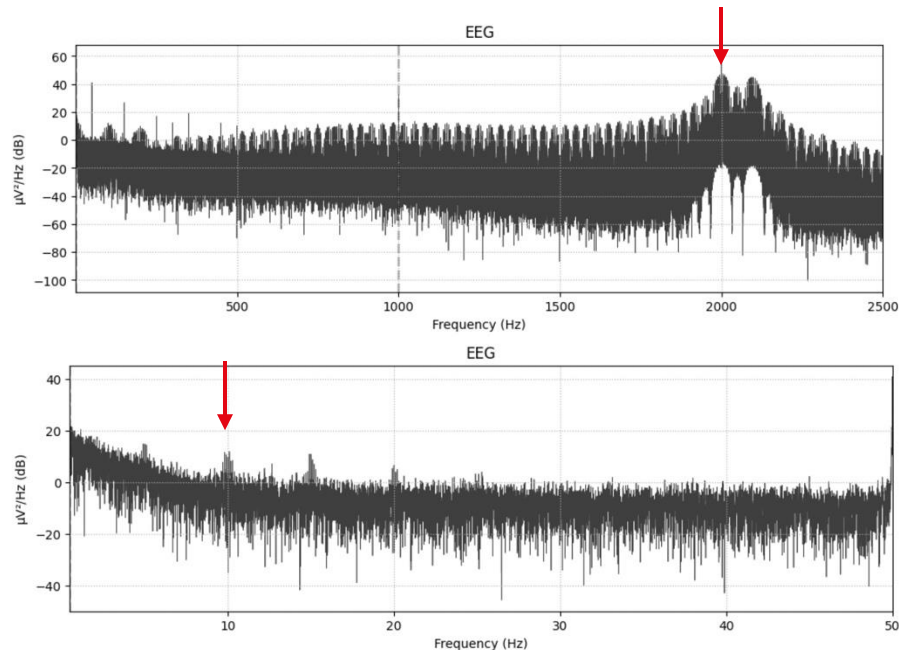
tTIS creates voltage potential that is above the limits of commercially available EEG amplifiers: **non-linear system**

EEG recording will be distorted by non-linear artefacts, as a result of the tTIS

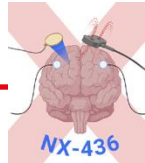


**Intermittent theta burst stimulation pattern**  
Maximilian J. Wessel, Elena Beanato et al. 2023

### Example of stimulation artefacts



*Red arrows:* Carrier TI frequencies (2kHz, 2.1kHz), TI stimulation artefact at 5Hz (FFT)

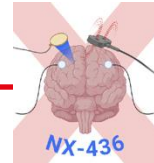


### Stimulation artefacts can be approximated by Taylor expansion:

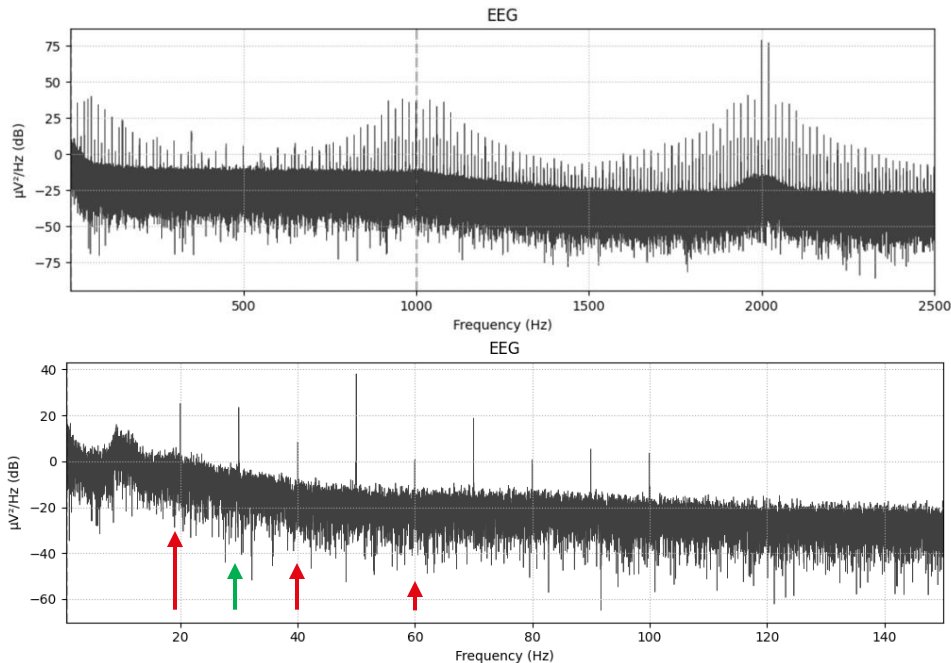
Is an infinite sum of terms which represent an approximation of a function around a specific point on the function. It allows any function (including non-linear ones, as long as it is infinitely differentiable) to be represented as the sum of terms scaled by the function's derivatives at a specific point (with approximation accuracy reducing the further one gets from the specified point)

**A Maclaurin Series** is the same thing as a Taylor Series but with the specified point around which to approximate defined as zero:

$$f(0) + \frac{f'(0)}{1!}x + \frac{f''(0)}{2!}x^2 + \frac{f'''(0)}{3!}x^3 + \dots = \sum_{n=0}^{\infty} \frac{f^{(n)}(0)}{n!}x^n$$



Example of stimulation artefacts with continuous TI stimulation, beat frequency at 20Hz

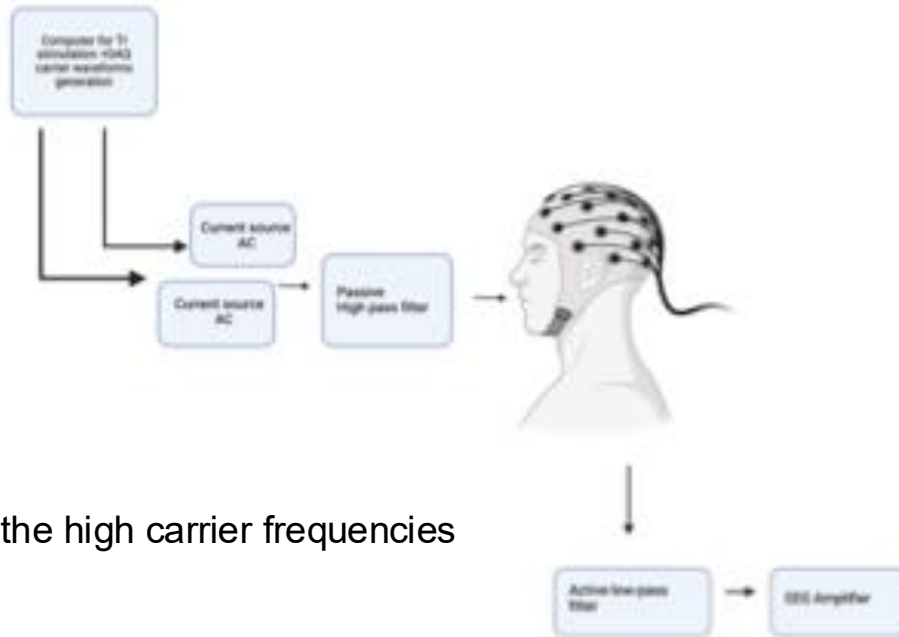
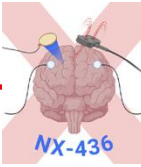


TI stimulation, beat frequency 20Hz (enveloppe graphical representation)

Carrier TI frequencies (2kHz, 2.02kHz)

Red arrows: TI stimulation artefact at 20Hz and its harmonics (FFT)

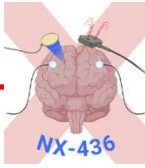
Green arrows: TI stimulation artefact at 30Hz (mixing with power line noise)



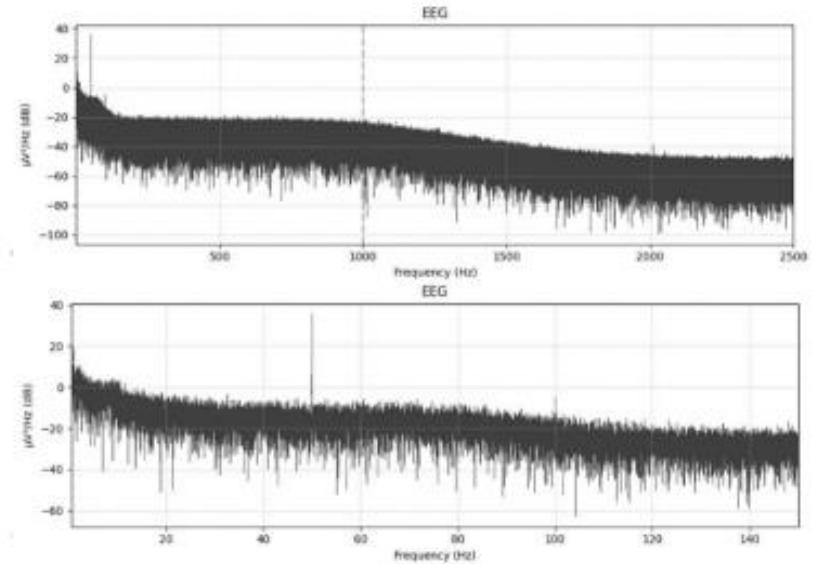
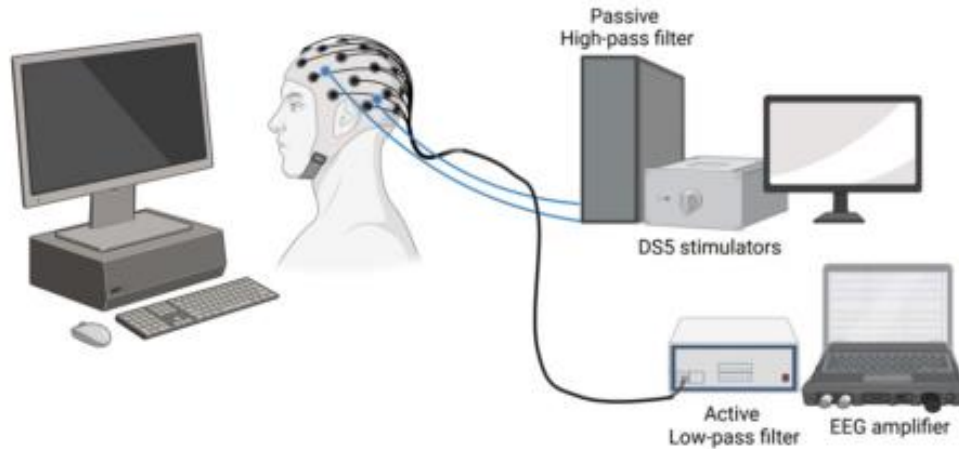
### TI-EEG set up configuration:

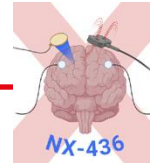
**Passive high-pass filter:** allows only the high carrier frequencies to pass, after the TI stimulators

**Active low-pass filter:** allows only the frequencies below 100Hz to pass, eliminating the carrier frequencies before reaching the EEG amplifier



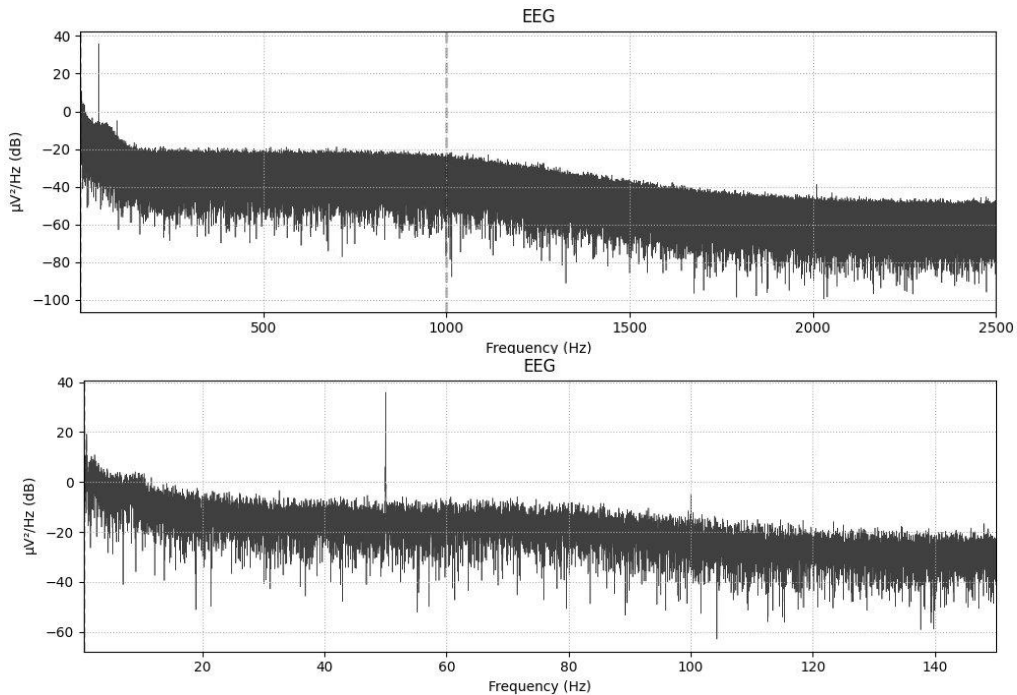
## Concurrent tTIS-EEG: Online Artefact-free EEG recording



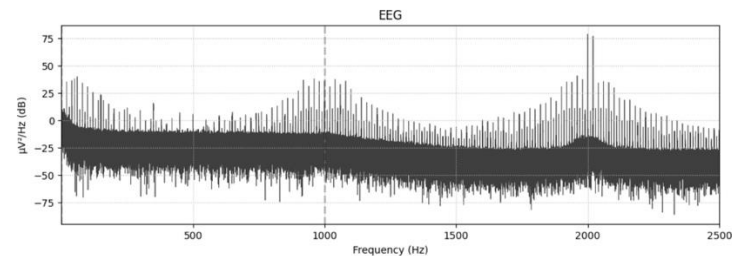


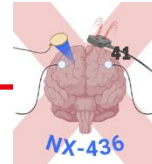
## Hardware filters, tTIS 2kHz, Beat frequency 20Hz

EEG recording with hardware filters, no artefacts for all the EEG channels



Without hardware filters:

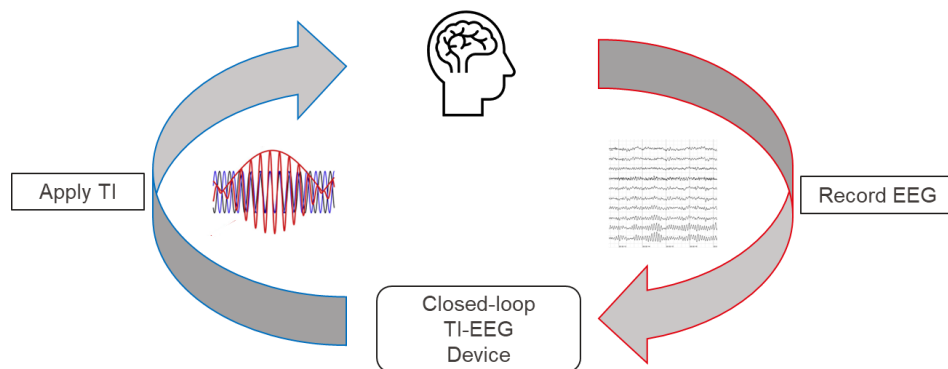


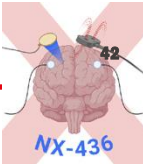


## Applications with tTIS-EEG recording and possible technological developments:

Closed-loop application based on neurofeedback and/or behavioral performance:

1. Optimize tTIS (beat frequency, pattern) based on cortical output EEG activity
2. Deliver pulsed-pattern stimulation, locked to endogenous cortical EEG activity
3. Enhance or disturb reinforcement learning, closed-loop with changes in cortical EEG recording
4. Modeling striatal sEEG activity in correlation with EEG cortical activity:  
adjust online envelope focus, beat frequency to endogenous rhythm, for example in Parkinson s disease
5. Phase-locking tTIS





## Applications with tTIS-EEG recording:

### Hippocampus tTIS and EEG cortical output:

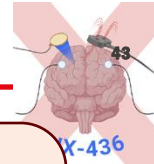
#### Alzheimer's disease (AD):

- Establish physiological rhythm patterns in DMN and FPN
- Cortical biomarkers of response to TI stimulation

### Striatum tTIS and EEG cortical output:

#### Parkinson's disease (PD):

- Establish physiological rhythm patterns in cortico-basal ganglia loop, targeting pathological beta activity
- PD apathetic patients and targeting altered EEG alpha and theta oscillations



### **Recording of brain activity simultaneously**

- focally and at the network level
- adds to mechanistic understanding
- safety monitoring
- state dependent close-loop applications

### **Online interference with brain activity**

- causal understanding
- network vs. local effects
- state dependent close-loop applications

### **Target selection, target validation**

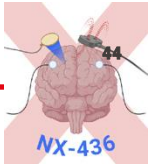
- personalization
- validation of approach

### **Challenges**

- safety
- artefacts
- feasibility
- accessibility, clinical translation
- cost

### **Selection of method**

- local vs network activity
- oscillatory vs. activation
- artefact profile



## Questions